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**Clinical Investigation**

# Prospective Validation of a High Dimensional Shape Model for Organ Motion in Intact Cervical Cancer

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## Summary

We sought to validate a strategy for planning target volume definition in patients with intact cervical cancer, based on a previously published shape model. Using daily cone beam computed tomography imaging from patients treated with intensity modulated radiation therapy, we found that 92.3% of target volumes were entirely encompassed within the 95% isodose structure, which was not significantly lower than our hypothesized probability of 95.0% ($P = .19$). Therefore, we consider this expansion strategy to be valid.

**Purpose:** Validated models are needed to justify strategies to define planning target volumes (PTVs) for intact cervical cancer used in clinical practice. Our objective was to independently validate a previously published shape model, using data collected prospectively from clinical trials.

**Methods and Materials:** We analyzed 42 patients with intact cervical cancer treated with daily fractionated pelvic intensity modulated radiation therapy and concurrent chemotherapy in one of 2 prospective clinical trials. We collected online cone beam computed tomography (CBCT) scans before each fraction. Clinical target volume (CTV) structures from the planning computed tomography scan were cast onto each CBCT scan after rigid registration and manually redrawn to account for organ motion and deformation. We applied the 95% isodose cloud from the planning computed tomography scan to each CBCT scan and computed any CTV outside the 95% isodose cloud. The primary aim was to determine the proportion of CTVs that were encompassed within the 95% isodose volume. A 1-sample $t$ test was used to test the hypothesis that the probability of complete coverage was different from 95%. We used mixed-effects logistic regression to assess effects of time and patient variability.

**Results:** The 95% isodose line completely encompassed 92.3% of all CTVs (95% confidence interval, 88.3%-96.4%), not significantly different from the 95% probability anticipated a priori ($P = .19$). The overall proportion of missed CTVs was small: the grand mean of covered CTVs was 99.9%, and 95.2% of misses were located in the anterior body of the uterus. Time did not affect coverage probability ($P = .71$).

**Conclusions:** With the clinical implementation of a previously proposed PTV

definition strategy based on a shape model for intact cervical cancer, the probability of CTV coverage was high and the volume of CTV missed was low. This PTV expansion strategy is acceptable for clinical trials and practice; however, we recommend daily image guidance to avoid systematic large misses in select patients. © 2016 Elsevier Inc. All rights reserved.

## Introduction

Radiation therapy is an important component of treatment of cervical cancer, but it can result in significant toxicity, especially to the genitourinary, gastrointestinal, and hematologic systems [1]. Advanced radiation therapy techniques, such as intensity modulated radiation therapy (IMRT), have the potential to reduce toxicity compared with conventional approaches. Dosimetric studies of IMRT have shown reduced dose to normal organs, including the bowel, bladder, rectum, and bone marrow [2-4]. Furthermore, reports describing patients treated with IMRT have been encouraging in terms of toxicity and clinical outcomes [5-13].

However, the use of IMRT in the setting of intact cervical cancer has been controversial. An important and potentially limiting factor is the degree to which the cervix and uterus move both between and during treatment fractions. Large interfraction and intrafraction target motions could lead to under-dosing and compromised clinical outcomes, whereas large planning margins to compensate for such motion can result in excess normal tissue dose, thereby increasing toxicity. How to define planning margins to optimize the tradeoff between target coverage and normal tissue sparing in the setting of intact cervical cancer is unclear.

Several groups have investigated interfractional and intrafractional cervical motion during radiation treatment and have reported relatively large movements [14-23]. However, prior studies have generally been retrospective, involving less than daily online imaging and relatively small sample sizes, whereas well-powered studies to validate various proposed models independently and prospectively have been lacking. Although contouring guidelines for clinical target volume (CTV) delineation for cervical cancer exist [24, 25], guidelines for planning margins do not. Previously, Khan et al [23] proposed a shape model to describe interfractional CTV variation and estimated that an anisotropic expansion of 10 to 14 mm around the anterior surface at the level of the uterus, 5 to 10 mm along the interface of the CTV with the bladder and rectum, and 1 to 3 mm around the superior and lateral regions of the CTV would ensure a 95% probability of complete target coverage. These results served as the basis for anisotropic planning target volume (PTV) recipes used in several clinical trials [26-28], which have used expansions of 15 mm around the uterus and cervix, 10 mm around the vagina and parametria, and 5 to 7 mm around the nodal CTV (summarized in Table 1). Given the ongoing lack of

consensus about the optimal strategy to define PTVs for intact cervical cancer, studies prospectively evaluating proposed methods would be of value. Therefore, the primary aim of our study is to evaluate the validity of this approach to PTV definition, using prospectively collected data from 2 clinical trials. This validation study was a prespecified aim for one of the trials.

## Methods and Materials

### Population and sampling methods

This analysis was approved by our Institutional Review Board. The population consisted of patients with cervical cancer receiving daily fractionated radiation therapy with concurrent chemotherapy. Eligible patients for this study had unresected, biopsy-proven stage IB to IVA cervical carcinoma registered for one of 2 prospective clinical trials at our institution. We also included sets of images from 2 patients who were ineligible for trial participation because of a hemoglobin level <10 g/dL but who were treated according to protocol and received daily cone beam computed tomography (CBCT) imaging. Patients treated postoperatively or with extended field radiation therapy were ineligible.

### Simulation and treatment planning

All patients underwent simulation in the supine position from T12 to mid femur with a customized vacuum immobilization device (Vac-Lok; Med-Tech, Orange City, IA) by use of a 4-slice computed tomography (CT) scanner (Lightspeed; GE Medical Systems, Waukesha, WI) with a 2.5-mm slice thickness. Patients with adequate renal function received intravenous contrast. Patients were simulated with both a full bladder and empty bladder and treated in a consistent bladder-filling state (ie, either always full or

**Table 1**   Summary of PTV expansion strategy based on model of Khan et al [23].

| Region of CTV | Anisotropic expansion |
| --- | --- |
| Uterus and cervix (CTV1) | 15 mm |
| Vagina and parametria (CTV2) | 10 mm |
| Nodal CTV (CTV3) | 5-7 mm |
| CTV$_{boost}$ | 7 mm |

*Abbreviations:* CTV = clinical target volume; PTV = planning target volume.

always empty) according to the preference of the treating physician. If patients required re-simulation during treatment, the new planning CT scan was used for the analysis.

All patients were treated with IMRT followed by an intracavitary brachytherapy boost. A parametrial boost after intracavitary brachytherapy was optionally used at the discretion of the treating physician. The CTV was defined on the planning CT scan and consisted of 3 subvolumes: CTV1 (gross tumor, cervix, and uterus), CTV2 (upper half of the vagina and parametria), and CTV3 (pelvic lymph nodes, including the common iliac, external and internal iliac, and presacral lymph nodes). For patients with gross nodal disease, a boost volume was generated consisting of the diseased node. The PTV was generated by applying a 15-mm margin around CTV1, a 10-mm margin around CTV2, and a 5- to 7-mm margin around CTV3. If applicable, a 7-mm margin was applied around $CTV_{boost}$ to generate $PTV_{boost}$. The bladder, rectum, bowel, pelvic bone marrow, and femoral heads were contoured on each planning CT scan as organs at risk. The prescription dose for patients without gross nodal disease was 45 Gy in 25 daily fractions to the PTV. The prescription dose for patients with gross nodal disease was 47.6 Gy in 28 daily fractions to the PTV and 2.0 to 2.12 Gy to $PTV_{boost}$ depending on adjacent normal tissue tolerance. Treatment plans were generated using the Eclipse treatment planning system (Varian, Palo Alto, CA) with either 7 to 8 static coplanar beams or 2 coplanar arcs, with 6- or 15-MV photons. Patients received 5 to 6 cycles of concurrent cisplatin (40 mg/m$^2$ weekly), with or without concurrent gemcitabine (50-125 mg/m$^2$ weekly), according to the trial protocol.

## Daily CBCT

All patients were treated by use of a linear accelerator equipped with a gantry-mounted imager for obtaining CBCT scans before each fraction. Each patient was initially set up with tattoo markers, and on-board planar kilovolt (kV) x-ray imaging was used to align bony anatomy before treatment each day. Prior to delivery of the first fraction, a CBCT scan was acquired and reviewed by the therapists and treating physicians to ensure adequate target volume coverage. For subsequent fractions, the CBCT scan was reviewed by therapists before treatment delivery and offline by a physician after each delivery. In instances of poor target coverage, small (<3 mm) shifts were applied based on manual soft tissue alignment. If larger shifts (>3 mm) were required (eg, because of rectal filling), patients were removed from the treatment table to void prior to treatment. In cases of systematic miss, the patient underwent a re-simulation.

The CBCT scan parameters were 125 kV (peak), 80 mAs, and 25 ms per frame. The images were taken at a source-image distance of 150 cm with 440 projections. The device was operated in half-fan mode with a bowtie filter to reduce scatter and adequately encompass the patient's anatomy. The typical length of a CBCT scan was 16 cm in the superior-inferior direction, which was generally sufficient to encompass the bladder, rectum, upper vagina, presacral lymph nodes, parametria, cervix, and uterus.

## Assessment of CTV coverage

CBCT scans for each fraction were rigidly registered to the planning CT scan based on alignment of bony anatomy, by use of the MIM platform (MIM Software, Cleveland, OH). The CTV1 and CTV3 contours from the planning CT scan were cast onto each registered CBCT scan and manually redrawn to account for organ motion and deformation, creating a new CTV1 and CTV3 for each fraction. The 95% isodose volume was generated from the planning CT scan for each patient and was then overlaid onto each registered CBCT scan for that patient. The investigators involved in defining the new target volumes were blinded to the location of the 95% isodose volume. The volumes of the new targets lying outside the 95% isodose cloud (if any) were then computed. We expected to observe an overall probability of complete target coverage within the 95% isodose volume of at least 95%.

## Statistical considerations

The primary aim of the study was to determine the percentages of CTV1 and CTV3 that were fully encompassed within the 95% isodose volume across all patients and fractions. The null hypothesis was that there is a 95% probability that the 95% isodose volume will entirely encompass the union of CTV1 and CTV3 for any given fraction, based on the model described by Khan et al [23]. We computed the proportion of scans with complete coverage for each patient and used a 1-sample $t$ test to test the alternative hypothesis that the overall probability of coverage was significantly different from 95%. We specified a priori that we would consider the prior shape model valid if the grand mean of fully encompassed scans was not significantly less than 95%. We also performed sensitivity analyses on the primary outcome by using a nonparametric Wilcoxon rank sum test and by fitting a generalized estimating equation model.

On the basis of preliminary results from 15 patients, we estimated the sample standard deviation for this probability to be 13%. We calculated that a sample size of 42 patients would provide 80% power to detect a mean difference of 5% or more and would provide 90% power to detect a mean difference of 6% or more, with a 1-sided type I error of 5%. We used mixed-effects, random-intercept logistic regression modeling on the binary outcome of any missed CTV versus complete coverage at each visit, regressed on linear time and including a subject-specific random intercept. In addition, we modeled demographic and tumor characteristics to identify potential predictors of missed target volume.

To assess the reliability and interobserver agreement of the CBCT contouring, another radiation oncologist independently determined the extent of CTV coverage on 3 randomly selected scans per patient. We calculated the Cohen κ statistic for the agreement between the investigators. The second investigator was blinded to the 95% isodose cloud as well as the contours generated by the first investigator. Paired t tests were used to evaluate differences between CTVs on the initial planning CT scans compared with volumes on CBCT scans. Data were prepared and analyzed using R (version 3.2.2; R Foundation for Statistical Computing, Vienna, Austria [http://www.r-project.org]) and SPSS (version 23; IBM, Armonk, NY).

## Results

We analyzed a total of 1084 daily CBCT scans from 42 eligible patients (25.8 scans per patient; SD, 2.0). Figure 1 shows representative images of a completely encompassed CTV and a CTV that was partially missed. Because of limitations in the CBCT frame of view, the superior-inferior margins of the CBCT scans occasionally cut off portions of the CTV. This was most pronounced for CTV3, where a mean of 2.6 cm was cut off across the entire sample (SD, 2.1 cm; range, 0-9.9 cm). For CTV1, a mean of 0.04 cm (SD, 0.2 cm; range, 0-2 cm) was below the inferior border of the CBCT scan. However, 1015 of 1084 CTV1 contours (94%) were completely imaged.

Demographic characteristics of the sample are shown in Table 2. The median age was 47.5 years (interquartile range, 40-57 years), and the mean body mass index was 28.5 (SD, 6.2). Most patients were white, had squamous cell carcinoma, and had a Karnofsky Performance Status of 100 prior to treatment.

The 95% isodose line completely encompassed the CTV on 92.3% (95% confidence interval [CI], 88.3%-96.4%) of all daily CBCT scans for all patients, which was not significantly different from the 95% hypothesized a priori (P = .19). Because our primary outcome data were skewed (Fig. 2), with most percentages near the maximum of 100%, we performed sensitivity analyses by calculating a nonparametric Wilcoxon rank sum test and fitting a generalized estimating equation model. Both of these analyses were consistent with the t test; the choice of test did not affect the inference that our sample mean was not significantly different from 95% (P = .46 and P = .11, respectively). Figure 3 shows the daily proportion of CTV that fell outside the 95% isodose cloud throughout the course of external beam radiation therapy.

A total of 81 CBCT images showed at least 1 area of missed CTV; because 2 scans showed missed volume in 2
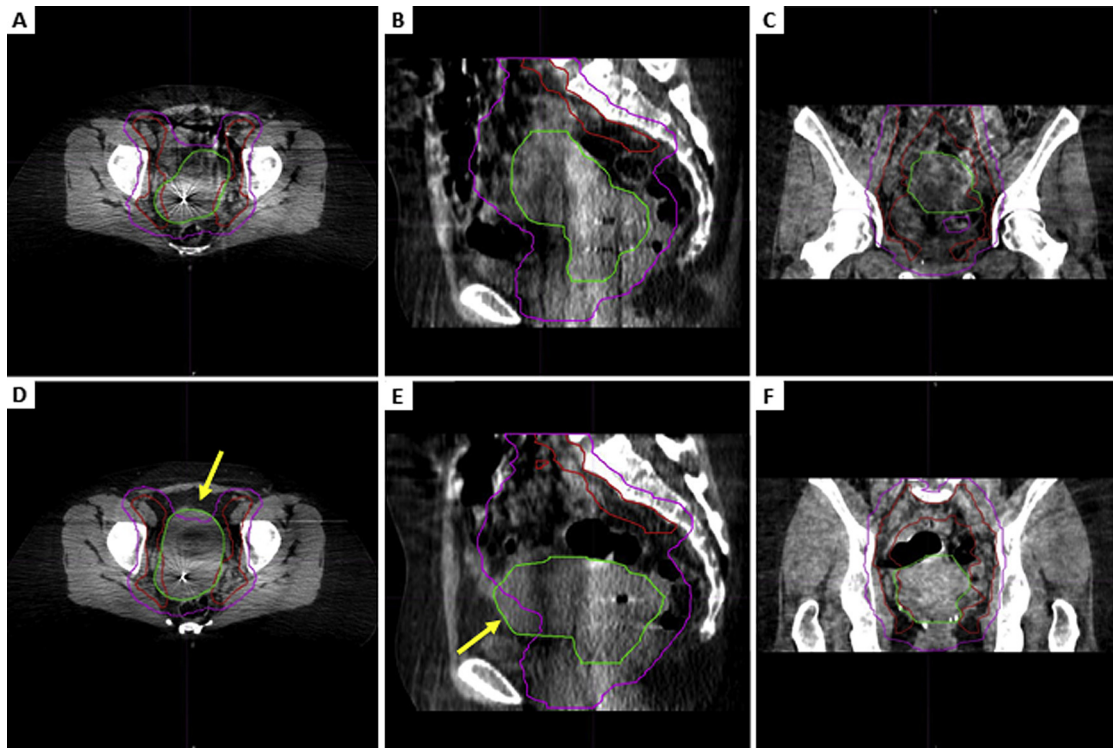


**Fig. 1.** Representative cone beam computed tomography slices showing a fully encompassed clinical target volume (CTV) compared with a partially missed CTV. Axial (A), sagittal (B), and coronal (C) views of CTV comprising gross tumor, cervix, and uterus (CTV1) (green) and CTV comprising pelvic lymph nodes (CTV3) (red) that are completely encompassed within the 95% isodose structure (pink) and axial (D), sagittal (E), and coronal (F) views from a scan with an anterior CTV1 miss in the uterine body. The arrows point to the missed CTV1. (A color version of this figure is available at www.redjournal.org.)

**Table 2** Sample descriptive statistics

|  | Data (N=42) |
| --- | --- |
| Age, y |  |
|     Mean (SD) | 48.5 (12.3) |
|     Median (IQR) | 47.5 (40-57) |
| Race or ethnicity |  |
|     Asian | 3 (7.1) |
|     Black | 3 (7.1) |
|     Hispanic | 13 (31.0) |
|     White | 22 (52.4) |
|     Other | 1 (2.4) |
| Mean body mass index (SD) | 28.5 (6.2) |
| Karnofsky Performance Status |  |
|     100 | 33 (78.6) |
|     90 | 5 (11.9) |
|     80 | 2 (4.8) |
|     NA | 2 (4.8) |
| Histology |  |
|     Squamous cell carcinoma | 32 (76.2) |
|     Adenocarcinoma | 9 (21.4) |
|     Adenosquamous carcinoma | 1 (2.4) |
| Grade |  |
|     1 | 1 (2.4) |
|     2 | 16 (38.1) |
|     3 | 16 (38.1) |
|     NA | 9 (21.4) |
| Stage |  |
|     IB2 | 12 (28.6) |
|     IIA1 | 1 (2.4) |
|     IIB | 15 (35.7) |
|     IIIB | 14 (33.3) |

*Abbreviations:* IQR = interquartile range; NA = not available.
Results are presented as number (percentage) unless otherwise specified. Some percentages may not add up to 100% because of rounding.

regions, there were 83 portions of missed CTVs in total (Table 2). Almost all of the scans that included a miss (95.2%) were in the region of the body of the uterus, whereas the cervix and lateral external iliac lymph nodes were each missed on 2 scans. The range of scans with any CTV miss per patient was 0 to 11, which translated to a coverage percentage ranging from 0% to 45.8%. Of 42
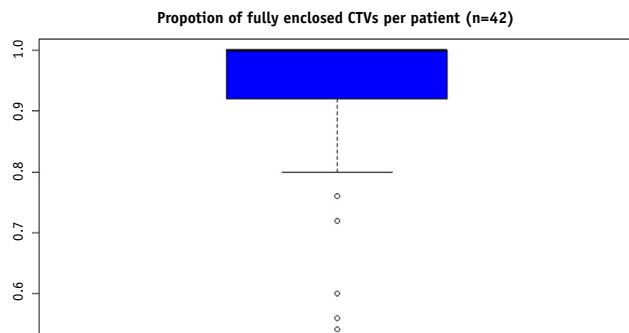


**Fig. 2.** Box plot showing skewed distribution of primary outcome. *Abbreviation:* CTV = clinical target volume.

patients, 17 (40.5%) had at least 1 miss. On average, 1.9 scans per patient (SD, 3.2) showed a miss. Across all patients, the percentage of encompassed CTV was 99.9% (SD, 0.003). The volume of missed CTV was <1 cm$^3$ in 22.2% of all of the misses and >10 cm$^3$ in 24.7% of all misses.

We investigated potential differences between CTV contours that were generated by the treating physician on the planning CT scan and those delineated on the daily CBCT scans. A paired *t* test comparing the total volume of CTV from the planning CT scan with the CTV from the first CBCT scan showed no difference (P=.36). Similarly, a comparison of the CTV from the planning CT scan with the mean CTV from all CBCT scans for each patient showed no difference (P=.57). We also measured interobserver agreement of binary hit or miss status by calculating the Cohen κ for measurements taken by an independent reviewer. The second investigator reviewed 3 scans per patient (11% of the entire sample). The Cohen κ was 0.80 (95% CI, 0.65-0.94). Percent agreement between the 2 investigators was 94%.

Mixed-effects longitudinal logistic regression modeling showed an odds ratio of 0.994 for a miss per daily treatment fraction (95% CI, 0.960-1.028), which was not statistically significant (P=.71). However, the random intercept term was significant (P<.001), indicating that the misses tended to be clustered in some patients rather than randomly distributed between patients. We sought to identify potential predictors of miss by assessing age, ethnicity, body mass index, Karnofsky Performance Status, tumor histology, tumor grade, tumor stage, and initial CTV as covariates in the mixed-effects model. None of these predictors were statistically significant at a P value threshold of .05.

## Discussion

The mean percentage of completely encompassed CTVs on daily CBCT imaging was not significantly lower than 95%. Therefore, CTV coverage was consistent with expectations from the model proposed by Khan et al (23), and we consider this expansion strategy to be valid. Previous reports have generally recommended margins of approximately 15 mm around the uterus and cervix, which is in line with the Khan et al model and with our results (15-18, 29). To our knowledge, this is the first well-powered, independent and hypothesis-driven validation of a model for PTV margin expansion in the setting of intact cervical cancer that takes advantage of prospectively collected daily imaging data.

The observed target volume misses were predominantly located in the anterior body of the uterus, with rare misses in the cervix and lymph nodes. Given the incidence of small misses, a reasonable strategy for improving target coverage could be to add a small expansion of 1 to 3 mm to the anterior uterine CTV. However, the clinical impact of relatively small misses in the body of the uterus is
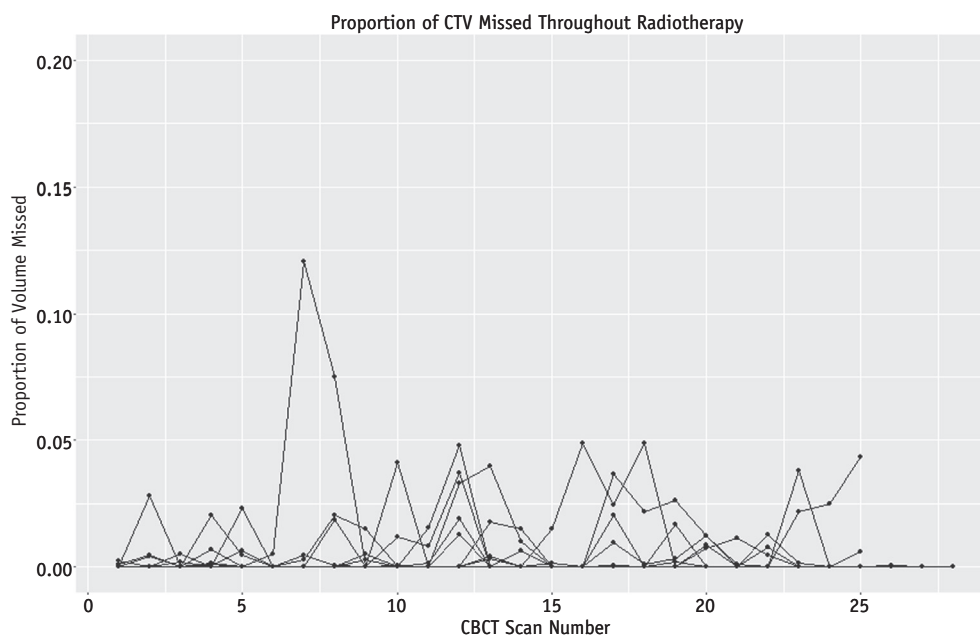
**Fig. 3.**   Daily proportion of missed clinical target volume (CTV). Each line represents 1 patient (N=42). *Abbreviation:* CBCT = cone beam computed tomography.

uncertain. Although most patients had no misses, some patients had several, and mixed-effects logistic regression showed that the misses were clustered in certain patients. We modeled the effect of time and assessed several potential predictors of missed CTVs, including initial CTV1 size. However, none of these variables were statistically significant. Given that misses were relatively rare events, perhaps the sample size is insufficient to identify such predictors. Other potential drivers of miss include bowel and bladder filling (30), which were not assessed in this study. Moreover, internal uterus motion, such as conversion between anteflexed and retroflexed states, likely plays a large role (29, 31). Baseline uterine position (ie, anteverted, midplane, retroverted) and/or intention to treat with a full or empty bladder could also affect coverage. Future work addressing the contribution of these anatomic considerations is warranted. Prior studies have shown regression in tumor and target volumes with time (14, 15, 20), but we found that time did not predict coverage likelihood. Assuming that tumor regression does not lead to increased mobility of the uterus and cervix, it should not affect coverage.

A limitation of this study is the range in quality of CBCT scans, which provide lower resolution than planning CT scans. However, daily CBCT scans have been used successfully in prior studies (20-22), and this technology is currently the most widely available option for daily online image guidance and soft tissue imaging. Despite some variability in scan quality, CTV delineation was in most cases straightforward. The frame of the CBCT scans occasionally cut off portions of the CTV, which led to the assumption that volumes outside the frame were concordant in coverage with what we were able to observe. Most of the

volumes that were cut off were small and located in the superior aspect of CTV3. Given that the pelvic lymph nodes are closely associated with relatively fixed large blood vessels that are in turn relatively fixed to bone, we did not anticipate and did not observe a substantial number of nodal misses. Therefore, the presence of minimally truncated CTV3s is not likely to substantially affect our conclusion.

We compared the planning CT scan−derived CTV with both the initial CBCT scan−derived CTV and the mean CBCT scan−derived CTV to assess for systematic size differences, but there was no difference found with either comparison. Furthermore, we calculated the Cohen κ to explore consistency with primary outcome measurements and found it to be 0.8, which is considered strong agreement (32), along with a high raw percentage agreement. Disagreement occurred in scans where either the miss or the margin of coverage was very small or where CBCT scan quality was relatively lower, making close distinctions more difficult. Taken together, this methodology appears to be reliable.

In conclusion, target coverage was high for patients with intact cervical cancer treated with PTV expansions based on the model described by Khan et al (23) (specifically, a 15-mm margin around the uterus and cervix, a 10-mm margin around the superior vagina and parametria, and a 5-mm margin around the nodal CTV, using daily bone-bone kV matching for setup). When misses occurred, they tended to be minimal in size and located in the anterior body of the uterus rather than the cervix. As a result, this expansion strategy is acceptable for use in clinical trials and practice. However, given uncertainty about risk factors for missing target volumes, we recommend daily image guidance (eg,

kV or CBCT imaging) to avoid systematic large misses in select patients. This method does not preclude the use of an internal target volume, and future studies comparing alternative strategies for defining PTVs in this population, including the use of an internal target volume, would be useful.

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