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# Pretreatment Dynamic Contrast-Enhanced MRI Improves Prediction of Early Distant Metastases in Patients With Nasopharyngeal Carcinoma

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Abstract: The identification of early distant metastases (DM) in patients with newly diagnosed, previously untreated nasopharyngeal carcinoma (NPC) plays an important role in selecting the most appropriate treatment approach. Here, we sought to investigate the predictive value of distinct MRI parameters for the detection of early DM.

Between November 2010 and June 2011, a total of 51 newly diagnosed NPC patients were included. All of the study participants were followed until December 2014 at a single institution after completion of therapy. DM was defined as early when they were detected on pretreatment FDG-PET scans or within 6 months after initial diagnosis. The following parameters were tested for their ability to predict early DM: pretreatment FDG-PET standardized uptake value (SUV), MRIderived AJCC tumor staging, tumor volume, and dynamic contrastenhanced (DCE) values. The DCE-derived  $v_e$  was defined as the volume fraction of the extravascular, extracellular space.

Compared with patients without early DM, patients with early DM had higher SUV, tumor volume, DCE mean (median)  $v_e$ ,  $v_e$  skewness,  $v_e$ kurtosis, and the largest mean  $v_e$  selected among sequential slices  $(P < 0.05)$ . No differences were identified when early DM were defined only according to the results of pretreatment FDG-PET. Among different quantitative DCE parameters, the mean  $v_e$  had the highest area under curve (AUC, 0.765). However, the AUCs of SUV, tumor volume,

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mean  $v_e$ ,  $v_e$  skewness,  $v_e$  kurtosis, or the largest mean  $v_e$  selected among the sequential slices did not differ significantly from one another  $(P = 0.82)$ .

Taken together, our results suggest that DCE-derived  $v_e$  may be a useful parameter in combination with SUV and tumor volume for predicting early DM. Dynamic contrast-enhanced MRI may be complementary to FDG-PET for selecting the most appropriate treatment approach in NPC patients.

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Abbreviations: AJCC = American Joint Committee on Cancer, AUC = area under curve, CCRT = concurrent chemoradiation, CT = computed tomography, DCE-MRI = dynamic contrast-enhanced magnetic resonance imaging, DM = distant metastases, FDG-PET = fluorodeoxyglucose positron emission tomography,  $K^{\text{trans}}$  = forward volumetric transfer constant, NCCN = National Comprehensive Cancer Network, NPC = nasopharyngeal carcinoma, ROC = receiver operating characteristic, ROI = region of interest, RT = radiotherapy, SD = standard deviation, SUV = standardized uptake value,  $v_e$  = volume fraction of the extravascular extracellular space,  $v_p$  = volume fraction of blood plasma.

#### INTRODUCTION

 $N_{\text{Asia}}$ , with a reported annual incidence >20 cases per [1](#page-8-0)00,000 persons per year.<sup>1</sup> Definitive radiotherapy (RT) or concurrent chemoradiotherapy (CCRT) remain the mainstay of treatment for NPC.<sup>[2,3](#page-8-0)</sup> Current pretreatment diagnostic imaging modalities—including MRI and FDG-PET—can provide precise tumor delineation, ultimately improving the efficacy of intensity-modulated RT and widening the therapeutic window. Recently published data have shown that contemporary treatment protocols have markedly improved outcomes, with 5-year local control and nodal control rates of  $\sim$ 90% and  $\sim$ 95%, respectively.<sup>[3](#page-8-0)</sup> Unfortunately, the occurrence of distant metastases (DM) remains a major clinical issue, with a reported 5 year incidence as high as  $28\%$ <sup>[4,5](#page-8-0)</sup> Efforts aimed at reducing failures from occult DM through the use of neoadjuvant or adjuvant chemotherapy in patients with advanced stages have been unsatisfactory.<sup>[6](#page-8-0)</sup> Beyond traditional prediction strategies based on AJCC staging, the development of new tools for identifying patients at risk of occult DM is eagerly awaited for improving treatment outcomes. Although different strategies have been proposed, their clinical utility and the reciprocal relationships among different parameters remain unclear.<sup>[7,8](#page-9-0)</sup> Several factors have been linked to the presence of occult DM,

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including tumor volume, angiogenesis, the percentage of hypoxic tumor cells, the fraction of connective tissue and necrosis, and the interstitial fluid pressure. Moreover, the risk of DM has been related to AJCC N-stage and standardized uptake values (SUV) on FDG-PET images.<sup>[9,10](#page-9-0)</sup> In contrast, the current T-stage has limited value in the prediction of DM-free  $\,$ survival. $^{11}$  $^{11}$  $^{11}$ 

Dynamic contrast-enhanced (DCE) MRI is a method based on the acquisition of subsequent T1-weighted images before, during, and after the administration of a contrast agent (gadolinium) through a rapid scanning technique. DCE-MRI parameters have been successfully used for assessing tumor response to chemoradiation and antiangiogenesis therapies.[12,13](#page-9-0) Studies of DCE-MRI have been conducted for determining the response to treatment in patients with head and neck tumors, although no data on its usefulness for the detection of DM are currently available.<sup>7,13-15</sup> However, semiquantitative DCE-MRI and the enhancement washout parameter have been shown to predict early DM in patients with breast cancer.<sup>[7](#page-9-0)</sup> In this scenario, we designed the present study to investigate the potential utility of FDG-PET and DCE-MRI in the identification of early DM in a cohort of 51 NPC patients followed for a median of 3 years. Specifically, quantitative parameters including SUV, tumor volume, and DCE-derived variables (ie, forward volumetric transfer constant  $[K<sup>trans</sup>]$ , volume fraction of the extravascular extracellular space [EES]  $[v_e]$ , and volume fraction of blood plasma  $[v_n]$ ) were examined.

### PATIENTS AND METHODS

#### Patient Characteristics and Treatment Modalities

The study protocol followed the tenets of the Helsinki declaration and ethical approval was granted by the local Institutional Review Board. The research was designed a retrospective review of prospectively collected data. Between November 2010 and June 2011, patients with newly diagnosed, histology-proven NPC were considered for inclusion. All patients with a World Health Organization classification type I (squamous cell carcinoma), type II (keratinizing and nonkeratinizing undifferentiated carcinoma), and papillary adenocarcinoma were deemed eligible. Staging was based on MRI and PET/CT imaging according to the AJCC staging system (seventh edition). Patients were treated according to the NCCN guidelines at a single tertiary medical center by a multidisci-plinary head and neck cancer team.<sup>[2](#page-8-0)</sup> No patient received RT, but cisplatin-based CCRT was given with curative intent to all patients with stage II-IVB disease. Patients with DM (ie, stage IVC) were initially treated with chemotherapy and then switched to CCRT in the presence of a positive response. Patients with DM located in the cervicothoracic spine (ie, an area that could be covered by the RT field) were treated directly with CCRT.

### Follow-Up Protocol

Patients were followed at the radiation oncology clinic every week during treatment, then every 3 months for 2 years, and every 4 months for the subsequent 2 years. The initial surveillance MRI and FDG-PET scans were performed within 6 months after RT completion, and then on a yearly basis. Patients with suspected disease recurrence underwent additional imaging. Whenever possible, fiberscopic-guided or imaging-guided biopsies were obtained in the presence of suspicious malignant lesions. If a lesion biopsy was not feasible or yielded negative results, close clinical and imaging followup was pursued for the subsequent 3 months. Patients with tumors confined to the primary site or the neck were classified as having local disease or regional residual/recurrent tumors. Patients with malignant disease beyond the head and neck region were classified as having DM. With regard to DM, patients were divided into the following 3 groups: patients without DM; patients with early DM (ie, DM identified before treatment or up to 6 months after the initial diagnosis); patients with late DM (ie, DM identified after  $>6$  months from the initial diagnosis). Patients with DM identified within 6 months of treatment were categorized into the early DM group (because distant lesions were missed in the pretreatment staging workup and considered as occult). Cases with early DM diagnosed within 6 months of treatment were identified through surveillance FDG-PET and MRI scans and subsequently verified by pathology whenever possible. When pathological confirmation was not possible, patients were followed using clinical and imaging methods for at least 3 years.

## MRI Imaging

DCE-MRI studies were performed on a 3T GE Discovery MR750 scanner (GE Healthcare, Waukesha, WI) with a dedicated head and neck coil. Initial  $T_2$ -weighted anatomical scans were acquired by an expert radiologist (Chin SC) to select an axial plane through the tumor center. Twelve slices centered on this plane were collected for the DCE-MRI study. A 3-dimensional spoiled gradient-echo sequence with different flip angles was applied to obtain  $T_1$  maps before contrast injection  $(T_{10}$  maps). The imaging parameters were as follows: repetition time (ms)/echo time (ms) =  $4.9/1.3$ , flip angle =  $2, 5, 10, 20$ , and 30°, field-of-view =  $256 \times 256$  mm, matrix size =  $256 \times 128$ ,  $ASSET = 2$ , and slice thickness = 6 mm. The same sequence and parameters (the only exception being a fixed flip angle of  $30^{\circ}$ ) were used for T<sub>1</sub>-weighted DCE-MRI. Sixty dynamic measurements were acquired during a total acquisition time of 234 s (sampling interval =  $3.9$  s). A bolus (0.1 mmol/kg) of a gadolinium-based contrast agent (Magnevist; Bayer Schering Pharma AG, Berlin, Germany) was injected through an antecubital vein using a power injector (injection rate  $=$  4 mL/s). The injection of contrast agent began at the tenth measurement after starting of the dynamic scan. The postcontrast  $T_1$ -weighted images were acquired after DCE-MRI acquisition.

#### Data Analysis

DCE-MRI data were analyzed using an in-house software platform [\(http://kyungs.bol.ucla.edu/software/\)](http://kyungs.bol.ucla.edu/software/), a freely available plug-in tool for OsiriX (an open-source medical imaging processing software) implemented in the Cocoa environment of Mac OS X<sup>[16](#page-9-0)</sup> Quantitative MRI parameters (ie, individual tumor area, tumor volume, and  $K<sup>trans</sup>$ ,  $v<sub>e</sub>$ , and  $v<sub>p</sub>$  based on the extended Tofts model) were obtained from either the entire tumor or individual slices. The MRI-derived primary tumor volume including the gross tumor volume of the primary malignancy and possibly the confluent retropharyngeal nodes with indistinct margins—was calculated. Based on postcontrast axial T1 weighted images, the delineation of solid and enhancing nasopharyngeal tumor was performed slice-by-slice. Intratumor necrotic areas and encased vessels were avoided. The tumor ROIs were subsequently copied to physiological DCE-MRI parameters. The spoiled gradient echo signal equation was used

to obtain the T10 map for each participant by fitting the images obtained with different flip angles,  $S(\alpha)$ :

$$
S(\alpha) = k \frac{\left(1 - \exp(-TR/T_{10})\right) \cdot \sin \alpha}{1 - \exp(-TR/T_{10}) \cdot \cos \alpha} \tag{1}
$$

where  $\alpha$  is the flip angle and k is a proportional constant. To convert the DCE signal time curve,  $S(t)$ , to the concentration time curve of the contrast agent,  $C(t)$ , the following equation was used under the assumption that C(t) was proportional to the changes in the longitudinal relaxation rate,  $\Delta R_1(t)$ :

$$
C(t) \propto \Delta R_1(t) = -\frac{1}{TR} \ln \left( \frac{K \cdot S(t)/S_0 - 1}{K \cdot S(t) \cdot \cos \alpha - 1} \right) - R_{10} \tag{2}
$$

where  $S_0$  is the baseline signal before the bolus injection  $R_{10} = 1/T_{10}$  and  $K = (1 - \exp(-TR \cdot R_{10}))/(1 K = (1 - \exp(-TR \cdot R_{10})) / (1 \exp(-TR \cdot R_{10}) \cdot \cos \alpha$ 

The quantitative physiological parameters  $K<sup>trans</sup>$ ,  $v<sub>p</sub>$ , and  $v<sub>e</sub>$ were obtained pixel-by-pixel using the extended Tofts model. The concentration time curves of the tissue,  $C_T(t)$ , were fitted to the following equation using the least-squares algorithm:

$$
C_T(t) = v_P \cdot C_P(t) + K^{\text{trans}} \int_0^t C_P(\tau)
$$

$$
\cdot \exp\left(\frac{-K^{\text{trans}}}{V_e} \cdot (t - \tau)\right) d\tau \tag{3}
$$

where  $C_P(t)$  is the arterial input function obtained from a voxel in the internal carotid artery of each individual patient, detected using a semiautomated DCE tool in the OsiriX software.

We avoided necrotic tissue for analyzing DCE-MRI data using postcontrast  $T_1$  images as a reference to draw the tumor ROI. We did not include zero or unphysiological  $v_e$  (ie, values not between 1 and 0) when analyzing all results, including the smallest mean  $v_e$  selected among sequential slices.

#### PET/CT Imaging

PET/CT imaging was performed with a PET/CT scanner (Discovery ST 16 integrated PET/CT system; GE Healthcare, Milwaukee, WI ). Helical CT was performed from the head to proximal thigh before FDG-PET acquisition. PET/CT scans were performed 50 to 70 min after injection of  $^{18}$ F-FDG (370) MBq). PET images were obtained in the 2-dimensional mode with a 3-min scanning time per table position. CT images were used for attenuation correction of PET images and acquired with the following settings: 120 kV, automatic mA (ranging from 10 to 300 mA), pitch 1.75:1, collimation  $16 \times 3.75$  mm, and rotation cycle 0.5 s. The maximal standardized uptake value (SUV) of the primary tumor was recorded.

#### Statistical Analysis

The OsiriX-generated DCE-MRI parametric values from the entire tumor volume and individual slices were analyzed with the SPSS software (version 17; SPSS Inc., Chicago, IL). The  $\chi^2$  test, Fisher's exact test, and trend test were used to compare categorical variables, as appropriate. The Mann– Whitney  $U$  test was used for continuous parameters. We compared the accuracy of the prediction models using ROC analysis with simple logistic regression analysis. A 2-tailed  $P$  value  $< 0.05$  was considered statistically significant.

#### RESULTS

#### Patient Characteristics

A total of 51 patients were included in the study. Of them, 37 (72.5%) were men. The median age was 48.68 years (range: 11–78 years; mean: 49.5 years; Table 1). The median follow-up time was 42 months (from January 2011 to December 2014). Eight (15.7%) patients had local recurrence, 10 (19.6%) neck nodal recurrence, and 15 (29.4%) DM. Patients were



 $AJCC =$  American Joint Committee on Cancer, NPC = nasopharynnasopharyngeal carcinoma,  $SD =$ standard deviation, WHO = World Health Organization.

categorized into 3 groups according to the presence and timing of DM, as follows: no DM ( $n = 36$ ), early DM ( $n = 9$ ), and late DM ( $n = 6$ ). In the early DM group, 6 patients were diagnosed by pretreatment FDG-PET imaging, whereas the remaining 3 were detected up to 6 months after the initial diagnosis.

[Table 2](#page-5-0) depicts the clinical characteristics of patients with DM ( $n = 15$ ). Cases #8, 11, 16, 21, 31, and 51 were diagnosed in the pretreatment phase as having M1 disease. Of them, cases # 8 and 51 were treated with CCRT due to DM limited to the neck area. The remaining 4 cases received chemotherapy. Of them, cases # 11 and 21 were subsequently treated with CCRT because M1 lesions responded well. [Figure 1](#page-6-0) presents the co-registered pretreatment anatomical MR images and colorcoded DCE-MRI  $v_e$  maps for 2 patients with and without DM, respectively. Notably, case # 16 (having T1N2 disease) showed DM (lower tumor volume but higher  $v_e$  mean and  $v_e$  mean\_slice\_max). In contrast, case # 24 (having T4N3a disease) was free of DM (higher tumor volume but lower  $v_e$  mean and  $v_e$ \_mean\_slice\_max).

# Differences in Histology and AJCC TNM Parameters Between Early DM Group and Other Groups (No DM and Late DM)

We then divided the study participants in subjects with early DM  $(n = 9, 17.6%)$  and grouped together patients with either no DM or late DM  $(n=42, 82.3\%)$ . Both AJCC Nclassification and AJCC staging were significant predictors of early DM (both  $P < 0.001$ ), whereas AJCC T-classification was not ( $P = 0.204$ ; [Table 3](#page-6-0)).

When all patients with DM were grouped together (early DM plus late DM), we found that the proportion of DM increased in parallel with the AJCC N-classification (N0 to  $N3b = 12.5\%, 13.0\%, 50.0\%, 33.3\%, \text{and } 100.0\%, \text{respectively};$ trend test,  $P = 0.001$ ; Fisher's exact test,  $P = 0.003$ ). The proportion of DM also increased significantly in parallel with the initial disease stage (stage I, II, III, IVa, and IVb =  $0\%, 0\%,$ 26.7%, 23.1%, 25.0%, and 100.0%, respectively; trend test,  $P = 0.001$ ; Fisher's exact test,  $P = 0.001$ ). In contrast, the proportion of DM did not significantly increase according to the T-classification (T1 to T4 = 6.7 %, 60.0%, 35.7%, and 35.3%, respectively; trend test,  $P = 0.116$ , Fisher's exact test,  $P = 0.065$ ; [Table 3](#page-6-0)). In addition, the occurrence of early DM did not correlate with histology, possibly because the great majority of cases were classified as WHO Type III (92.2%, 47/51, data not shown in [Table 3\)](#page-6-0).

# Differences in SUV, Tumor Volume, and Pharmacokinetic Parameters Between Early DM Group and Other Groups (No  $DM +$  Late DM)

[Table 4](#page-7-0) compares the imaging parameters in the early DM group versus the no DM and late DM (combined) group. Both mean SUV and tumor volume were significantly higher in the early DM group than in the other group (SUV:  $15.876 \pm 3.599$ [SD] vs  $11.986 \pm 4.297$ , respectively;  $P = 0.014$ ; tumor volume  $\text{[cm}^3$ : 30.798  $\pm$  18.844 vs 17.160  $\pm$  18.050, respectively;  $P = 0.008$ ). The mean  $v_e$  of tumor volume was significantly higher in the early DM group than in the other group  $(0.249 \pm 0.116 \text{ vs } 0.186 \pm 0.118, \text{ respectively}; P = 0.018).$ We also observed a significantly higher mean  $v_e$  selected among sequential slices in the early DM group than in the other group  $(0.359 \pm 0.147 \text{ vs } 0.265 \pm 0.156, \text{ respectively}; P = 0.014)$ . In addition, the histographic patterns of  $v_e$  skewness and kurtosis were significantly lower in the early DM group. Mean  $K<sup>trans</sup>$  and  $v_p$  did not differ significantly in the 2 groups ( $P > 0.05$ ). The differences in SUV, tumor volume, and  $v_e$ -related parameters between the early DM and late DM groups were similar to those observed when the early DM group was compared with the no DM and late DM groups ([Table 4\)](#page-7-0). The analysis of median values produced similar results.

## Diagnostic Performance of SUV, Tumor Volume, and Pharmacokinetic Parameters in Differentiating Early DM, No, and Late DM Groups

[Table 5](#page-7-0) summarizes the AUCs, sensitivities, and specificities for differentiating the early DM group  $(n = 9)$  from the other groups (n = 42) using SUV, tumor volume, and  $v_e$ -related parameters. Significant differences were identified between the 2 groups. The mean  $v_e$  had the highest AUC (0.765) for distinguishing the early DM group from the other groups. In contrast, SUV showed the lowest AUC, the highest sensitivity, and the lowest specificity. However, no significant differences were identified between the AUCs of SUV, tumor volume, mean  $v_e$ ,  $v_e$  skewness,  $v_e$  kurtosis, or the largest mean  $v_e$  selected among sequential slices  $(P = 0.82)$ .

#### **DISCUSSION**

The treatment approach for newly diagnosed NPC differs according to their AJCC TNM stage. In general, treatment with curative intent is not performed when DM are diagnosed before treatment. Currently, the detection of early DM is entirely based on the presence of FDG-avid lesions on pretreatment FDG-PET scans. In the present study, we hypothesized that pretreatment FDG-PET could underestimate the occurrence of early DM and investigated whether other imaging modalities may improve their diagnosis. Here, we tentatively included in the early DM group all of the patients with metastases detected up to 6 months after their initial diagnosis. The result revealed that SUV, tumor volume, and  $v_e$ -related parameters had the potential to discriminate newly diagnosed NPC patients with early DM from those with either late or no DM ([Figure 2\)](#page-8-0). Patients with early DM generally showed larger tumor volume, SUV, and  $v_e$ -related values than those with late DM and no DM. This difference was not evident when the early DM group was defined solely according to pretreatment FDG-PET results.

Albeit limited by the small sample size, this pilot study shows the potential value of DCE-MRI compared with the traditional imaging modalities. Differently from pretreatment FDG-PET, conventional MRI does not currently allow a wholebody survey for the detection of DM. Our current findings indicate that DCE-MRI may be even superior to FDG-PET for the detection of early DM (occurring within 6 months from the initial diagnosis). Accordingly, some patients with early DM were missed when the initial FDG-PET scans were retrospectively reviewed. In line with previous studies, we failed to demonstrate a statistically significant association between the AJCC T-classification and DM. In contrast, the AJCC Nclassification, AJCC staging, SUV, and tumor volume were found to predict the presence of DM in line with the published literature.<sup>[9,18–20](#page-9-0)</sup>

DCE-MRI-derived parameters (including  $K^{\text{trans}}$  and  $v_e$ ) as well as hypoxia and microvascular density are frequently used to assess several outcomes, including (1) tumor response to CCRT, (2) the presence of neck lymph node metastases, and (3) patient's prognosis. Preclinical research demonstrated an

<span id="page-5-0"></span>

<span id="page-6-0"></span>

FIGURE 1. (A–F) Representative pretreatment MR images of 2 NPC patients. The upper row depicts a patient (case # 16, panels A–C) with an AJCC T1N2 malignancy and DM. The lower row depicts a patient (case # 24, panels D–F) with an AJCC T4N3a and no DM. The measurements of tumor volume (panels A, D),  $v_e$  values (panels B, E), and overlying postcontrast T1WI (C, F) images are shown for comparison purposes. AJCC = American Joint Committee on Cancer, DM = distant metastases, MR = magnetic resonance,  $NPC =$  nasopharyngeal carcinoma.



 $AJCC =$  American Joint Committee on Cancer,  $DM =$  distant metastases.

TABLE 3. Relations Between AJCC Staging and Distant Metastases (Fisher's Exact Test)



<span id="page-7-0"></span>TABLE 4. Comparisons of SUV, Tumor Volume, and DCE-MRI Parameters in the Early DM Group Versus No DM and Late DM Groups (Combined) and Early DM Group Versus Late DM Group (Mann–Whitney U Test)

 $DCE-MRI =$  dynamic contrast-enhanced magnetic resonance imaging,  $DM =$  distant metastases,  $SD =$  standard deviation,  $SUV =$  standardized uptake value.

association between low  $v_e$  and local tumor resistance as well as lymphogenous dissemination, but no data on the potential relationship with DM are available. $21$  Moreover, the potential mechanisms by which DCE-MRI parameters could be linked with metastatic spread remain to be established. DCE-MRIderived  $v_e$ —reflecting the extravascular extracellular space consisting of interstitial fluid and connective tissue, but not the vascular compartment—has been used as a proxy for tumor aggressiveness. $22$  In our study, we hypothesize that the tumor microenvironment associated with a large  $v_e$  may promote metastatic dissemination before treatment and could be linked to a higher radiosensitivity to local treatment. Based on our clinical experience, tumors that are macroscopically less solid are more sensitive to RT but tend to metastasize distantly. The current findings may offer a potential explanation for this phenomenon. Accordingly, an elevated  $v_e$  may be associated with a higher rate of early DM rate because it reflects the presence of an abundant and well vascularized extracellular space that may favor distant metastatic spread. Conversely, a high  $v_e$  can be linked to a reduced likelihood of local recurrence

because the most abundant and vascularized extracellular space portends a reduced risk of hypoxia and a better penetration of anticancer drugs. Unpublished observations from our group also suggest that compact tumors with a smaller  $v_e$  are less likely to respond to RT and have a higher propensity for local recurrence. In this study, we did not specifically investigated whether the tumors had hypoxic components or the main underlying metastatic route (ie, hematogenous vs lymphatic spread). The risk of local recurrence may be explained by cell density and hypoxia inasmuch as higher  $v_e$  values reflect a lower cell density and hypoxia. In contrast, the mechanisms underlying the occurrence of DM may be more complex (possibly involving different gene mutations facilitating the passage of cancer cells into the vascular and/or lymphatic systems). Two recent studies have shown the utility of pretreatment tumor  $v_e$  for the prediction of treatment response, a clinical value which was not evident for other DCE-MRI parameters.<sup>[23,24](#page-9-0)</sup> Our current results are consistent with the published literature.

Identifying the largest and smallest  $K^{trans}$ ,  $v_e$ , and  $v_p$ values among sequential slices may be a concern, because



AUC = area under curve, CI = confidence interval, DM = distant metastases, SUV = standardized uptake value. <sup>\*</sup> No statistically significant difference between values ( $P = 0.82$ ).

<span id="page-8-0"></span>

FIGURE 2. Flow of the participants through the study. Asterisk (\*) indicates statistically significant values, P<0.05. The  $v_e$ -related parameters included mean, median, skewness, and kurtosis of the entire tumor  $v_e$  and the largest mean  $v_e$  selected among sequential slices.  $A$ JCC-N = American Joint Committee on Cancer N-classification, DM = distant metastases.

tumor heterogeneity may be averaged out with an entire tumor<br>volume approach.<sup>[25,26](#page-9-0)</sup> Histogram analysis is considered useful for exploring the significance of tumor heterogeneity. In particular, skewness reflects the pattern of value distribution, whereas kurtosis represents the position of the peak height indicating the values of maximum frequency. The histographic pattern of skewness and kurtosis of cerebral blood volume have been successfully utilized for differentiating early tumor progression from pseudoprogression in patients<br>with newly diagnosed glioblastomas.<sup>[27](#page-9-0)</sup> Among the mean and median values of  $v_e$  from entire tumor and individual slices,  $v_e$ skewness and  $v_e$  kurtosis were also found to be different between the early and late DM groups. Although our results showed that the skewness and kurtosis were useful parameters for differentiating the timing and occurrence of DM, further investigation using pixel-based histogram analysis of DCE-MRI data (rather than a ROI-based analysis) would be useful for further investigating the trend. Our findings did not support the value of  $K^{\text{trans}}$  and  $v_p$  for the identification of early DM, probably because  $K^{\text{trans}}$  and  $v_p$  are more closely linked to perfusion and permeability (thus being related to tumor angiogenesis). The lack of significant associations between these 2 parameters and early DM suggests that the angiogenic state of the primary NPC is not a main determinant of its metastatic spread.

Some caveats of the present study merit comment. The sample size was relatively small compared with previous studies conducted in NPC patients. Larger sample sizes are needed to increase the statistical power when comparing patients with early and late DM. Diffusion restriction reflects cell density in solid tumors, including head and neck malig-nancies.<sup>[28–30](#page-9-0)</sup> However, the association between  $v_e$  and the apparent diffusion coefficient (ADC) may be questioned. In future studies, the collection of ADC data will be necessary to confirm the assumption that higher  $v_e$  is a proxy for lower cell density. Finally, the potential incremental value of combining FDG-PET SUV and DCE-MRI parameters needs to be investigated in prospective studies.

### **CONCLUSION**

FDG-PET imaging may underestimate the occurrence of early DM in NPC patients. Such lesions may probably become evident only in the presence of clinical manifestations and/or radiological progression. The reliable detection of early DM is of paramount importance for determining the most appropriate treatment alternatives. The results of this pilot study indicate that SUV, tumor volume, and  $v_e$ -related parameters are potentially useful for achieving this goal. Increased  $v_e$  reflects a lower tumor cell density and a higher likelihood of early metastatic spread. Notably, the statistically significant difference in  $v_e$ values between patients with early DM and the other groups was not evident unless patients with DM occurring within 6 months of the initial diagnosis were included.

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