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Journal

European Journal of Radiology, 84(4)

ISSN

0720-048X

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Publication Date

2015-04-01

DOI

10.1016/j.ejrad.2014.12.029

Peer reviewed



Published in final edited form as:

Eur J Radiol. 2015 April ; 84(4): 611–616. doi:10.1016/j.ejrad.2014.12.029.

Accuracy of 3T versus 1.5T breast MRI for pre-operative assessment of extent of disease in newly diagnosed DCIS

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Abstract

Objectives—While 3 tesla (T) breast magnetic resonance imaging has increased in use over the past decade, there is little data comparing its use for assessing ductal carcinoma in situ (DCIS) versus 1.5T. We sought to compare the accuracies of DCIS extent of disease measures on pre-operative 3T versus 1.5T MRI.

Methods—This institutional review board-approved prospective study included 20 patients with ductal carcinoma in situ diagnosed by core needle biopsy (CNB) who underwent pre-operative breast MRI at both 3T (resolution=0.5×0.5×1.3 mm) and 1.5T (0.85×0.85×1.6 mm). All patients provided informed consent, and the study was HIPPA compliant. Lesion sizes and imaging characteristics (morphologic and kinetic enhancement) were recorded for the 3T and 1.5T examinations. Lesion size measures at both field strengths were correlated to final pathology, and imaging characteristics also were compared.

Results—Of the initial cohort of 20 patients with CNB-diagnosed DCIS, 19 underwent definitive surgery. Median DCIS sizes of these 19 patients were 6 mm (range: 0–67 mm) on 3T, 13 mm (0–60 mm) on 1.5T, and 6 mm (0–55 mm) on surgical pathology. Size correlation between MRI and pathology was higher for 3T (Spearman's $\rho=0.66$, $p=0.002$) than 1.5T ($\rho=0.36$, $p=0.13$). In 10 women in which a residual area of suspicious enhancement was identified on both field strengths, there was agreement of morphologic description (NME vs. mass) in nine, and no significant difference in dynamic contrast enhanced kinetics at 3T compared to 1.5T.

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Previous presentations: This study was presented at the 2013 annual RSNA meeting in Chicago, IL, USA.

Conflict of Interest Statement

The authors of this manuscript declare relationships with the following companies: 1) GE Healthcare, grant support (DeMartini) and consultant (Lehman), 2) Philips Healthcare, grant support (DeMartini and Partridge), and 3) Bayer Healthcare, consultant (Lehman)

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Conclusions—Pre-operative breast MRI at 3T provided higher correlation with final pathology size of DCIS lesions compared to 1.5T, and may be more accurate for assessment of disease extent prior to definitive surgery.

Keywords

Ductal Carcinoma in Situ; pre-operative; Breast MRI; 3 tesla

Introduction

The use of 3 tesla (T) MRI systems has increased for dynamic contrast-enhanced (DCE) breast imaging over the past decade. The primary benefit of imaging at 3T over 1.5T is increased signal-to-noise ratio, which can allow higher spatial resolution¹. In addition, 3T MRI potentially could improve the conspicuity or contrast resolution of enhancing lesions compared to that seen at 1.5T, due to differential effects of higher field strength on T1 relaxation times of non-enhancing compared to gadolinium-enhancing tissue². This concept is supported by several studies showing a greater degree of enhancement for a given dose of gadolinium-based contrast with higher field strengths³⁻⁵.

Accurate pre-operative determination of breast cancer extent can be a valuable guide to surgical planning. Multiple studies have shown that MRI is the most sensitive means of assessing the extent of malignancy, including the presence of multifocal and multicentric disease, in women newly diagnosed with breast cancer⁶. This benefit may be particularly important for the pre-invasive malignancy ductal carcinoma in situ (DCIS) since positive surgical margins are a predictor of disease recurrence and pre-operative underestimation of DCIS extent by mammography has been found to occur in one quarter of women⁷.

Although breast MRI was initially thought to be less useful for evaluating DCIS than invasive breast cancer, it has subsequently been shown to have both a higher sensitivity for detection at screening⁸ and correlation to final pathologic size^{9, 10} of DCIS lesions. Thus, breast MRI used in conjunction with mammography may help guide clinical management of DCIS^{11, 12}. However, challenges remain assessing DCIS extent at 1.5T, perhaps because DCIS is more likely than invasive cancer to present on MRI as poorly defined non-mass enhancement (NME)¹³⁻¹⁵. Accordingly, the improved spatial and contrast resolution offered by 3T imaging may be particularly useful for the evaluation of ductal carcinoma in situ (DCIS).

There are few studies to date examining the overall accuracy of breast MRI performed at 3T compared to 1.5T^{16, 17} and only one prospective study that includes intra-individual comparisons¹⁸. In their initial experience with DCE breast MRI performed at 1.5T and 3T in the same patients, Kuhl and colleagues found higher image quality scores and higher diagnostic confidence at 3T compared to 1.5T¹⁸. Only three of the 37 women in their study had pure DCIS, and lesion sizes were not compared between field strengths. The purpose of this study was to compare the accuracies of extent of disease measures of DCIS at 3T versus 1.5T MRI, and to assess differences in imaging features between field strengths.

Methods

This Health Insurance Portability and Accountability Act (HIPAA)-compliant, Institutional Review Board-approved, prospective study was performed over a two-year period from June 2010 through May 2012. All patients provided written informed consent prior to participating in the trial.

Patient Population

Sixty-nine patients were diagnosed with pure DCIS (defined as DCIS with no foci of invasion) by core needle biopsy (CNB) and underwent a standard pre-operative 3T clinical breast MRI within 6 weeks of DCIS diagnosis during the study interval. Four patients were not approached due to barriers (language and/or cognitive) to obtaining informed consent. An additional six patients were ineligible because they underwent an additional biopsy after the 3T breast MRI was performed and before 1.5T imaging could be performed. Of the remaining 59 eligible patients, 20 consented to participate and underwent an additional pre-operative breast MRI at 1.5T within 4 weeks following 3T imaging. Thus, the final cohort included 20 consecutive patients who sequentially underwent both clinical 3T and research 1.5T breast MRI after CNB-diagnosis of pure DCIS and prior to surgical treatment.

Image-guided Biopsy Technique

Diagnosis of DCIS was made prior to MRI and surgery by image-guided CNB. CNB was performed with either a 9-gauge vacuum-assisted breast biopsy device (Eviva, Hologic, Bedford, MA, USA) for lesions biopsied under stereotactic guidance or a spring loaded 14-gauge device (Achieve, CareFusion, San Diego, CA, USA) for lesions biopsied under sonographic guidance.

MRI Acquisition

The MRI protocols followed guidelines established by the American College of Radiology breast MRI accreditation program¹⁹. Both 3T and 1.5T MRI protocols included a 3D T1-weighted fast gradient echo-based DCE series with one pre-and three sequential post-gadolinium contrast-enhanced sequences. For both field strengths, DCE sequences were acquired with comparable scan durations of approximately 3 minutes each. A summary of the DCE-MRI technical parameters at both field strengths is provided in Table 1.

3T MRI was performed on a Philips Achieva Tx system (Philips Medical Systems, Best, the Netherlands) with a 16-channel breast coil (Mammotrak, Philips Healthcare) with the following DCE-MRI parameters: TR/TE=5.9/3 msec, flip angle=10°, spatial resolution = 0.5 × 0.5 × 1.3 mm. Post-contrast sequences were acquired with k space centered at 120, 300, and 480 seconds after contrast injection. 1.5T MRIs were performed on a GE LX system (GE Medical Systems, Waukesha, WI) with a Sentinelle 8-channel breast coil (Hologic, Bedford, MA) with the following DCE-MRI parameters: TR/TE=5.6/3 msec, flip angle=10°, spatial resolution = 0.85 × 0.85 × 1.6 mm. Post-contrast sequences were acquired with k space centered at 90, 270, and 450 seconds. Gadolinium contrast-material dose and delivery was the same for both protocols: 0.1 mmol/kg at 2 cc/sec followed by a 15 cc saline flush. Gadodiamide (Omniscan, GE Healthcare) was used for all examinations from June 2010 to

November 2010 (6 of 20 cases) and Gadoteridol (ProHance, Bracco Diagnostics, Monroe Township, NJ) was used from November 2010 to May 2012 (14 of 20 cases). The same contrast agent was used at 3T and 1.5T for each study patient.

Breast MRI Interpretation

Each 1.5T and 3T breast MRI was prospectively interpreted by one of seven fellowship-trained radiologists specializing in breast imaging. Images were reviewed on a picture archiving and communication system (PACS) (Centricity, GE Healthcare, Fairfield, CT) with the assistance of commercially available computer-aided evaluation software (CADstream, Merge Healthcare, Chicago, IL). MRI interpretation was performed in conjunction with the clinical history and correlative breast mammograms and ultrasound, when available. For each patient, the 3T examination was interpreted prior to the 1.5T MRI, and a different radiologist interpreted each 1.5T study (blinded to the corresponding 3T images and report). All examinations were interpreted prior to surgery, and thus the radiologists were unaware of the final surgical extent of the DCIS lesion in question. Index lesion morphologic descriptors (NME or mass) and maximum sizes (defined as the largest value in anterior-posterior, cranial-caudal, or transverse dimension) were described at the time of radiologist interpretation using the first post-contrast series (including axial acquired as well as coronal and sagittal multi-planar reformats) in the DCE MR examination. In cases where no residual suspicious enhancement was described at the site of known DCIS, a maximum lesion size of 0 mm was assigned.

Kinetic enhancement data also were assessed using in-house software developed with ImageJ (NIH open source software). Semi-quantitative DCE kinetic parameters were calculated for whole tumor regions of interest (ROIs) based on the signal enhancement ratio (SER) method as previously described²⁰. The initial phase kinetic parameters characterized at the first post-contrast time-point were as follows: 1) peak enhancement (PE) (defined as the greatest signal intensity [SI] increase on the initial post-contrast MR sequence compared to the pre-contrast sequence for the $3 \times 3 \times 3$ volume of voxels with maximum SI change within the lesion), 2) percentage of the lesion with medium enhancement (SI increase = 50–100% from pre-contrast), 3) percentage of the lesion with rapid enhancement (SI increase > 100% from pre-contrast). Delayed-phase kinetics characterizing the change in SI from the initial post-contrast series to the final post-contrast series were calculated on a voxel-by-voxel basis for all voxels demonstrating at least medium initial enhancement. The following delayed phase kinetic features were recorded: 1) percentage of the lesion with persistent delayed enhancement (SI increase > 10% between initial and final post-contrast acquisitions), 2) percentage of the lesion with plateau (change in SI = 10%), and 3) percentage of the lesion with washout (SI decrease > 10%).

Clinical Data

Patient features, including age at diagnosis, modality guiding CNB, and times between diagnosis of the index DCIS lesion, MR examinations, and final surgical excision were recorded. Pathologic assessment of maximum lesion sizes, nuclear grade, and presence of invasive disease were obtained from the final surgical pathology reports.

Statistical Analysis

Differences in DCIS lesion sizes determined by pre-operative MRI and final surgical pathology were evaluated by Bland-Altman analysis. The accuracies of 3T and 1.5T MRI for measuring size of DCIS as determined by pathology were further assessed and compared by calculating Spearman correlation coefficients (ρ) and by Wilcoxon signed-rank test. MRI morphology types at 3T and 1.5T were compared by Fisher's Exact test and differences in MRI kinetic features at 3T and 1.5T were evaluated by Wilcoxon signed-rank test. All computations were performed using statistical software (SAS version 9.3, SAS Institute Inc., Cary, NC), and p values less than 0.05 were considered statistically significant for all comparisons.

Results

The mean patient age was 54.9 (range 40–74) years. Seventeen women (85%) underwent stereotactic CNB and three (15%) underwent ultrasound-guided CNB for the pre-operative diagnosis of DCIS. All 20 patients subsequently underwent pre-operative MRI at both 3T and 1.5T; 19 patients underwent surgical resection at our institution, and one patient was lost to follow-up (no final surgical pathology available). Mean biopsy, MRI, and surgery times were as follows: between lesion biopsy and clinical 3T MRI = 17.1 days (range 4–34), between 3T and 1.5T MRIs = nine days (range 1–24), and between CNB and surgical resection = 50.5 days (range 20–93). Of the 19 cases with final surgical pathology available, 12 lesions were high nuclear grade, five were intermediate nuclear grade, and two had no residual disease (Table 2). Two of the 19 cases had foci (<2 mm) of invasive disease on final surgical excision, and both were associated with high nuclear grade DCIS lesions.

3T vs. 1.5T MRI DCIS Size Comparisons

The median radiologist-assessed maximum DCIS size was 6 mm (range 0–67 mm) on 3T and 13 mm (range 0–60 mm) on 1.5T. The median pathologist-assessed maximum size for DCIS lesions was 6 mm (range 0–55 mm) on final surgical excision (Table 3). In the three cases in which a lesion was identified on 1.5T but no lesion was identified on 3T, one patient had 20 mm of NME at 1.5T and no residual DCIS on surgical excision, one had 30 mm of NME at 1.5T and 3 mm of high nuclear grade DCIS, and one patient had 23 mm of NME at 1.5T and 15 mm of intermediate nuclear grade DCIS. In the single case in which a lesion was visible on 3T but not identified on 1.5T, the patient had 59 mm of NME on 3T and 50 mm of high nuclear grade DCIS on surgical excision, Figure 1. Of the six cases in which no finding was described on both the 3T or 1.5T exams, the median final pathology size was 4 mm (range= 0–11 mm, Table 1).

Bland-Altman plots of the 19 lesions that underwent surgery indicated MRI sizes more closely matched pathologic extents for 3T compared to 1.5T, illustrated by narrower 95% limits of agreement (Figure 2). Size correlation between MRI and pathology was higher for 3T (mean difference 7.5 mm, range 0–35 mm; $\rho=0.66$, $p=0.002$) than for 1.5T (mean difference 11.5 mm, range 0–50 mm; $\rho=0.36$, $p=0.13$, Table 3).

3T vs. 1.5T MR Imaging Features of DCIS

As a secondary aim, we further assessed the agreement of morphological and kinetic features for the subset of 10 lesions in which an area of enhancement suspicious for residual DCIS was described at both 3T and 1.5T. Of those 10 lesions, there were no significant differences in morphology ($p=1.0$), as nine were given the same morphologic descriptor (7 NME, 2 mass) on both field strengths (Table 4). In the single discordant case, the finding was described as a mass on 3T MRI and as NME on 1.5T MRI. Overall, there were no statistically significant differences ($p>0.05$ for all comparisons) in initial or delayed phase kinetic features at 1.5T compared to 3T (Table 4).

Conclusions

In this prospective study, the first comparing same-patient MRI features of newly diagnosed pure DCIS at both 3T and 1.5T field strengths, we found that maximum lesion size on 3T MRI more highly correlated with final pathology size than maximum lesion size on 1.5T examinations. This suggests pre-operative evaluation of extent of disease for DCIS is more accurate when performing breast MRI at higher field strength. We observed no significant differences in morphological and kinetic features between the field strengths despite higher spatial resolution and a hypothesized increase in contrast resolution at 3T.

Defining the optimal imaging and management algorithm of newly diagnosed DCIS remains an area of active research that has been identified to be of high priority for investigation by the National Institutes of Health²¹. There is longstanding controversy regarding the ultimate benefit of treating all patients with newly diagnosed DCIS, and it is estimated that less than 50% of all lesions would affect a woman's life if left untreated²². Accordingly, it has been suggested that small DCIS lesions of lower biologic activity may require less treatment²³. However, because current risk-stratification methods do not accurately identify which DCIS lesions will remain indolent, uniform treatment of all lesions including complete surgical resection with clear margins remains the prevailing treatment approach. Thus, improved pre-operative determination of DCIS extent of disease with imaging could aid in treatment decision-making and potentially the evolution of optimal DCIS management²⁴.

Mammography is limited for the determination of the full extent of DCIS since it typically detects only calcified portions of the process. A study by Dillon and colleagues showed considerable underestimation of DCIS size (defined as imaging-to-pathology discrepancy of greater than 1 cm) with mammography in 40% of patients who had positive surgical margins compared to only 14% of patients with negative margins⁷. Over the past decade due to an increased emphasis on spatial resolution, it has become clear that breast MRI is superior to mammography for both DCIS detection^{8, 11, 25} and correlation with pathologic size^{9, 10}.

Imaging at 3T offers several theoretical advantages over 1.5T, including potential for higher spatial, temporal, and contrast resolution. Because kinetic features have not been found to be as useful as morphologic features for diagnostic breast MRI, particularly for DCIS^{12, 13, 15}, MRI protocols at our institution emphasize spatial resolution over temporal resolution. Accordingly, we hypothesized that MRI performed at 3T field strength with higher spatial resolution than achievable at 1.5T could incrementally improve assessment of DCIS extent

of disease through improved morphologic depiction or conspicuity. Our finding of greater correlation of 3T size with pathology size supports this hypothesis. It is important to note that across institutions not all 3T protocols emphasize spatial resolution, which may limit the improved depiction of size found in our study ².

As secondary analyses, we compared morphological and kinetic features for the 10 cases in which an area of residual suspicious enhancement was identified on MRI at the site of known cancer for both field strengths. We found that there was morphological agreement (mass vs. NME) in 90% of cases (9/10) between field strengths. This suggests that the effect of higher spatial resolution may have less of an impact on qualitative morphologic assessment than on accurate size depiction. In addition, we observed no significant differences in initial and delayed phase kinetic enhancement features between field strengths. It should be noted, however, that because only 10 lesions were compared between field strengths, this study was underpowered to identify differences in kinetic features and validation of our findings in larger cohorts is warranted.

Our study had several additional limitations. All MR examinations were performed after CNB. While this reflects the normal clinical care pathway for patients in the pre-operative setting, assessment of some of the lesions was likely impacted by post-biopsy changes such as hematoma formation and in some cases removal of the majority of the DCIS lesion. It is possible that this affected 3T assessments to a greater extent than at 1.5T since these exams were universally performed closer to the CNB. Due to a desire to not delay the normal treatment pathway for patients, we could not account for differences in background enhancement related to differences in menstrual cycle phase in pre-menopausal women, which could have impacted size measurements of non-mass enhancement lesions. Another potential limitation of the study is that the center of k space for the first post-contrast T1-weighted series was later for the 3T studies when compared to 1.5T (120 sec vs. 90 sec). Because it is known that DCIS lesions can reach peak enhancement later than invasive tumors, it is possible that this difference in timing could have contributed to the improved determination of lesion extent observed at 3T. Finally, this study was designed to determine the effect of using 3T MRI for DCIS characterization in the pre-operative setting compared to 1.5T. As a result, the effect on specific clinical outcomes (e.g. rate of negative margins or local recurrence) was not assessed.

In summary, this prospective study of women with newly diagnosed DCIS demonstrated that pre-operative MRI at 3T emphasizing greater spatial resolution provided higher correlation with final pathology size of DCIS lesions compared to 1.5T. This suggests that 3T MRI may be more accurate for assessment of extent of DCIS prior to surgery and could thereby improve treatment outcomes. Further investigation of the use of 3T MRI to pre-operatively characterize newly diagnosed DCIS is warranted given potential patient management advantages.

Acknowledgments

Funding support: This study was supported by a Research Grant from Phillips Healthcare (Koninklijke Philips Electronics NV Research Grant) and a 2014–2016 RSNA Research Scholar Grant.

This study was supported by a Research Grant from Philips Healthcare (Koninklijke Philips Electronics NV Research Grant), a 2014–2016 Radiological Society of North America (RSNA) Research Scholar Grant, and a National Institutes of Health (NIH) R01 grant (R01CA151326).

Role of Funding Sources

Grant funding from Philips Healthcare provided support to perform additional MRI scans on patients in this trial as well as salary support for W.B.D. Grant funding from RSNA provided salary support for H.R. Grant funding from NIH provided salary support for S.C.P.

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Highlights

- We compared sizes of known ductal carcinoma in situ (DCIS) on pre-operative breast MRI at 3 tesla (T) and 1.5 T with final pathology sizes.
- DCIS sizes on 3T MRI correlated better with pathologic sizes than 1.5T MRI.
- Imaging features of DCIS, including morphology and kinetics, were similar at 3T and 1.5T MRI.

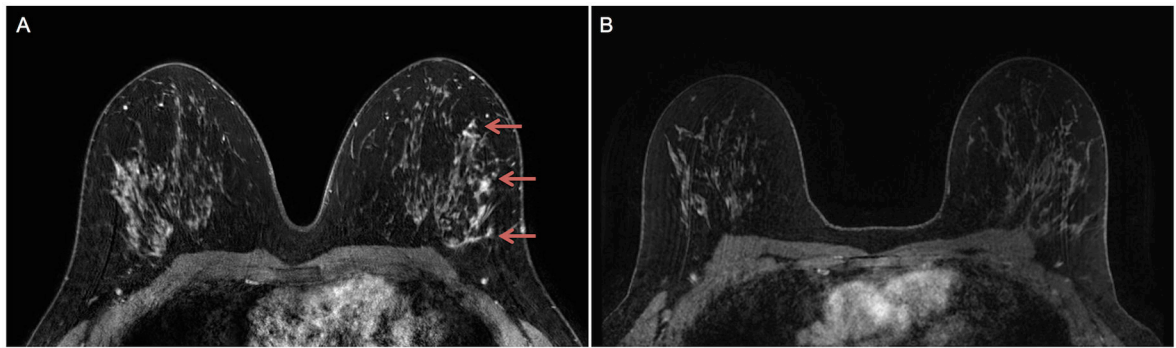


Fig. 1. Same-patient initial post-contrast T1-weighted with fat suppression pre-operative MR images at A) 3 tesla (T) and B) 1.5T in a woman diagnosed with high nuclear grade ductal carcinoma in situ (DCIS) by core needle biopsy. Assessed DCIS lesion size at 3T was 59 mm (non-mass enhancement, arrows), while at 1.5T no lesion was described (size = 0 mm). 3T MRI extent better correlated with the final pathology size of 50 mm of high nuclear grade DCIS.

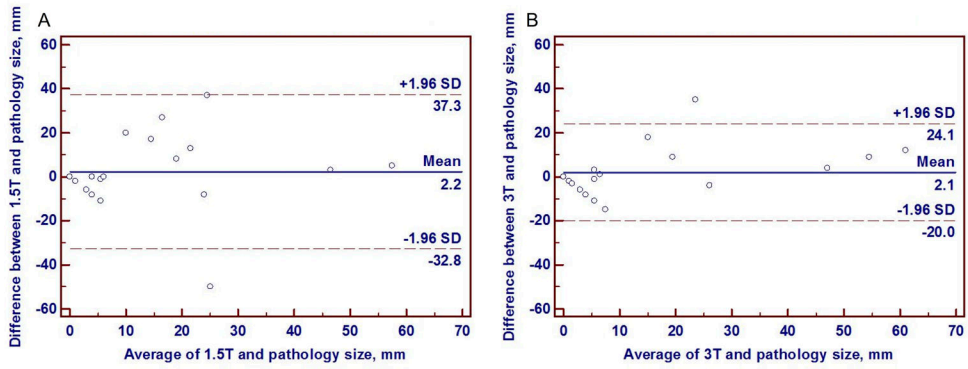


Fig. 2. Bland-Altman plots of DCIS displaying the differences in lesion sizes versus pathology sizes on 1.5 tesla (T) breast MRI (A) and 3T breast MRI (B). Note that the limits of agreement with pathology size are narrower for 3T size (B) than 1.5T size (A), indicating greater agreement of 3T DCIS lesion sizes with final pathology sizes.

Table 1

Technical parameters for the 3 tesla (T) and 1.5T imaging protocols utilized in this study. Note that the 3T protocol achieves 41% greater in plane spatial resolution than the 1.5T protocol in a similar overall scan time.

Parameter	3 tesla	1.5 tesla
Plane	Axial	Axial
Breast coil type	16 channel	8 channel
Mode	3D	3D
Sequence type	Fast gradient echo	Fast gradient echo
Fat Suppression	SPAIR	SPIR
Parallel Imaging Factor	2.7 R/L, 2.0 S/I	1.5 R/L
TR (msec)	5.9	5.6
TE (msec)	3	3
Flip angle (degrees)	10	10
Field of View (cm ²)	22 A/P × 33 R/L	36 A/P × 36 R/L
Matrix	440 × 660	420 × 420
In-plane voxel size (mm)	0.5	0.85
Slice thickness (mm)	1.3 → 0.65 recon	1.6
Scan time (min)	2:51	2:53

Abbreviations: SPAIR = Spectral Attenuated Inversion Recovery, SPIR = Spectral Presaturation with Inversion Recovery, R = right, L = left, A = anterior, P= posterior, recon = reconstructed

Table 2

Summary of 3 tesla (T) MRI, 1.5T MRI, final pathology sizes, and final nuclear grade for all ductal carcinoma in situ (DCIS) lesions.

DCIS Lesion	MRI		Surgical Excision	
	3T Size (mm)	1.5T Size (mm)	Pathologic Size (mm)	Nuclear Grade
1	5	5	6	Intermediate
2	0	0	6	Intermediate
3	7	4	4	Intermediate
4	59	0	50	High
5	0	0	8	High
6	0	0	2	High
7	0	20	0	-
8	24	28	15	High
9	0	0	0	-
10	67	60	55	Intermediate
11	0	30	3	High
12	0	0	11	High [#]
13	24	23	6	High [#]
14	7	6	6	High
15	41	43	6	High
16	49	48	45	High
17	57	53	Unknown	Unknown
18	24	20	28	High
19	0	23	15	Intermediate
20	0	0	2	High

Abbreviations: DCIS: ductal carcinoma in situ; T: tesla

[#] focus of invasive disease <2mm in size was present on surgical excision specimen

Table 3

Correlations of 3 tesla (T) and 1.5 T ductal carcinoma in situ sizes with final surgical pathology size.

	Maximum Size (mm)			Correlation to Pathology
	Median	Mean	Range	ρ (p) *
3T MRI (n=20)	6.0	18.2	0–67	0.66 (0.002) *
1.5T MRI (n=20)	13.0	18.2	0–60	0.36 (0.13)
Pathology (n=19)	6	14.1	0–55	

Abbreviations: mm: millimeters, T: tesla, ρ = Spearman's correlation coefficient (rho)

* Indicates statistically significant difference

P values calculated by Wilcoxon signed-rank test

Table 4

Imaging features of the 10 DCIS lesions described on both 3 tesla (T) and 1.5 T protocols.

Imaging Feature	3T MRI	1.5T MRI	P value
<u>Morphology</u>			
Mass	N=3 (30%)	N=2 (20%)	1.0
Non-mass enhancement	N=7 (70%)	N=8 (80%)	
<u>Initial enhancement</u>			
Mean peak enhancement (%)	173.8	118.2	0.08
Mean percent medium (%)	66.7	80.2	0.12
Mean percent rapid (%)	33.3	19.8	0.12
<u>Delayed enhancement</u>			
Mean percent persistent (%)	54.6	62.8	0.29
Mean percent plateau (%)	23.2	21.0	0.05
Mean percent washout (%)	22.2	16.1	0.22

Abbreviations: T: tesla

P values were determined by Wilcoxon signed-rank test except morphology comparison, which was determined by Fisher's Exact test.