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Authors

Hu, Lechuan
Fortin, Norbert J
Ombao, Hernando

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Modeling High-Dimensional Multichannel Brain Signals

Lechuan Hu¹ · Norbert J. Fortin² · Hernando Ombao^{1,3} 

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Abstract Our goal is to model and measure functional and effective (directional) connectivity in multichannel brain physiological signals (e.g., electroencephalograms, local field potentials). The difficulties from analyzing these data mainly come from two aspects: first, there are major statistical and computational challenges for modeling and analyzing high-dimensional multichannel brain signals; second, there is no set of universally agreed measures for characterizing connectivity. To model multichannel brain signals, our approach is to fit a vector autoregressive (VAR) model with potentially high lag order so that complex lead-lag temporal dynamics between the channels can be captured. Estimates of the VAR model will be obtained by our proposed hybrid LASSLE (LASSO + LSE) method which combines regularization (to control for sparsity) and least squares estimation (to improve bias and mean-squared error). Then we employ some measures of connectivity but put an emphasis on partial directed coherence (PDC) which can capture the directional connectivity between channels. PDC is a frequency-specific measure that explains the extent to which the present oscillatory activity in a sender channel influences the future oscillatory activity in a specific receiver channel relative to all possible receivers in the network. The proposed modeling approach provided key insights into potential functional relationships among simultaneously recorded sites during performance of a complex memory task. Specifically, this novel method was successful in quantifying patterns of effective con-

✉ Hernando Ombao
hernando.ombao@kaust.edu.sa

¹ Department of Statistics, University of California, Irvine, USA

² Department of Neurobiology and Behavior, University of California, Irvine, USA

³ Statistics Program, King Abdullah University of Science and Technology (KAUST), Thuwal, Saudi Arabia

nectivity across electrode locations, and in capturing how these patterns varied across trial epochs and trial types.

Keywords Electroencephalograms · Local field potentials · Brain effective connectivity · Multivariate time series · Vector autoregressive model · Partial directed coherence

1 Introduction

Connectivity between populations of neurons is crucial to fully characterize brain processes during cognition (e.g., memory and learning) and even during resting-state. Moreover, alterations in brain connectivity are widely believed to be implicated in a number of neurological and mental diseases such as obsessive compulsive disorder and Alzheimer’s disease. However, the underlying mechanisms of brain connectivity remain elusive. First, there is no set of universally agreed measures for characterizing connectivity. Second, there are major statistical and computational challenges for modeling and analyzing multichannel brain signals—especially when the number of parameters is large which often happens when the number of channels is large and/or the temporal lag for parametric models such as vector autoregressive (VAR) is high. Our contribution in this paper is a scalable approach to estimate connectivity in multichannel brain physiological signals modeled with high-dimensional parameters.

The work is motivated by our current collaborations with the Fortin Laboratory (UC Irvine) whose research requires developing a systematic statistical framework to quantify functional and effective connectivity among multi-site neural activity signals recorded in rats performing complex memory tasks. The electrophysiological data recorded from rats include local field potentials (LFPs) and an example of a recording for one epoch (here an epoch is 1 second time block) is given in Fig. 1. LFP signals have excellent temporal resolution (here 1000 observations per second). It is comparable to electroencephalograms (EEGs) in terms of temporal resolution and both capture electrical activity of the neurons. However, LFPs are recorded invasively since these are obtained from electrodes that are chronically implanted inside the brain. Because LFPs are obtained from implanted electrodes, they have lower contamination compared to scalp EEGs. They contain less non-neuronal physiological activity (e.g., muscular activity) and therefore possess a higher signal-to-physiological-noise ratio. One disadvantage of LFPs, however, is its limited utility in humans due to its invasive nature. However, these will continue to be a valuable tool for investigating brain function in animals which can then provide useful information for modeling brain function in humans. One of the challenges to fitting statistical models to LFPs is that the parameter space can be high dimensional. The number of recording tetrodes (P) in LFPs can range from 8 to 100; and the temporal order (d) of parametric models such as vector autoregressive (VAR) models needs to be sufficiently large in order to accurately capture the dynamics in these complex processes. In this setting, the number of parameters in a VAR model is P^2d , which can be large.

In this paper, we will develop a computationally scalable method for fitting high-dimensional complex models that addresses two important goals in brain science:

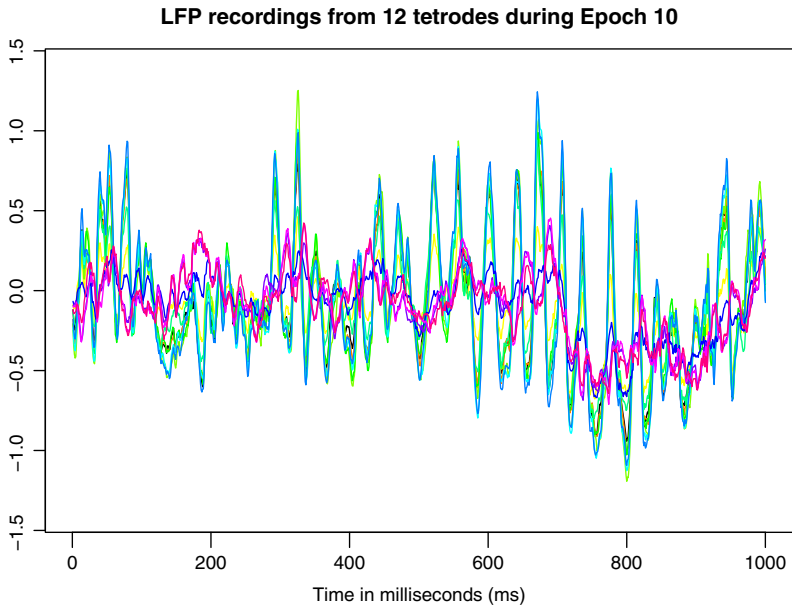


Fig. 1 Local field potential (LFP) recordings from 12 tetrodes during one epoch (1000 ms; $T = 1000$). Each time series with color indicates the LFP recording from one tetrode

(1) To identify the connectivity structure between channels in a brain network and (2) to quantify both the strength and directionality of connectivity between these channels. Our approach is to fit a VAR model with potentially high temporal lag in order to more accurately capture complex lead-lag temporal dynamics between the channels or leads. Estimates of the VAR model will be obtained by a combination of regularization to maintain high specificity and least squares estimation to reduce bias and mean-squared error. The method will be applied to LFPs obtained from a rat performing an odor sequence memory task, in which he is required to identify each odor as being presented in the correct or incorrect sequence position.

To characterize connectivity in a multichannel LFP signal, we shall use the vector autoregressive (VAR) model [24]. A P -dimensional brain signal \mathbf{X}_t is said to follow a VAR model of order d , denoted VAR(d), if it has the representation

$$\mathbf{X}_t = \Phi_1 \mathbf{X}_{t-1} + \dots + \Phi_d \mathbf{X}_{t-d} + \varepsilon_t, \quad t = d + 1, \dots, T, \tag{1.1}$$

where Φ_ℓ 's $\in \mathfrak{R}^{P \times P}$ are the autoregressive coefficient matrices and $\varepsilon_t \stackrel{iid}{\sim} N_P(\vec{0}, \Sigma)$. The interconnectivity between channels is determined by the autoregressive coefficient matrices $\{\Phi_\ell\}_{\ell=1}^d$ and spatial covariance matrix Σ . Thus, the VAR model provides a broad framework for capturing complex temporal and cross-sectional interrelationship among the time series (in particular, directionality of frequency-specific connectivity). Consequently, it can be applied to model the Granger-causal relation between channels [14].

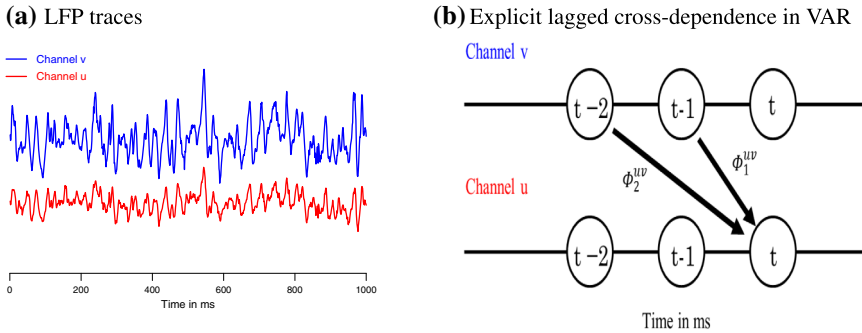


Fig. 2 LFP traces and VAR. Φ_ℓ^{uv} ($\ell = 1, 2$) captures the impact of the input from v th channel at time $t - \ell$ to brain activity at u th channel at the current time t (Color figure online)

To illustrate connectivity via the VAR matrix, consider Fig. 2 and denote the LFP traces of brain region to be u th and v th channel. Then the entry Φ_ℓ^{uv} shows the impact of the input from v th channel at time $t - \ell$ to brain activity at u th channel at the current time t . If $\Phi_\ell^{uv} = 0$ and $\Phi_\ell^{vu} = 0$ for all lags ℓ then, there is no connectivity between these two channels as determined by VAR model. A positive value indicates that the signal of v th channel at time $t - \ell$, conditional on LFP values at other times, has positive linear dependence with u th channel at time t . That is, a marginal increase in activity in v th channel leads to a increased future activity in u th channel. Thus, the entries of $\{\Phi_\ell\}_{\ell=1}^d$ contain the information of brain connectivity between channels. In this paper, we shall use partial directed coherence (PDC) [4, 5] to characterize effective (directed) connectivity. This measure is more specific and provides more information, in particular frequency-specific directionality, than simply the coefficients of the VAR matrices. PDC is frequency specific: it measures how an oscillatory activity (at a particular frequency band) at a present time in one channel may impact oscillatory activity of the same frequency band at another channel at a future time point.

As noted above, effective connectivity between channels will be characterized by the VAR coefficient matrices. This is challenging because the parameter space of a VAR model for brain signals is usually high. For example, if we fit a VAR(10) model to 12 leads or channels, there are $10 \times 12^2 = 1440$ parameters in total to estimate, which subsequently requires intensive computation. One could suggest fitting a model with low temporal lag in order to reduce the number of parameters. The problem with this suggestion, unfortunately, is that a low temporal order might miss potentially important features of the data such as multiple peaks in the spectra.

One classic estimation approach is via least squares which (as long as there are sufficient data points) provides unbiased estimator for the elements of the VAR coefficient matrices but at the cost of high demand of computing. The least squares estimate (LSE) does not possess the specificity for coefficients with true value of zero. Hence, it cannot provide an adequate answer to the first question about identifying functionally connected regions in brain network. Another common estimation approach is the LASSO (least absolute shrinkage and selection operator) method which is a particular representative of the penalized regression family [12, 25–27]. Compared with LSE, the

LASSO approach requires smaller computation time [19]. Most importantly, LASSO has higher specificity of zero-coefficients. The main limitation of the LASSO (and most regularization methods) is that the estimators of the non-zero coefficients are biased. Thus, it could lead to misleading results when investigating strength of brain effective connectivity. Inspired by the strengths of each of the two classical approaches (i.e., LSE and the LASSO), we propose to combine these in a two-step estimation procedure which we call the LASSLE method. We demonstrate that LASSLE has inherited low bias for non-zero estimates and high specificity for zero-estimates from LSE and the LASSO separately. As a result, the proposed two-step method has higher specificity and significantly lower mean-squared error (MSE) in the simulation study. At this stage, the full theoretical justification is being developed but the numerical experiments are encouraging.

A natural question to ask is whether or not the LASSO method is appropriate for fitting VAR models to brain signals. The answer lies in whether or not brain signals such as LFPs and EEGs indeed exhibit sparse connectivity structure. Due to volume conduction for EEGs, it is not likely that the connectivity structure between channels is sparse. However, though LASSO aims to shrink many of the VAR coefficients to zero but this does not necessarily lead to a sparse connectivity structure. Keep in mind that a pair of channels are functionally disconnected only if *all* of the its corresponding VAR coefficients at *all* lags are estimated to be zero. Thus, imposing sparsity on the VAR coefficient matrices helps to weed out the less important parameters in the VAR model but does not oversimplify the connectivity structure.

The remainder of this paper is arranged as follows: In Sect. 2, we present the proposed hybrid LASSLE (LASSO + LSE) method followed by finite sample simulation studies in Sect. 3 and analysis of LFP signals in Sect. 4 and conclusion in Sect. 5.

2 A Proposed Two-Step LASSO + LSE Procedure for Fitting a VAR Model

First, we note that the VAR(*d*) model can be alternatively written in a form

$$\underbrace{\begin{bmatrix} (\mathbf{X}_T)' \\ \vdots \\ (\mathbf{X}_{d+1})' \end{bmatrix}}_Y = \underbrace{\begin{bmatrix} (\mathbf{X}_{T-1})' \cdots (\mathbf{X}_{T-d})' \\ \vdots \quad \ddots \quad \vdots \\ (\mathbf{X}_d)' \cdots (\mathbf{X}_1)' \end{bmatrix}}_X \underbrace{\begin{bmatrix} (\Phi_1)' \\ \vdots \\ (\Phi_d)' \end{bmatrix}}_B + \underbrace{\begin{bmatrix} (\varepsilon_T)' \\ \vdots \\ (\varepsilon_{d+1})' \end{bmatrix}}_E. \tag{2.1}$$

Next, denote $Y = [y_1, y_2, \dots, y_P]$, $B = [b_1, b_2, \dots, b_P]$, $E = [e_1, e_2, \dots, e_P]$. Denote the k^{th} column vector of the matrices Y , B and E ($k = 1, 2, \dots, P$) to be y_k , b_k , e_k . Then we have

$$\underbrace{y_k}_{m \times 1} = \underbrace{X}_{q \times 1} \underbrace{b_k}_{m \times 1} + \underbrace{e_k}_{m \times 1}, \quad e_k \overset{indep}{\sim} N_m(\vec{0}, \sigma_{kk} I_m) \tag{2.2}$$

where $m = T - d$, $q = P \times d$, and σ_{kk} is the k^{th} diagonal element of the covariance matrix Σ . Note that Eq. (2.1) is finally decomposed into many sub-linear regression

problems of estimating $\{b_k\}_{k=1}^P$ in a parallel manner and all the entries of connectivity matrices are included in $\{b_k\}_{k=1}^P$.

2.1 Least Squares Estimation (LSE)

To fit a linear regression model, the most common approach is via least squares estimation so that the least squares estimator \widehat{b}_k satisfies

$$\widehat{b}_k = \underset{b_k \in \mathcal{R}^q}{\operatorname{argmin}} \|y_k - \mathbb{X}b_k\|^2 \quad (2.3)$$

which gives the unbiased estimator $\widehat{b}_k = (\mathbb{X}'\mathbb{X})^{-1}\mathbb{X}'y_k$. Some papers [11] argue that in high-dimensional case the number of parameters q can be larger than the number of observations m , and thus, this method has limitations due to the non-singular matrix $\mathbb{X}'\mathbb{X}$. However, we do not worry about this when analyzing the LFP data since normally we have replicated measurements from multiple epochs. The biggest problem here is that LSE has poor specificity for coefficients with true value of zero. It always produces estimates that are very close to zero rather than exactly zero, which reflects non-connectivity between channels. Indeed when LFP channels are not effectively connected with each other, then an excess non-zero estimate could lead to incorrect characterizations of connectivity through partial directed coherence. Moreover, even a trivial amount of bias for one coefficient, when added across thousands of coefficients, can produce large mean-squared error (as demonstrated in the simulation study).

2.2 LASSO Family Estimation

In order to overcome the problem of non-specificity by the LSE method, recent attention has been focused on the family of penalized regression models as viable solutions to this problem. One of the well-known methods of this family is LASSO regression (with L_1 penalty term). The estimates given by LASSO are the solution to the minimization of the criterion

$$\widetilde{b}_k = \underset{b_k \in \mathcal{R}^q}{\operatorname{argmin}} \|y_k - \mathbb{X}b_k\|^2 + \lambda \|b_k\|_1. \quad (2.4)$$

The penalty term will force a lot of excess non-zero estimates to exact zero, which provides good estimate for the sparsity of the VAR coefficient matrices $\{\Phi_\ell\}_{\ell=1}^d$ and could consequently greatly simplify the calculation of connectivity measures (e.g., PDC) by focusing only on the more important coefficients. In the implementation of the algorithms for LASSO, we take advantage of the results demonstrated by Friedman et al. [10] where estimation of generalized linear models with convex penalties can be handled by cyclical coordinate descent and computed along a regularization path. The price of LASSO is that the non-zero estimates are biased of true values which leads to incorrect estimates of the strength of connectivity between channels (PDC).

2.3 LASSLE: Proposed Two-Step Estimation Method

Motivated by both the advantages and limitation of each of the previous approaches, we propose a two-step procedure to estimate VAR model parameters. Our method consists of these two steps:

Step 1. Apply LASSO to identify entries in $\{\Phi_\ell\}_{\ell=1}^d$ whose estimates are not set to 0.

$$\widehat{S}_k = \{j \in \{1, \dots, q\} : \widehat{b}_k^j \neq 0\}. \tag{2.5}$$

Step 2. Fit LSE with the constraint that “zero” entries estimates from Step 1 are fixed to 0

$$\widetilde{b}_{kLAS} = \underset{b_k: b_k^j=0, j \in \widehat{S}_k^c}{\operatorname{argmin}} \|y_k - \mathbb{X}b_k\|_2^2. \tag{2.6}$$

LASSLE Algorithm

- 1: **procedure** TWO-STEP ESTIMATION
 - 2: *Step 1:*
 - 3: Generate a sequence of (d, λ) and randomly divide data to K folds
 - 4: For a possible choice of (d, λ) , leave one fold as test data at each time
 - 5: Train 2.2 with LASSO method on other folds and compute $\{\widehat{\Phi}_\ell\}_{\ell=1}^d$ for $\{\Phi_\ell\}_{\ell=1}^d$
 - 6: Based on $\{\widehat{\Phi}_\ell\}_{\ell=1}^d$, calculate prediction error on test set and finally take average
 - 7: Select (d, λ) with the lowest average prediction error
 - 8: Obtain estimate $\{\widehat{b}_k\}_{k=1}^P$ for $\{b_k\}_{k=1}^P$ in Equation (2.2) of lag d using LASSO method with λ
 - 9: *Step 2:*
 - 10: **if** $\widehat{b}_k^j = 0$ **then**
 - 11: Set $b_k^j = 0$.
 - 12: **if** $\widehat{b}_k^j \neq 0$ **then**
 - 13: Keep b_k^j .
 - 14: Obtain estimate $\{\widetilde{b}_{kLAS}\}_{k=1}^P$ for $\{b_k\}_{k=1}^P$ in Equation (2.2) with LSE under above constriction
 - 15: Obtain estimate $\{\widehat{\Phi}_{\ell LAS}\}_{\ell=1}^d$ for $\{\Phi_\ell\}_{\ell=1}^d$ by arranging $\{\widetilde{b}_{kLAS}\}_{k=1}^P$
-

To obtain the optimal tuning parameter λ , we employ a K -fold cross-validation test in Step 1. A sequence of candidates of λ will be pre-specified and the optimal value is selected such that the average of prediction error on test data is minimized.

2.4 Theoretical Consideration

For linear regression, under Irrepresentable Condition¹, $\{\widehat{b}_k\}_{k=1}^P$ have sign consistency assured by LASSO estimator [28], which means for sufficient large sample size $T - d$

¹ Assume $b_k = (b_k^1, \dots, b_k^J, b_k^{J+1}, \dots, b_k^q)^T$, where $b_k^j \neq 0$ for $j = 1, \dots, J$ and $b_k^j = 0$ for $j = J + 1, \dots, q$. Let $b_k^{(1)} = (b_k^1, \dots, b_k^J)^T$ and $b_k^{(2)} = (b_k^{J+1}, \dots, b_k^q)^T$. Denote Gram matrix $\Psi = \frac{1}{n} \mathbb{X}' \mathbb{X} = \begin{pmatrix} \Psi_{11} & \Psi_{12} \\ \Psi_{21} & \Psi_{22} \end{pmatrix}$, then Irrepresentable Condition is satisfied if there exists a positive constant vector η , such that $|\Psi_{21}(\Psi_{11})^{-1} \operatorname{sgn}(b_k^{(1)})| \leq 1 - \eta$.

$$\mathbb{P}(\text{sgn}(\widehat{b}_k) = \text{sgn}(b_k)) \rightarrow 1 \tag{2.7}$$

where $\text{sgn}(b_k)$ is the sign function with value of 1, 0 or -1 corresponding to $b_k > 0$, $b_k = 0$ or $b_k < 0$, respectively. Therefore, $\mathbf{P}(\widehat{S}_k \neq S_k) \rightarrow 0$, which implies high specificity of true zero VAR coefficients. Then our inaccurate non-zero estimate will be updated in Step 2. Since we put a constraint for LSE in Step 2, the computing is much simplified compared with merely LSE. Moreover, the bias and mean-squared error of LASSLE estimator will be bounded [18]

$$\|E(\widetilde{b}_{kLAS}) - b_k\|_2^2 \leq 2\mathbf{P}(\widehat{S}_k \neq S_k) \left\{ O\left(\frac{1}{m}\right) + \|b_k\|_2^2 + \tau\sigma_{kk} \right\} \tag{2.8}$$

$$E\|\widetilde{b}_{kLAS} - b_k\|_2^2 \leq 2\frac{\sigma_{kk}}{m} \text{tr}(\Psi_{11}^{-1}) + \sqrt{\mathbf{P}(\widehat{S}_k \neq S_k)} \left\{ O\left(\frac{1}{m}\right) + \|b_k\|_2^2 + \tau\sigma_{kk} \right\} \tag{2.9}$$

Thus, our non-zero estimates are almost unbiased, which is significantly improved from LASSO. Final estimates given by LASSLE in simulation study have substantially lower general mean-squared error. Thus, our approach is able to both indicate the most important effective connectivity and give a more precise estimate of the strength of connectivity.

2.5 Measure of Dependence

In this section, we enumerate the different measures of dependence between components of a multivariate time series (or between different channels) using the VAR model. First, a P -channel time series, denoted $\{\mathbf{X}_t = (\mathbf{X}_t^1, \dots, \mathbf{X}_t^P)'\}$, $t = 1, 2, \dots$, is weakly stationary if the following are satisfied:

- (a) $E(\mathbf{X}_t)$ is constant over all time t , and
- (b) the autocovariance function matrix

$$\text{cov}(X_t, X_{t+h}) = \Gamma(h) = \begin{pmatrix} \gamma_{11}(h) & \gamma_{12}(h) & \dots & \gamma_{1P}(h) \\ \gamma_{21}(h) & \gamma_{22}(h) & \dots & \gamma_{2P}(h) \\ \vdots & \vdots & \ddots & \vdots \\ \gamma_{P1}(h) & \gamma_{P2}(h) & \dots & \gamma_{PP}(h) \end{pmatrix}$$

depends only on the lag h , where $\gamma_{uv}(h) = \text{cov}(X_t^u, X_{t+h}^v)$ for all pairs of channels $u, v = 1, \dots, P$.

Moreover, if the sequence of auto- and cross-covariance between any pair of channels u and v is absolutely summable, i.e., $\sum_{h=-\infty}^{\infty} |\gamma_{uv}(h)| < \infty$, then we define the spectral density matrix of $\{\mathbf{X}_t\}$ to be

$$f(\omega) = \sum_{h=-\infty}^{\infty} \Gamma(h)e^{-2\pi i\omega h}, \quad -1/2 \leq \omega \leq 1/2. \tag{2.10}$$

The spectral matrix has dimension $P \times P$ whose diagonal elements $f_{uu}(\omega)$ are the auto-spectra of the channels at frequency ω and the off-diagonal elements $f_{uv}(\omega)$ are the cross-spectra of channels u and v at frequency ω .

The first dependency measure that we will consider is coherency. Coherency between the u th and v th channels at frequency ω , is defined as

$$\rho_{uv}(\omega) = \frac{f_{uv}(\omega)}{\sqrt{f_{uu}(\omega)}\sqrt{f_{vv}(\omega)}}. \quad (2.11)$$

One can interpret coherency as the cross-correlation between the ω -oscillatory component in channel u and the ω -oscillatory component in channel v [20].

The second dependency measure is coherence. Coherence between the u th and v th channels at frequency ω is defined as

$$\rho_{uv}^2(\omega) = \frac{|f_{uv}(\omega)|^2}{f_{uu}(\omega)f_{vv}(\omega)}. \quad (2.12)$$

When $\rho_{uv}^2(\omega)$ is close to 1 then both channels u and v share a common ω -oscillatory activity. Moreover, when the cross-correlation between the u and v channels is 0 at all time lags, then the coherency (and coherence) between these channels at *all* frequencies is 0. A large coherence value between channels u and v could be due to direct connectivity between these two channels or could be indirectly due to the intervening effect of other channel(s). To measure the strength of connectivity between a pair of channels—with the effect of all intervening channels removed—we shall use partial coherence.

The third dependency measure is partial coherence. Define the matrix $g(\omega) = f^{-1}(\omega)$ and denote the diagonal elements as $g_{pp}(\omega)$. Let $h(\omega)$ be a diagonal matrix whose elements are $g_{pp}^{-1/2}(\omega)$. Define the matrix $C(\omega)$ to be

$$C(\omega) = -g(\omega)h(\omega)g(\omega). \quad (2.13)$$

Then, the partial coherence between the u th and v th channels is the modulus squared of the (u, v) th element of $C(\omega)$ [7, 8]

$$\zeta_{uv}^2(\omega) = |C_{uv}(\omega)|^2. \quad (2.14)$$

We now present the fourth dependency measure which is partial directed coherence developed in Baccalá and Sameshima [4] and refined in Baccalá and Sameshima [5]. Consider a VAR(d) model given by Eq. (1.1), define

$$A(\omega) = I - \sum_{\ell=1}^d \Phi_{\ell} \exp(-i2\pi\omega\ell/\Omega) \quad (2.15)$$

be the transform of sequence $\{\Phi_{\ell}\}_{\ell=1}^d$ at frequency ω , where Ω is the sampling frequency. The partial directed coherence from channel v to channel u at frequency ω is defined as

$$\pi_{uv}^2(\omega) = \frac{|A_{uv}(\omega)|^2}{\sum_{m=1}^P |A_{mv}(\omega)|^2} \quad (2.16)$$

which measures the direct influence from channel v to channel u conditional on all the outflow from channel v . PDC gives an indication on the extent to which present frequency-specific oscillatory activity from a sender channel explains future oscillatory activity in a specific receiver channel relative to all channels in the network.

2.6 Model Selection

To determine the best order \hat{d} of VAR, we first use least squares estimation to obtain $\{\hat{\Phi}_\ell\}_{\ell=1}^{d_j}$ for each candidate order in the set $\{d_j\}_{j=1}^J$. We search among a class of reasonable temporal lag orders. From our analysis of LFPs where there are usually less than 4 peaks in the spectrum, it would be reasonable to use an upper bound of 12 as the temporal lag order. Then we calculate the sum of squared errors

$$SSE(d_j) = \sum_{t=d_j+1}^T \left(\mathbf{X}_t - \sum_{\ell=1}^{d_j} \hat{\Phi}_\ell \mathbf{X}_{t-\ell} \right) \left(\mathbf{X}_t - \sum_{\ell=1}^{d_j} \hat{\Phi}_\ell \mathbf{X}_{t-\ell} \right)'. \quad (2.17)$$

Consequently, the conditional MLE of the error covariance matrix Σ for a candidate order d_j is

$$\hat{\Sigma}(d_j) = SSE(d_j)/(T - d_j) \quad (2.18)$$

which is analogous to univariate regression case. To choose the optimal lag, we compute three information criteria—the Akaike Information criterion (AIC), Bayesian Information criterion (BIC), and Hannan-Quinn information criterion (HQC), respectively, for each candidate order d_j :

$$AIC(d_j) = \log |\hat{\Sigma}(d_j)| + 2/T(P^2 d_j) \quad (2.19)$$

$$BIC(d_j) = \log |\hat{\Sigma}(d_j)| + \log T/T(P^2 d_j) \quad (2.20)$$

$$HQC(d_j) = \log |\hat{\Sigma}(d_j)| + 2 \log \log T/T(P^2 d_j). \quad (2.21)$$

The optimal order for each criterion, denoted \hat{d} is the minimizer of the cost functions and thus gives the optimal balance between fit (as measured by SSE) and model complexity (as expressed by the penalty terms). It has been noted that $\hat{d}^{BIC} \leq \hat{d}^{HQC} \leq \hat{d}^{AIC}$ when $T \geq 16$ [13]. In the analysis of LFPs, the difference between \hat{d}^{BIC} and \hat{d}^{AIC} is at most 1, and therefore, we choose \hat{d}^{AIC} to capture more temporal correlation by fitting a VAR of slightly higher lag order.

2.7 Bootstrap-Based Inference

To conduct inference on the VAR parameters, a general idea is to derive the asymptotic property of the estimated VAR coefficient matrices. However, this is not trivial and is still under investigation given the high dimensionality of the VAR parameter space.

An alternative is to develop a bootstrap-based inference, which has been used in time series [15, 17, 21–23]. After obtaining the estimates of the VAR(d) coefficient matrices, $\{\tilde{\Phi}_\ell\}_{\ell=1}^d$, we use these estimates and corresponding residuals to generate new bootstrapped trials. Denote

$$R_t = \mathbf{X}_t - \tilde{\Phi}_1 \mathbf{X}_{t-1} - \dots - \tilde{\Phi}_d \mathbf{X}_{t-d}, \quad t = d + 1, \dots, T \tag{2.22}$$

by residual at time t . Then, to generate a bootstrapped trial $\{\mathbf{X}_t^{(b)}\}_{t=1}^T$, we shall use the following bootstrap algorithm. Define the bootstrapped residuals to be $\{R_t^{(b)}\}_{t=d+1}^T$, which are selected with replacement from $\{R_t\}_{t=d+1}^T$. Let $\mathbf{X}_t^{(b)} = \mathbf{X}_t$ when $t = 1, \dots, d$, then $\mathbf{X}_t^{(b)} = \sum_{\ell=1}^d \tilde{\Phi}_\ell \mathbf{X}_{t-\ell}^{(b)} + R_t^{(b)}$ are bootstrapped data at time t when $t = d + 1, \dots, T$.

Bootstrap Algorithm

- 1: For $b = 1, \dots, B$
 - 2: *Step 1:*
 - 3: Let $\mathbf{X}_t^{(b)} = \mathbf{X}_t$ for $t = 1, 2, \dots, d$
 - 4: *Step 2:*
 - 5: Randomly sample bootstrapped residuals $\{R_t^{(b)}\}_{t=d+1}^T$ from $\{R_t\}_{t=d+1}^T$ with replacement
 - 6: *Step 3:*
 - 7: Let $\mathbf{X}_t^{(b)} = \sum_{\ell=1}^d \tilde{\Phi}_\ell \mathbf{X}_{t-\ell}^{(b)} + R_t^{(b)}$ be bootstrapped data at time t when $t = d + 1, \dots, T$
-

Given the b th bootstrap time series $\{\mathbf{X}_t^{(b)}\}_{t=1}^T$, we compute the VAR coefficient estimates which we denote by $\{\tilde{\Phi}_\ell^{(b)}\}_{\ell=1}^d$ using the LASSLE method and then compute partial directed coherence estimate. We repeat this procedure a sufficient large number of times, then we can find the empirical distribution and obtain the 95% bootstrap confidence interval of both VAR parameters and PDCs.

3 Simulation Study

3.1 Simulation Design

To compare the performance of the proposed LASSLE approach with the classical methods (i.e., LSE only and LASSO only), we conducted a simulation study of VAR(d) model for two different brain network types. The first is “Cluster,” which is a type of network that has high level local and global connectivity efficiency. In Fig. 3, channels (red nodes) are located in four brain regions, while the edge between two red nodes indicates connectivity at channel level. Auto-connectivity inside each region makes channels from the same region connect like a cluster, and cross-connectivity between brain regions determines whether these clusters are connected with each other. For example, Cluster 2 is independent from other regions, but Cluster 1 and Cluster 4 are connected due to the cross-connectivity at region level.

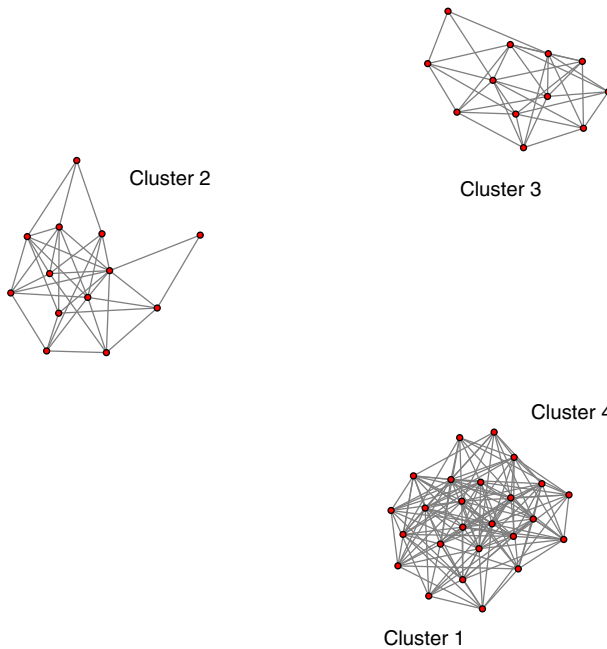


Fig. 3 50 brain channels of “Cluster” type

In the second type “Scale-free,” shown in Fig. 4, there is no significant auto-connectivity or cross-connectivity at the region level, but all the brain channels are connected within the network. Most of the channels have several connections with other channels, with the exception that a few channels are heavily connected. The idea is that these channels play a central role in the organization of entire brain network, as they are mostly responsible for the connectivity efficiency.

For both network types, we use Eq. (1.1) to generate time series data sets. The VAR matrix Φ_1 of setting $\{P = 50, d = 1\}$ is visualized in Figs. 5a and 6a. Each small square represents the non-zero entry of Φ_1 and different colors indicate different values according to the color bar. The blank part of coefficient matrix is the zero entries. In addition, ε_t follows a Gaussian distribution and the covariance matrix is not necessary to be diagonal. We run $N = 1000$ simulations for each VAR setting, respectively, and the time series data of each channel contains $T = 10,000$ time points. Then we apply LSE, LASSO, and our LASSLE method to estimate coefficient matrices, and compare their results with two important criteria. The first one evaluates how successful the estimate identifies the specific entries with true value of zero, as shown by the visualization of absolute difference between true coefficient matrix and estimated one. The second criterion is their mean-squared error, which is defined as

$$MSE = \frac{\sum_{n,\ell,i,j} (\Phi_\ell^{ij} - \widehat{\Phi}_\ell^{ij})^2}{N}, \quad (3.1)$$

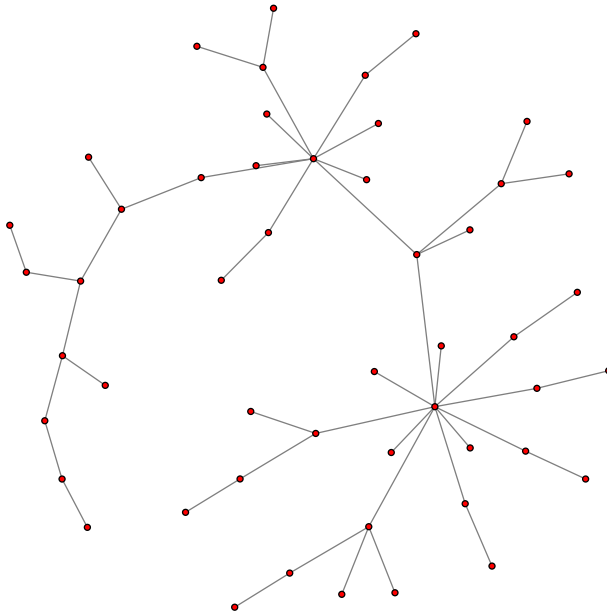


Fig. 4 50 brain channels of “Scale-free” type

where $\{\Phi_\ell^{ij}\}_{\ell=1}^d$, $\{\widehat{\Phi}_\ell^{ij}\}_{\ell=1}^d$ represent entries of $\{\Phi_\ell\}_{\ell=1}^d$ and $\{\widehat{\Phi}_\ell\}_{\ell=1}^d$, respectively. Lower MSE indicates better centering at true connectivity matrix.

3.2 Simulation Results

Due to the display limit of high-dimensional matrix, we only demonstrate visualized results of VAR setting $\{P = 50, d = 1\}$.

3.2.1 Results from the “Cluster” Setting

In this setting, 50 channels represent measurements in four brain regions and only region 1 and region 4 have cross-connectivity. In the coefficient matrix, all non-zero entries are first randomly assigned either 0.1 or -0.1 , then 0.5 is added to all diagonal entries (shown in Fig. 5a). Figure 5b–d yields the absolute difference between true connectivity matrix and estimated one by LSE, LASSO, and LASSLE method. The color of small squares ranging from white to red indicates the value of absolute difference of each entry. The blank part of the matrix implies that the estimate has given correct zero-estimate for those true zero entries so that there is no need to distinguish the difference with color. Table 1 demonstrates the MSE results of all three methods under different VAR parameter settings $\{P, d\}$.

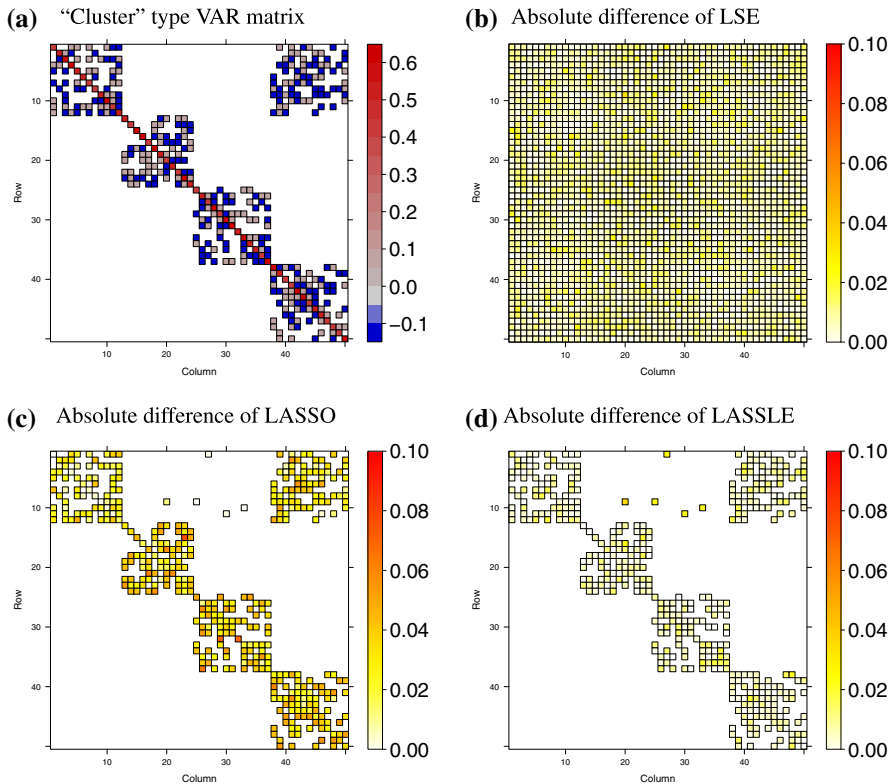


Fig. 5 Comparison of specificity of true zero on “Cluster” type data with Gaussian noise. **a** demonstrates the true VAR(1) coefficient matrix with $P = 50$. **b–d** yield the absolute difference between true matrix and estimated matrix by LSE, LASSO, and LASSLE method, respectively (Color figure online)

Table 1 Comparison of MSE between three methods on “Cluster” type data

VAR parameter setting			MSE $\times 10^{-3}$		
Number	P	d	LSE	LASSO	LASSLE
100	10	1	8	93	4*
500	10	5	58	326	36*
1000	10	10	134	412	82*
2500	50	1	176	464	24*
5000	50	2	457	739	93*
10,000	100	1	697	1016	65*

* Lowest MSE among three methods under each VAR parameter setting

3.2.2 Results from the “Scale-Free” Setting

To generate “Scale-free” type data, we assign 0.5 to all diagonal entries of connectivity matrix, and 0.1 or -0.1 randomly to other non-diagonal entries with small probability (seen in Fig. 6a). Fig. 6b–d give the visualized estimate results given by LSE, LASSO, and LASSLE method separately. MSE comparison is found in Table 2.

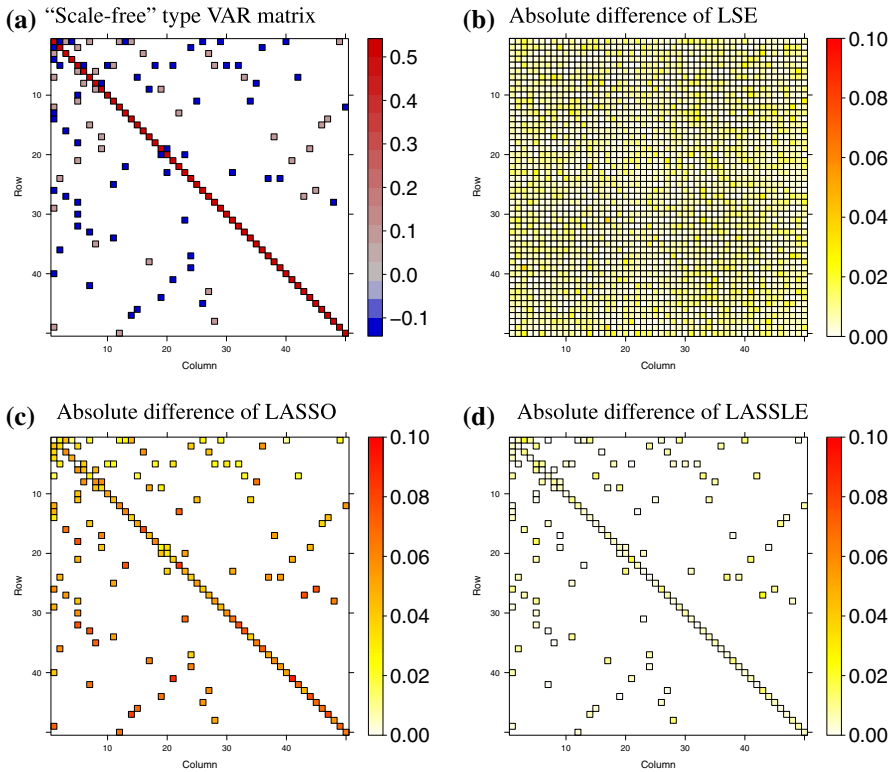


Fig. 6 Comparison of specificity of true zero on “Scale-free” type data with Gaussian noise. **a** demonstrates the true VAR(1) coefficient matrix with $P = 50$. **b–d** yield the absolute difference between true matrix and estimated matrix by LSE, LASSO, and LASSLE method, respectively (Color figure online)

Table 2 Comparison of MSE between three methods on “Scale-free” type data

VAR parameter setting			$MSE \times 10^{-3}$		
Number	P	d	LSE	LASSO	LASSLE
100	10	1	7	86	2*
500	10	5	53	158	16*
1000	10	10	130	472	72*
2500	50	1	191	432	9*
5000	50	2	480	877	37*
10,000	100	1	762	921	19*

* Lowest MSE among three methods under each VAR parameter setting

3.2.3 Discussion

From visualized results, we can find that LSE is unable to give specificity for true zero coefficients, since its estimates do not contain blank squares. However, its estimate has general lower bias across all the entries, which is implied by the light color of absolute difference. LASSO is able to identify most true zero entries, but darker color

of rectangles indicates that this method has high bias for the estimate. Our method, constrained with LASSO in Step 1, has inherited the specificity of true zero values from LASSO, and consequently can capture true zero values as well as LASSO. Thus in the sense of specificity of true zero, the comparison result is as follows: LASSLE = LASSO \gg LSE.

For another important criteria MSE, the proposed LASSLE approach has substantial advantage over LSE and LASSO. In 50-channel “Cluster” setting, the MSE given by LSE and LASSO are approximately 5 times and 10 times the MSE provided by our method, respectively. Also, in 50-channel “Scale-free” settlement, LSE and LASSO provide at least 10 times and 20 times higher MSE compared with LASSLE, respectively. With the increase of dimensions, the advantage is also increasing geometrically. Therefore, LASSLE performs better with respect to the MSE criterion compared to both LSE and LASSO.

3.3 Bootstrap-Based Inference

For each VAR setting and its simulation, we follow the bootstrap algorithm in Sect. 3.3 to generate 1000 bootstrapped trials and re-estimate the VAR parameters with LASSLE method. We (1) investigated whether the 95% bootstrap confidence interval given by the empirical distribution of each VAR parameter captured the true value and (2) compared the center of the bootstrap distribution to the true value of the quantities of interest (VAR parameters and true PDC values). To answer (1), we plot the empirical distribution of each VAR parameter and compare its 95% empirical confidence interval with the true value. To compare (2), we obtain the median of bootstrapped estimates for each entry, then use these medians to form a matrix and compare its absolute difference with the true connectivity matrix.

Figures 7 and 8 demonstrate examples of empirical distribution derived from 1000 bootstrap estimates. The red-dashed line indicates the true value of these example coefficients. The blue curve is the smoothed estimated density curve of each empirical distribution. For some coefficients, e.g., Φ_1^{20} , Φ_{15}^{25} in Fig. 7 and Φ_{15}^{40} , Φ_{30}^{25} in Fig. 8, we are not able to provide a density curve as the empirical distribution is a point-mass density at $x = 0$, in other words, all 1000 bootstrapped LASSLE estimates of these zero coefficients are exactly zero. We can conclude that 95% confidence interval or set of the empirical distribution can capture the true parameter value in the simulation study.

Figure 9a, b demonstrates the median of 1000 bootstrapped LASSLE estimates of “Cluster” and “Scale-free” type data under previous setting $\{P = 50, d = 1\}$, respectively. Figure 9c, d yields their absolute difference with the true connectivity matrix. Given that the color of most non-zero median estimates of LASSLE is very light, we can conclude that the empirical distributions generated by bootstrap are well centered around the true coefficient values.

3.4 Robustness of LASSLE Method

Previous simulation study is conducted under the assumption that ε_t , the noise of VAR(d) at time t , follows a multivariate Gaussian distribution. In addition to Gaus-

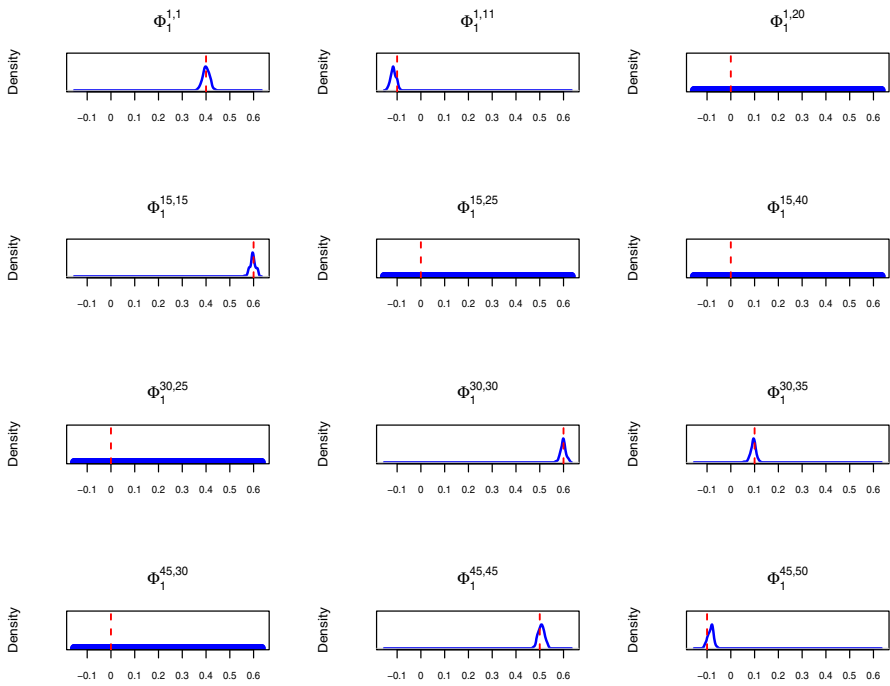


Fig. 7 Sample empirical distribution of “Cluster” type bootstrapped estimates. Red-dashed line indicates the true value of these example coefficients. Blue curve is the smoothed estimated density curve of each empirical distribution. All 1000 bootstrap estimates of $\Phi_1^{1,20}$, $\Phi_1^{15,25}$, $\Phi_1^{15,40}$, $\Phi_1^{30,25}$, and $\Phi_1^{45,30}$ are zero, so we are not able to plot the point-mass density for these coefficients

sian noise, we are interested to investigate whether the LASSLE method has better specificity, lower bias, lower variance (and thus lower MSE) than the LSE and LASSO methods for other noise distributions, e.g., student’s t -noise (with low degree of freedom) and shifted χ^2 noise. To explore this, we generated time series datasets using Eq. (1.1) under different VAR settings $\{P, d\}$ with P independent t -noise and P independent χ^2 noise, respectively. Then we apply all three methods to estimate the VAR coefficient matrices under each setting and compare their performance in terms of both the specificity of true zero and the general mean-squared error.

3.4.1 Results from Student’s t -Noise

We use P independent $\sqrt{0.06} * t(5)$, of which mean equals to 0 and variance equals to 0.1, to generate the student’s t -noise at time t . Figures 10 and 11 demonstrate the performance comparison of three methods on “Cluster” type and “Scale-free” type data regarding their specificity of true zero under setting $\{P = 50, d = 1\}$. The visualization results imply that LASSLE can capture the true zero coefficient substantially better than LSE. In addition, LASSLE has much lower absolute difference on non-zero coefficients compared to LASSO.

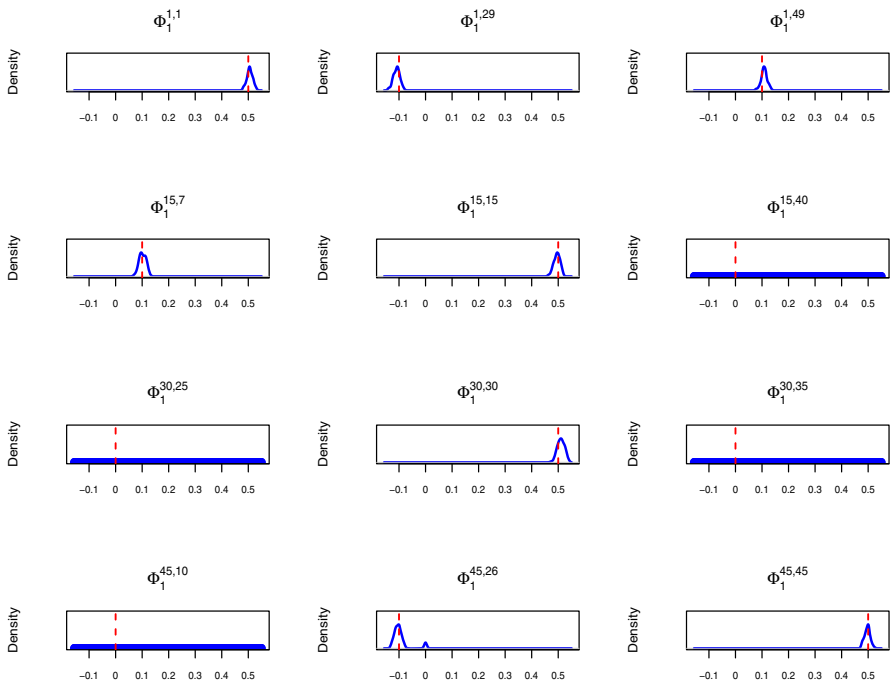


Fig. 8 Sample empirical distribution of “Scale-free” type bootstrapped estimates. Red-dashed line indicates the true value of these example coefficients. Blue curve is the smoothed estimated density curve of each empirical distribution. All 1000 bootstrap estimates of $\Phi_1^{15,40}$, $\Phi_1^{30,25}$, $\Phi_1^{30,35}$, and $\Phi_1^{45,10}$ are zero, so we are not able to plot the point-mass density for these coefficients

Tables 3 and 4 list the MSE results of all three methods on both “Cluster” type and “Scale-free” type data with student’s t -noise under different VAR parameter settings. We can see that LASSLE method still has overwhelming advantage over LSE and LASSO when the number of parameter is large enough (≥ 2500). On the other hand, LSE has slightly lower MSE than LASSLE under low-dimensional parameter setting.

3.4.2 Results from Shifted Zero-Mean χ^2 Noise

To generate P -dimensional shifted χ^2 noise at time t , we employ P independent $\sqrt{0.0125} * \chi_4^2 - \sqrt{0.2}$, with mean of 0 and variance of 0.1. Figures 12 and 13 demonstrate the comparison results of three methods on “Cluster” type and “Scale-free” type data in terms of their specificity of true zero under setting $\{P = 50, d = 1\}$. Based on the visualization results, we can see that LASSLE estimate has very good specificity of true zero coefficients regardless of χ^2 noise.

Tables 5 and 6 list the MSE results of all three methods on both “Cluster” type and “Scale-free” type data with shifted χ^2 noise under different VAR parameter settings. It implies that LASSLE method has significantly lower MSE under most high dimension parameter setting than LSE and LASSO.

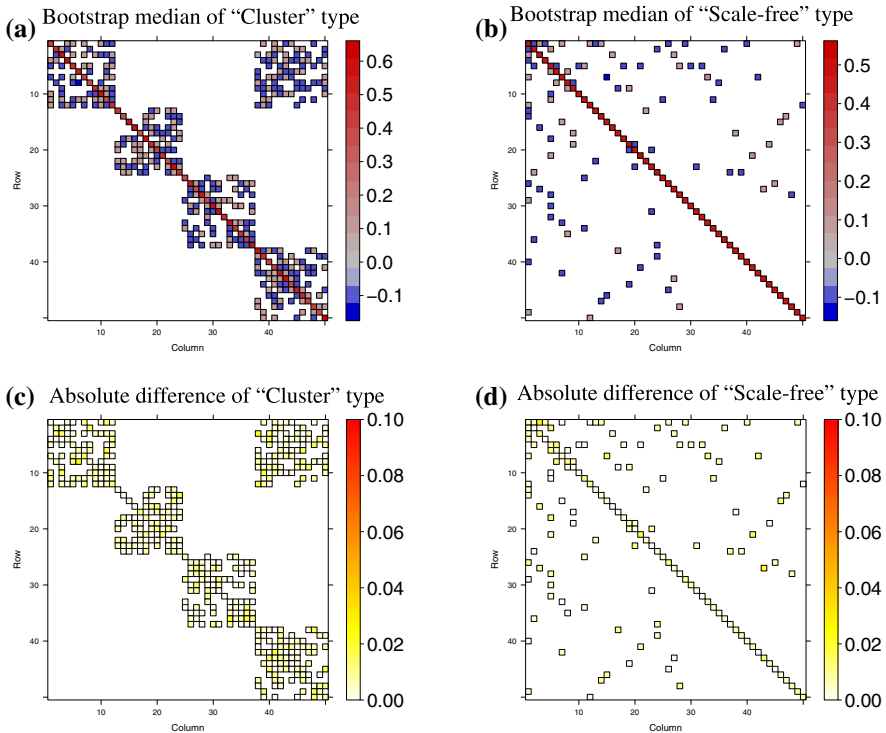


Fig. 9 Bootstrap median of 1000 bootstrapped LASSLE estimates. **a, b** give the median of 1000 bootstrapped LASSLE estimates for “Cluster” type and “Scale-free” type data. **c, d** demonstrate the absolute difference between the median estimated matrix and true coefficient matrix (Color figure online)

4 Application to Effective Connectivity in Multichannel LFPs

In this section, we will fit a VAR model to LFP data recorded from multiple electrodes as rats perform a non-spatial sequence memory task [3] and apply the LASSLE method to estimate the VAR parameters and consequently partial directed coherence. Our objective is to examine and quantify potential connectivity (i.e., effective) among electrodes located in hippocampal region CA1, which is clinically meaningful as this form of sequence memory shows strong behavioral parallels in rats and humans [1], and depends on the hippocampus for both species [6, submitted], [9], and is impaired in normal aging [2].

4.1 Data Description

In the experiment (shown in Fig. 14), rats were presented with repeated sequences of five odors in a single odor port. They were trained to identify whether each odor was presented “in sequence” (by holding their nose poke until the signal) or “out of sequence” (by withdrawing their nose poke before the signal) to

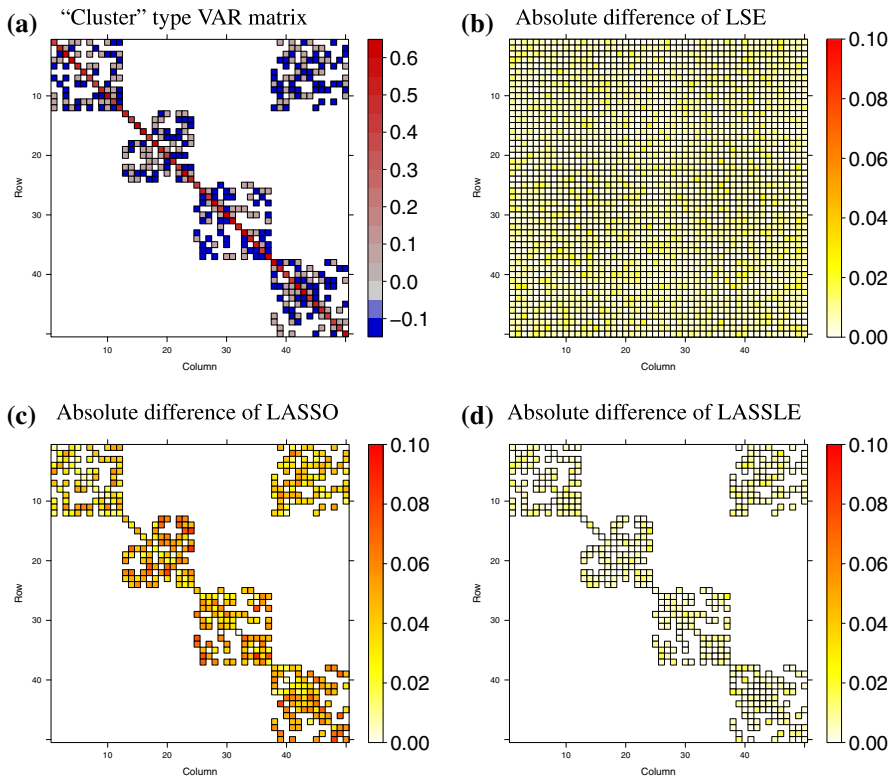


Fig. 10 Comparison of specificity of true zero on “Cluster” type data with student’s t -noise. **a** demonstrates the true VAR(1) coefficient matrix with $P = 50$. **b–d** give the absolute difference between true matrix and estimated matrix by LSE, LASSO, and LASSLE method, respectively (Color figure online)

receive a water reward. The LFP data included here were recorded from CA1 electrodes during a session in which a well-trained rat performed the task at a high level [3].

The full dataset includes LFPs from 23 tetrodes located in the hippocampus and $n = 247$ epochs, where $n = 219$ epochs are “in sequence” (InSeq) and $n = 28$ epochs are “out of sequence” (OutSeq). Each epoch is recorded roughly 1 second with sampling frequency of 1000 Hz and thus has $T = 1000$ time points. We specifically focused our analyses on LFPs from $P = 12$ tetrodes, a subset of electrodes that also recorded clear single-cell spiking activity and were confirmed to be located in the pyramidal layer of CA1 (see estimated tetrode locations in Fig. 15). In addition, LFPs of Epoch 10 are found in Fig. 16. We observe that time series of LFPs from tetrode T13 to tetrode T23 have highly similar temporal pattern, while time series of the remaining tetrodes are highly similar. This is because tetrodes near each other are likely to behave more similarly than those that are far apart.

Figure 17 (left) displays the LFPs from tetrode T22 during the first 30 epochs; the boxplots of its auto-correlation function (ACF) across all 247 epochs; and the boxplots of the partial auto-correlation function (PACF) across all epochs. We

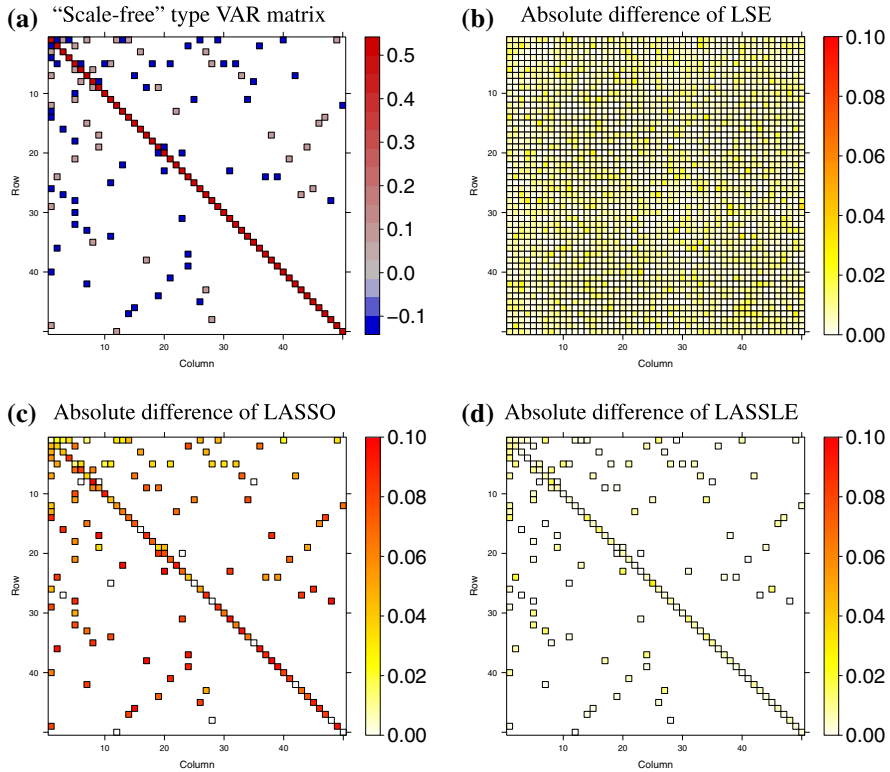


Fig. 11 Comparison of specificity of true zero on “Scale-free” type data with student’s t -noise. **a** demonstrates the true VAR(1) coefficient matrix with $P = 50$. **b–d** give the absolute difference between true matrix and estimated matrix by LSE, LASSO, and LASSLE method, respectively (Color figure online)

Table 3 Comparison of MSE for “Cluster” type data with student’s t -noise

VAR parameter setting			MSE $\times 10^{-3}$		
Number	P	d	LSE	LASSO	LASSLE
100	10	1	7*	184	28
500	10	5	57*	603	73
1000	10	10	147*	741	216
2500	50	1	175	836	37*
5000	50	2	455	1242	98*
10,000	100	1	686	1726	88*

* Lowest MSE among three methods under each VAR parameter setting

observe that the boxplots of ACF fail to drop to zero even after very long lags and there is a cyclical behavior in the pattern. Both of these could be evidence of non-stationarity (or long-memory). These suggest pre-processing the data by taking a first-order difference. The results of LFPs after differencing are shown on the right side of Fig. 17. Compared to the previous plots, the ACF boxplots eventually

Table 4 Comparison of MSE for “Scale-free” type data with student’s *t*-noise

VAR parameter setting			MSE $\times 10^{-3}$		
Number	<i>P</i>	<i>d</i>	LSE	LASSO	LASSLE
100	10	1	6*	134	11
500	10	5	44	278	12*
1000	10	10	124*	728	217
2500	50	1	181	778	50*
5000	50	2	450	1056	24*
10,000	100	1	747	1641	160*

* Lowest MSE among three methods under each VAR parameter setting

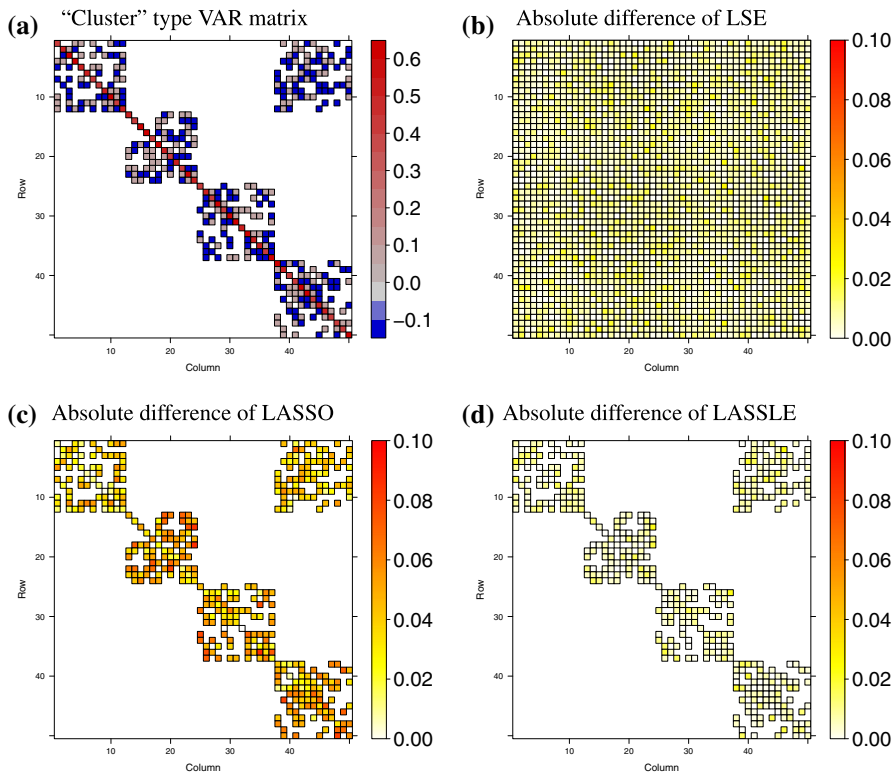


Fig. 12 Comparison of specificity of true zero on “Cluster” type data with shifted zero-mean χ^2 noise. **a** demonstrates the true VAR(1) coefficient matrix with $P = 50$. **b–d** give the absolute difference between true matrix and estimated matrix by LSE, LASSO, and LASSLE method, respectively (Color figure online)

decay to zero with smaller interquartile range, which means that the pre-processed data look more stationary and the correlation drops to zero faster than the original LFPs. Therefore, we will fit the VAR model to the first-order differenced LFPs.

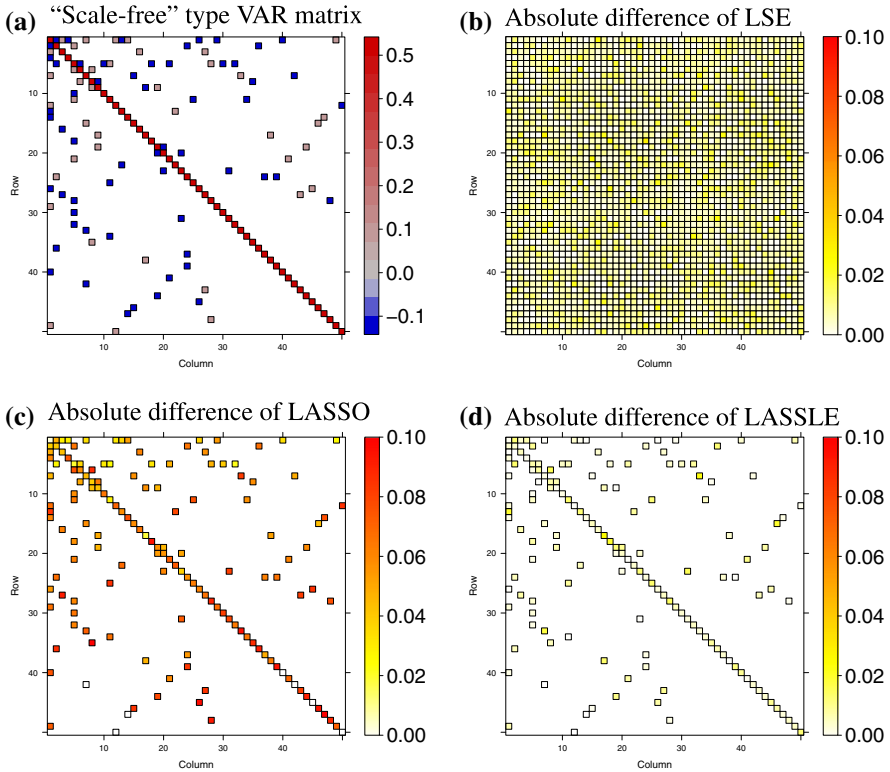


Fig. 13 Comparison of specificity of true zero on “Scale-free” type data with shifted zero-mean χ^2 noise. **a** demonstrates the true VAR(1) coefficient matrix with $P = 50$. **b–d** give the absolute difference between true matrix and estimated matrix by LSE, LASSO, and LASSLE method, respectively (Color figure online)

Table 5 Comparison of MSE for “Cluster” type data with shifted zero-mean χ^2 noise

VAR parameter setting			$MSE \times 10^{-3}$		
Number	P	d	LSE	LASSO	LASSLE
100	10	1	7*	159	14
500	10	5	56	465	41*
1000	10	10	139	561	136*
2500	50	1	182	666	31*
5000	50	2	453	1039	75*
10,000	100	1	696	1572	87*

* Lowest MSE among three methods under each VAR parameter setting

4.2 Preliminary Analysis of a Single Epoch

We first demonstrate fitting the VAR model to a single epoch (Epoch 10 in this example). To select the best lag order \hat{d} , we fit a VAR(d_j) model with candidate order $d_j \in \{1, 2, \dots, 12\}$ and use LSE to estimate the coefficient matrices. Then we apply

Table 6 Comparison of MSE for “Scale-free” type data with shifted zero-mean χ^2 noise

VAR parameter setting			MSE $\times 10^{-3}$		
Number	P	d	LSE	LASSO	LASSLE
100	10	1	8	143	3*
500	10	5	55	224	16*
1000	10	10	129*	654	153
2500	50	1	194	663	22*
5000	50	2	451	967	23*
10,000	100	1	747	1291	40*

* Lowest MSE among three methods under each VAR parameter setting

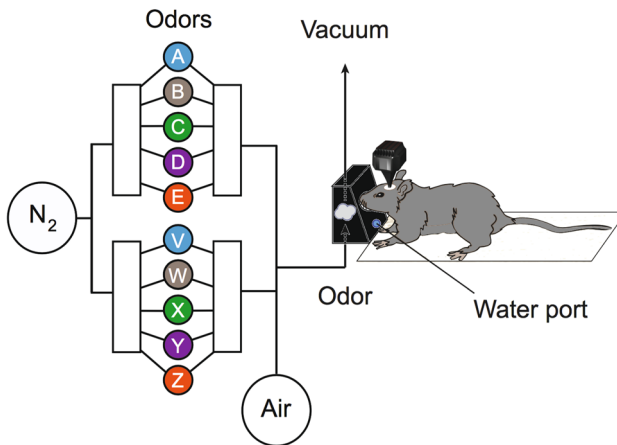


Fig. 14 A non-spatial sequence memory experiment in rats. Rats were presented with repeated sequences of five odors (A, B, C, D, and E) in a single odor port. Each odor presentation was initiated by a nose poke and rats were required to correctly identify the odor as either InSeq (ABCDE) by holding their nose poke until the signal or OutSeq (e.g., ABDDE) by withdrawing their nose poke before the signal

Eqs. (2.17), (2.18), and (2.19) to compute AIC for each candidate order d_j . For epoch 10, the best order (or the minimizer of AIC) was $\hat{d} = 3$. Consequently, there were 3 coefficient matrices (each of dimension 12×12) to estimate.

Figure 18 shows the LASSLE estimates of Φ_1 , Φ_2 , and Φ_3 for Epoch 10. Blanks are assigned to entries whose value is zero, so non-dependence between tetrodes is easy to tell. For entries whose value is not zero, we assign them with colors of red for positive value and blue for negative value, and the strength of dependence is implied by the color-key. As we can see, most diagonal entries of Φ_1 are either red or orange, which implies that signals have strong positive auto-dependence. In addition, upper off-diagonal entries in column 9 to 12 of Φ_1 are mostly blue, which could be evidence that signal of tetrode T7, T8, T9, and T2 at time $t - 1$ has significant negative dependence with signals from other tetrodes location at time t . Compared to Φ_1 , more than half entries in Φ_2 are blank, suggesting that there is no auto- and cross-dependence between those tetrodes at time $t - 2$ and at time t . Column 1 to 8 in Φ_2 are light blue, which implies weak negative dependence between signals from

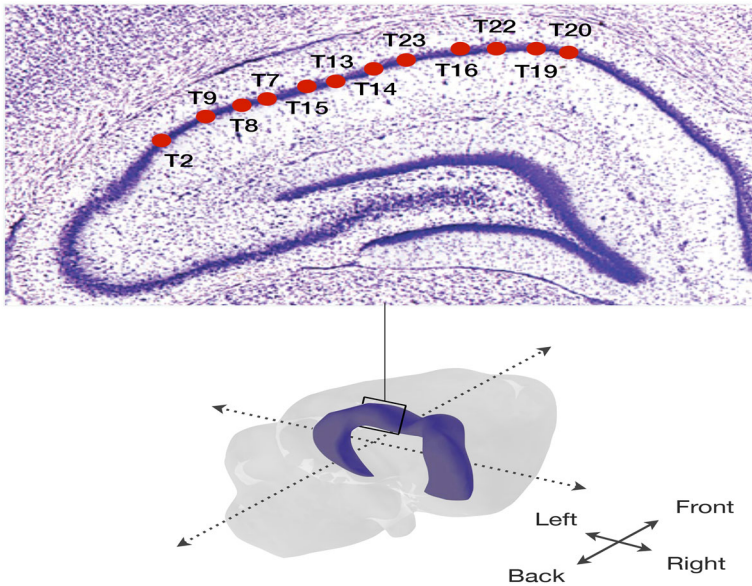


Fig. 15 Estimated location within the hippocampus (dorsal CA1 region) of subset of 12 tetrodes included in the analyses (Color figure online)

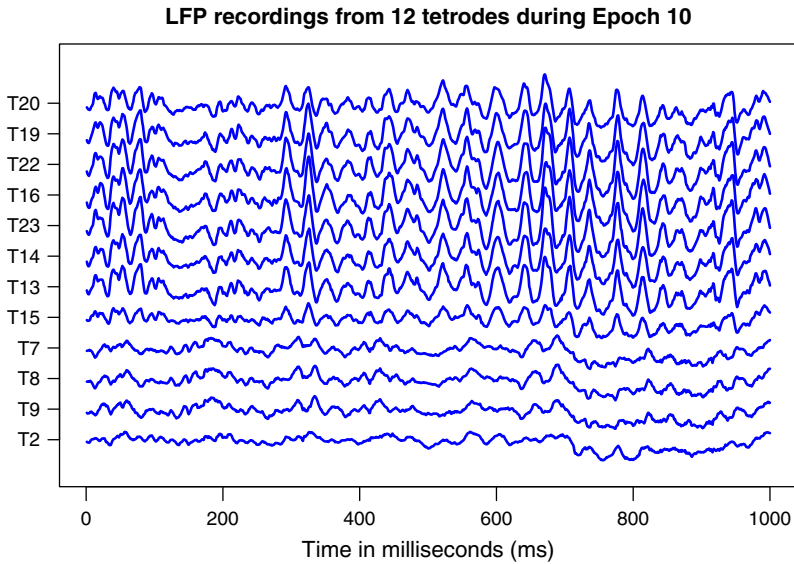


Fig. 16 LFPs from 12 tetrodes studied in this paper during Epoch 10. These LFPs have temporal patterns that can be separated into two clusters. The first consists of T7, T8, T9, and T2 which are all on the posterior (back) portion of the dorsal CA1 region. The second consists of the remaining channels which are all on the anterior portion (front)

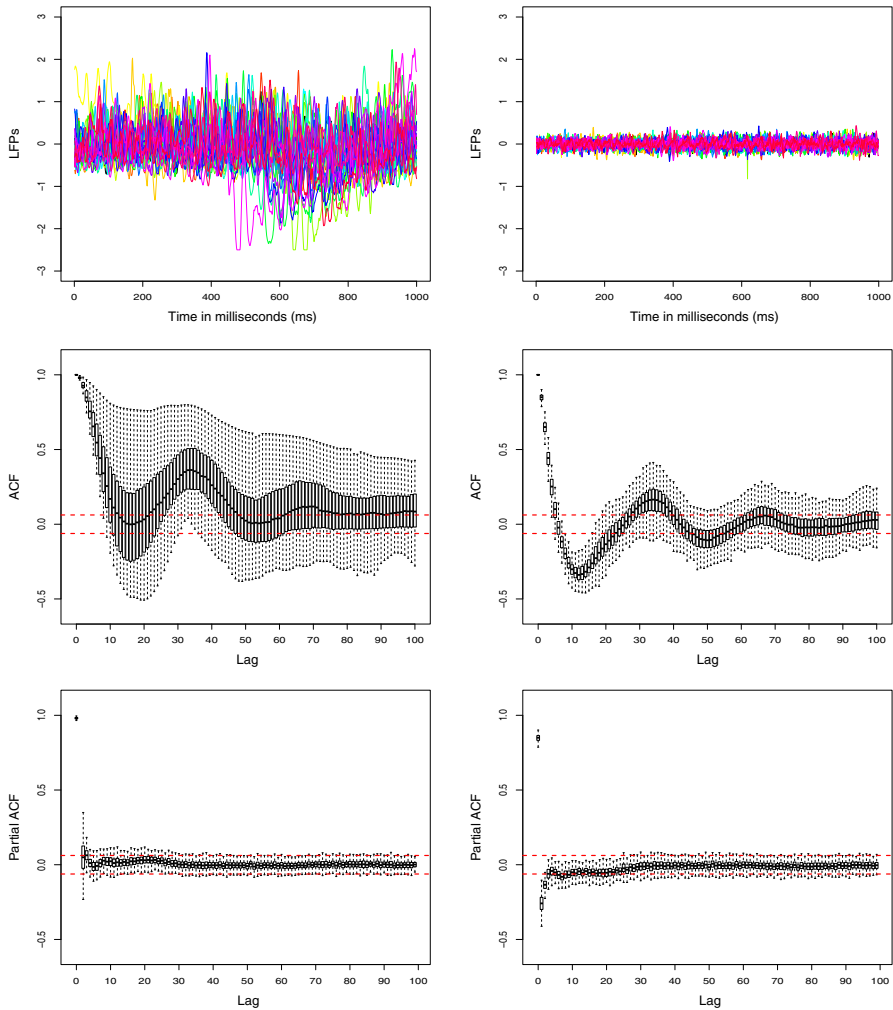


Fig. 17 Top: The LFPs time series plots of the first 30 epochs at tetrode T22 before (left) and after (right) processing. Middle: The boxplots of auto-correlation function (ACF) from tetrode T22 before (left) and after (right) processing across all epochs. Bottom: The boxplots of partial auto-correlation function (PACF) from tetrode T22 before (left) and after (right) processing across all epochs (Color figure online)

tetrode T20, T19, ..., T15 at time $t - 2$ and signals from these tetrodes location at time t . Also, we believe that there is positive dependence between signals from tetrode T7, T9, T2 at time $t - 2$ and signals from tetrode T20, T19, ..., T13 at time t as the color of column 9, 11, and 12 in Φ_2 is orange. However, most entries of Φ_3 are blank and limited non-zero estimates are close to zero, which implies that the dependence between LFPs at time $t - 3$ and time t is very weak.

Next we applied Eqs. (2.15) and (2.16) to the LASSLE estimates to calculate partial directed coherence. PDC was computed at the following frequency bands in the study: δ band (0–4 Hz), θ band (4–8 Hz), α band (8–12 Hz), β band (12–32 Hz), and γ band

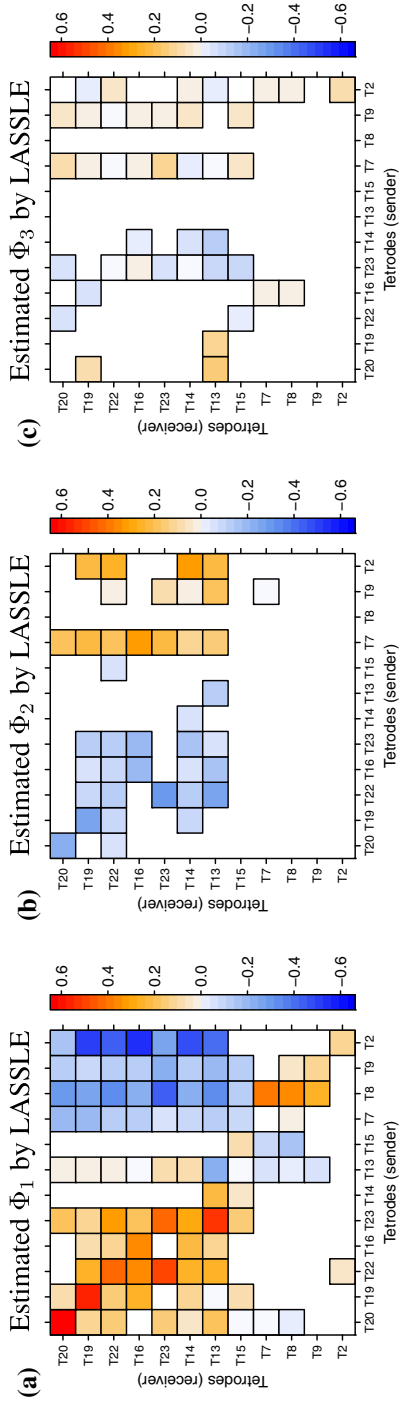


Fig. 18 Estimated coefficient matrices Φ_1 , Φ_2 , Φ_3 in Epoch 10 using the LASSLE method (Color figure online)

(32–50 Hz), which are standard in brain signals analysis. To estimate PDC at specific frequency band, we calculate the average of estimates of PDC over all singleton frequencies in that band. Figure 19 demonstrates the estimated PDC results of these frequency bands in Epoch 10. Since there is only slight change on the estimated PDC across different frequency bands, we use the results of the γ band (shown in Table 7) as representative to explain the PDC. For tetrodes T16, T14, T13, T15, T7, and T9, over 75% of their information can be explained by their own past while most of their information flowing to other tetrodes are very close to 0. More specifically, tetrode T14 has 2.4% information that flows to tetrode T13, and 6.1% information of tetrode T16 flows to tetrode T14. This implies that they tend to have communication with specific tetrodes instead of the entirety. Unlike these tetrodes, tetrodes T20, T19, T22, T23, T8, and T2 have significant amount of information flowing to other tetrodes. For example, the proportion of current tetrode T8 that is explained by its own past is only about 30.0%. This could be evidence that these tetrodes play an important role of passing information to other tetrodes while the rat was engaged in a non-spatial memory task. Estimated PDCs from tetrodes T20, T19, T22, T16, T23, T14, T13, T15 (sender) to tetrodes T7, T8, T9, T2 (receiver) are almost none (the blank on the bottom left of PDC), which suggest that previous oscillatory activity at the γ band of first 8 tetrodes can hardly explain future oscillatory activity at the γ band of last 4 tetrodes as they are far apart in spatial distance.

4.3 Change of Brain Connectivity Across Epochs

We repeat the same procedure for all epochs and select the best VAR order separately. Figure 20 demonstrates the AIC curves of the first 15 epochs, from which we can see some epochs reach the lowest AIC at $\hat{d} = 3$ and some of them are $\hat{d} = 4$. Table 8 shows the distribution of \hat{d} across all 247 epochs. We fit $\text{VAR}(\hat{d})$ to each epoch and estimate the corresponding coefficient matrices by LASSLE method. Figure 21 shows the boxplots of ACF and PACF of residuals fitted from tetrode T22 across all 247 epochs, which is strong evidence that the residuals from tetrode T22 are white noise. The same phenomenon is observed for residuals fitted from other tetrodes.

After computing all the PDCs, we obtain the 95% confidence interval of PDC by summarizing from the empirical distribution if we assume all epochs carry the same connectivity information. However, this assumption may not be true and we are more interested in the variation of PDCs across all epochs, which can help us understand the dynamics of rat's brain connectivity in this memory experiment. To visualize the evolution, we develop Figs. 22 and 23, where PDC matrix (12×12) is converted to a column vector of $12 \times 12 = 144$ elements at each epoch and x-axis indicates the index of epochs. We can clearly see that estimated PDCs at the γ band are quite stable on some tetrode pairs, e.g., tetrode T13 to tetrode T13 (always red color), while PDC estimates of other tetrode pairs are varying with epochs.

To compare the variation of estimated PDCs at the γ band between InSeq epochs and OutSeq epochs, the Kolmogorov–Smirnov (KS) test is used [16]. The null hypothesis of KS test is that the empirical distribution of PDCs from InSeq epochs and that of OutSeq epochs are identical. Here, we use permutation to obtain the empirical

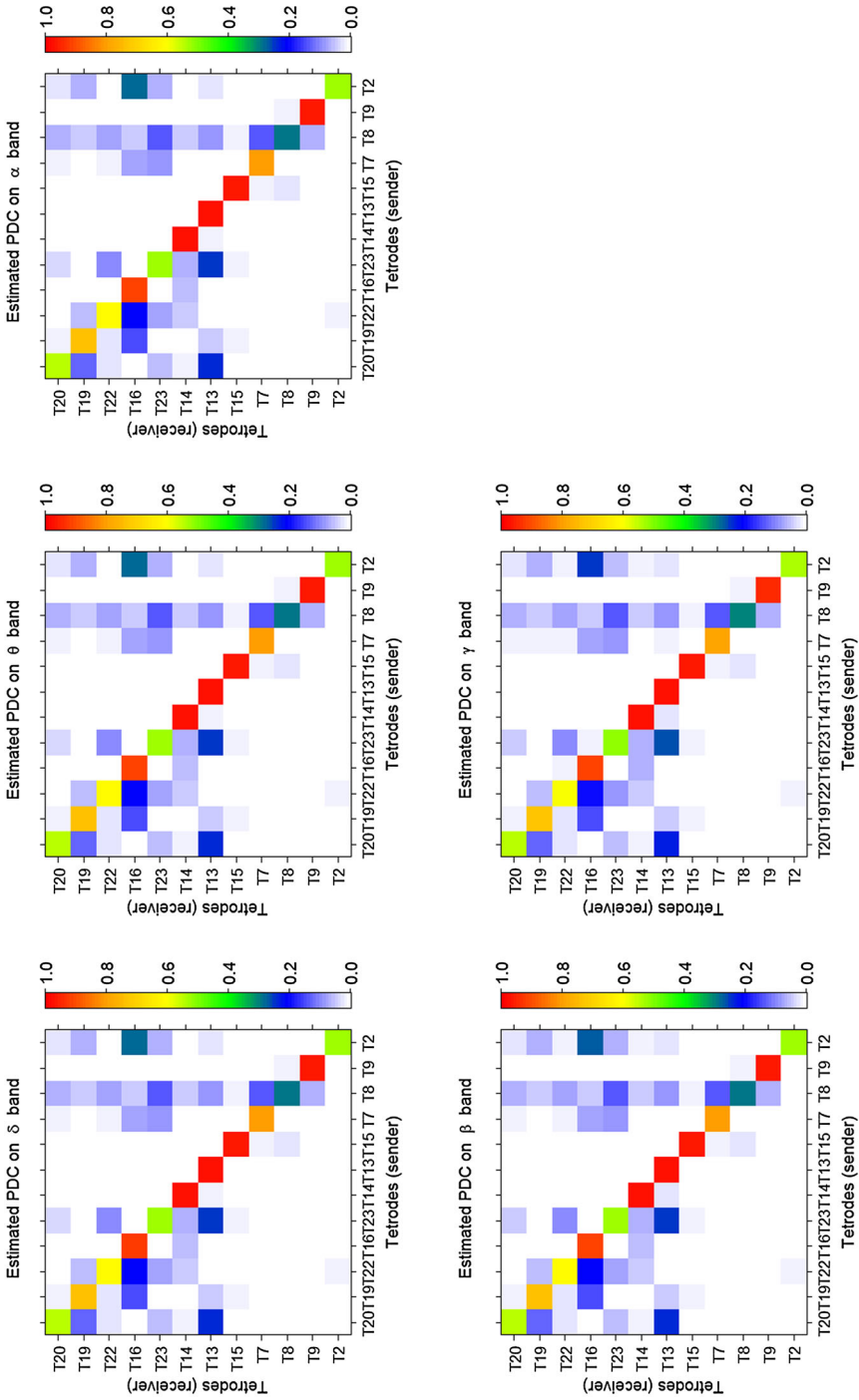


Fig. 19 Estimated PDC by LASSLE of Epoch 10 (Color figure online)

Table 7 Estimated PDC value at the γ band in Epoch 10. The estimated PDC from tetrode T16 to tetrode T22 is 0.010. The estimated PDC from tetrode T22 to T16 is 0.200

Tetrode (receiver)	Tetrode (sender)											
	T20	T19	T22	T16	T23	T14	T13	T15	T7	T8	T9	T2
T20	0.548	0.019	0.005	0.000	0.041	0.000	0.002	0.000	0.018	0.060	0.004	0.021
T19	0.126	0.734	0.054	0.005	0.003	0.000	0.001	0.000	0.011	0.048	0.002	0.062
T22	0.026	0.026	0.593	0.010	0.091	0.000	0.001	0.003	0.017	0.078	0.006	0.019
T16	0.000	0.147	0.200	0.909	0.010	0.000	0.000	0.000	0.073	0.041	0.009	0.252
T23	0.056	0.000	0.085	0.000	0.513	0.000	0.007	0.000	0.082	0.139	0.007	0.058
T14	0.010	0.007	0.043	0.061	0.068	0.971	0.006	0.000	0.001	0.042	0.004	0.019
T13	0.232	0.048	0.008	0.003	0.258	0.024	0.979	0.000	0.009	0.081	0.004	0.029
T15	0.000	0.019	0.000	0.000	0.016	0.005	0.000	0.962	0.002	0.014	0.004	0.000
T7	0.000	0.000	0.000	0.006	0.000	0.000	0.001	0.010	0.786	0.133	0.002	0.002
T8	0.001	0.000	0.000	0.006	0.000	0.000	0.001	0.025	0.001	0.300	0.012	0.002
T9	0.000	0.000	0.000	0.000	0.000	0.000	0.002	0.000	0.000	0.063	0.946	0.000
T2	0.000	0.000	0.012	0.000	0.000	0.000	0.000	0.000	0.000	0.000	0.000	0.536

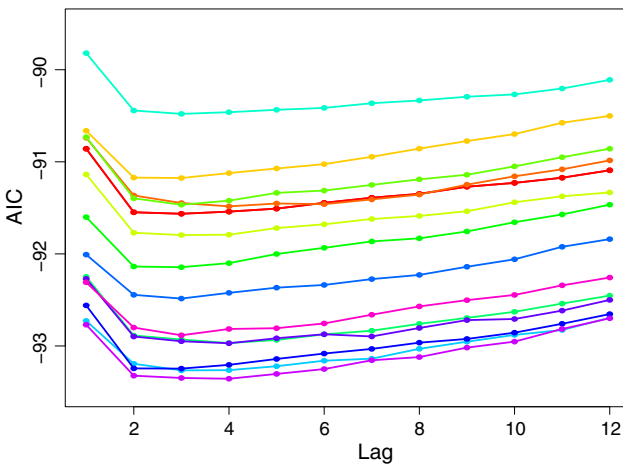


Fig. 20 AIC of fitted VAR on first 15 epochs, lag order range: 1,2,...,12 (Color figure online)

Table 8 Distribution of selected VAR lag order

Selected lag order	2	3	4	5
Number of epochs	64	158	23	2
Proportion (%)	25.9	64.0	9.3	0.8

distribution of KS test statistics. Since it is necessary to preserve the inherent correlation across different epochs, the entire 247 epochs were partitioned into 50 groups where 5 consecutive epochs are within the same group (for the last group, we replicate Epoch 246 and Epoch 247 to make 5 epochs). This idea is inspired by the block

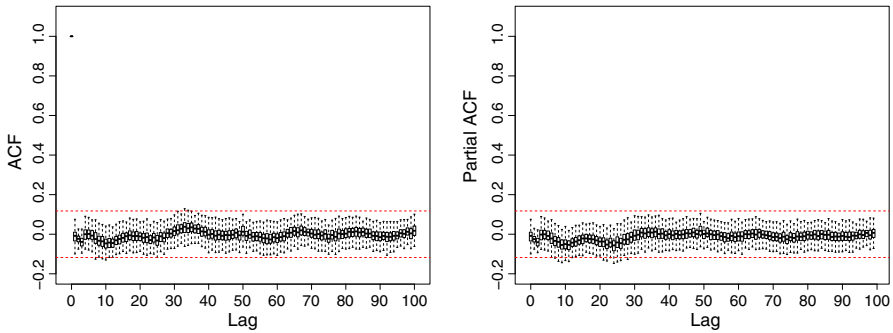


Fig. 21 The boxplots of auto-correlation function (ACF) of residuals fitted from tetrode T22 across all epochs (left). The boxplots of partial auto-correlation function (PACF) of residuals fitted from tetrode T22 across all epochs (right) (Color figure online)

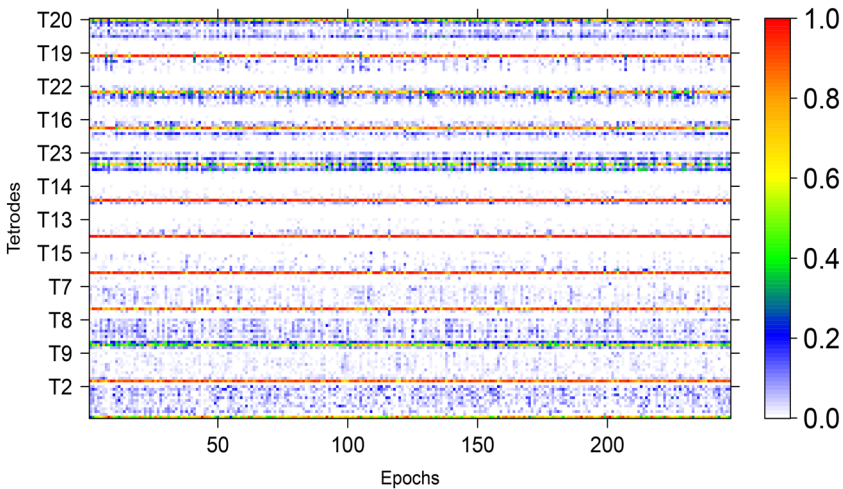


Fig. 22 PDC on γ band across all epochs. X-axis is the index of epochs. At each epoch, PDC matrix (12×12) is converted to a column vector of $12 \times 12 = 144$ elements, where every 12 elements are the PDC values of one tetrode to all 12 tetrodes (Color figure online)

bootstrap procedure for time series. Then, we randomly selected 5 groups (containing 25 epochs) from 50 groups as experimental OutSeq epochs, using the rest as experimental InSeq epochs, and compute the KS-statistic for this new Inseq and OutSeq grouping. This procedure is repeated 10,000 times to obtain the empirical distribution of KS-statistics. Finally, the proportion of permuted KS-statistics with larger values than the real KS-statistic is used as the p value.

Figures 24 and 25 demonstrate the empirical distributions of estimated PDCs for all tetrodes given by Inseq epochs (blue curve) and Outseq epochs (red curve). Based on the p values of KS test, there is strong evidence showing that the variation of auto-PDC of tetrode T19, T22, T23, and T13 is different between Inseq epochs and Outseq epochs (Fig. 24). For these tetrodes, the proportion of their current oscillatory activity that can be explained by their own past activity is influenced by whether odors are presented

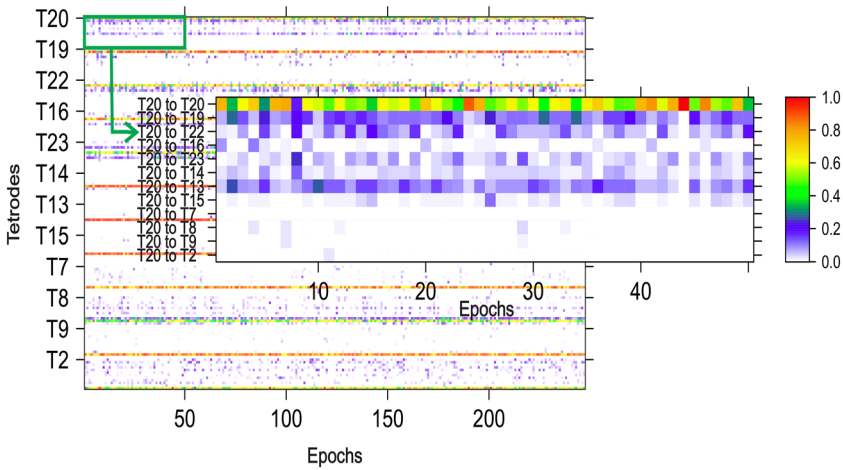


Fig. 23 Illustration of Fig. 22. Every 12 rows in Fig. 22 indicate the PDCs from one tetrode to all 12 trodes across 247 epochs. For example, the first 12 rows demonstrate the PDCs from T20 to T20, T19, ..., T2 at all epochs (Color figure online)

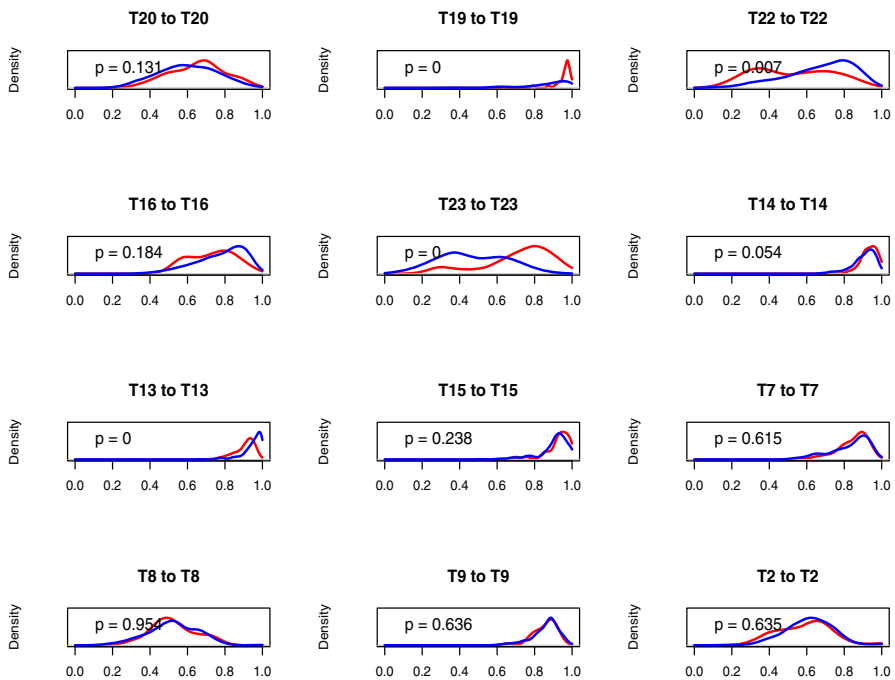


Fig. 24 Density curves of auto-PDCs across all 247 epochs. Blue one is the density curve of InSeq epochs only. Red one is the density curve of OutSeq epochs only. Kolmogorov–Smirnov test is used, where the null hypothesis is that two empirical distributions are the same. p value is obtained from permutation and we reject the null hypothesis when $p <= 0.05$ (Color figure online)

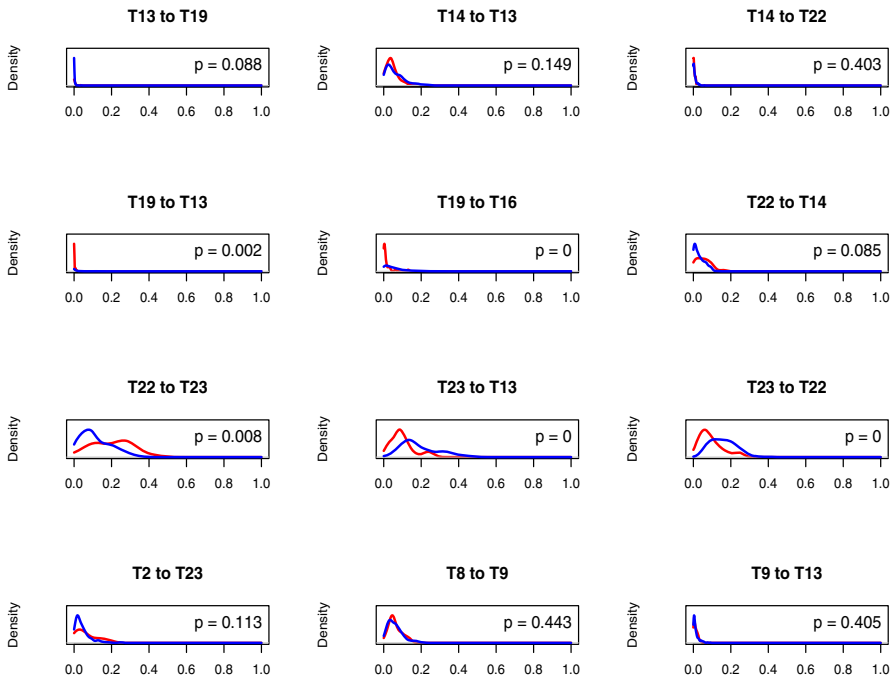


Fig. 25 Density curves of some cross-PDCs across all 247 epochs. Blue one is the density curve of InSeq epochs only. Red one is the density curve of OutSeq epochs only. Kolmogorov–Smirnov test is used, where the null hypothesis is that two empirical distributions are the same. p value is obtained from permutation and we reject the null hypothesis when $p \leq 0.05$ (Color figure online)

in the correct or incorrect sequence position (Inseq or Outseq, respectively). However, for the remaining tetraodes, the variation in their estimated auto-PDC is quite stable across Inseq epochs and Outseq epochs. As shown in Fig. 25, p values also indicate that the variation of estimated PDC from tetraode T19, T22, and T23 (sender) to some other tetraodes (receiver) is significantly different between Inseq epochs and Outseq epochs, which suggests that the information flowing from these tetraode locations to others is also influenced by the Inseq/Outseq status of the presented odor.

4.4 Comparison of Three Methods on PDC Across All Epochs

We also apply traditional methods (LSE only and LASSO only) to estimate VAR coefficients and then compute the PDC for each epoch separately. Figures 26 and 27 demonstrate the density curve of auto-PDCs and some cross-PDCs estimated by three methods across all epochs. The red curve is given by LASSLE method; the blue one is via LSE, and the green one is achieved by LASSO. As we can see, the red curve is close to the blue one for most PDCs. This is because each estimated PDC is mostly influenced by some dominant non-zero VAR coefficients, of which the estimates are close to each other by LASSLE and LSE separately. Noted that LASSO method has shrunk many VAR coefficients to zero and its non-zero estimates are very different

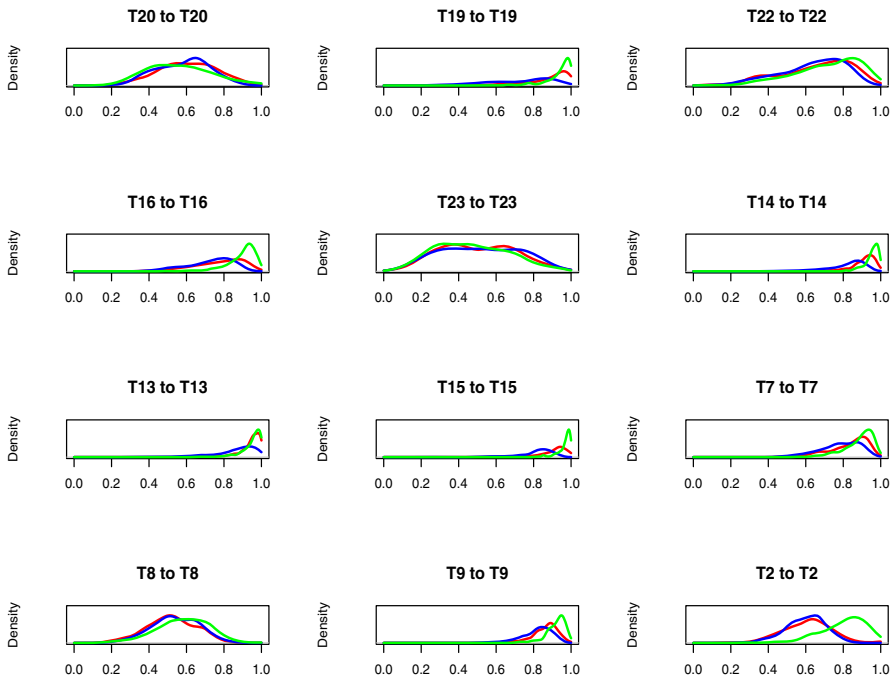


Fig. 26 Density curves of auto-PDCs across all 247 epochs given by three methods. The red curve is LASSLE; the blue one is LSE, and the green one is LASSO (Color figure online)

from those by LSE. Consequently the green curve is dissimilar to the blue one for most PDCs.

5 Conclusion

In this paper, we proposed a hybrid LASSLE (LASSO + LSE) method to estimate the coefficients of vector autoregressive models characterizing the effective and directional connectivity for multichannel brain physiological signals. This method uses regularization to control for sparsity on the first stage and then use least squares to improve bias and mean-squared error of the estimator on the second stage. Compared to the separate LASSO and LSE, the advantage of our method is that it is able to both indicate the most important effective connectivity and give a more accurate estimate of the connectivity strength. Note that sparse VAR coefficient estimates can still capture complex dependency structures in a multivariate time series. In addition, we employ partial directed coherence to measure the directional connectivity between the channels. PDC is a directed frequency-specific measure that explains the extent to which the present oscillatory activity in a sender channel influences the future oscillatory activity in a specific receiver channel relative to all possible receivers in the network. The proposed modeling approach provided key insights into potential functional relationships among simultaneously recorded sites during performance of a complex memory task.

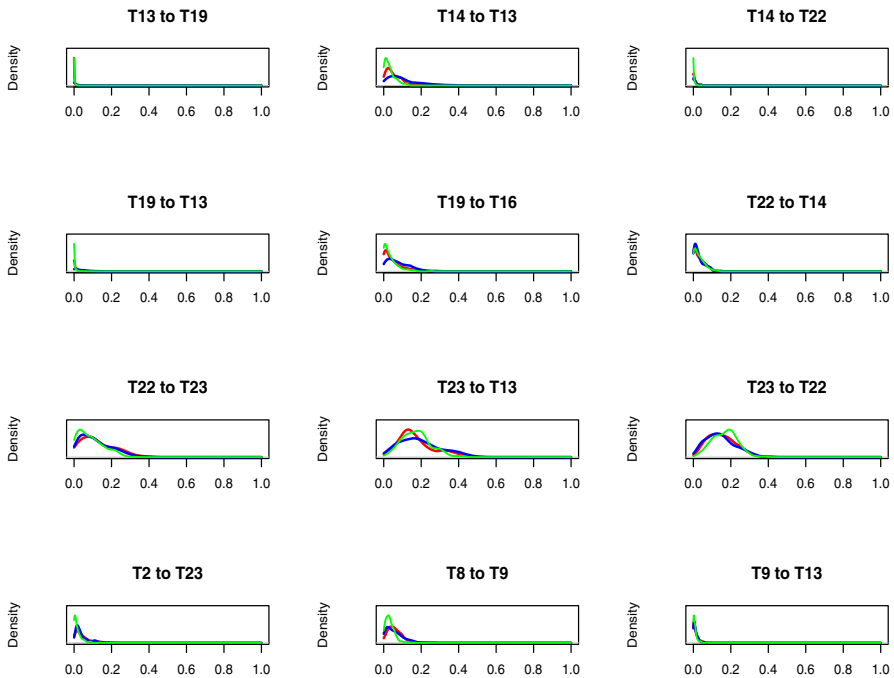


Fig. 27 Density curves of some cross-PDCs across all 247 epochs given by three methods. The red curve is LASSLE; the blue one is LSE, and the green one is LASSO (Color figure online)

Specifically, this novel method was successful in revealing patterns of effective connectivity across tetrode locations, by quantifying how present oscillatory activity in each tetrode is influenced by past oscillatory activity in other tetrodes. This approach was also successful in capturing how this effective connectivity varied across trial epochs and trial types (Inseq or Outseq).

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