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UNIVERSITY OF CALIFORNIA,  
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Spatial Memory Networks in Aging and Alzheimer's Disease

DISSERTATION

submitted in partial satisfaction of the requirements  
for the degree of

DOCTOR OF PHILOSOPHY

in Biological Sciences

by

Freddie Márquez

Dissertation Committee:  
Professor Michael A. Yassa, Chair  
Associate Professor John Guzowski  
Professor Elizabeth Head

2021



## **DEDICATION**

To Alfonso and Dolores Marquez.

To Monica and Agustin Segura.

To Alfonso Luis Marquez.

To Drs. Silliker, Stutzmann, Garcia-Añooveros, and Cantú.

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## LIST OF ABBREVIATIONS

A $\beta$  Beta-Amyloid

ACC Anterior Cingulate Cortex

AD Alzheimer's disease

ADRC Alzheimer's Disease Research Center

AFNI Analysis of Functional NeuroImages

CIND Cognitively Impaired Non-Demented

CDR Clinical Dementia Rating Scale

DG Dentate gyrus

EC Entorhinal cortex

MCI Mild cognitive impairment

MMSE Mini-Mental State Exam

MPFC Medial Prefrontal Cortex

MPRAGE Magnetization-Prepared Rapid Acquisition Gradient Echo MRI Magnetic resonance  
imaging

MTL Medial temporal lobe

PCC Posterior Cingulate Cortex

PHC Parahippocampal cortex

POR Postrhinal cortex

PRC Perirhinal cortex

RAVLT Rey Auditory Verbal Learning Test

ROI Region of Interest

RSC Retrosplenial

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Neurobiology and Behavior Laboratory – 20 Students, 25% WQ 2018  
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## ABSTRACT OF THE DISSERTATION

Spatial memory networks in aging and Alzheimer's disease

By

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Doctor of Philosophy in Biological Sciences

University of California, Irvine, 2021

Professor Michael A. Yassa, Chair

An estimated 6.1 million Americans currently suffer with Alzheimer's disease (AD) and in the absence of effective treatment or a cure, this number could increase to 13.8 million by 2060. One of the most common changes that occurs in aging and Alzheimer's disease is decline in memory for everyday experiences (episodic memory). Computational models suggest that the brain uses a neural computation known as *pattern separation* to distinguish among highly similar inputs during memory recall. Furthermore, episodic memory has several components: *what* happened, *where* it happened, and *when* it happened. The posteromedial cortices are regions that are thought to be involved in spatial memory and are early sites that are affected by AD pathology. Neuropathological hallmarks of AD include the presence of beta-amyloid (A $\beta$ ) plaques, and the formation of neurofibrillary tangles (NFT) and neuropil threads. Eventually, this is followed by neurodegeneration. *In vivo* candidate biomarkers for AD include pathological aggregations of misfolded proteins (e.g. amyloid plaques, [A $\beta$ ], and hyperphosphorylated tau tangles, as measured by CSF assays, and PET imaging), neuronal dysfunction or atrophy (as measured by functional or structural MRI, and total tau levels as measured by CSF assays), and cognitive impairment (as measured by neuropsychological tests). However, the relationship between the



pathological, neuroimaging, behavioral, and cognitive markers in the aging brain and in AD remains unclear. The goal of this dissertation was to understand how regions of the brain that support memory for where events occur (spatial memory) are altered in the context of Alzheimer's disease. We gave participants a spatial pattern separation task, in which we showed participants a series of objects on different locations on a screen and tested participants on their ability to remember the spatial location of the objects after a delay. We found that cortical regions known as the posteromedial network may support spatial pattern separation. Spatial pattern separation task performance was associated with word list delayed recall test commonly used in a clinical setting, a relationship that is conditional upon the level of amyloid burden. Spatial pattern separation task performance was also associated with AD pathology, and cognitive decline. These findings suggest that the pattern separation framework may provide an account for understanding mechanistic changes that occur in the progression of AD. Future studies of spatial memory should investigate associations between regionally specific effects of AD pathology, vascular and immune contributions to AD, and include community-based samples of ethnically diverse populations.

## **CHAPTER 1: Background and Significance**

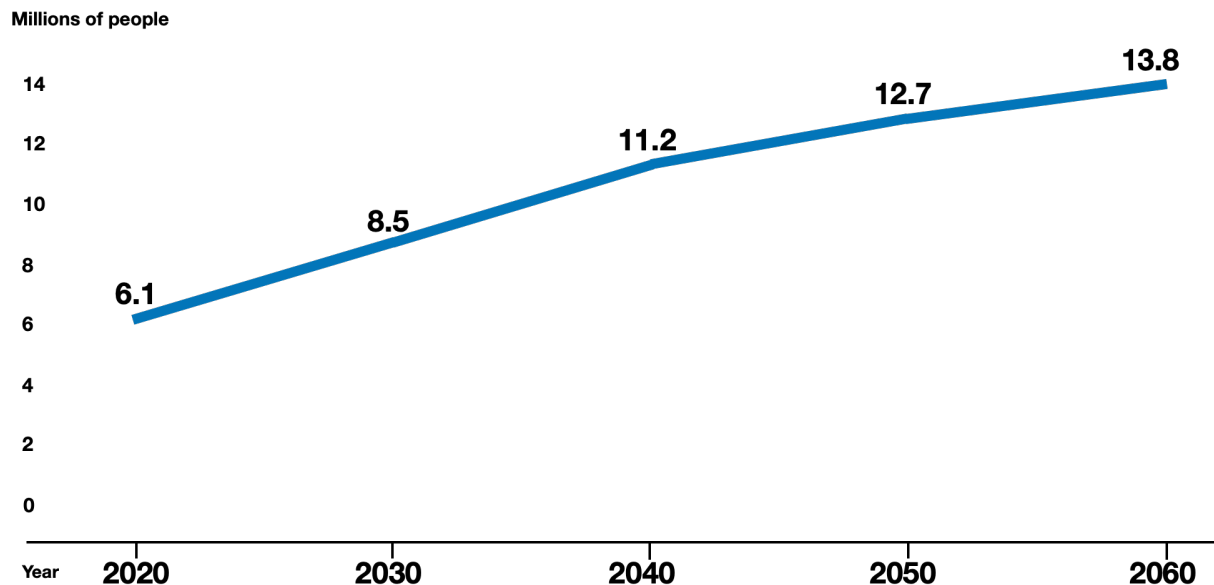
### **1.1 Background and public health relevance**

Alzheimer's disease (AD) is the most common age-related dementia, with prevalence continuing to increase (Alzheimer's disease facts and figures, 2020). With the exception of AD cases caused by genetic mutations (i.e. familial AD), age is the greatest risk factor. Currently, one in ten people 65 years of age or older have AD. In addition, the average life expectancy of a person in the United States has increased by 9 years and the population of people 65 years of age and above has increased by 34 million people (16 million to 50 million) over the last 60 years. Today, an estimated 6.1 million Americans are living with AD and in the absence of effective treatment or a cure, this number could increase to 13.8 million by 2060 (Alzheimer's disease facts and figures, 2020). Thus, a critical goal of biomedical research is to establish indicators (i.e. biomarkers) of AD during the preclinical stage allowing for early diagnosis and intervention. Understanding the neurobiological processes that support memory could help find links between age-related and AD-related changes in the brain and the cognitive changes observed.

A critical goal of biomedical research is to establish cognitive and biological indicators of AD during preclinical and prodromal stages allowing for early diagnosis and intervention (Öhman et al., 2021). Biomarkers quantify characteristics of biological processes that can be linked to cognitive and clinical endpoints, thus can be used as surrogates of the disease process.

Computerized cognitive assessments can serve as “digital biomarkers” by probing subtle features of cognitive decline during the earliest stages of the disease and can be linked with mechanistic biomarkers in a comprehensive approach to improve the efficiency of clinical trials (Papp et al., 2021).

### Projected Number of People with Alzheimer's Dementia in the U.S. Population, 2020 to 2060



**Figure 1.** Projected number of people with AD in the US population, 2020 to 2060

## 1.2 Biomarkers for Assessing Aging and Alzheimer's Disease

### 1.2.1 The current classification of Alzheimer's disease

Identification of pathologic processes prior to the onset of disease symptoms is of critical importance to the field. Biomarkers are quantifiable characteristics of biological processes related to Alzheimer's disease that are linked to clinical endpoints and thus can be used as surrogates for the disease process. Historically, AD has been viewed as a disease of clinical symptoms in the clinical setting. By classifying AD in this manner, its diagnosis would likely include a considerable amount of non-AD cases as defined by its pathological characteristics. In 2011, the National Institute on Aging and the Alzheimer's Association (NIA-AA) Working Group put forth staging criteria that incorporate neuroimaging biomarkers (Sperling et al., 2011). The authors presented a conceptual framework and operational research criteria for preclinical AD where Stage 1 is characterized by the presence of asymptomatic  $\beta$ -amyloidosis, or increased

amyloid burden. Stage 2 includes neuronal injury and evidence of neurodegenerative change. Lastly, stage 3 additionally includes evidence of subtle cognitive decline, which is not yet sufficient for clinical diagnosis. The new research framework proposed by the NIA-AA defines AD pathologically with the use of biomarkers, which could potentially differentiate cases that clinically resemble AD such as hippocampal sclerosis. This framework additionally allows for staging using either fluid or neuroimaging biomarkers. However, certain features, which may be critical for the pathophysiology of the disease, could only be detected using imaging techniques. Hippocampal hyperactivity on task-activated functional MRI is one such example. Ewers et al. (Ewers et al., 2011) and Leal and Yassa (Leal and Yassa, 2013) include this feature in staging the disease and highlight that it seems to appear within a temporally constrained window. Jack and Holtzman (Jack and Holtzman, 2013) proposed several time-dependent models of AD that take into consideration varying age of onset as well as co-morbid pathologies.

### **1.2.2 Pathology and spatiotemporal spread**

Neuropathological staging criteria of AD-related changes originally indicated that although the distribution of beta-amyloid (A $\beta$ ) neuritic plaques varies widely, neurofibrillary tangles and neuropil threads show a distribution pattern that allow for the differentiation of six stages (Braak and Braak, 1991). Stages I-II show alterations that are confined to the transentorhinal region, which spread to limbic (Stage III-IV), and finally to isocortical regions (Stage V-VI). More recently, pathology studies have indicated that intraneuronal aggregations of the protein tau seem to precede the extracellular deposition of A $\beta$  by approximately a decade (Braak and Del Tredici, 2011; Duyckaerts and Hauw, 1997). Notably, non-argyrophillic tau lesions are thought to first appear in the locus coeruleus prior to the appearance of argyrophillic tau lesions caused by neurofibrillary tangles (NFTs) within the transentorhinal region of the cerebral cortex (Braak and

Tredici, 2015). Intraneuronal inclusions consisting of aggregated protein tau appear in selectively vulnerable cell types that appear to spread in a regionally and temporally specific manner that is independent of proximity to affected area (Braak and Braak, 1999). One advantage of using brain imaging techniques is that they operate at a higher level of spatiotemporal sensitivity than fluid biomarkers, thereby offering an opportunity to stage progression of the disease. Thus far, imaging using combinations of in vivo tau-PET and MRI techniques have shown progression patterns that largely recapitulate staging based on post-mortem histology (Schöll et al., 2015).

### 1.2.3 Biomarker-based staging of Alzheimer's disease

Out of the five biomarkers proposed by the NIA-AA, three were imaging biomarkers (amyloid PET, structural MRI, and FDG PET). Anatomical information from imaging biomarkers may provide crucial disease-staging information. This would imply an advantage for imaging biomarkers over fluid biomarkers because imaging can distinguish the different phases of the disease both temporally and anatomically. However, in recent years, assays to measure CSF biomarkers have been developed for measurement on high-throughput automated platforms, including the Fujirebio Lumipulse assay, resulting in a more consistent analytical process. Few studies have assessed the agreement of amyloid PET and CSF biomarkers on Lumipulse. Consistent with other studies, our data show that when comparing amyloid-PET and composite CSF measures of A $\beta$ , 18F-Florbetapir was highly correlated with A $\beta$ 42/40 ( $r = -0.810$ ,  $p < 0.0001$ ), and p-tau/A $\beta$ 42 ( $\rho = -0.841$ ,  $p < 0.0001$ ) (**APPENDIX A**). Additionally, using pre-established cutoffs that were defined based on receiver operating characteristic analysis of amyloid PET and the CSF measures, classification performance was high between 18F-

Florbetapir and composite measures of A $\beta$  such as p-tau/A $\beta$ 42 (AUC = 0.95), and A $\beta$ 42/40 (AUC = 0.92) (**APPENDIX A**).

The NIA-AA research framework has more recently been updated (Jack et al., 2018; Jack Jr et al., 2013) to focus on A/T/N criteria, first proposed by Jack and colleagues (Jack et al., 2016) and pave the path to more personalized diagnosis and treatment. The new framework highlights the value of positive amyloid biomarkers (A) to specifically indicate AD-related processes.

Pathological tau (T) is only taken to indicate an AD-related process in the presence of amyloid positivity. Finally, (N) biomarkers are thought to provide nonspecific information about neuronal injury and neurodegenerative change. The combination of amyloid with other biomarkers can then be used to stage AD progression. Additionally, according to this new framework, the presence of tau and neurodegeneration in the absence of amyloidosis is considered evidence for non-AD pathological processes. An important aspect of the 2018 NIA-AA working group framework is the flexibility to include additional biomarkers in future iterations. We recently reviewed established and emerging neuroimaging biomarkers for Alzheimer's disease (Márquez and Yassa, 2019).

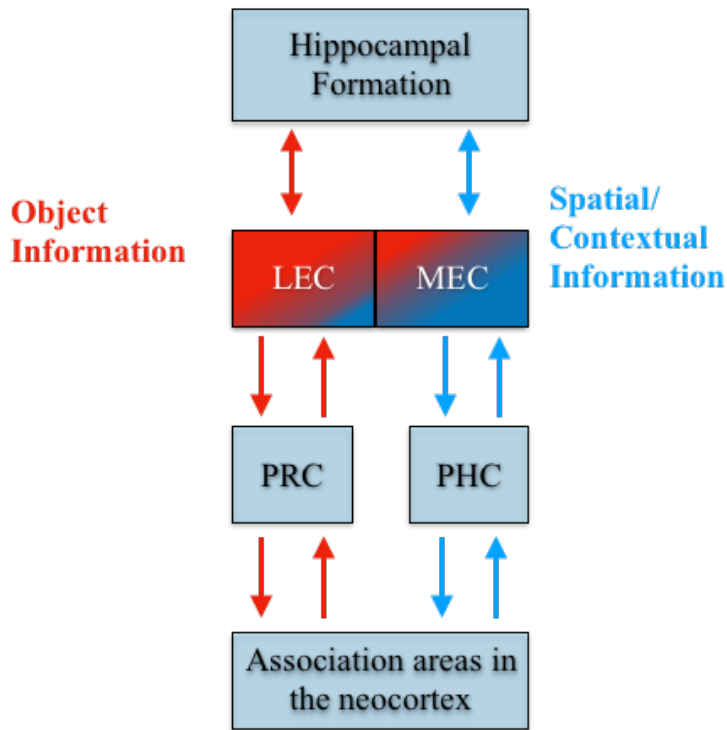
## **1.3 Memory systems and Episodic Memory**

### **1.3.1 The role of the medial temporal lobe in episodic memory**

The medial temporal lobe contains a set of structures that play an important role in declarative long-term memory (facts and events) processing, which is severely impacted in amnesic forms of AD. It consists of the hippocampal formation (HF: CA1-4, dentate gyrus – DG, subiculum, presubiculum, parasubiculum), perirhinal (PRC), entorhinal (EC), and

parahippocampal/postrhinal (PHC/POR) cortices. These structures are highly interconnected and support distinct information processing streams (Ranganath and Ritchey, 2012). The lateral (LEC) contains neurons and circuits representing information about objects and their complexity, object traces over time, and sequences of an event (parameters that represent the specific content and temporal order of an event (Deshmukh and Knierim, 2011; Montchal et al., 2019; Reagh and Yassa, 2014; Rodo et al., 2017; Tsao et al., 2013, 2018; Van Cauter et al., 2013; Wang et al., 2018; Wilson et al., 2013a, 2013b). In contrast, studies in animals and in humans indicate that the medial EC (MEC) stream contains a high percentage of spatially modulated neurons such as grid, head direction, border, aperiodic spatial and object-vector cells (parameters necessary for spatial navigation) (Doeller et al., 2010a; Hafting et al., 2005; Høydal et al., 2019; Jacobs et al., 2013; Killian et al., 2012; Miao et al., 2017; Sargolini et al., 2006; Solstad et al., 2008).

Neuroanatomical and neuroimaging studies have indicated that the PHC (homologous to the POR in rodents) carries visuospatial/contextual information ('where' stream) to the MEC, and the PER carries item/object information to the LEC ('what' stream) (Burwell and Amaral, 1998; Maass et al., 2015; Naber et al., 1997; Navarro Schröder et al., 2015; Schultz et al., 2015; Suzuki and Amaral, 1994). These two streams converge in the HF, where they are combined and further processed to construct a complete memory representation (Eichenbaum et al., 2007; Ranganath and Ritchey, 2012; Yassa and Stark, 2011; Yonelinas and Ritchey, 2015).



**Figure 2.** MTL circuits involved in episodic memory

### 1.3.2 Pattern separation in the hippocampus

Episodic memory is often defined as records of unique experiences and events that guide adaptive behavior; a feature of the brain that is thought to be reliant on the hippocampus (Milner et al., 1998; Squire et al., 2004). A key feature of episodic memory is the ability to discriminate among highly similar experiences thus creating dissociable experiences from one day to the next. Computational models suggest that the brain uses a neural computation known as *pattern separation* to distinguish among highly similar items during memory performance (Marr, 1971). This computation is thought to be heavily reliant on the dentate gyrus (DG) and CA3 of the hippocampus and serves to create orthogonalized representations from similar inputs (Yassa and Stark, 2011). More specifically, the DG is thought to be capable of pattern separation while the



CA3 region acts in an auto-associative network capable of both pattern separation as well as *pattern completion* via its recurrent collateral network. Pattern completion in this sense, refers to the process by which incomplete representations are “filled in” based on previously stored information (Yassa and Stark, 2011).

### 1.3.3 Pattern separation and neurocognitive aging

Through the advances made in neurocognitive aging studies, it is now possible to develop and validate behavioral paradigms that can dissociate and provide information about the functional integrity of underlying systems. The hippocampal dentate gyrus (DG)/CA3 network is hypothesized to engage in minimization of interference among overlapping memories, i.e. pattern separation (Yassa and Stark, 2011). This capacity is diminished in aged rats with memory impairment (Wilson et al., 2006). Using high-resolution functional MRI, object discrimination performance is linked to functional rigidity, or the inability to pattern separate unless interference is minimal, as well as hyperactivity in the DG/CA3 region in older adults (Yassa et al., 2011a, 2011b). The hyperactivity reported is consistent with other studies of hippocampal memory in MCI patients (Dickerson et al., 2004, 2005; Miller et al., 2008a) and in older adults *with* subclinical memory impairments (defined by the RAVLT Delay) (Miller et al., 2008b; Yassa et al., 2010). Other work has also shown that increased hippocampal activity negatively correlates with thinning in several regions, including the entorhinal cortex (EC) (Putchala et al., 2011). This work has recently been extended beyond object discrimination to show that aging is associated with impaired spatial (Reagh et al., 2014) and temporal (Roberts et al., 2014) discrimination.

Using a task concurrently taxing object versus spatial mnemonic discrimination, thought to tax pattern separation (orthogonalization of similar inputs into dissimilar outputs) in the

hippocampus, shows that while older adults *without* subclinical memory impairments (defined by the RAVLT Delay) have major deficits on object discrimination, they only show subtle deficits on the comparable spatial discrimination task when compared to young adults (Reagh et al., 2016). Recent human fMRI studies have identified a functional dissociation within the EC, with anterolateral (aLEC) and posteromedial (pMEC) subregions similar to what is found in rodents (Maass et al., 2015). In the task-activated fMRI version of the object versus spatial task, the results show domain-general hippocampal engagement, but selective engagement of PRC and LEC during object discrimination and engagement of PHC and MEC during spatial discrimination (Reagh and Yassa, 2014). Furthermore, engagement of the DG/CA3 and aLEC correlate with performance on the object discrimination task to reveal an imbalance of the DG/CA3-aLEC circuit (hyperactivity of DG/CA3 and hypoactivity of the aLEC) in the absence of structural thinning of the regions in healthy older adults (Reagh et al., 2018).

Although it is presently unclear whether dysfunction in these brain regions is exclusive to pathological aging, or is also a feature of healthy aging, much evidence suggests that the PRC and LEC are among the earliest areas affected (Reagh et al., 2018). As PRC and LEC project to the hippocampus, it is likely that disruptions in these input regions also disrupt hippocampal computations during object discrimination, but less so during spatial discrimination. Conversely, other neighboring cortices thought to process spatial or contextual information (such as PHC and MEC) may be relatively spared in the absence of age-related neuropathology. Older adults *with* subclinical memory impairments (defined by the RAVLT Delay) show impaired performance on both aspects of the task, which suggests that both the item/object and context/spatial neural circuits may be negatively impacted. Studies evaluating mnemonic discrimination of spatial information were based on early work in hippocampal-lesioned rodents (Gilbert et al., 1998),

which assessed the ability to judge whether stimuli had moved from locations in which they were originally presented. The difficulty of discrimination is typically tested by systematically varying the metric distance between the study and test phases. Recent studies have used spatial mnemonic discrimination tasks and have found that a subset of older adults who were impaired (based on the RAVLT) were significantly impaired on the spatial discrimination task compared to unimpaired older adults and young adult groups (Reagh et al., 2014; Stark et al., 2010). Another study (Holden and Gilbert, 2012), using a delayed-match-to-sample discrimination task also showed impairments in the ability for older adults to discriminate spatial information.

### **1.3.4 Functional neocortical networks**

Functional MRI techniques are based on blood-oxygenation-level-dependent (BOLD) contrast, which is associated with neural activity at the population level. Resting-state functional magnetic resonance imaging (rsfMRI) studies examine the temporal correlation of the BOLD signal between the regions of interest (or functional connectivity) by analyzing task-independent spontaneous fluctuations in brain networks (Biswal et al., 1995; Fox and Raichle, 2007). An emerging systems-based model of AD considers the large-scale disruptions across the course of AD. In preclinical AD, studies have generally noted that resting state fMRI (rsfMRI) is linked to metabolic changes (indexed by PET imaging) and precedes neurodegeneration (review by Sheline and Raichle, 2013). Most analyses have focused on the default mode network (DMN) (Gusnard and Raichle, 2001; Raichle et al., 2001) - a network that involves the medial prefrontal cortex, posterior cingulate cortex, precuneus, anterior cingulate cortex, parietal cortex, and the medial temporal lobe, including the hippocampus (Buckner et al., 2008; Greicius and Menon, 2004). As regions within the DMN are highly overlapping with the spatial distribution of both

amyloid and tau pathology (Buckner et al., 2008), resting state fMRI can offer important information on the integrity of these circuits and the degree to which their synaptic connectivity may be affected by the disease process. While some studies have found that alterations to DMN connectivity become more dramatic with disease progression, others have found dynamic changes that relate to A $\beta$  and tau-specific profiles (Jones et al., 2016; Petrella et al., 2011; Sanz-Arigitia et al., 2010; Schultz et al., 2017; Sepulcre et al., 2016; Supekar et al., 2008; Zhang et al., 2010). Connectivity changes in other networks have also been reported (Fredericks et al., 2018). For example, the interaction between the DMN and the salience network, which consists of anterior insula, dorsal anterior cingulate cortex, is associated with increased connectivity in amyloid-positive individuals with low neocortical tau, and decreased connectivity as a function of elevated Tau-PET signal (Schultz et al., 2017).

In addition to changes in the DMN, some studies have suggested that connectivity within the MTL is also disrupted with aging and AD. For example, Yassa et al. (Yassa et al., 2011a) showed an age-related decrease in connectivity between the entorhinal cortex and the dentate and CA3 regions of the hippocampus, the extent of which was correlated with memory deficits. Functional connectivity is thought to be an early marker of synaptic pathology that may be associated with isolation of the hippocampus from its cortical input.

Beyond the MTL network, the EC is interconnected with a broader neocortical network and is thought to provide the neural substrate for integrating spatial and object information (Ranganath and Ritchey, 2012). Evidence from the rodent indicates that the lateral entorhinal cortex is associated with cortical inputs including the orbitofrontal cortex and the amygdala while the medial entorhinal cortex is associated with cortical inputs such as the retrosplenial cortex and postrhinal cortex, among others (Witter et al., 2017). It is thought that the functions of each of

these regions are, in part, due to their connections with these cortical inputs. However, how these regions and their computations are altered in Alzheimer's disease is not understood.

The RSC plays a key role in spatial memory and navigation, which means that this area represents a very important node in a broader spatial processing that includes the HF. The retrosplenial cortex (RSC) serves as a source of substantial, direct input to the EC, and projections from RSC account for nearly 20% of the total cortical input to the EC (Insausti et al., 1987). Neuroanatomical tracing data in the nonhuman primate show that the RSC has strong connections with the EC. Afferents to the EC originate in both Broca's area 29 and 30. Although these projections are restricted to the caudal one-half of the EC ( $E_I$ ,  $E_C$  and  $E_{CL}$  subfields), whereas the rostral one-half of the EC receives little to no projections from the RSC. RSC afferents to the EC terminate mostly in layer I in a restricted topographical manner (Insausti and Amaral, 2008). Retrograde transport studies have shown that both PRC [area 35] (Kobayashi and Amaral, 2003) and PHC [areas TH and TF] project to RSC as well (Kobayashi and Amaral, 2003).

### **1.3.5 Memory systems and PMAT networks**

Although episodic memory is supported by the circuitry of the medial temporal lobes (MTL), including the hippocampus, the MTL interacts extensively with a number of specific distributed cortical and subcortical structures (Dickerson and Eichenbaum, 2010). Spatial and nonspatial information seem to follow distinct parallel processing streams through the medial temporal lobes, with the hippocampus combining spatial and non-spatial information to form unified cohesive representations of an experience (Inhoff and Ranganath, 2017; Ranganath and Ritchey, 2012). In this model, spatial processing relies on a posteromedial (PM) system that includes the

entorhinal cortex, parahippocampal cortex, retrosplenial cortex, and posterior cingulate cortex, whereas object processing relies on an anterior-temporal (AT) system that includes the perirhinal cortex, the medial prefrontal cortex, and the anterior cingulate. Previous MRI studies have indicated early deterioration of anterior-temporal regions in aging that is linked to deficits in object memory (Berron et al., 2018; Reagh et al., 2018). Less attention has focused on the structural and functional integrity of the PM network. This is of importance to AD since the PM network is one of the earliest regions to show aggregation of beta-amyloid ( $A\beta$ ) pathology (Klunk et al., 2004; Palmqvist et al., 2017). Furthermore, functional MRI studies have reported amyloid- $\beta$ -related hyperactivation in hippocampus and posterior-medial regions that seems to reflect a failure in task-related deactivation (Elman et al., 2014; Huijbers et al., 2014; Leal et al., 2017; Mormino et al., 2012; Sperling et al., 2009; Vannini et al., 2012).

### **1.3.6 Mild cognitive Impairment and Alzheimer's Disease**

One of the most common features of AD is decline in the ability to encode and retrieve our daily personal experiences, or episodic memory. A crucial component of episodic memory is pattern separation, the ability to independently represent and store similar experiences using unique neural codes (Marr, 1971; McClelland et al., 1995; Treves and Rolls, 1994; Yassa and Stark, 2011). Accumulating evidence suggests that the hippocampus possesses unique circuitry that is computationally capable of resolving mnemonic interference by using pattern separation (Leal and Yassa, 2018). This computation prevents overgeneralization of information and allows for efficient storage of episodic memories. Moreover, functional integrity of the hippocampus and decline in episodic memory can be attributed to loss of pattern separation (Leal and Yassa, 2015). Cognitive studies in aged humans have now reliably reported mnemonic discrimination

impairment (Stark et al., 2010, 2013; Yassa et al., 2011b) with more dramatic loss in aMCI (Bakker et al., 2012; Yassa et al., 2010).

Spatial memory is a special case of episodic memory that is known to be compromised very early in individuals with Alzheimer's disease (Hope et al., 1994; Lithfous et al., 2013), including in preclinical AD (Allison et al., 2016). In healthy brains of both humans and rodents, place cells in the hippocampus and grid cells in the medial entorhinal cortex (MEC) form a neural circuit that is critical for spatial memory (Doeller et al., 2010b; Ekstrom et al., 2003; Fyhn et al., 2004; Morris et al., 1982; O'Keefe and Dostrovsky, 1971; Scoville and Milner, 1957; Steffenach et al., 2005). The MEC, in particular, contains a high percentage of spatially modulated neurons such as grid, head direction, border, aperiodic spatial and object-vector cells (parameters necessary for spatial navigation) (Doeller et al., 2010b; Hafting et al., 2005; Jacobs et al., 2013; Killian et al., 2012; Miao et al., 2017; Sargolini et al., 2006; Solstad et al., 2008). Recent evidence has pointed to alterations in the neural coding properties in these networks in AD patients (Jun et al., 2020; Kunz et al., 2015).

## **CHAPTER 2: Establishing convergent validity of spatial pattern separation**

### **Introduction**

Remembering where you saw something is important for future behavior. Previous studies have demonstrated that mnemonic discrimination tasks are sensitive to hippocampal pattern separation, including the spatial pattern separation task. Word list recall is a standard memory task that is widely used in the clinical setting. In the current study, our goal was to establish convergent validity with a standardized memory task that is often used in a clinical setting. We hypothesized that the spatial pattern separation performance would be associated with a

standardized word list recall memory task. The current investigation builds on prior work by further specifying the nature of the memory phenotype associated with spatial pattern separation (e.g., learning vs. interference vs. retention).

## **Materials and Methods**

### **Participants**

A total sample of 84 older adults between 61 and 91 years of age (54 F, mean age = 73.3 years, SD = 6.10 years) were included in this study. Forty-five older adults were recruited from the Alzheimer's Disease Research Center (ADRC) Longitudinal Cohort at the University of California, Irvine and 39 were recruited from the surrounding Orange County community as part of the Biomarker Exploration in Aging, Cognition, and Neurodegeneration (BEACoN) study. Participants gave written informed consent in accordance with the Institutional Review Board of the University of California, Irvine, and were compensated for their participation.

Participants in the ADRC subsample ( $n = 45$ ) were administered the Uniform Data Set (UDS-3) battery by a neuropsychologist in order to characterize the sample in accordance with the National Alzheimer's Coordinating Center (NACC) criteria (Weintraub et al., 2018). This is a standardized set of neuropsychological tests used by Alzheimer's Disease Centers across the United States. The battery includes the Montreal Cognitive Assessment (Nasreddine et al., 2005), Craft Story (Craft et al., 1996), Digit Span (Wechsler, 1987), Trail making Test Parts A and B (Reitan and Wolfson, 1985), and the Benson Complex Figure Test (Possin et al., 2011). For statistical comparison between groups, participants were dichotomized into cognitively normal (CN) or cognitively impaired (CI), which include Mild Cognitively Impaired (MCI) and Cognitively Impaired, Non-Demented (CIND) participants. All participants ( $n = 84$ ) were



administered the spatial pattern separation task, Rey Auditory Verbal Learning Test (RAVLT), Mini-Mental State Exam (MMSE). Seven participants from the ADRC subsample were excluded from analysis due to confusion with the task instructions.

### **Neuropsychological testing**

The spatial pattern separation task was an optimized version of a paradigm previously developed by our group (Reagh et al., 2014, 2016, 2018). Participants first studied the location of objects during an incidental encoding task with an “Indoor or Outdoor” judgement. A surprise test phase was subsequently conducted during which participants viewed the same images again, half of which were presented in the same locations (targets) and half were presented in different locations (lures). Participants were asked to judge “Same” to correctly identify nondisplaced targets or “Different” to correctly identify displaced lures. The Spatial Lure Discrimination Index (LDI) was calculated as the proportion of lures correctly identified as “Different” minus the proportion of targets incorrectly identified as “Different” to correct for response bias. The Rey Auditory Verbal Learning Test (RAVLT) is a standard memory test that was developed to assess a variety of memory processes and assesses rate of learning, retention after short- and long-delay intervals, and recognition memory. We chose to focus on the RAVLT Delayed Recall component of the test (out of 15), as this has been shown to be sensitive to cognitive decline and episodic memory deficits with age (Andersson et al., 2006; Vakil and Blachstein, 1997). We have also previously reported correlations between spatial pattern separation performance and RAVLT word list delayed recall in older adults (Reagh et al., 2014), further motivating our use of this measure here to provide convergent validity for the spatial pattern separation task.

## **Results**

## Spatial pattern separation is associated with word list recall

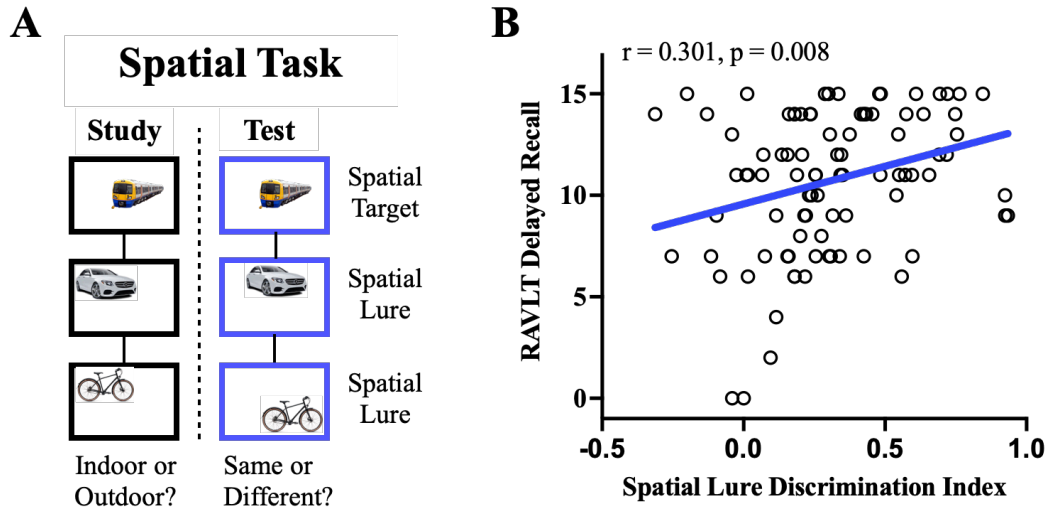
A schematic of the spatial pattern separation task is shown in **Figure 3A**, and a more detailed description can be found in the Methods. Briefly, participants made discrimination/recognition judgments on items that were displaced from their original locations during study. The Spatial Lure Discrimination Index (LDI) was used as a summary measure of their performance. See Methods for details. Demographic information about the participants is displayed in **Table 1**.

<b>Demographics</b>		
	<b>Full Sample</b>	<b>CSF subsample</b>
<b>Sample Size</b>	77 (54 F)	38 (24 F)
<b>Age (years)</b>	73.3 (6.10)	74.5 (6.22)
<b>Education (years)</b>	16.5 (2.51)	16.2 (2.58)
<b>Race</b>		
White	59 (76.6%)	34 (89.5%)
Asian	15 (19.5%)	4 (10.5%)
Black or African American	1 (1.3%)	0 (0%)
More than One Race	2 (2.6%)	0 (0%)
<b>Ethnicity</b>		
Hispanic	4 (5.2%)	1 (2.6%)
Non-Hispanic	73 (94.8%)	37 (97.4%)
<b>Diagnosis</b>		
Normal (n)	67 (52 F)	28 (22 F)
Impaired (QCI, MCI) (n)	10 (2 F)	10 (2 F)
<b>Baseline MMSE</b>	28.2 (1.52)	28.3 (1.50)
<b>RAVLT – learning slope</b>	1.51 (0.543)	1.73 (0.616)
<b>RAVLT – retroactive interference</b>	0.829 (0.180)	0.798 (0.181)

<b>RAVLT – percent forgetting</b>	0.184 (0.219)	0.242 (0.257)
<b>RAVLT – delayed recall</b>	10.5 (3.59)	9.66 (4.05)
<b>A<math>\beta</math>42/A<math>\beta</math>40</b>	0.071 (0.025)	0.071 (0.205)
<b>t-tau (pg/mL)</b>	405 (266)	405 (266)
<b>p-tau181 (pg/mL)</b>	55.6 (46.0)	55.6 (46.0)

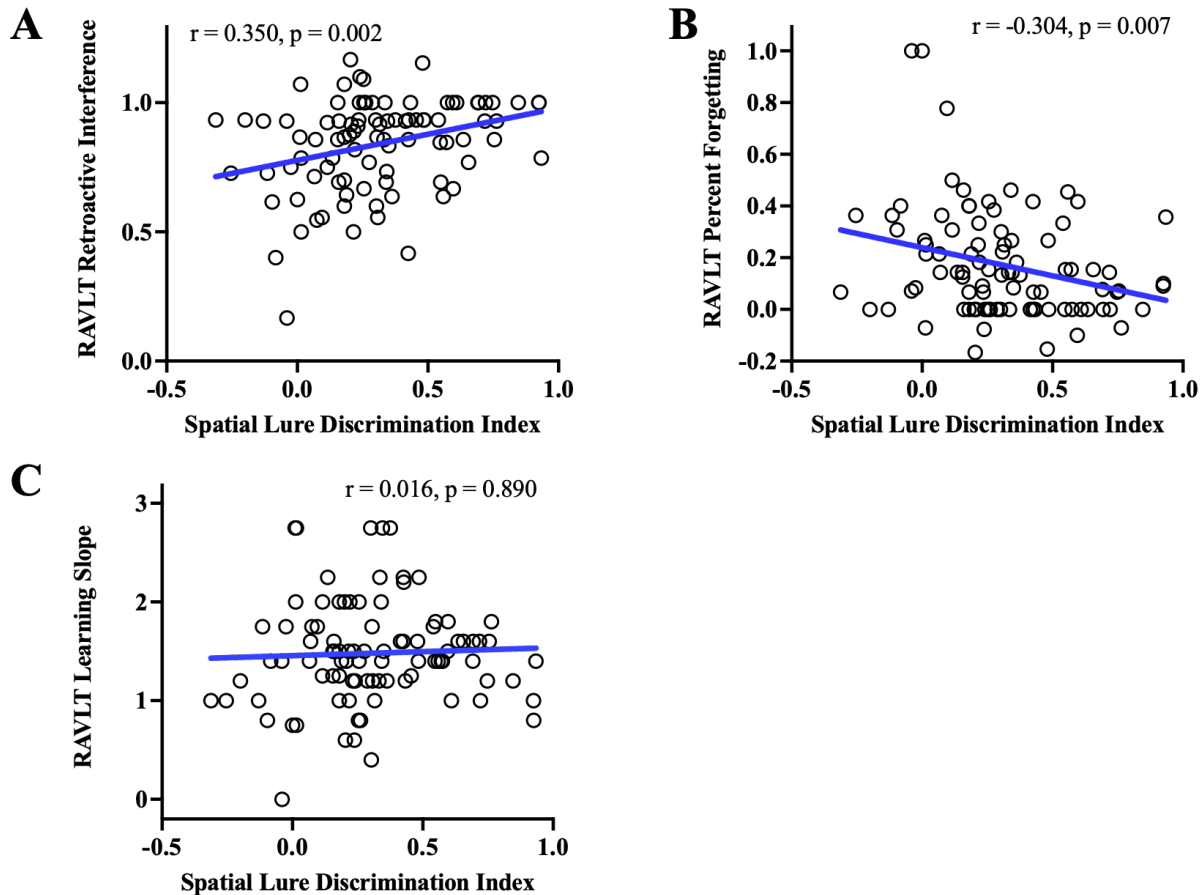
**Table 1: Demographics and neuropsychological test scores.** Unless otherwise stated, variables denote mean ( $\pm$  SD). Subjects in the CSF subsample were part of the full sample.

Consistent with our prior work, we observed a significant correlation between Spatial LDI and delayed recall performance (Pearson’s  $r = 0.301$ ,  $p = 0.008$ ; **Figure 3B**). In considering covariates, we observed that sex and clinical status were highly correlated in this sample (Pearson  $r = 0.423$ ,  $p < 0.001$ ), as the cognitively impaired sample was predominantly male. Since our past work with pattern separation tasks had not observed sex differences in performance, we opted to only include age and clinical status as covariates in multiple regression. The overall model was statistically significant ( $r = 0.531$ ,  $F_{(3,73)} = 9.54$ ,  $p < 0.001$ ), revealing a significant main effect of clinical status ( $B = -4.059$ ,  $SE = 1.106$ ,  $t = -3.671$ ,  $p < 0.001$ ). Spatial LDI ( $B = 2.553$ ,  $SE = 1.377$ ,  $t = 1.854$ ,  $p = 0.068$ ) and age ( $B = -0.115$ ,  $SE = 0.060$ ,  $t = -1.910$ ,  $p = 0.060$ ) were only marginally significant once clinical status was accounted for.



**Figure 3.** Spatial lure discrimination is associated with RAVLT delayed recall. (A) Schematic of the task. Participants first completed an encoding task with an incidental “Indoor or Outdoor” judgment, during which location objects were studied. Subsequently, a surprise test phase was conducted during which participants observed identical targets, and similar lure items with varying displacements. Subjects were asked to judge “Same or Different” with the former judgment accurately identifying targets and the latter accurately rejecting lures. (B) Spatial Lure Discrimination Index was related to performance on the RAVLT Delayed Recall (Pearson  $r = 0.301$ ,  $p = 0.008$ ).

To determine whether Spatial LDI was more specifically associated with measures that may be more sensitive to robustness against interference, retention across a delay, or learning across trials, we further assessed the relationship between Spatial LDI and other measures of memory and learning performance derived from the RAVLT. We calculated indices for (1) *retroactive interference* (List A Trial 6/List A Trial 5), a measure of whether new learning is inhibiting recall of previously learned information (Loewenstein et al., 2004; Yeung et al., 2019), (2) *percent forgetting* ( $[\text{List A Trial 5} - \text{List A Trial 7}] / [\text{List A Trial 5}]$ ), a measure of retention over the delay period (Estévez-González et al., 2003; Moradi et al., 2015, 2017), and (3) *learning slope* ( $[\text{List A Trial 5} - \text{List A Trial 1}] / 4$ ), a measure of learning over multiple trials.



**Figure 4. Spatial lure discrimination is associated with Retroactive Interference.** (A-C) A higher Spatial LDI was related to higher Rey Auditory Verbal Learning Test (RAVLT) *retroactive interference* (Pearson  $r = 0.350, p = 0.002$ ). A higher Spatial LDI was related to lower Rey Auditory Verbal Learning Test (RAVLT) *percent forgetting* (Pearson  $r = -0.304, p = 0.007$ ). Spatial LDI was not associated with Rey Auditory Verbal Learning Test (RAVLT) *learning slope* (Pearson  $r = 0.016, p = 0.890$ ).

We found that Spatial LDI was positively associated with *retroactive interference* scores (**Figure 4A**; Pearson  $r = 0.350, p = 0.002$ ). We further assessed this relationship using multiple linear regression with age and clinical status as covariates. The overall model was statistically significant ( $r = 0.425, F_{(3,73)} = 5.354, p = 0.002$ ), revealing a significant main effect of Spatial LDI ( $B = 0.193, SE = 0.073, t = 2.654, p = 0.010$ ) and clinical status ( $B = -0.126, SE = 0.059, t = -2.149, p = 0.035$ ). Age ( $B = -0.001, SE = 0.003, t = -0.424, p = 0.673$ ) was not a significant

predictor. These results suggest that Spatial LDI and clinical status were significantly associated with neuropsychological measures *retroactive interference*.

We also found that higher Spatial LDI was related to lower *percent forgetting* (**Figure 4B**; Pearson  $r = -0.304$ ,  $p = 0.007$ ). We further assessed this relationship using multiple linear regression with age and clinical status as covariates. The overall model was statistically significant ( $r = 0.480$ ,  $F_{(3,73)} = 7.28$ ,  $p < 0.001$ ), revealing a significant main effect of clinical status ( $B = 0.206$ ,  $SE = 0.069$ ,  $t = 2.988$ ,  $p = 0.004$ ). Spatial LDI ( $B = -0.171$ ,  $SE = 0.086$ ,  $t = -1.985$ ,  $p = 0.051$ ) was only a marginally significant predictor and age ( $B = 0.006$ ,  $SE = 0.004$ ,  $t = 1.596$ ,  $p = 0.115$ ) was not a significant predictor. We found that Spatial LDI was not associated with learning slope (**Figure 4C**; Pearson  $r = 0.016$ ,  $p = 0.890$ ). Overall, this suggests that Spatial LDI is generally more associated with memory interference as opposed to learning or retention-related deficits per se.

## Discussion

In a sample of nondemented older adults, we found that performance on a spatial pattern separation task was associated with RAVLT retroactive interference in word list recall. RAVLT is a standard neuropsychological test of episodic memory and retroactive interference is assumed to rely at least partially on the integrity of the hippocampus, providing a strong case for its use in assessing memory function (Kuhl et al., 2010; Wagner et al., 2016). We note the RAVLT is widely used for cognitive assessment in pre-dementia and dementia in a clinical setting, and is helpful for discriminating normally aging individuals from those with mild cognitive impairment (MCI) and AD (Balthazar et al., 2010).

Our previous work demonstrated that a subset of older adults who scored outside of the young norms on RAVLT delayed word list recall (but within age-matched norms) were significantly impaired on spatial pattern separation compared to older adults scoring within young adult norms as well as young adult groups (Reagh et al., 2014, 2016, 2018; Stark et al., 2010). This suggests that the task is sensitive to individual differences with aging. We note that in these studies spatial pattern separation performance was significantly correlated with word list recall scores in older adults, but not in young adults, although this could be driven by the reduced variability in recall scores in young adults.

Here, we extend and build on prior work by further specifying the nature of the memory phenotype associated with spatial pattern separation (e.g., learning vs. interference vs. retention). We calculated learning slope, retroactive interference, and percent forgetting scores. We showed that the Spatial LDI was significantly associated with retroactive interference, but not with percent forgetting or learning slope suggesting that performance on the spatial pattern separation task is more likely driven by interference rather than learning or retention deficits. This is consistent with prior studies demonstrating that aMCI patients are more susceptible to retroactive interference effects than cognitively normal older adults with a task similar to the RAVLT (Crocco et al., 2014).

Overall, our results suggest that spatial pattern separation is a sensitive marker of memory, and in particular, to the robustness of memory across interference. This is perhaps not surprising, since pattern separation is a computational mechanism that allows us to overcome interference from similar experiences (Yassa and Stark, 2011).

## **CHAPTER 3: Spatial pattern separation and PMAT framework**

### **Introduction**

Cortical pathways to the hippocampus appear to extend from two large-scale cortical systems: a posteromedial (PM) system that includes the parahippocampal cortex, retrosplenial cortex, and posterior cingulate cortex, and an anterior temporal (AT) system that includes the perirhinal cortex (Ritchey et al., 2015). The PMAT framework accounts for differences in the anatomical and functional connectivity of the medial temporal lobes. Using data-driven, graph theoretical analysis of resting-state functional connectivity data, networks strongly resembling PM and AT systems have been identified, in which connectivity was stronger within each network than between networks (Ritchey et al., 2014). Links between connectivity and function within the PM and AT networks have also been reported in task-activated fMRI studies, in which the PM system is associated with spatial processing and the AT system is associated with object processing, and temporal precision (Montchal et al., 2019; Reagh and Yassa, 2014). We hypothesized that PM functional connectivity would be associated with spatial pattern separation task performance.

### **Materials and Methods**

#### **Participants**

Forty-five older adults between 61 and 91 years of age were recruited from the Alzheimer's Disease Research Center (ADRC) Longitudinal Cohort at the University of California, Irvine. Participants gave written informed consent in accordance with the Institutional Review Board of the University of California, Irvine, and were compensated for their participation. Participants were administered the Uniform Data Set (UDS-3) battery by a neuropsychologist in order to



characterize the sample in accordance with the National Alzheimer's Coordinating Center (NACC) criteria (Weintraub et al., 2018). This is a standardized set of neuropsychological tests used by Alzheimer's Disease Centers across the United States. The battery includes the Montreal Cognitive Assessment (Nasreddine et al., 2005), Craft Story (Craft et al., 1996), Digit Span (Wechsler, 1987), Trail making Test Parts A and B (Reitan and Wolfson, 1985), and the Benson Complex Figure Test (Possin et al., 2011). For statistical comparison between groups, participants were dichotomized into cognitively normal (CN) or cognitively impaired (CI), which include Mild Cognitively Impaired (MCI) and Cognitively Impaired, Non-Demented (CIND) participants.

All participants (n = 45) were administered the spatial pattern separation task, Rey Auditory Verbal Learning Test (RAVLT), Mini-Mental State Exam (MMSE). Seven participants from the ADRC subsample were excluded from analysis due to confusion with the task instructions. Participants in the ADRC subsample additionally underwent resting state fMRI imaging. Of the 38 participants in the ADRC subsample, two participants were excluded in the imaging analyses due to poor signal in the medial temporal lobes.

### **MRI data acquisition**

Neuroimaging data were acquired on a 3.0 Tesla Philips Achieva scanner, using a 32-channel sensitivity encoding (SENSE) coil at the Neuroscience Imaging Center at the University of California, Irvine. A high-resolution 3D magnetization-prepared rapid gradient echo (MP-RAGE) structural scan (0.65 mm isotropic voxels) was acquired at the beginning of each session and used for co-registration. For each subject, resting state EPI scans consisted of a T2\*-weighted echo planar imaging (EPI) sequence using blood-oxygenation-level-dependent (BOLD) contrast: repetition time (TR)=3500 ms, echo time (TE)=26 ms, flip angle=70 degrees, 55 slices,

100 dynamics per run, 1.8 x 1.8 mm in plane resolution, 1.8 mm slice thickness with a 0.2 mm gap, field of view (FOV)=180x109.8x180. Slices were acquired as a partial axial volume and without offset or angulation. Four initial “dummy scans” were acquired to ensure T1 signal stabilization.

### **MRI data preprocessing**

All neuroimaging data were preprocessed and analyzed using Analysis of Functional NeuroImages (AFNI) (Cox, 1996). on GNU/Linux and Mac OSX platforms. Analyses largely took place in accordance with the standardized afni\_proc.py pipeline. Specifically, data were corrected for motion (3dvolreg) and slice timing shifts (3dTshift), masked to exclude voxels outside the brain (3dautomask), and were smoothed (3dmerge) to a 2.0mm using a Gaussian FWHM kernel. Each run was also despiked to further reduce the influence of motion on the data (3dDespike). Functional scans were aligned to each subject’s skull-stripped MP-RAGE (align\_epi\_anat.py). We defined ROIs based on our prior work (Reagh and Yassa, 2014; Yushkevich et al., 2015). We used Advanced Normalization Tools (ANTs) (Avants et al., 2008) to warp each individual participant's MP-RAGE structural scan into our custom in-house high-resolution template space using nonlinear, diffeomorphic transformation. Parameters from these warps were used to also warp functional scans into template space for group analyses. Masks were resampled to match the resolution of the fMRI data (1.8x1.8x2.0mm) and were further masked to exclude partially sampled voxels within and across runs (3dcalc). Once we obtained models of ongoing BOLD activity per subject (3dDeconvolve), we extracted the average time course across ROIs (3dmaskave). A Fisher's r-to-z transformation was applied to each correlation map, to obtain an approximately normal distribution of the functional connectivity values and accordingly apply parametric statistics (3dcalc). PHC, and RSC ROIs were generated from masks used previously

by our group (Reagh and Yassa, 2014). Other cortical ROIs were merged with our mask based on the Freesurfer cortical atlas (Dale et al., 1999; Fischl et al., 1999). To assess functional connectivity, we calculated the Pearson correlation coefficient between the mean signal intensity time courses of each ROI pair.

### **Statistical analysis**

All statistical analyses on voxel-averaged data and data visualizations were conducted in Jamovi (Version 1.6.23.0), R (version 3.6.3) and GraphPad Prism (Version 8.4.3). Preprocessing and first-level analyses of neuroimaging data were conducted in AFNI (Version 16.0) using the functions described throughout the Methods section.

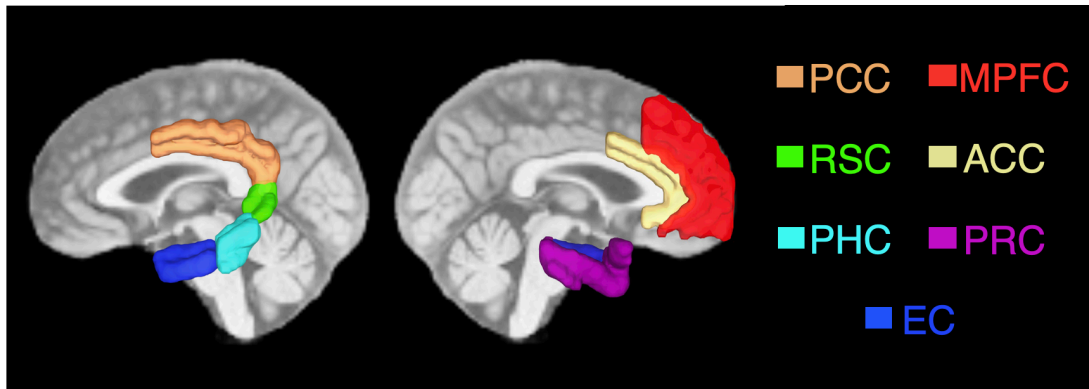
## **Results**

### **Spatial pattern separation is associated with PM network functional connectivity**

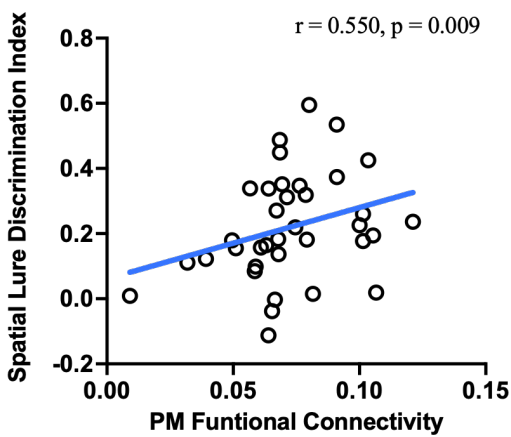
A subset (n=36) of our participants underwent resting state functional MRI scans, allowing us to assess the relationship between spatial pattern separation and functional connectivity in the PMAT system. Since our hypotheses were specific to PM regions, we conducted region of interest (ROI) analyses in PM and AT cortex and assessed whether resting state fMRI functional connectivity among regions constituting these networks is associated with spatial pattern separation task performance. Correlation coefficients were calculated between the mean signal intensity time courses of each ROI pairs were calculated. ROIs are shown in **Figure 5A**.

Regression coefficients were then averaged across all ROI pairs to determine the PM functional connectivity and AT functional connectivity. See Methods for details on how fMRI data were processed and analyzed.

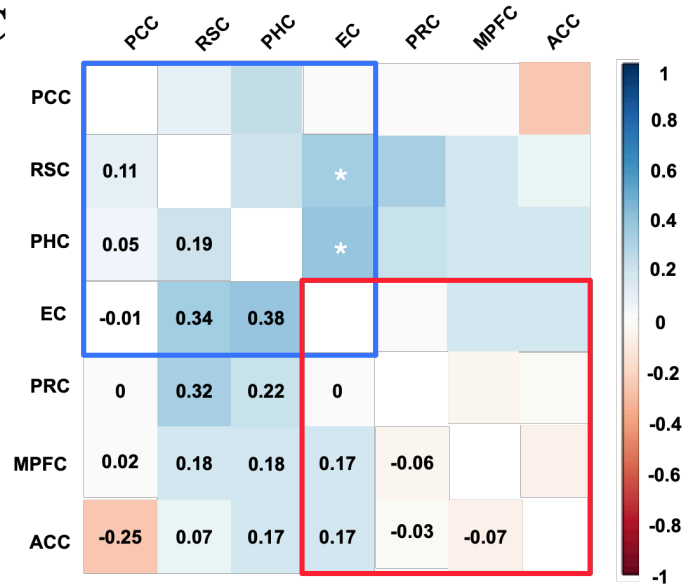
A



B



C



**Figure 5. Functional connectivity of the posteromedial system associated with Spatial Lure Discrimination Index** (A) Anatomical regions of interest (ROIs) used to mask functional data. ROIs were generated from masks used previously by our group (PCC = posterior cingulate cortex, RSC = retrosplenial cortex, PHC = parahippocampal cortex, EC = entorhinal cortex, PRC = perirhinal cortex, mPFC = medial prefrontal cortex, ACC = anterior cingulate cortex). (B) Higher Spatial LDI was related to higher functional connectivity across posteromedial (PM) regions ( $r = 0.550$ ,  $p = 0.008$ ). (D) Functional connectivity of each pairwise correlation, with PM connectivity shown in the blue square and AT connectivity shown in the red square. Asterisks indicate that the correlation is significant ( $p < 0.05$ ).

We conducted two multiple regressions. First, we assessed the relationship between PM functional connectivity and Spatial LDI, with age and clinical status as covariates. The overall

model was statistically significant ( $r = 0.550$ ,  $F_{(3,32)} = 4.62$ ,  $p = 0.009$ ; **Figure 5B**), revealing PM functional connectivity ( $B = 2.601$ ,  $SE = 1.083$ ,  $t = 2.40$ ,  $p = 0.022$ ), and age ( $B = -0.008$ ,  $SE = 0.004$ ,  $t = -2.15$ ,  $p = 0.039$ ) were significant predictors of Spatial LDI. Clinical status was only a marginal predictor of Spatial LDI ( $B = -0.110$ ,  $SE = 0.054$ ,  $t = -2.03$ ,  $p = 0.051$ ). Second, we assessed the specificity of this relationship by conducting a multiple regression to test whether AT functional connectivity predicted Spatial LDI, covarying for age and clinical status. The overall model was statistically significant ( $r = 0.487$ ,  $F_{(3,32)} = 3.31$ ,  $p = 0.032$ ). However, neither AT functional connectivity ( $B = 2.982$ ,  $SE = 1.878$ ,  $t = 1.59$ ,  $p = 0.122$ ), nor age ( $B = -0.008$ ,  $SE = 0.004$ ,  $t = -1.92$ ,  $p = 0.063$ ) or clinical status ( $B = -0.114$ ,  $SE = 0.058$ ,  $t = -1.99$ ,  $p = 0.056$ ) were significant predictors of Spatial LDI. Overall, this suggests that spatial pattern separation is associated with PM, but not AT functional connectivity. **Figure 5C** shows the matrix of individual ROI-pair correlations. PM connectivity is shown in the blue square and AT connectivity is shown in the red square.

## Discussion

We have previously shown that object and spatial pattern separation engage parallel networks in the rhinal cortex, which are extensions of the PM and AT networks. Specifically, object pattern separation engaged the perirhinal and lateral entorhinal cortices (components of the AT network), while spatial pattern separation engaged the parahippocampal and medial entorhinal cortices (components of the PM network) (Reagh and Yassa, 2014). Recent fMRI studies have also demonstrated age-related deficits in object-related processing related to lateral entorhinal cortex hypoactivity (Berron et al., 2018; Reagh et al., 2018) and to dysfunction of the AT system (Maass et al., 2018). However, an important and open question is to understand how dysfunction of the PM network is linked to spatial pattern separation. Our results here address this question

by showing that spatial pattern separation is associated with functional connectivity of the larger PM network. Interestingly, we do not observe the same associations with AT network connectivity. Overall, these results suggest that spatial pattern separation is a sensitive measure of cognitive change in older adults that have higher levels of pathological aggregates (A $\beta$  and t-tau) and is associated with functional connectivity in the PM network, which is implicated in spatial memory processing.

Recent evidence has suggested that AD pathologies differentially target these networks, with A $\beta$  preferentially targeting the PM network and tau preferentially targeting the AT network (Maass et al., 2019). Several studies have also suggested that in the presence of neocortical A $\beta$  plaques, tau pathology in the temporal lobe further increases but also ‘spreads’ to posteromedial regions (Leal et al., 2018; Lockhart et al., 2017; Vemuri et al., 2017) where pathologies converge. Thus, an emerging view from recent studies suggest that amyloid potentiates the spread of tau into neocortical regions (Schwarz et al., 2016). These regional relationships could not be assessed directly here, since CSF measures do not offer insights into network-specific distributions of pathology, however, future work with longitudinal PET imaging can be used to further shed light on these relationships.

## **CHAPTER 4: Spatial pattern separation and Alzheimer’s disease pathology**

### **Introduction**

While previous studies have reported spatial pattern separation deficits in older adults, these studies have been limited in examining the relationship between spatial pattern separation and Alzheimer’s disease-related pathology. Previous studies have shown that regions involved in

spatial memory are early sites of A $\beta$  pathology and that A $\beta$  deposition is higher in PM regions than in AT regions (Koychev et al., 2020; Maass et al., 2019; Palmqvist et al., 2017). We hypothesized that amyloid pathology underlies spatial pattern separation performance deficits and alters in the functional connectivity of the PM network.

## Materials and Methods

### Participants

A total of 45 older adults between 61 and 91 years of age were included in this study. Forty-five older adults were recruited from the Alzheimer's Disease Research Center (ADRC) Longitudinal Cohort at the University of California, Irvine. Participants gave written informed consent in accordance with the Institutional Review Board of the University of California, Irvine, and were compensated for their participation. Demographic information about the participants is displayed in **Table 1**.

Participants were administered the Uniform Data Set (UDS-3) battery by a neuropsychologist in order to characterize the sample in accordance with the National Alzheimer's Coordinating Center (NACC) criteria (Weintraub et al., 2018). This is a standardized set of neuropsychological tests used by Alzheimer's Disease Centers across the United States. The battery includes the Montreal Cognitive Assessment (Nasreddine et al., 2005), Craft Story (Craft et al., 1996), Digit Span (Wechsler, 1987), Trail making Test Parts A and B (Reitan and Wolfson, 1985), and the Benson Complex Figure Test (Possin et al., 2011). For statistical comparison between groups, participants were dichotomized into cognitively normal (CN) or cognitively impaired (CI), which include Mild Cognitively Impaired (MCI) and Cognitively Impaired, Non-Demented (CIND) participants.

All participants were administered the spatial pattern separation task, Rey Auditory Verbal Learning Test (RAVLT), Mini-Mental State Exam (MMSE). Seven participants from the ADRC subsample were excluded from analysis due to confusion with the task instructions.

Cerebrospinal fluid (CSF) was obtained via lumbar puncture ( $n = 38$ ).

## Results

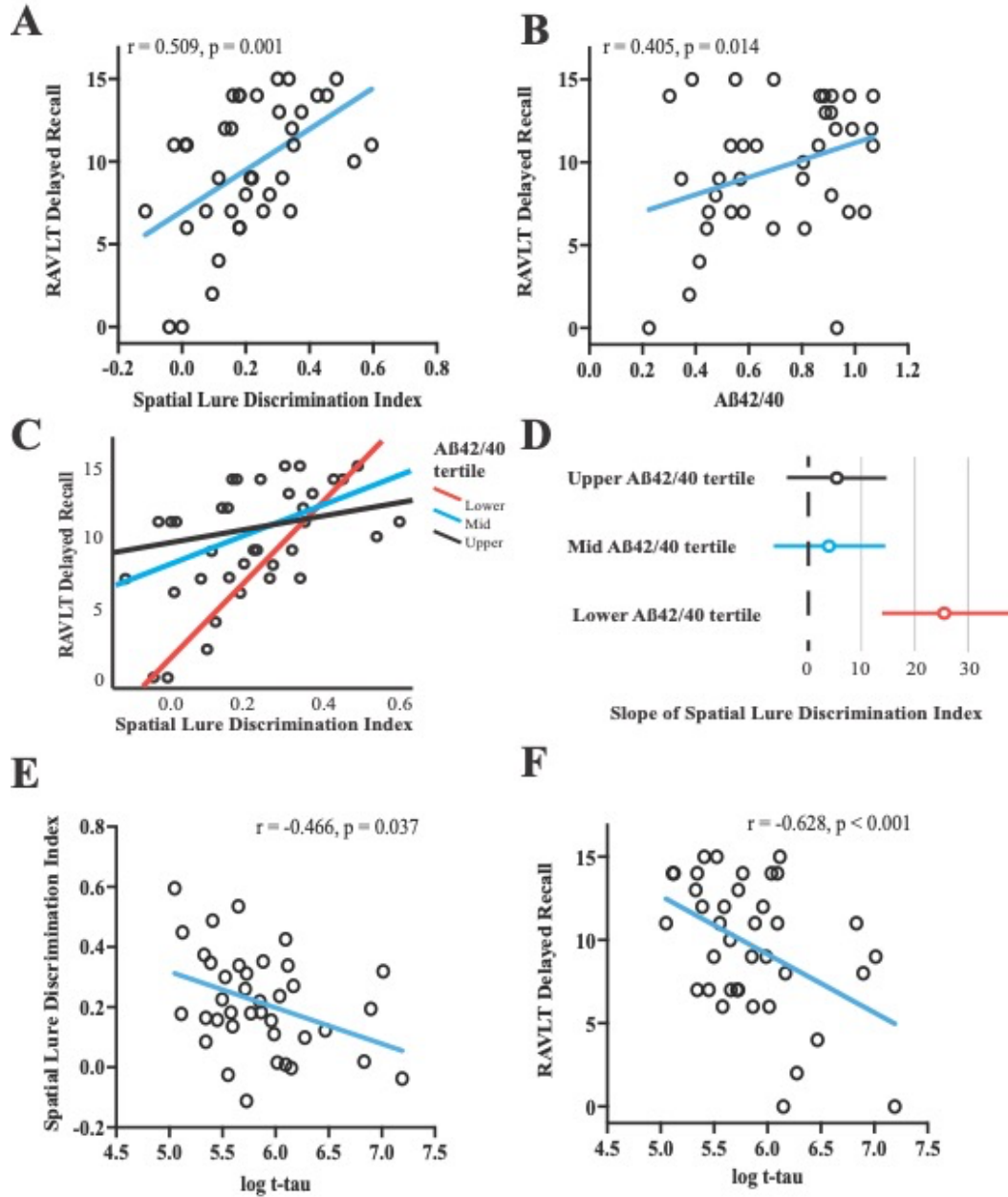
### Spatial pattern separation is associated with CSF pathology

A subset ( $n=38$ ) of our participants underwent CSF lumbar punctures, allowing us to assess the relationship between spatial pattern separation and AD pathological features. First, we confirmed that the previously identified behavioral relationship between task performance and RAVLT delayed recall was present in this subsample (Pearson  $r = 0.509$ ,  $p = 0.001$ ; **Figure 6A**). We considered three key CSF pathology measures, A $\beta$ 42/40 ratio, total tau (t-tau), and phospho-tau-181 (p-tau). Within our sample, A $\beta$ 42/40 ratio was correlated with t-tau (Pearson  $r = -0.475$ ,  $p = 0.003$ ), and p-tau (Pearson  $r = -0.560$ ,  $p < 0.001$ ). T-tau was also highly correlated with p-tau (Pearson  $r = 0.961$ ,  $p < 0.001$ ).

Adjusting for age, and clinical status, A $\beta$ 42/40 ratio was not directly correlated with Spatial LDI (partial  $r = 0.108$ ,  $p = 0.531$ ), but we observed a significant correlation between A $\beta$ 42/40 ratio and delayed recall scores (partial  $r = 0.405$ ,  $p = 0.014$ ; **Figure 6B**). We then examined the effect of A $\beta$ 42/40 as a potential moderator of the relationship between Spatial LDI and delayed recall using multiple linear regression with age and clinical status as covariates. The overall regression was statistically significant ( $r = 0.769$ ,  $F_{(5,32)} = 9.280$ ,  $p < 0.001$ ). This model revealed significant main effects of Spatial LDI ( $B = 28.715$ ,  $SE = 9.251$ ,  $t = 3.104$ ,  $p = 0.004$ ), A $\beta$ 42/40 ( $B = 12.082$ ,



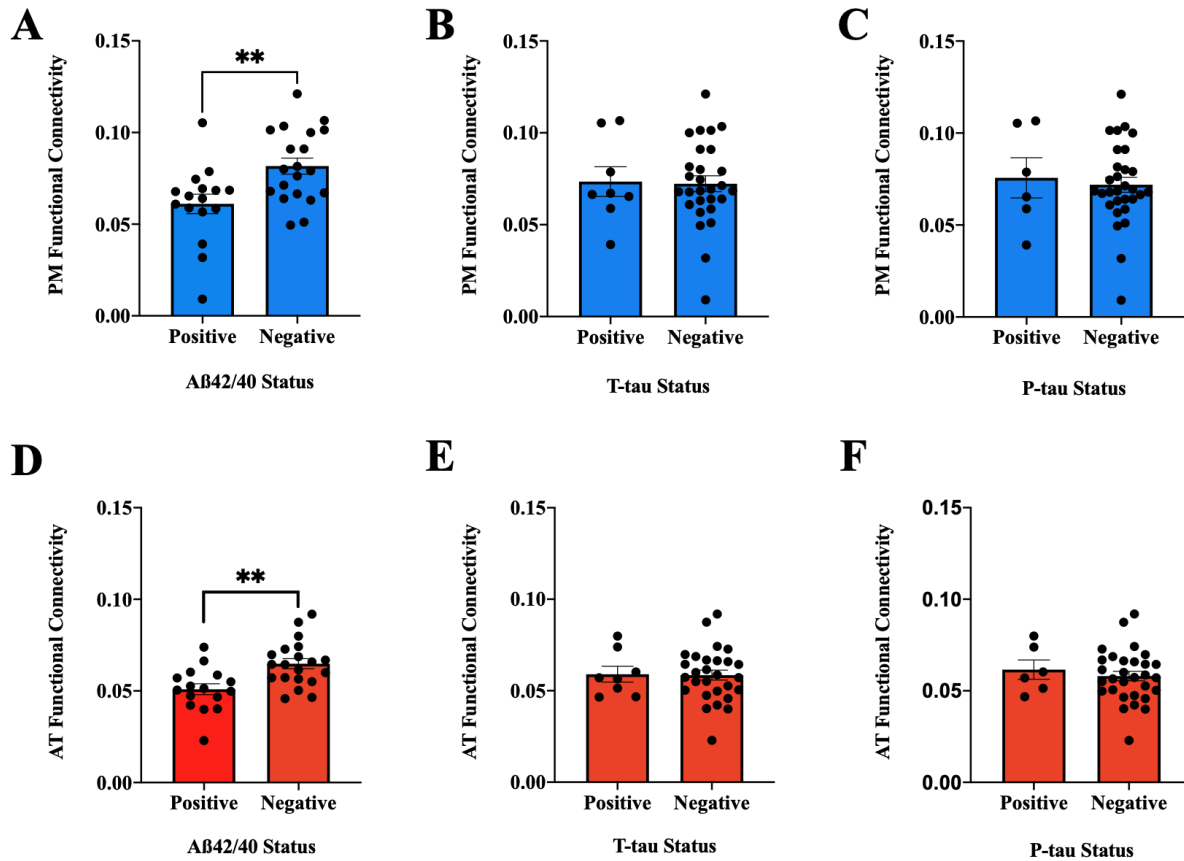
$SE = 3.547, t = 4.407, p = 0.002$ ), and age ( $B = -0.225, SE = 0.084, t = -2.684, p = 0.011$ ). The interaction between Spatial LDI and A $\beta$ 42/40 ratio was also significant ( $B = -27.842, SE = 11.803, t = -2.359, p = 0.025$ ). Clinical status was not a significant predictor of delayed recall ( $B = -2.023, SE = 1.199, t = -1.687, p = 0.101$ ). A simple slopes analysis for the relationship between Spatial LDI and delayed recall at upper, middle, and lower tertiles of A $\beta$ 42/40 shows the conditional effect by which A $\beta$ 42/40 moderates the relationship between Spatial LDI and RAVLT delayed recall (**Figure 6C**). Slopes and 95% confidence intervals for the relationship between Spatial LDI and delayed recall at upper, middle, and lower tertile of A $\beta$ 42/40 ratio levels show that the slope of Spatial LDI is significant only in the lower tertile ( $B = 25.60, SE = 5.85, t = 4.38, p < 0.001$ ), but not the upper ( $B = 5.36, SE = 4.76, t = 1.13, p = 0.27$ ), or middle tertiles ( $B = 3.99, SE = 5.20, t = 0.77, p = 0.45$ ; **Figure 6D**).



**Figure 6. Relationship between CSF biomarkers, spatial lure discrimination index (LDI), and RAVLT delayed recall.** (A) Higher Spatial Lure Discrimination Index (LDI) performance was related to better performance on the Rey Auditory Verbal Learning Test (RAVLT) delayed recall in the CSF subsample (Pearson  $r = 0.509$ ,  $p = 0.001$ ). (B) Lower  $A\beta_{42/40}$  is associated with worse performance on RAVLT Delayed Recall (partial  $r = 0.405$ ,  $p = 0.014$ ). (C, D) Slopes and 95% confidence intervals for relationship between Spatial LDI and RAVLT delayed recall at upper, middle, and lower tertiles of  $A\beta_{42/40}$  ratio levels. (E, F) Higher log-transformed levels of total tau (log-tau) were significantly related to worse performance on the Spatial LDI ( $r = -0.466$ ,  $p = 0.037$ ), and worse performance on the RAVLT Delayed Recall ( $r = -0.628$ ,  $p < 0.001$ ).

Next, we turned our attention to tau pathology measures. Since t-tau and p-tau levels were not normally distributed, we log-transformed them. First, we examined the relationship between log t-tau and Spatial LDI using multiple linear regression with age and clinical status as covariates. The overall model was significant (**Figure 6E**;  $r = 0.466$ ,  $F_{(3,34)} = 3.15$ ,  $p = 0.037$ ), revealing a significant main effect of log t-tau ( $B = -0.108$ ,  $SE = 0.053$ ,  $t = -2.045$ ,  $p = 0.049$ ). Age ( $B = -0.007$ ,  $SE = 0.004$ ,  $t = -1.619$ ,  $p = 0.115$ ) and clinical status ( $B = -0.037$ ,  $SE = 0.062$ ,  $t = -0.596$ ,  $p = 0.555$ ) were not significant predictors. Then, we examined the relationship between log t-tau and RAVLT delayed recall using multiple linear regression with age and clinical status as covariates. The overall model was significant (**Figure 6F**;  $r = 0.628$ ,  $F_{(3,34)} = 7.38$ ,  $p < 0.001$ ), revealing a significant main effect of log t-tau ( $B = -0.005$ ,  $SE = 0.002$ ,  $t = -2.11$ ,  $p = 0.042$ ), age ( $B = -0.200$ ,  $SE = 0.089$ ,  $t = -2.24$ ,  $p = 0.032$ ), and clinical status ( $B = -2.933$ ,  $SE = 1.373$ ,  $t = -2.14$ ,  $p = 0.040$ ).

We then repeated the same analyses for p-tau. We first examined the relationship between log p-tau and Spatial LDI using multiple linear regression with age and clinical status as covariates. The overall regression showed that log p-tau was associated with Spatial LDI ( $r = 0.386$ ,  $F_{(3,34)} = 1.98$ ,  $p = 0.135$ ). Log p-tau ( $B = -0.053$ ,  $SE = 0.051$ ,  $t = -1.045$ ,  $p = 0.304$ ), age ( $B = -0.006$ ,  $SE = 0.004$ ,  $t = -1.475$ ,  $p = 0.150$ ), and clinical status ( $B = -0.056$ ,  $SE = 0.067$ ,  $t = -0.842$ ,  $p = 0.406$ ) were not significant predictors. Then, we examined the relationship between log p-tau and RAVLT delayed recall using multiple linear regression with age and clinical status as covariates. The overall regression showed that log p-tau was associated with delayed recall ( $r = 0.628$ ,  $F_{(3,34)} = 7.83$ ,  $p < 0.001$ ), revealing a significant main effect of log p-tau ( $B = -0.005$ ,  $SE = 0.002$ ,  $t = -2.11$ ,  $p = 0.042$ ), age ( $B = -0.200$ ,  $SE = 0.089$ ,  $t = -2.24$ ,  $p = 0.032$ ), and clinical status ( $B = -2.933$ ,  $SE = 1.373$ ,  $t = -2.14$ ,  $p = 0.040$ ).



**Figure 7. CSF biomarker group differences in functional connectivity.** (A,D) A two-tailed two sample t-test showed that the Aβ positive group had lower PM functional connectivity than the Aβ negative group ( $t_{(34)} = 3.014, p = 0.005$ ) and the Aβ positive group had lower AT functional connectivity than the Aβ negative group ( $t_{(34)} = 3.418, p = 0.002$ ). (B, C, E, F) No differences in PM or AT functional connectivity between positive and negative groups of groups of t-tau or p-tau.

We then examined the relationship between CSF pathology markers and PMAT functional connectivity. We dichotomized the sample based on published cutoffs for Aβ42/40, t-tau and p-tau and ran two-tailed two-sample t-tests to determine whether there are group differences in PMAT functional connectivity. We found that the Aβ positive group had lower PM functional connectivity ( $t_{(34)} = 3.014, p = 0.005$ ; **Figure 7A**) and lower AT functional connectivity ( $t_{(34)} = 3.418, p = 0.002$ ; **Figure 6D**) than the Aβ negative group. No significant t-tau or p-tau group differences in PM or AT functional connectivity were noted (**Figure 7B, C, E, F**).

## Discussion

Neuropathologically, the presence of protein aggregates comprising of beta amyloid (i.e. neuritic plaques) and hyperphosphorylated tau (i.e. neurofibrillary tangles) are hallmark features of AD (Jack et al., 2018; McKhann et al., 2011). In AD, abnormal accumulation of amyloid and tau proteins in the brain is thought to begin 10–20 years before clinical symptom onset (Bateman et al., 2012; Hof et al., 1996; Perl, 2010). Currently, the predominant modalities for assessments of these pathologies are cerebrospinal fluid (CSF) and positron emission tomography (PET). CSF A $\beta$ 42 becomes abnormal in the earliest stages of AD before amyloid PET detection and before neurodegeneration starts (Palmqvist et al., 2016). Additionally, the concordance between CSF A $\beta$ 42 and amyloid PET imaging is high, but not perfect (Hansson et al., 2018; Schindler et al., 2018; Toledo et al., 2015). The ratio of A $\beta$ 42/40 has been shown to have better agreement with amyloid PET imaging compared to levels of A $\beta$ 42 alone (Alcolea et al., 2019; Janelidze et al., 2016, 2017; Lewczuk et al., 2017; Schindler et al., 2018). Previous studies have shown that CSF A $\beta$ 42/40 is a sensitive measure of A $\beta$  plaques, CSF t-tau is a sensitive measure of neurodegeneration, and CSF p-tau is a biomarker associated with both the phosphorylation state of tau and neurofibrillary tangle formation (Blennow et al., 2010; Jack et al., 2018; Strozyk et al., 2003). It is important to also note that while t-tau and p-tau levels in CSF are thought to vary proportionately with brain pathology levels, A $\beta$  measures in CSF are thought to vary inversely with brain pathology (i.e., the higher the CSF A $\beta$ , the lower the brain A $\beta$ ; (Tapiola et al., 2009). Our findings support the notion that while CSF measures have often been dichotomized into “positive” and “negative” based on reliable cutoffs (Jack et al., 2018), pathological burden can be conceptualized on a continuum with a progressively increasing risk of cognitive decline. Here

we show that RAVLT delayed recall is associated with A $\beta$ 42/40, t-tau, and p-tau. However, Spatial LDI is only directly associated with t-tau, but not A $\beta$ 42/40 or p-tau. Importantly, we showed that the relationship between Spatial LDI and RAVLT delayed recall is conditional upon the level of  $\beta$ -amyloid burden. This suggests Spatial LDI may be a more specific marker to the concurrent pathologies of AD, as its sensitivity to tau pathology is increased in the presence of lower levels of CSF A $\beta$  (i.e. higher levels of brain A $\beta$ ).

The relationships among CSF pathology, functional connectivity in specific neural systems, and cognition may hold the key to better understanding of how early AD evolves in the aging brain. Considerable evidence suggests that pathological processes involving amyloid and tau affect brain network function, which in turn may affect cognitive performance (Huijbers et al., 2019; Marks et al., 2017; Mormino et al., 2012; Sperling et al., 2009). Converging evidence has demonstrated that two distinct cortical pathways converge in the hippocampus: the anterior-temporal (AT) network and the posteromedial (PM) network (Ranganath and Ritchey, 2012). While the AT network has been associated with object memory, the PM network has been associated with spatial and contextual memory (Ritchey et al., 2015). The involvement of the PM system in spatial processing and spatial memory has been reliably shown in past studies. For example, the PM network's retrosplenial cortex has been associated with spatial updating and orienting (Burles et al., 2017), as well as spatial navigation and path integration (Sherrill et al., 2013).

This study has a few limitations to consider. We cannot exclude the possibility that our results reflect sources of amyloid or tau hypothesized to be non-AD related, such as primary age-related tauopathy (Crary et al., 2014; Duyckaerts et al., 2015). As CSF measures of AD pathology are

not regionally specific, we cannot determine with certainty whether our findings are the result of local or regional effects of AD pathology.

## **CHAPTER 5: Spatial pattern separation and cognitive decline**

### **Introduction**

Given the clinical relevance of spatial memory deficits in early AD as well as the vulnerability of the PM network to amyloid pathology, we asked the question: Could a mechanistically validated spatial memory task be used as an early diagnostic or predictor of cognitive decline? To address this question, we tested a sample of nondemented older adults that includes cognitively normal and cognitively impaired individuals. We used a memory task tailored to probe spatial pattern separation, a high-precision form of object-location association and hypothesized that performance on the task would predict longitudinal cognitive decline.

### **Materials and Methods**

#### **Participants**

A total sample of 45 older adults between 61 and 91 years of age were included in this study. Forty-five older adults were recruited from the Alzheimer's Disease Research Center (ADRC) Longitudinal Cohort at the University of California, Irvine. Participants gave written informed consent in accordance with the Institutional Review Board of the University of California, Irvine, and were compensated for their participation.

Participants were administered the Uniform Data Set (UDS-3) battery by a neuropsychologist in order to characterize the sample in accordance with the National Alzheimer's Coordinating Center (NACC) criteria (Weintraub et al., 2018). This is a standardized set of neuropsychological

tests used by Alzheimer's Disease Centers across the United States. The battery includes the Montreal Cognitive Assessment (Nasreddine et al., 2005). Craft Story (Craft et al., 1996), Digit Span (Wechsler, 1987), Trail making Test Parts A and B (Reitan and Wolfson, 1985), and the Benson Complex Figure Test (Possin et al., 2011). For statistical comparison between groups, participants were dichotomized into cognitively normal (CN) or cognitively impaired (CI), which include Mild Cognitively Impaired (MCI) and Cognitively Impaired, Non-Demented (CIND) participants.

All participants were administered the spatial pattern separation task, Rey Auditory Verbal Learning Test (RAVLT), Mini-Mental State Exam (MMSE). Seven participants from the ADRC subsample were excluded from analysis due to confusion with the task instructions. Longitudinal MMSE scores were obtained as part of a larger battery of tests used at an annual evaluation (n=37).

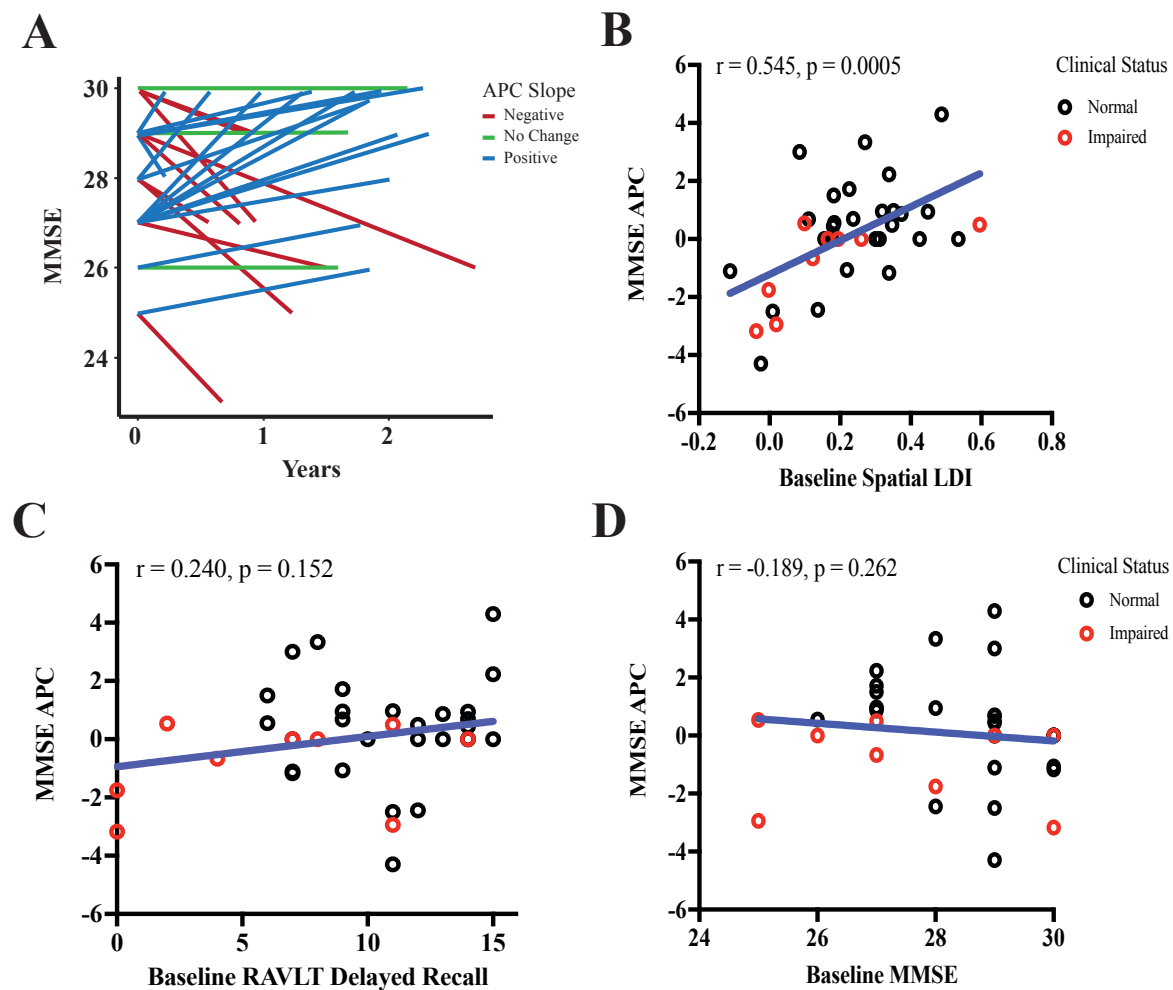
## Results

### **Spatial pattern separation predicts annualized decline in MMSE scores**

We assessed the predictive validity of spatial pattern separation by testing whether task performance predicted longitudinal cognitive decline. Demographic information about the participants is displayed in **Table 1**. Using the Mini-Mental State Exam (MMSE) as the key cognitive outcome of interest, we plotted the trend in individual subject scores over time relative to baseline MMSE score (**Figure 8A**). We calculated MMSE annualized percent change (MMSE APC) as the difference between the last MMSE score and the baseline MMSE score divided by time in between (in years). We found that baseline Spatial LDI was correlated with MMSE APC (Pearson  $r = 0.545$ ,  $p = 0.0005$ ; **Figure 8B**), but baseline RAVLT delayed recall scores (Pearson  $r = 0.240$ ,  $p = 0.152$ ; **Figure 8C**), and baseline MMSE scores (Pearson  $r = -0.189$ ,  $p = 0.262$ ;



Figure 7D) were not correlated with MMSE APC. We then assessed the relationship between Spatial LDI and MMSE APC using multiple regression with age, and clinical status as covariates. The overall model was significant ( $r = 0.580$ ;  $F_{(3,33)} = 5.48$ ,  $p = 0.003$ ), demonstrating that baseline Spatial LDI remained significantly associated with MMSE APC ( $B = 5.594$ ,  $SE = 1.595$ ,  $t = 3.508$ ,  $p = 0.001$ ). Age ( $B = 0.024$ ,  $SE = 0.041$ ,  $t = 0.583$ ,  $p = 0.564$ ), and clinical status ( $B = 0.752$ ,  $SE = 0.588$ ,  $t = -1.279$ ,  $p = 0.210$ ) were not significant predictors.



**Figure 8. Spatial discrimination predicts annualized percent change of MMSE scores (MMSE APC).** (A) MMSE distribution for each participant over time, relative to baseline MMSE score, where blue indicates positive changes, green indicates no change, and red represents negative changes. (B) Baseline Spatial LDI was significantly associated with MMSE APC (Pearson  $r = 0.545$ ;  $p = 0.0005$ ). (C) Baseline RAVLT Delayed Recall scores were not associated with MMSE APC (Pearson  $r = 0.240$ ,  $p = 0.152$ ). (D) Baseline MMSE scores were not associated with MMSE APC (Pearson  $r = -0.189$ ,  $p = 0.262$ ).

## **Discussion**

Our results indicate that spatial pattern separation performance may be an informative measure with respect to the trajectory of cognitive decline. Here we demonstrate a relationship between spatial pattern separation performance at baseline and cognitive decline as assessed by decreases in MMSE scores over a 1–2-year period. These relationships were not present with baseline RAVLT delayed recall scores, which is a standard neuropsychological tool for evaluating memory function and decline. This speaks to the predictive validity of the task and the promise it holds for potential use in clinical trials. Furthermore, our participant sample consisted of mostly white, highly educated individuals, thus limiting the generalizability of results. Future work should attempt to reproduce these findings in community-based samples drawn from ethnically diverse populations.

## **CHAPTER 6: Synthesis and Future Directions**

### **General Summary**

The goal of this dissertation was to investigate spatial memory networks in aging and Alzheimer’s disease. To investigate the neurobiological mechanisms involved, a series of experiments establish relationships between spatial pattern separation and the functional connectivity of spatial memory networks, AD pathology, and clinical measures of cognitive impairment and decline. Overall, we find that applying a pattern separation framework to the changes involved in spatial memory offers a potential mechanistic account for how spatial memory is affected in the context of Alzheimer’s disease. For the next sections, I will summarize the results from the experiments presented and discuss their impact and relevance more broadly.

## **Vulnerability of the PM network**

These findings suggest that older adults may have distinct changes occurring in the PMAT networks that are dependent on the content of the memory being recalled. Previous work reports that the spatial pattern separation task to probe spatial memory with a high level of fidelity in older adults (Reagh and Yassa, 2014; Reagh et al., 2016, 2018). The task, which is modeled after work in rodents, utilizes simple metric displacement to evaluate whether individuals can discriminate, across a delay, whether objects moved from their original locations. In this way, it is analogous to an object-location memory task but with distance varied being an operational metric to specifically test for spatial pattern separation deficits. Previous studies demonstrated that spatial pattern separation task performance in healthy older adults was not statistically different than that of young adults, despite deficits in the object domain (Reagh et al., 2018).

In this study of older adults with a range of cognitive performance (nondemented, but clinically impaired and unimpaired), we look beyond the hippocampus to formulate a mechanistic account for spatial pattern separation performance and use this to understand spatial memory deficits and their relationship to Alzheimer's pathology. These findings suggest that spatial memory deficits may arise due to changes in the functional connectivity of the PM network. While pattern separation is a computational process that is hypothesized to be supported by the hippocampus, specifically the DG, some studies have implicated regions beyond the hippocampus that are related to behavioral deficits in aging (Berron et al., 2018; Reagh et al., 2018). These results extend on this idea by demonstrating that the PM network, a network that is involved in processing of spatial information, helps support pattern separation. Here, we highlight that functional connectivity across regions in the PM network is strongly associated with out-of-scanner performance on the task, consistent with our hypothesis.

Here we find that the relationship between spatial pattern separation performance and verbal list recall (a standard test of hippocampal integrity) is contingent upon CSF levels of A $\beta$ 42/40, a hallmark pathology of Alzheimer's disease. Spatial pattern separation performance was also inversely correlated with CSF tau levels, consistent with AD-related impairment. These findings would suggest that spatial memory is affected by Alzheimer's disease pathology. However, it is unclear whether tau and A $\beta$  deposition are driven by an upstream regulator.

### **Spatial memory dysfunction and cognitive decline**

Determining how PMAT networks are altered in aging alone versus Alzheimer's disease may help in developing therapeutic targets to alleviate symptoms and potentially shift the PM network back to a normal state. In a recent randomized clinical trial with antiseizure drug levetiracetam (LEV), the study shows improved performance on spatial memory and executive function tasks in patients with Alzheimer's disease with subclinical epileptiform activity, which account for an estimated 60 percent of cases (Vossel et al., 2021). The study concludes that additional neuropsychological measures of network hyperexcitability are needed to determine the effects of antiseizure drugs on network dysfunction in patients with AD.

Our results show that performance on the spatial pattern separation task was predictive of longitudinal cognitive decline over a 1-2 year period (measured via the Mini-Mental State Exam). This would suggest that the spatial pattern separation task is a computerized assessment that can potentially serve as a "digital biomarker" by probing subtle features of cognitive decline during the earliest stages of the disease. While the task is a highly controlled version of what one would experience, and it is not a naturalistic environment, we would encounter similar experiences in our everyday lives. For example, older adults may have a difficult time

remembering where they parked their car or where they put their keys. These experiences would have overlapping representations since they contain information that is highly similar.

Overall, our results strongly suggest that spatial pattern separation may be a novel candidate for a digital biomarker that is mechanistically validated and predictive of cognitive decline.

## **Future Directions**

### **Retroactive interference**

While previous studies have reported relationships between pattern separation tasks and word list delayed recall (Reagh et al., 2014; Roberts et al., 2014), our studies show that retroactive interference is potentially driving this relationship. Future studies should examine retroactive interference as an early indicator of memory dysfunction.

### **Vascular and immune contributions**

Our results show that dysfunction of the PM network and Alzheimer's disease pathology might underlie deficits in spatial pattern separation. However, it is unclear how network dysfunction and pathological changes are related. Novel candidates for elucidating whether upstream regulators are mediating or moderating this effect include inflammatory and neurovascular biomarkers. Future work should examine how inflammatory, and vascular indicators interact with established indicators such as amyloid and tau.

### **Regionally specific effects of AD pathology**

One of the limitations in these experiments is that CSF biomarkers does not allow us to examine network specific burden. *In vivo* detection of amyloid pathology is possible with PET utilizing

amyloid-specific radiotracers. These tracers are Food and Drug Administration (FDA) approved and routinely being used to detect amyloid in the brains of patients with mild cognitive impairment (MCI) and AD. Numerous small-molecule PET tracers suitable for measuring A $\beta$  in the living human brain have been developed over the past decade. Three of those tracers have been approved to interrogate brain A $\beta$  plaque burden in suspected AD patients. One of those tracers is [ $^{18}\text{F}$ ]AV-45 Florbetapir to screen for amyloid positivity.

PET tracers designed to interrogate NFT burden are under development as a complement to PET assessment of A $\beta$ -burden at a pre-symptomatic stage of disease. In addition, a quantifiable biomarker of *in vivo* NFT pathology burden is of great interest as a tool to interrogate disease status with direct relevance to target pathology and clinical outcomes to support clinical evaluation of novel therapies for AD or other tauopathies. One of the limitations in the development of NFT PET tracers preventing the smooth translation of these tracers into clinical imaging studies is that NFT pathology and pattern of spread found in AD brain cannot be replicated in an animal model of disease. This inability to image pathological NFT burden using PET in animal models removes a valuable screening tool for tracer development and hampers the ability to translate imaging techniques directly from preclinical to clinical evaluation. Consequently, *in vivo* preclinical imaging signals are not possible and human studies are required to validate the utility of tau tracers. Several putative NFT imaging agents have been undergoing testing including [ $^{18}\text{F}$ ]T-807 (Avid/Lilly), GTP-1 (Genentech), and several compounds developed by Tohoku university, such as [ $^{18}\text{F}$ ]THK-5117 or [ $^{18}\text{F}$ ]THK-5351 (GE Healthcare). Of these, [ $^{18}\text{F}$ ]T-807 is the most extensively characterized having been studied in several hundred subjects. These PET tracers have all been generally well tolerated in early clinical studies (Villemagne et al., 2015; Xia et al., 2013). These ligands show increased tracer uptake and retention in brain regions generally consistent with

known distribution of NFT pathology in AD brains (i.e. the MTL). Furthermore, [<sup>18</sup>F]T-807 PET imaging has also demonstrated increased uptake and signal retention in patients with prodromal AD (i.e., mild cognitive impairment) (Villemagne et al., 2015). It has also demonstrated its capacity to detect Braak-stage specific tau binding (Schöll et al., 2015), as well as specificity of regional retention in the MTL to memory and hippocampal/entorhinal volume and cortical thickness.

The new [<sup>18</sup>F]MK-6240 tracer (Merck) showed impressive results in early testing (Hostetler et al., 2016). Its binding pattern *in vitro* was consistent with the distribution of phosphorylated tau in human AD brain slices. It bound with high affinity to AD brain homogenates rich in NFTs but bound poorly to amyloid-plaque rich, NFT-poor AD brain homogenates. PET studies in monkeys showed rapid and homogeneous distribution, indicating favorable tracer kinetics. Importantly, MK-6240 does not appear to suffer from the off-target binding issues (Hostetler et al., 2016).

### **Community-based samples of ethnically diverse populations**

Currently in the United States, Latinos or Hispanics are the second largest racial or ethnic group accounting for 18.5% of the population, and Black or African Americans are the third largest racial or ethnic group accounting for 13.4% of the population (US Census Bureau, 2020).

Latinos or Hispanics and Black or African Americans are also disproportionately affected by Alzheimer's disease-related dementia (ADRD; Matthews et al., 2019; Mayeda et al., 2016; Tang et al., 2001). However, they are both underrepresented in observational and clinical studies, which limits the generalizability of many findings (McGarry and McColley, 2016).

Latinos or Hispanics, the largest and fastest growing minority in the United States, are an admixed group that includes White, Native American, and African ancestry (Hanis et al., 1991).

By 2060, the number of Latinos age 65 and older is expected to nearly quadruple, and Latinos are projected to have the largest increase in ADRD cases of any racial/ethnic group in the United States (Matthews et al., 2019). In the United States, the Food and Drug Administration (FDA) recently approved Aduhelm (aducanumab) for the treatment of Alzheimer's disease. Two double-blind, randomized, placebo-controlled dose-ranging studies were conducted: EMERGE and ENGAGE. However, in the EMERGE drug trial, out of 1638 participants, 4.1% were Latino or Hispanic, 0.7% were Black or African American, and 0.1% were American Indian or Alaskan Native (Biogen, 2021a). In the ENGAGE drug trial, out of 1647 participants, 2.2% were Latino or Hispanic, and 0.5% were Black or African American (Biogen, 2021b). Furthermore, the most common adverse events of the Aduhelm studies were due to cerebrovascular complications such as microhemorrhages and Amyloid-Related Imaging Abnormalities – Edema (ARIA-E). This may be of concern for Latinos since Latinos also face a high prevalence of cerebrovascular disease and higher prevalence of mixed pathologies (Filshtein et al., 2019). Risk factors that may contribute to the higher incidence of cerebrovascular disease include a higher prevalence of diabetes, cardiovascular disease, high blood pressure, obesity, and sleep apnea (Redline et al., 2014).

In California, Latinos or Hispanics are the largest racial or ethnic group accounting for 39.4% of the population, and in Orange County they are the largest minority accounting for 34.1% of the population (US Census Bureau, 2020). One of the limitations in our study is that the lack of racial and ethnic diversity in our sample, consisting of predominantly white individuals, thus limiting the generalizability of results. Future work should attempt to reproduce these findings in community-based samples drawn from ethnically diverse populations. One advantage with the spatial pattern separation task is that whereas auditory verbal learning tasks are dependent on



language, the spatial pattern separation task is not, potentially allowing for it to be easily adaptable.

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(2020). 2020 Alzheimer’s disease facts and figures.

## APPENDIX A

### **CSF biomarkers of Alzheimer's pathology are highly concordant with amyloid-PET in cognitively normal older adults**

#### **Introduction**

The presence of protein aggregates comprising of amyloid- $\beta$  (A $\beta$ ; i.e. amyloid plaques) and hyperphosphorylated tau (i.e. neurofibrillary tangles) are hallmark features of Alzheimer's disease (AD) (Blennow et al., 2010; Jack et al., 2018; McKhann et al., 2011; Strozyk et al., 2003). Abnormal accumulation of A $\beta$  and tau proteins in the brain begins 10–20 years before clinical symptom onset (Jack Jr et al., 2010), making biomarkers of these proteins key components of research criteria for preclinical AD and critical for inclusion criteria and outcome measures of clinical trials (Bateman et al., 2012; Dubois et al., 2014; Hof et al., 1996; Perl, 2010).

Currently, the predominant and best-established modalities for assessing A $\beta$  and tau pathologies *in vivo* are measuring concentrations within cerebrospinal fluid (CSF) and visualizing deposition with positron emission tomography (PET). While PET has the advantage of providing information about not only the quantity but the spatial distribution of these proteins, CSF can be more easily acquired and therefore may have more utility for early detection of pathology. However, validating CSF measures against gold-standard PET is critical to fully understanding their utility due to variations in collection and processing methods across studies.

Recent advances in automated assays to quantify AD biomarkers within CSF overcome this variation due to a consistent analytical process. Recent studies comparing the automated

Fujirebio Lumipulse assay with the more widely used INNOTEST ELISAs have shown good concordance between the two platforms, with the Lumipulse demonstrating reduced intra- and inter-assay variability (Bayart et al., 2019). While few studies have assessed the agreement of amyloid-PET and CSF biomarkers on the Lumipulse assay, they have consistently shown that both ratios of A $\beta$  pathology (i.e. A $\beta$ 42/40) and overall Alzheimer's pathology (i.e. ptau/A $\beta$ 42) have high agreement with amyloid-PET in classifying amyloid-positivity (Alcolea et al., 2019; Campbell et al., 2021; Willems et al., 2021). However, participants in these studies have mostly been clinical or mixed memory cohorts, with a limited number of cognitively normal participants, which makes the utility of the Lumipulse assay and its published thresholds for amyloid-positivity in preclinical samples undetermined, although critical for research on the development of AD.

In the current study, we validate CSF AD biomarkers derived from the Lumipulse assay against amyloid-PET in an entirely cognitively normal sample. We examined the CSF biomarkers of A $\beta$ <sub>1-40</sub>, A $\beta$ <sub>1-42</sub>, phospho-tau (p-tau<sub>181</sub>), total tau (t-tau), as well as the A $\beta$ 42/40 and p-tau/A $\beta$ 42 ratios, to test a range of pathological markers against the widely used <sup>18</sup>F-Florbetapir PET. In this cognitively normal sample, our aims were to (1) determine the strength of continuous associations between CSF biomarkers and levels of amyloid-PET, (2) test the concordance of previously published thresholds for “positive” CSF biomarkers (i.e. A $\beta$ 42/40 and ptau/A $\beta$ 42) derived from a predominantly clinical sample (Alcolea et al. 2019) with A $\beta$  -PET positivity; and (3) determine which CSF biomarkers are most predictive of A $\beta$ -PET classification.

## Participants

Thirty-two (N = 32) cognitively normal (Clinical Dementia Rating [CDR] = 0) older adults between 64 and 86 years of age (24 F, mean = 73.5 years, SD = 4.72 years) were recruited from the Alzheimer's Disease Research Center (ADRC) Longitudinal Cohort at the University of California, Irvine. Demographic information about the participants is displayed in **Table A1**.

Participants gave written informed consent in accordance with the Institutional Review Board of the University of California, Irvine, and were compensated for their participation.

Demographics	
Sample Size	32
Age (years)	73.5 (4.72)
Sex	24F (75%)
Education (years)	16.4 (2.42)
MMSE (points)	28.2 (1.59)
APOE Status	
e4 +	12 (38.7%)
e4 -	19 (61.3%)
Missing	1
A $\beta$ 42 (pg/mL)	616 (298)
t-tau (pg/mL)	307 (128.00)
p-tau (pg/mL)	42.4 (20.10)
A $\beta$ 42/40	0.069 (0.23)
p-tau/A $\beta$ 42	0.098 (0.11)
FBP Mean SUVR	1.14 (0.18)
Time between CSF-PET (years)	0.92 (0.82)

**Table A1.** Demographics and summary measures of the cognitively normal older adult cohort. Data represents mean (standard deviation) or N (%). MMSE, Mini Mental State Exam; APOE, Apolipoprotein E; t-tau, total tau; p-tau, phosphorylated tau<sub>181</sub>; FBP, <sup>18</sup>F-Florbetapir PET; SUVR, standardized uptake value ratio.

### **CSF Acquisition and Processing**

Cerebrospinal fluid (CSF) was obtained from participants via lumbar puncture, performed with standard clinical research methods in aseptic fashion by a board-certified neurologist. The CSF was collected in a 15mL Falcon tube, placed on ice until processed (within 2 hours), aliquoted into 250 microliter volumes and stored at -80 degrees Celsius until use. CSF was always collected during a separate session from PET imaging visit with an average time interval of 0.96 years.

A $\beta$ <sub>1-42</sub>, A $\beta$ <sub>1-40</sub>, phosphorylated tau<sub>181</sub> (p-tau), and total tau (t-tau) were quantified in human CSF on the Lumipulse G 1200 automated platform using a chemiluminescent enzyme immunoassay (CLEIA) by the UCSD Shirley-Marcos ADRC Biomarker Core.

### **PET Acquisition and Processing**

All participants in the current study received positron emission tomography (PET) with the <sup>18</sup>F-Florbetapir (FBP) tracer to quantify A $\beta$ . PET was performed on an ECAT high Resolution Research Tomograph (HRRT, CTI/Siemens, Knoxville, TN, USA). Ten mCi of tracer was injected, and four five-minute PET scan frames were collected from 50-70 min post-injection. Reconstruction was performed using 3D ordinary Poisson ordered subset expectation maximization with attenuation correction, and 4mm Gaussian smoothing. SUVR images were coregistered to the T1 image and normalized by a whole cerebellum reference region. Additional smoothing using a 6mm Gaussian kernel was then applied to achieve an effective resolution of

8mm<sup>3</sup>. The mean SUVR of a previously validated cortical composite region (FreeSurfer ROIs including frontal, cingulate, parietal, and temporal regions; see (Alcolea et al., 2019; Campbell et al., 2021; Willemsse et al., 2021) was quantified, and used to determine FBP positivity using a threshold of >1.11 SUVR.

### **Structural MRI**

All participants received a structural MRI on a 3T Prisma scanner (Siemens Medical System) with a 32-channel head coil. A whole-brain high resolution T1-weighted volumetric magnetization prepared rapid gradient echo image (MPRAGE) was acquired (TR/TE/TI = 2300/2.38/902 ms, flip angle = 8°, resolution = 0.8mm isotropic, 240 slices acquired sagittally). Structural MRIs were used for PET coregistration and were processed through FreeSurfer v.6.0 to obtain native-space regions of interest for FBP quantification.

### **Statistical Analysis**

Bivariate correlations were used to examine the relationship between CSF biomarkers and FBP mean SUVR, covarying for the time between PET and CSF acquisition. Correlation plots were generated using GraphPad Prism (v.9.2.0).

Receiver operator characteristics (ROC) were performed using random forest models with A $\beta$ -PET status as the outcome and CSF biomarkers status as predictors. CSF cutoffs were based on Alcolea et al. (2019), with a cutoff of 0.062 for A $\beta$ 42/40, and 0.068 for p-tau/A $\beta$ 42 (Alcolea et al., 2019). We compared false positive rate with true positive rate to generate the area under the ROC curve (AUC) for each ratio.

We investigated the most relevant features associated with A $\beta$ -PET positivity using random forest feature selection importance rates. The Gini impurity importance indicates how



often a particular feature was selected for a split, and how large its overall discriminative value was to the classification. The top importance features are the ones whose Gini node purity is higher, because its absence shows the largest change in the prediction.

We used `cutpointr`, a statistical software for the selection of optimal cutoffs implemented in R statistical software (version 3.6.3). CSF measures were compared to A $\beta$ -PET positivity with ROC, and cutoffs showing the highest Youden index were selected. We then compared specificity with sensitivity to generate the area under the ROC curve (AUC) for each ratio.

## **Demographics**

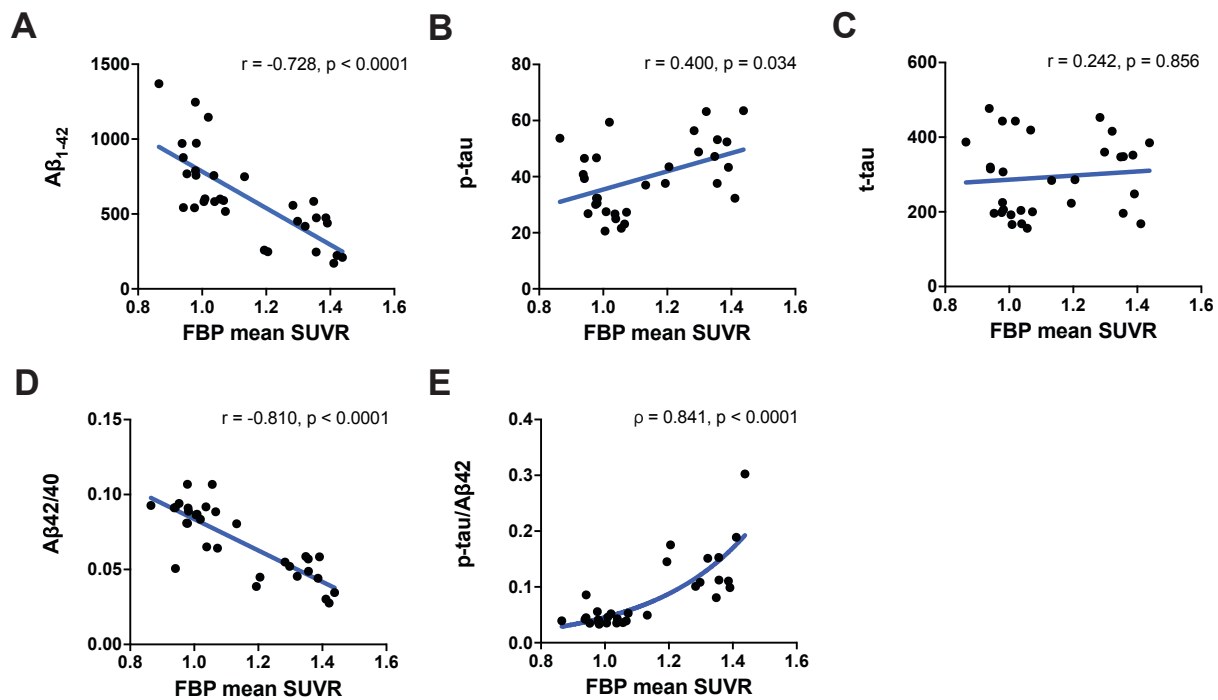
A total of 32 participants received both CSF and PET measures of A $\beta$  and were included in the present analysis. Full demographic information of the sample is presented in **Table A1**.

Participants were an average age of 73.5 years old, were predominantly female (75%), and received CSF and PET measurements within an average of 0.92 years. One participant had 5.75 years between CSF and PET (classified as positive on both measurements) – all analysis were conducted with and without this participant, although results remained consistent regardless of inclusion. One participant's p-tau and t-tau levels were a significant outlier (>2 SD of sample mean); this data point was removed from analyses involving these measures.

## **Associations between CSF and PET Measures**

First, we examined the relationship between mean FBP SUVR and CSF measures of AD pathology in our cognitively normal sample. There was a significant correlation between FBP SUVR and both A $\beta$ 42 ( $r = -0.728$ ,  $p < 0.001$ ; **Fig A1A**) and p-tau ( $r = 0.40$ ,  $p = 0.034$ ; **Fig A1B**), but not t-tau ( $r = 0.24$ ,  $p = 0.86$ ; **Fig A1C**). Additionally, mean FBP SUVR was associated with the A $\beta$ 42/40 ratio ( $r = -0.81$ ,  $p < 0.001$ ; **Fig A1D**), indicating that FBP has a strong relationship with

AD-specific A $\beta$  pathology. Finally, there was a strong association between FBP and p-tau/A $\beta$ 42, a ratio representing total levels of AD-related pathology, which was strongest when using a curvilinear model (curvilinear fit:  $\rho=0.84$ ,  $p<0.001$ ; linear fit:  $r = 0.65$ ;  $p<0.001$ ; **Fig A1E**). All associations remained significant and of similar correlational values when removing the one participant with 5.75 years between PET and CSF.



**Figure A1. CSF biomarkers are highly correlated with A $\beta$ -PET in cognitively normal older adults.** Increased  $^{18}\text{F}$ -Florbetapir (FBP) mean SUVR was significantly correlated with decreased CSF A $\beta_{1-42}$ , indicating more A $\beta$  (A) and increased p-tau, indicating more phosphorylated tau $_{181}$ ; (B). There was no association between FBP Mean SUVR and total tau (t-tau) (C). FBP mean SUVR was also significantly associated with decreased A $\beta$ 42/40 ratio, indicating more A $\beta$  specific to Alzheimer’s disease (D), and increased p-tau/A $\beta$ 42, indicating more overall Alzheimer’s pathology (E).

### Concordance between CSF and PET A $\beta$ Positivity

We next determined whether participants classified as A $\beta$ <sup>+</sup> on PET using a validated threshold (>1.11 SUVR; (Landau et al., 2012) would also be considered positive for CSF A $\beta$ 42/40 using a threshold calculated in a mixed memory cohort (<0.062; (Alcolea et al., 2019).

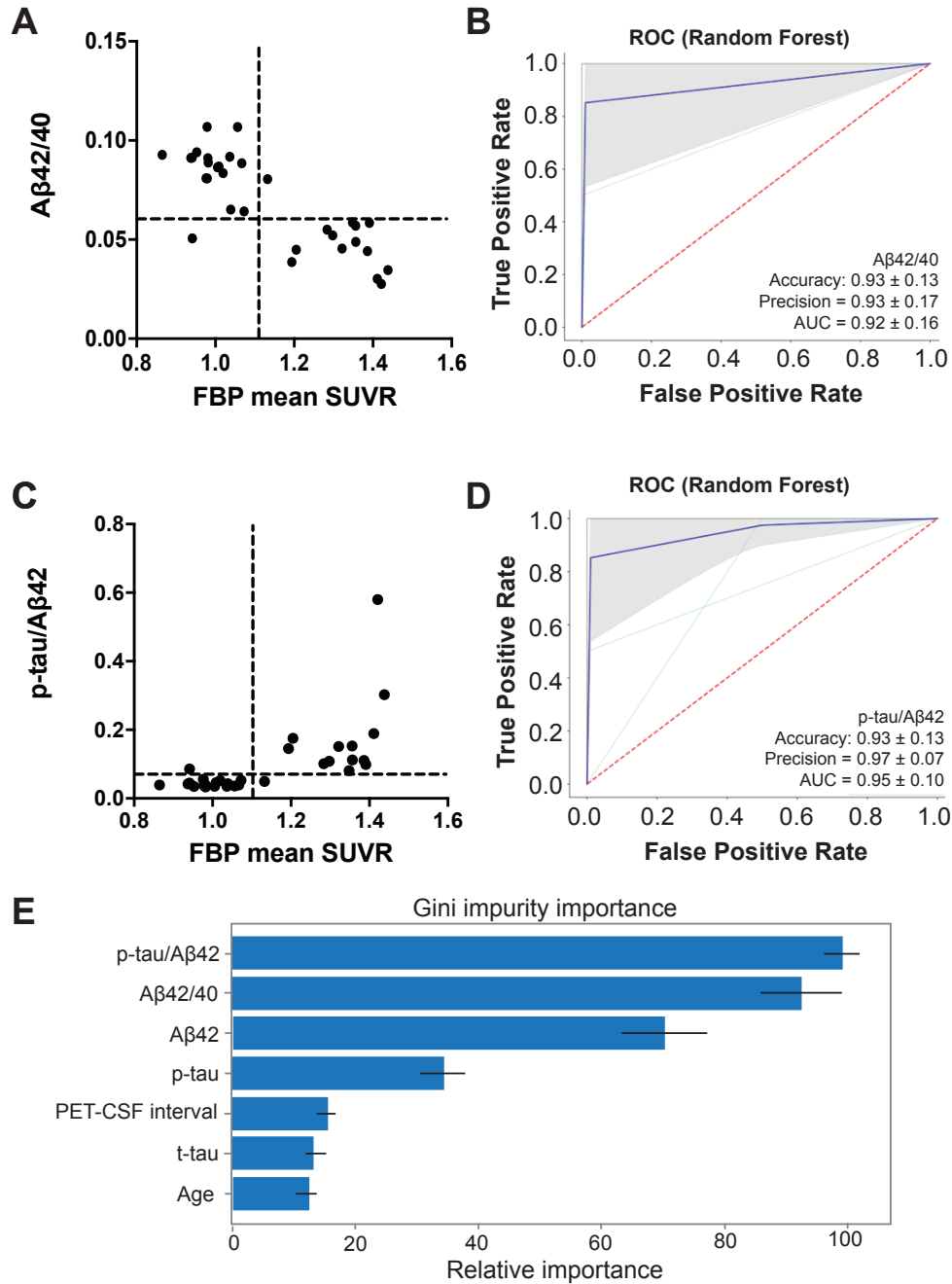
The majority of subjects were concordant on the two measures (30/32, 93.8%; **Fig A2A**).

Thirteen participants were classified concordant positive (40.5%), 17 participants as concordant negative (53.1%), and one participant was classified into each of the discordant groups.

To determine the classification performance of CSF A $\beta$ 42/40 positivity compared to A $\beta$ -PET positivity, we next conducted random forest ROC analyses. CSF A $\beta$ 42/40 status predicted A $\beta$ -PET status with high accuracy ( $0.93 \pm 0.13$ ) and precision ( $0.93 \pm 0.17$ ), with an AUC value of  $0.92 \pm 0.16$  (**Fig A2B**). Results were consistent when using logistic regression models to ensure the random forest model did not overfit the data.

We next tested whether A $\beta$ -positivity on PET was also consistent with a positive p-tau/A $\beta$ 42 ratio ( $>0.068$ , Alcolea et al 2019). Consistent with A $\beta$ 42/40, the majority of subjects were concordant between p-tau/A $\beta$ 42 and A $\beta$ -PET (30/32, 93.8%; **Fig A2C**), with 13 participants were classified concordant positive (40.5%), 17 participants as concordant negative (53.1%), and one participant was classified into each of the discordant groups. Random forest ROC analyses showed that classification performance of p-tau/A $\beta$ 42 status had high accuracy ( $0.93 \pm 0.13$ ) and precision ( $0.97 \pm 0.17$ ) when compared to A $\beta$ -PET status, with an AUC value of  $0.95 \pm 0.10$  (**Fig A2D**).

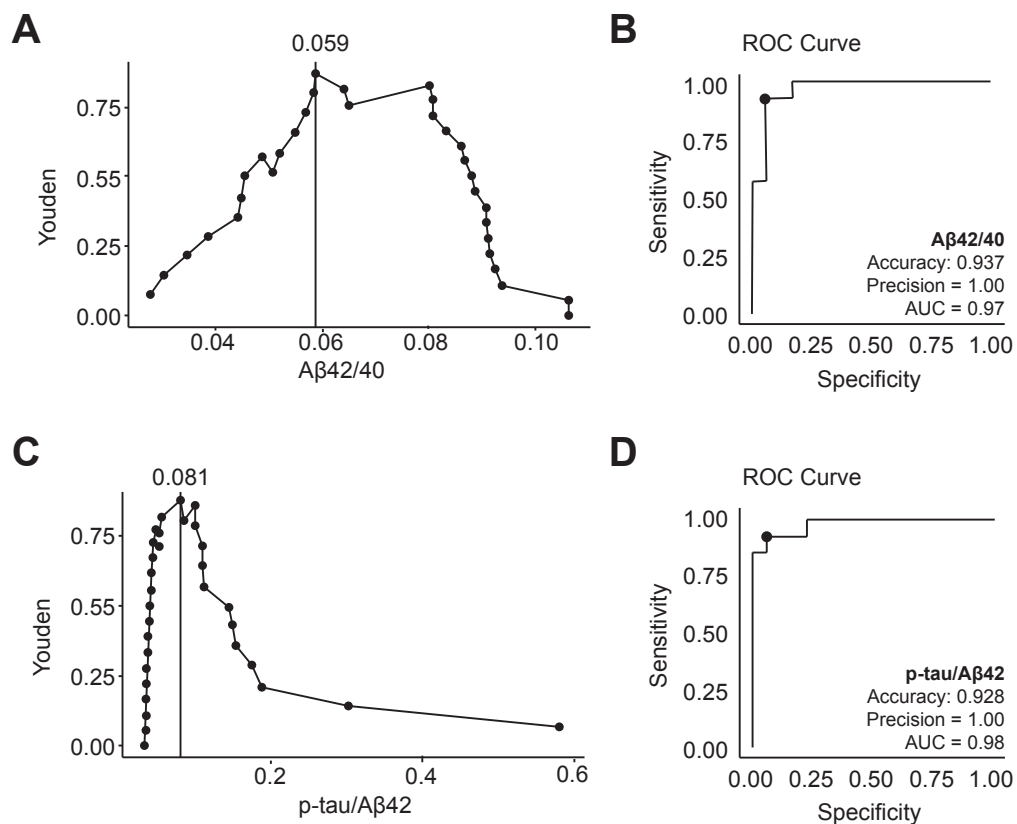
Finally, we conducted a Gini impurity analysis to test which CSF biomarkers were most important in predicting A $\beta$ -PET status, when also including age and PET-CSF interval (**Fig A2E**). We measured the importance of each feature with the Gini impurity importance, and these measures highlight p-tau/A $\beta$ 42 as the most relevant features for A $\beta$ -positivity, followed by A $\beta$ 42/40. The ranking indicated that the least influential features of the predictions are age, t-tau, and PET-CSF interval.



**Figure A2. Positivity on Aβ-PET and CSF biomarkers are highly concordant in cognitively normal older adults.** (A, C) Concordance for Aβ-PET and both CSF Aβ42/40 (A) and p-tau/Aβ42 (C) was 93.8% (13 concordant positive, 17 concordant negative, 2 discordant). (B, D) Random Forest ROC analyses indicated that both CSF Aβ42/40 (B) and p-tau/Aβ42 (D) predicted Aβ-PET status with high accuracy. (E) Gini impurity analysis indicated that CSF p-tau/Aβ42 was the more important feature in predicting Aβ-PET status, with nearly 100% relative importance. The bars represent the importance of each feature (error bars represent standard deviation), measured through the sum of all the Gini impurity index decreases for each specific feature.

## Replication of Data-driven CSF Thresholds

Finally, we recalculated data-driven thresholds for CSF biomarkers that were optimal for our cognitively normal sample. CSF measures were compared to A $\beta$ -PET positivity, and cutoffs showing the highest Youden index were selected. The optimal A $\beta$ 42/40 cutoff was 0.059 (Youden index of 0.873; **FigA3A**), which predicted A $\beta$ -PET status with high accuracy (0.937) and precision (1.00), with an AUC value of 0.97 (**FigA3B**). The optimal p-tau/A $\beta$ 42 cutoff was 0.081 (Youden index of 0.928; **FigA3C**), which predicted A $\beta$ -PET status with high accuracy (0.969) and precision (1.00), with an AUC value of 0.98 (**FigA3D**).



**Figure A3. Recalculation of thresholds for CSF A $\beta$ 42/40 and p-tau/A42 in a cognitively normal sample.** (A) The optimal threshold for A $\beta$ 42/40 was determined to be 0.059, representing the highest Youden index (0.929). (B) Using the 0.059 cut-off, CSF A $\beta$ 42/40 status predicted A $\beta$ -PET status with high accuracy and precision. (C) The optimal threshold for p-tau/A $\beta$ 42 was determined to be 0.081, representing the highest Youden index (0.928). (B) Using the 0.081 cut-off, CSF p-tau/A $\beta$ 42 status predicted A $\beta$ -PET status with high accuracy and precision.

## Discussion

Our findings support a strong association between CSF biomarkers of AD derived using an automated Lumipulse assay with A $\beta$ -PET for the first time in an entirely cognitively unimpaired sample. A $\beta$ -PET and CSF biomarkers of A $\beta$  (A $\beta$ 42/40 and A $\beta$ <sub>1-42</sub>), p-tau, and p-tau/A $\beta$ 42 were strongly correlated, which is consistent with previous findings in mixed memory cohorts (Alcolea et al., 2019; Campbell et al., 2021; Willemsse et al., 2021). We demonstrated that CSF A $\beta$ 42/40 and A $\beta$ -PET positivity are highly concordant in cognitively normal older adults using a threshold previously calculated in a mixed-memory cohort. Further, CSF p-tau/A $\beta$ 42, a marker of overall AD pathology, was the strongest predictor of A $\beta$ -PET. Together, our results support the accuracy of the automated Lumipulse assay to quantify CSF biomarkers of AD in cognitively normal samples, and the utility of these biomarkers in measuring emerging AD pathology in aging.

Our results expand on previous studies investigating CSF biomarker relationships with A $\beta$ -PET in mixed memory or clinical cohorts (Campbell et al., 2021). A previous study in a mixed memory cohort reported that A $\beta$ 42/40 and p-tau/A $\beta$ 42 ratios were equally predictive of A $\beta$ -PET status (Campbell et al., 2021). In our sample, while classification agreement and performance were similar between CSF A $\beta$ 42/40 and p-tau/A $\beta$ 42 in predicting A $\beta$ -PET positivity, p-tau/A $\beta$ 42 demonstrated slightly higher precision than A $\beta$ 42/40, resulting in a higher

AUC value. Furthermore, p-tau/A $\beta$ 42 was the most important feature selected in predicting A $\beta$ -positivity, followed by A $\beta$ 42/40. These findings indicate that the p-tau/A $\beta$ 42 ratio may be more sensitive in a cognitively normal sample, as it also accounts for the amount of phosphorylated tau pathology, and may more accurately represent overall AD pathology.

Recalculating data-driven CSF A $\beta$ 42/40 and p-tau/A $\beta$ 42 thresholds on our own dataset of cognitively normal older adults, we derived a very similar threshold to Alcolea et al. (Alcolea et al., 2019). However, our thresholds are slightly lower for A $\beta$ 42/40 (0.059) and higher for p-tau/A $\beta$ 42 (0.081) in our cognitively normal sample compared to the cutoff reported in Alcolea et al. (0.061 for A $\beta$ 42/40 and 0.068 for p-tau/A $\beta$ 42) in their mixed memory cohort. This difference may be due to our use of a quantitative threshold for defining A $\beta$ -PET positivity, while Alcolea et al. used visual reads. Further, our thresholds may more accurately measure emerging AD pathology, as they were derived without the influence of measures from clinically impaired subjects.

Limitations of the current study include the relatively small sample size, and the variation of time between CSF and PET measurements, however, this was controlled for in all analyses. We could not characterize why PET and CSF measures were discordant in our study due to the limited number of discordant observations (2 participants). Future research should investigate the longitudinal changes that occur in concordant individuals compared to those that are discordant, and determine whether CSF may be more sensitive and changes prior to PET in preclinical samples.

Overall, our findings support the utility of quantifying CSF biomarkers with the automated Lumipulse assay in studies of cognitively normal participants, and emphasize the

importance of CSF biomarkers to measure emerging AD pathology in cognitively normal samples.