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Original Investigation

Association Between Thoracic Spinal Cord Gray Matter Atrophy and Disability in Multiple Sclerosis

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IMPORTANCE In multiple sclerosis (MS), upper cervical cord gray matter (GM) atrophy correlates more strongly with disability than does brain or cord white matter (WM) atrophy. The corresponding relationships in the thoracic cord are unknown owing to technical difficulties in assessing GM and WM compartments by conventional magnetic resonance imaging techniques.

OBJECTIVES To investigate the associations between MS disability and disease type with lower thoracic cord GM and WM areas using phase-sensitive inversion recovery magnetic resonance imaging at 3T, as well as to compare these relationships with those obtained at upper cervical levels.

DESIGN, SETTING, AND PARTICIPANTS Between July 2013 and March 2014, a total of 142 patients with MS (aged 25-75 years; 86 women) and 20 healthy control individuals were included in this cross-sectional observational study conducted at an academic university hospital.

MAIN OUTCOMES AND MEASURES Total cord areas (TCAs), GM areas, and WM areas at the disc levels C2/C3, C3/C4, T8/9, and T9/10. Area differences between groups were assessed, with age and sex as covariates.

RESULTS Patients with relapsing MS (RMS) had smaller thoracic cord GM areas than did ageand sex-matched control individuals (mean differences [coefficient of variation (COV)]: 0.98 mm² [9.2%]; *P* = .003 at T8/T9 and 0.93 mm² [8.0%]; *P* = .01 at T9/T10); however, there were no significant differences in either the WM area or TCA. Patients with progressive MS showed smaller GM areas (mean differences [COV]: 1.02 mm² [10.6%]; *P* < .001 at T8/T9 and 1.37 mm² [13.2%]; *P* < .001 at T9/T10) and TCAs (mean differences [COV]: 3.66 mm² [9.0%]; *P* < .001 at T8/T9 and 3.04 mm² [7.2%]; *P* = .004 at T9/T10) compared with patients with RMS. All measurements (GM, WM, and TCA) were inversely correlated with Expanded Disability Status Scale score. Thoracic cord GM areas were correlated with lower limb function. In multivariable models (which also included cord WM areas and T2 lesion number, brain WM volumes, brain T1 and fluid-attenuated inversion recovery lesion loads, age, sex, and disease duration), cervical cord GM areas had the strongest correlation with Expanded Disability Status Scale score followed by thoracic cord GM area and brain GM volume.

CONCLUSIONS AND RELEVANCE Thoracic cord GM atrophy can be detected in vivo in the absence of WM atrophy in RMS. This atrophy is more pronounced in progressive MS than RMS and correlates with disability and lower limb function. Our results indicate that remarkable cord GM atrophy is present at multiple cervical and lower thoracic levels and, therefore, may reflect widespread cord GM degeneration.

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Corresponding Author: Regina Schlaeger, MD, University of California, San Francisco, 675 Nelson Rising Lane, Box 3206, San Francisco, CA 94158 (regina.schlaeger@ucsf .edu). S pinal cord (SC) atrophy in multiple sclerosis (MS) is a common and clinically important aspect of the disease^{1,2} and may be one of the principal substrates of MS progression.³ A reduction in the cross-sectional upper cervical cord area, as detected in vivo by magnetic resonance imaging, has been documented throughout the disease course, both in cross-sectional and longitudinal analyses.⁴⁻¹² This reduction is often considered to reflect axonal loss,¹³⁻¹⁵ although it is likely that other processes, such as loss of SC neurons¹⁶ and myelin,¹⁷ also contribute.

Until recently, the relative contributions of white matter (WM) and gray matter (GM) loss to the overall reduction of SC volume in patients with MS could only be assessed in postmortem studies, which provided conflicting results.^{14,18} Fixation artifacts that cause unpredictable swelling, shrinkage, or tissue deformation complicate postmortem studies¹⁹ and can affect GM and WM differently.²⁰ The in vivo assessment of SC GM and WM compartments was limited by insufficient contrast between GM and WM on conventional imaging and by artifacts related to physiological motion of the cord and adjacent tissues.^{21,22}

Phase-sensitive inversion recovery (PSIR) imaging^{23,24} has been used in MS to characterize lesions and to estimate total cord areas (TCAs).^{25,26} Our group developed a sensitive method to detect SC GM atrophy based on 2-dimensional PSIR image acquisitions that enable reliable assessment of TCA, GM, and WM structures in clinically feasible scanning times (<2 minutes/level).²⁷ Using this method, we demonstrated that the upper cervical SC GM can be reduced in RMS in the absence of WM atrophy, and that GM atrophy is substantially more pronounced in PMS compared with RMS.²⁸ In addition, the cervical SC GM area was inversely correlated with disability.

The objective of this study was to assess the associations between GM/WM compartments of the lower thoracic cord with measures of clinical disability and disease type in a large, single-center cohort of patients with MS. A secondary goal was to compare these relationships with those obtained at the upper cervical levels.

Methods

Research Participants

This study included 142 patients with MS²⁹ seen at the University of California, San Francisco Multiple Sclerosis Center between July 2013 and March 2014 as part of an observational study. Inclusion and exclusion criteria are listed in the eAppendix in the Supplement. We also studied 20 healthy control individuals who were age- and sex-matched with the RMS group. The Committee on Human Research at University of California, San Francisco approved the study protocol. Written informed consent was obtained from all participants.

Clinical Assessments

All patients were assessed by the Neurostatus/Expanded Disability Status Scale (EDSS), Timed 25-Foot Walk Test (T25FW), and 9-Hole Peg Test (9-HPT).³⁰⁻³² Hip flexion strength was evaluated and graded according to the Medical Research Council Scale. Results from each side were added to a score from 0 to 10 (with 10 indicating full strength bilaterally).

Image Acquisition

All participants were scanned at the same 3-T magnetic resonance scanner, patients within 2 weeks of their clinical evaluation. Axial 2-dimensional PSIR images were acquired perpendicular to the SC at the C2/C3, C3/C4, T8/T9, and T9/T10 intervertebral disc levels (**Figure 1**). We chose the disc level T9/ T10 (corresponding to the segmental level of L1/L2) because the GM at this cord level is involved in proximal leg function and because it is sufficiently removed from the lumbar enlargement (where the anatomic interindividual variability is thought to be greater) and from rostral thoracic segments (where imaging artifacts can be substantial).

In addition, the patients underwent standard highresolution T1-weighted and 3-dimensional fluid-attenuated inversion recovery (FLAIR) images of the brain; T2-weighted sagittal and axial images of the cervical cord and sagittal images

Figure 1. Phase-Sensitive Inversion Recovery Images Illustrating Gray Matter Atrophy in Multiple Sclerosis (MS)



Axial 2-dimensional phase-sensitive inversion recovery images at the intervertebral disc levels C2/C3, C3/C4, T8/T9, and T9/T10 of a woman with relapsing MS (RMS) and Expanded Disability Status Scale score of 1.0 (A-D) and an age-matched woman with progressive MS (PMS) and Expanded Disability Status Scale score of 4.0 (F-I) illustrating gray matter atrophy in PMS.

Segmentation of the cord area was conducted semiautomatically using an active surface model. Segmentation of the gray matter area was performed manually. Acquisition of the images perpendicular to the cord at the intervertebral disc levels C2/C3 and C3/C4 (E) and T8/T9 and T9/T10 (J).

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of the thoracic cord were also obtained. For detailed acquisition parameters, see the eAppendix in the Supplement.

Image Analysis

Total cord areas and SC GM areas at all 4 levels were measured on the phase-sensitive reconstructed images using the software JIM6 (Xinapse Systems, http://www.xinapse.com) (Figure 1). Reliability assessments have previously been published for this segmentation method.²⁷ Based on these results, GM and TCA assessments were made by a single reader (R.S.), who was masked to the clinical data. Total cord area measurements were performed in a semiautomated fashion.³³ Spinal cord GM areas were manually segmented as described previously.²⁸

Analyses of brain MPRAGE, FLAIR, and SC T2 images are described in the eAppendix in the Supplement.

Statistical Analysis

Correlations between PSIR-derived measures and clinical characteristics (EDSS, T25FW, 9-HPT, and hip flexion strength) were assessed using Spearman rank correlation owing to the nonnormal distribution of clinical characteristics. The Bonferroni method was performed to correct for multiple comparisons across 2 independent cord areas at 4 levels for 4 clinical metrics (correction factor 32). Similarly, the comparison of PSIRderived measures between cord levels was performed using Spearman rank correlation owing to the non-normal distribution of WM areas at C3/C4 and T9/T10. Linear regression analyses were used to estimate differences in PSIR-derived measures at each level between control individuals and patients with RMS and PMS, adjusting first for age and sex and second for sex and disease duration.

The relative contribution of demographics, clinical characteristics, and PSIR-derived measures to the observed EDSS score variability was investigated using analyses of relative importance of regressors in a linear model (Relaimpo Package in R).^{34,35} Specifically, the relative contribution of cervical and thoracic SC GM areas to EDSS was quantified along with the following variables: cervical and thoracic SC WM areas, normalized brain GM and WM volumes, brain T1 lesion and FLAIR lesion volumes, SC lesion number, age, sex, and disease duration. The variables with the largest contribution to EDSS were further examined for an association with the probability of a progressive disease course (adjusted for age) based on probability maps.

Moreover, receiver operating characteristic (ROC) curves were compiled (eAppendix in the Supplement). Partial regression analysis was performed to assess the added value of thoracic SC GM areas in correlating with EDSS, while adjusting for other variables (including cervical SC GM areas) (eAppendix in the Supplement). The levels T9/T10 and C2/C3 were selected for this analysis because they had previously been shown to have the highest measurement reliability in the thoracic and cervical cord²⁷ and additionally demonstrated consistently good image quality in the present cohort.

Results

Demographic and clinical characteristics are summarized in eTable 1 in the Supplement. Of the 142 patients with MS, 99 had a relapsing and 43 had a progressive disease course.³⁶ The control group showed similar distributions of age and sex compared with the patients with RMS (eTable 1 in the Supplement). Gray matter segmentation was impossible owing to image distortion by either motion or lesion artifacts in 9%, 9%, 15%, and 12% of the images at the levels C2/C3, C3/C4, T8/T9, and T9/T10, respectively.

At all 4 levels, there was an inverse correlation of the EDSS score with the SC GM area (C2/C3: $\rho = -0.64$, C3/C4: $\rho = -0.63$, T8/T9: $\rho = -0.47$, and T9/T10: $\rho = -0.48$; all P < .001), with the SC WM area (C2/C3: $\rho = -0.36$, C3/C4: $\rho = -0.30$, T8/T9: $\rho = -0.33$, and T9/T10: $\rho = -0.37$; all P < .001), and with the TCA (C2/C3: $\rho = -0.48$, C3/C4: $\rho = -0.45$, T8/T9: $\rho = -0.41$, and T9/T10: $\rho = -0.40$; all P < .001). Moreover, the T25FW showed significant inverse correlations with the GM areas, WM areas, and TCAs at all levels (all P < .001). These associations all remained significant after Bonferroni correction (eTable 2 in the Supplement).

The 9-HPT showed significant moderate negative associations only with the TCA and SC GM area at the cervical levels but not at the thoracic levels after correction for multiple comparisons (eTable 2 in the Supplement).

Hip flexion strength was moderately correlated with thoracic SC GM areas ($\rho = 0.52$; P < .001) and WM areas ($\rho = 0.40$; P < .001) at T9/10 and at T8/T9 ($\rho = 0.42$; P < .001 and $\rho = 0.39$, P < .001, respectively) and showed significant correlations with thoracic SC GM areas, independently from the EDSS score. On the other hand, hip flexion strength did not show a significant association with cervical SC GM areas when accounting for EDSS score.

Total cord areas and cord GM and WM areas showed significant moderate-to-strong correlations with the corresponding measures at all other levels, with particularly strong associations between corresponding measures at adjacent levels (eTable 3 in the Supplement).

When adjusted either for age and sex (**Table**) or for disease duration and sex (eTable 4 in the Supplement), the mean SC GM areas and TCAs at all levels were significantly smaller in patients with PMS compared with those with RMS, while the SC WM areas were only significantly different at the 2 cervical levels. The SC GM areas differed between these groups at C2/C3 by 19.3% (coefficient of variation [COV]), at C3/C4 by 20.3%, at T8/T9 by 10.6%, and at T9/T10 by 13.2% (with adjustment for age and sex).

Patients with RMS had significantly smaller mean GM areas at C2/C3 (COV, 12.1%), T8/T9 (COV, 9.2%), and T9/T10 (COV, 8.0%) compared with control individuals. Gray matter areas at C3/C4 also followed this trend but did not reach statistical significance. No significant differences in SC WM areas and TCAs were found between these groups at any level.

The analyses of relative contribution of age, sex, disease duration, the PSIR-derived cord measures along with brain WM and GM volumes, T1 and FLAIR lesion loads and SC lesion num-

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Table. Comparison of Cervical PSIR Imaging-Derived Measures Between Control Individuals and Patients With RMS and PMS Using Linear Regression, With Age and Sex as Covariates

		Difference Between	and b	Difference Between
PSIR Measure	Adjusted Mean (SE)	Means, Mean (SE)"	P Value [®]	Means, 95% Cl ^a
Mean GM area mm ²				
Controls	20 53 (0 47)			
RMS	18 20 (0.23)	2 34 (0 52)	< 001	1 31 to 3 37
PMS	15.00 (0.37)	3 20 (0 44)	< 001	2 32 to 4 07
Mean WM area mm ²	15.00 (0.57)	5.20 (0.44)	1.001	2.52 10 4.07
Controls	57 66 (1 57)			
RMS	59 33 (0 75)	-1 67 (1 71)	33	-5.06 to 1.72
PMS	55.55 (0.75)	3 91 (1 46)	008	1 03 to 6 79
TCA mm ²	55.12 (1.21)	5.51 (1.10)	.000	1.05 to 0.75
Controls	78 44 (2 02)			
RMS	77 46 (0 94)	0 98 (2 20)	66	-3 37 to 5 33
PMS	68 12 (1 43)	9 34 (1 75)	< 001	5.90 to 12.79
C3/C4				
Mean GM area. mm ²				
Controls	22.07 (0.56)			
RMS	21.19 (0.28)	0.89 (0.62)	.16	-0.34 to 2.11
PMS	17.29 (0.46)	3.90 (0.56)	<.001	2.80 to 5.00
Mean WM area. mm ²				
Controls	59.92 (1.72)			
RMS	59.68 (0.87)	0.25 (1.90)	.90	-3.53 to 4.02
PMS	55.21 (1.43)	4.46 (1.71)	.01	1.07 to 7.85
TCA, mm ²				
Controls	82.31 (2.16)			
RMS	80.37 (1.07)	1.94 (2.38)	.42	-2.77 to 6.66
PMS	71.46 (1.65)	8.91 (2.01)	<.001	4.93 to 12.88
T8/T9				
Mean GM area, mm ²				
Controls	11.17 (0.30)			
RMS	10.19 (0.14)	0.98 (0.32)	.003	0.34 to 1.62
PMS	9.16 (0.25)	1.02 (0.29)	<.001	0.45 to 1.60
Mean WM area, mm ²				
Controls	33.29 (0.94)			
RMS	32.05 (0.44)	1.23 (1.03)	.23	-0.80 to 3.28
PMS	30.58 (0.78)	1.47 (0.93)	.12	-0.37 to 3.30
TCA, mm ²				
Controls	44.49 (1.18)			
RMS	42.40 (0.52)	2.09 (1.28)	.10	-0.44 to 4.63
PMS	38.74 (0.82)	3.66 (0.99)	<.001	1.69 to 5.62
T9/T10				
Mean GM area, mm ²				
Controls	12.04 (0.33)			
RMS	11.11 (0.16)	0.93 (0.36)	.01	0.22 to 1.65
PMS	9.73 (0.30)	1.37 (0.35)	<.001	0.69 to 2.06
Mean WM area, mm ²				
Controls	33.42 (0.91)			
RMS	32.81 (0.46)	0.61 (1.00)	.55	-1.38 to 2.59
PMS	31.55 (0.83)	1.26 (0.96)	.19	-0.64 to 3.17
TCA, mm ²				
Controls	45.50 (1.12)			

(continued)

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Table. Comparison of Cervical PSIR Imaging-Derived Measures Between Control Individuals and Patients With RMS and PMS Using Linear Regression, With Age and Sex as Covariates (continued)

PS	SIR Measure	Adjusted Mean (SE)	Difference Between Means, Mean (SE) ^a	<i>P</i> Value ^b	Difference Between Means, 95% Cl ^a
	RMS	43.90 (0.55)	1.60 (1.23)	.20	-0.84 to 4.02
	PMS	40.87 (0.86)	3.04 (1.04)	.004	0.97 to 5.10

Abbreviations: GM, gray matter; PMS, progressive multiple sclerosis; PSIR, phase-sensitive inversion recovery; RMS, relapsing multiple sclerosis; TCA, total cord area; WM, white matter.

^a Mean values are least square means with adjustment for age and sex. Mean differences: first line refers to the difference between control individuals and those with RMS, second line to the difference between those with RMS and PMS.

^b *P* values are 2-sided. The values in bold are significant.

ber demonstrated statistically significant contributions of all variables to EDSS score variance. **Figure 2** shows the relative contributions of GM and WM areas at C2/C3 and T9/T10 along with all other variables, normalized to sum 100% of explained variance in EDSS score. The GM area at C2/C3 had the highest relative importance in predicting EDSS score of all variables (0.41; 95% CI, 0.21-0.52), followed by the GM area at T9/T10 (0.20; 95% CI, 0.06-0.33) and the normalized brain GM volume (0.12; 95% CI, 0.03-0.24). This order of relative importance remained the same among variables regardless of the chosen combination of cervical and thoracic levels.

The results of the corresponding analyses with the 9-HPT and T25FW as outcomes are shown in eFigure 1 in the Supplement.

The C2/C3 and T9/T10 SC GM areas each contributed significant added value to accounting for EDSS score variance, both in bivariable and multivariable regression models. Analysis of the importance of the SC GM measures relative to all other variables (ie, when the SC measures entered the multivariable model last) reached similar conclusions (eTable 5 in the Supplement).





Relative contributions of the variables (cervical spinal cord gray matter [SGC] and white matter [SWC] areas at C2/C3, thoracic spinal cord gray matter [SGT] and white matter [SWT] at T9/T10, normalized brain gray matter volume [BG] and normalized brain white matter volume [BW], the number of spinal cord T2 lesions [SCL], brain T1 lesion volume [T1LV], brain fluid-attenuated inversion recovery lesion volume [FLV], age, sex, and disease duration [DD]) to the Expanded Disability Status Scale (EDSS) score using a linear model. $R^2 = 46.21\%$; metrics are normalized to sum 100%. Results are calculated using the Lindeman, Merenda, and Gold method. The error bars indicate 95% bootstrap Cls.

Probability maps demonstrated a significant association between cervical (**Figure 3**A and B) and thoracic GM area measures (Figure 3C and D) and the probability of a progressive (vs relapsing) disease course adjusted for age.

eFigure 2 in the Supplement displays ROC curves for the prediction of a progressive disease course by logistic models with the SC GM areas at each level as single predictors (eFigure 2A in the Supplement) and cervical and thoracic GM areas as combined predictors (eFigure 2B in the Supplement). The areas under the ROC curve (AUC) were 0.84, 0.83, 0.72, and 0.78 for the models based on SC GM area at the levels C2/C3, C3/C4, T8/T9, and T9/T10, respectively (eTable 6 in the Supplement).

Figure 3. Probability Maps of a Progressive Disease Course Based on Spinal Cord (SC) Gray Matter (GM) Assessments



Probability of a progressive disease course adjusted for age as assessed by SC GM area at the levels C2/C3 (A), C3/C4 (B), T8/T9 (C), and T9/T10 (D). Shaded areas indicate 95% CIs.

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Figure 4. Receiver Operating Characteristic Curves for the Prediction of a Progressive Disease Course Based on Gray Matter (GM) Assessments



Receiver operating characteristic curves for the prediction of a progressive vs relapsing disease course by binary logistic models with the normalized brain GM volume (BGMV) as the single predictor (dark blue line) (model a), the normalized BGMV along with the thoracic spinal cord GM area at T9/T10 (orange line) (model b), and the normalized BGMV along with the spinal cord GM areas at C2/C3 and T9/T10 (light blue line) (model c) as combined predictors. The areas under the curve were 0.68, 0.79, and 0.87, respectively.

Figure 4 displays the ROC curves for the models based on brain GM volume (model a), the combination of brain GM volume and SC GM area at T9/T10 (model b), and the combination of brain GM volume with SC GM areas at C2/C3 and T9/ T10 (model c) as predictors of a progressive vs relapsing disease course. The AUCs were 0.68, 0.79, and 0.87, respectively. The AUC of model c was significantly higher than the AUC for model a (P = .003). Model c predicted a progressive disease course, with a sensitivity and specificity of 0.81 and 0.80, respectively.

Discussion

Our results provide in vivo evidence of a significant association between the lower thoracic cord GM area and both MS disability and disease type.

In the lower thoracic cord, patients with RMS demonstrated selective GM atrophy. Patients with PMS showed more substantial GM and TCA reductions than did those with RMS. A model based on cervical and thoracic cord GM area together with brain GM predicted a progressive disease course, with a sensitivity of 0.81 and a specificity of 0.80. This model was superior to one based on brain GM alone. These findings extend and confirm the results of our previous report that quantitated upper cervical GM atrophy in a larger cohort including an increased number of progressive patients.

Lower thoracic cord GM areas were inversely correlated with EDSS score. Cervical and thoracic GM areas consistently had the greatest relative contribution to EDSS score in multivariable regression analyses, followed by brain GM volume. Thoracic cord GM contributed independently to EDSS score, even when the cervical GM area was accounted for. Both measures are reflective of a global process of GM degeneration in MS but at the same time also convey regional information concerning atrophy. While there is a global SC GM atrophy that is present throughout the cord cervical and thoracic levels, there may be individual variations within the thoracic cord superimposed that have direct functional consequences, which provide additional explanatory power for the EDSS score. We observed a moderate, but significant, association between the thoracic GM area at the disc level T9/T10 and the strength of muscles (ie, iliopsoas) innervated by the corresponding segmental level (L1/L2). In line with this observation, 9-HPT was only correlated with SC GM areas at cervical levels, not at the thoracic levels. These observations highlight potential clinical correlates of cord GM atrophy at a regional level.

To our knowledge, only a few magnetic resonance studies to date have investigated the thoracic cord in MS, and none have segregated the GM and WM compartments and assessed their relation to disability and disease type. Liu et al³⁷ reported a reduction of cervical TCAs in a relatively small, heterogeneous MS group; however, only a trend toward TCA reductions in the thoracic cord was found. The higher degree of total cord atrophy in the cervical compared with the thoracic region is in line with our findings.

Consistent with our findings, Klein et al³⁸ found significant cord volume reductions in PMS compared with RMS. In contrast to our observations and those of Liu et al,³⁷ they described a trend toward increased cervical and thoracic cord volumes in patients with RMS with shorter disease duration (mean, 6.3 years). We observed a trend to increased WM areas in patients with RMS compared with control individuals at C2/C3 but not at any other levels. The observed opposing volumetric effects of WM and GM might be linked to different pathological processes, such as edema/inflammation leading to WM expansion (potentially obfuscating the degree of axonal loss in WM) and neurodegenerative processes leading to cord volume/TCA reduction. Our data suggest that the TCA reduction might be driven primarily by a reduction in GM.

Our results are further corroborated by 2 studies that described microstructural changes in cord GM in vivo based on diffusion-weighted imaging techniques. These studies demonstrated a high association with MS disability, particularly in progressive MS.^{39,40}

Loss of SC neurons, loss of myelin, and additional changes in the neuropil may contribute to SC GM atrophy in MS. Histopathological data demonstrate that there is a 30.3% reduction in total neuronal numbers in the thoracic cord, with significant reductions in the motoneurons in myelinated GM.¹⁶ It is not known whether this neuronal loss is directly related to WM damage (eg, owing to anterograde trans-synaptic degeneration, as described for the visual system^{41,42}); whether it reflects an independent neurodegenerative process (caused or worsened by mitochondrial injury); or whether it is, at least in part, independent of focal WM damage.⁴³

Spinal cord GM demyelination can be extensive and exceeds the proportion of demyelinated WM.⁴⁴ In contrast to the subpial demyelinating lesions frequently observed in brain tis-

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sues in PMS, SC GM demyelination and neuronal loss occur distant from the meninges.^{44,45} Changes to the neuropil, such as reductions in synaptic densities, have been described in brain GM⁴⁶ but have not been quantified in the SC in MS.

There were a few limitations of this study. We only investigated 4 levels of the cord, not the entire cord. We selected these levels based on anatomic and pathological considerations and because a robust segmentation of GM is possible at these levels, with a high interrater reliability (intraclass correlation coefficients of 0.888-0.916, as shown previously).²⁷ Because a fully automated method is not yet available, GM segmentation was performed manually. Images at the T8/T9 level were more prone to artifacts than the other levels, as indicated by a higher percentage of images (15%) in which segmentation was not possible. This was typically owing to motion artifacts. Given the relative high correlations between TCAs and cord GM and WM areas of adjacent disc levels, and the results of the analysis of relative importance and partial regression analysis, it seems reasonable to focus future studies on the levels C2/C3 and T9/T10. These levels yield reliable measurements and additive information when used to model EDSS. With regard to the identification of a progressive phenotype, SC GM assessments at each level (in particular at C2/C3, C3/ C4, and T9/T10) are clinically informative, although most of the information is already captured by the cervical levels.

The presence of lesions has the potential to confound measurements in a few cases, namely, in those in which lesions were located adjacent to the GM or those in which lesions involved both the GM and WM. However, in most of these cases, one could see a GM/WM contrast despite the lesion. In those cases where the GM/WM boundary was not visible, the GM boundary was drawn as the shortest line between the 2 most adjacent clearly distinguishable GM/WM points, respecting the symmetry of the GM structure. Our high level of interobserver agreement demonstrates that this demarcation is robust. It is possible that lesions in these cases could have impacted either GM or WM area; however, the direction of this potential source of bias is difficult to estimate.

Finally, this was a cross-sectional study, thus causal connections cannot be inferred from the results. Future longitudinal studies will be needed to elucidate SC GM changes over time and their relationship with disability evolution to determine whether SC GM assessments are suited as a biomarker for MS progression.

Conclusions

This study provides evidence for the clinical impact of cord GM atrophy in MS, as measured in vivo by PSIR imaging. Cord GM atrophy is present at multiple levels, thus it may reflect widespread cord GM degeneration. These results add support to the growing understanding that GM loss is a key mediator of MS disability. The robust relationships between cord GM atrophy and disability are far stronger than those for any known cortical GM or WM metric. Thus, these data, perhaps, suggest a reorientation of current imaging practices. Magnetic resonance imaging-based estimations of cord GM that have strong correlations with MS disability may better track the disease process in the context of both clinical trials and longitudinal observational studies.

The central outstanding questions to be answered are (1) what is the temporal relationship of cord GM changes that we observed to the accumulation of MS disability and (2) whether these changes are dependent or independent of focal WM plaques. Longitudinal, prospective studies should help to clarify the role of cord GM changes in monitoring and predicting MS progression.

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Author Contributions: Drs Schlaeger and Henry had full access to all of the data in the study and take responsibility for the integrity of the data and the accuracy of the data analysis. Study concept and design: Schlaeger, Papinutto, Green, Hauser, Henry.

Acquisition, analysis, or interpretation of data:

Schlaeger, Papinutto, Zhu, Lobach, Bevan, Bucci, Castellano, Gelfand, Graves, Green, Jordan, Keshavan, Panara, Stern, von Büdingen, Waubant, Goodin. Cree. Henry.

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