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Authors

Savalli, Nicoletta
Angelini, Marina
Steccanella, Federica
[et al.](#)

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



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ARTICLE

Excitation-Contraction Coupling

The distinct role of the four voltage sensors of the skeletal Ca_v1.1 channel in voltage-dependent activation

Nicoletta Savalli¹, Marina Angelini¹, Federica Steccanella¹, Julian Wier¹, Fenfen Wu², Marbella Quinonez², Marino DiFranco², Alan Neely^{1,3}, Stephen C. Cannon², and Riccardo Olcese^{1,2a}

Initiation of skeletal muscle contraction is triggered by rapid activation of RYR1 channels in response to sarcolemmal depolarization. RYR1 is intracellular and has no voltage-sensing structures, but it is coupled with the voltage-sensing apparatus of Ca_v1.1 channels to inherit voltage sensitivity. Using an opto-electrophysiological approach, we resolved the excitation-driven molecular events controlling both Ca_v1.1 and RYR1 activations, reported as fluorescence changes. We discovered that each of the four human Ca_v1.1 voltage-sensing domains (VSDs) exhibits unique biophysical properties: VSD-I time-dependent properties were similar to ionic current activation kinetics, suggesting a critical role of this voltage sensor in Ca_v1.1 activation; VSD-II, VSD-III, and VSD-IV displayed faster activation, compatible with kinetics of sarcoplasmic reticulum Ca²⁺ release. The prominent role of VSD-I in governing Ca_v1.1 activation was also confirmed using a naturally occurring, charge-neutralizing mutation in VSD-I (R174W). This mutation abolished Ca_v1.1 current at physiological membrane potentials by impairing VSD-I activation without affecting the other VSDs. Using a structurally relevant allosteric model of Ca_v activation, which accounted for both time- and voltage-dependent properties of Ca_v1.1, to predict VSD-pore coupling energies, we found that VSD-I contributed the most energy (~75 meV or ~3 kT) toward the stabilization of the open states of the channel, with smaller (VSD-IV) or negligible (VSDs II and III) energetic contribution from the other voltage sensors (<25 meV or ~1 kT). This study settles the longstanding question of how Ca_v1.1, a slowly activating channel, can trigger RYR1 rapid activation, and reveals a new mechanism for voltage-dependent activation in ion channels, whereby pore opening of human Ca_v1.1 channels is primarily driven by the activation of one voltage sensor, a mechanism distinct from that of all other voltage-gated channels.

Introduction

The contraction of skeletal muscles is initiated by a brief (3–5 ms) action potential that causes a depolarization of muscle fibers (Bannister, 2016; Shishmarev, 2020). This sudden change of the sarcolemma membrane potential is detected by Ca_v1.1 channel voltage-sensing domains (VSDs), which are compelled to move by the change in electric field. The ensuing structural rearrangements of the VSDs not only open the Ca_v1.1 pore (allowing Ca²⁺ to enter the cell) but also propagate to ryanodine receptor 1 (RYR1) channel, located intracellularly in the membrane of the SR. As a result, the RYR1 channel, which cannot directly “sense” an

electrical excitation, acquires voltage dependence by physically coupling with a voltage-sensing protein (Ca_v1.1), such that sarcoplasmic Ca²⁺ release and muscle contraction become voltage-dependent (depolarization-driven) events (Rios and Brum, 1987; Ríos et al., 1992).

Seminal studies in the early 1970s recognized that an intramembrane “charge movement” was associated with, and necessary for, the skeletal muscle excitation–contraction (EC) coupling process (Schneider and Chandler, 1973; Hernández-Ochoa and Schneider, 2018). This charge movement is indeed

¹Department of Anesthesiology and Perioperative Medicine, Division of Molecular Medicine, David Geffen School of Medicine, University of California, Los Angeles, Los Angeles, CA; ²Department of Physiology, David Geffen School of Medicine, University of California, Los Angeles, Los Angeles, CA; ³Centro Interdisciplinario de Neurociencias de Valparaíso, Facultad de Ciencias, Universidad de Valparaíso, Valparaíso, Chile.

Correspondence to Riccardo Olcese: rolcese@ucla.edu.

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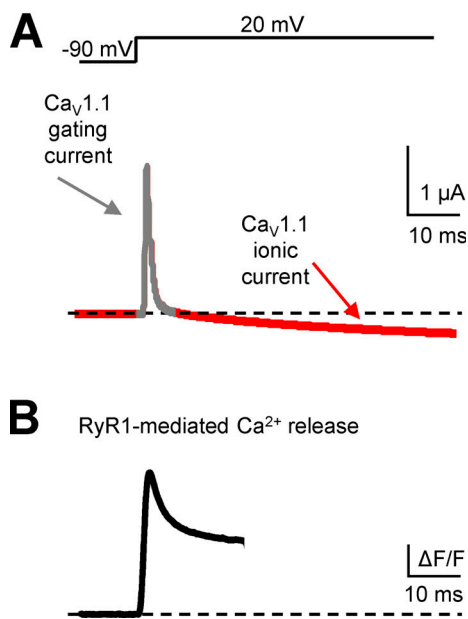


Figure 1. Time course of the activation of $Ca_v1.1$ and RYR1 channels. (A) Membrane current from $Ca_v1.1$ channels expressed in *Xenopus* oocytes displaying gating (gray) and ionic currents (red). (A and B) The rearrangement of $Ca_v1.1$ voltage sensors upon depolarization (gating currents, gray) activates two processes with very distinct kinetics: $Ca_v1.1$ ionic current (slow; red in A) and SR Ca^{2+} release (fast; in B) from dissociated mouse muscle fibers (flexor digitorum brevis) loaded with the Ca^{2+} dye OGB-5N. Recordings are shown on the same time scale to illustrate their drastically different kinetics.

the electrical manifestation of the voltage-dependent conformational changes of $Ca_v1.1$ voltage-sensing machinery composed of four VSDs (Fig. 1 A, gray trace). In this study, we sought to resolve the independent conformational rearrangements of the four $Ca_v1.1$ VSDs to answer a fundamental question in muscle physiology: how does the $Ca_v1.1$ channel voltage-sensing machinery govern two different events with very distinct voltage- and time-dependent properties, i.e., the slow opening of $Ca_v1.1$ pore and the fast activation of RYR1? In fact, $Ca_v1.1$ pore activation takes several tens of milliseconds to reach steady-state open probability (Fig. 1 A, red ionic current trace), while the kinetics of SR Ca^{2+} release through RYR1 is ~ 25 -fold faster than pore opening (Fig. 1 B, black trace). We postulated that the four homologous but not identical $Ca_v1.1$ VSDs possess different functional properties, enabling $Ca_v1.1$ to control both fast and slow molecular events.

Indeed, Ca_v channels are pseudo-tetramers composed of four concatenated repeats, each encompassing six transmembrane segments (S1–S6; Fig. S1 A): S1–S4 encode for the voltage sensors, while S5 and S6 from each repeat form the central pore (Dolphin, 2016; Hering et al., 2018; Catterall et al., 2020). Thus, a unique amino acid sequence pertains to each voltage sensor (Fig. S1 B), likely underpinning their distinct operation, as previously shown for the close relative $Ca_v1.2$ channel (Pantazis et al., 2014; Savalli et al., 2016) and for two Na_v isoforms (Cha et al., 1999; Chanda and Bezanilla, 2002; Varga et al., 2015). Until recently, studies of $Ca_v1.1$ biophysical properties have been hampered by negligible expression level of this channel in heterologous systems. With the discovery of Stac3-mediated trafficking of $Ca_v1.1$ channels (Polster et al., 2015; Flucher and Campiglio, 2019), it is now possible to express these proteins at the plasma membrane both in

HEK cells (Polster et al., 2015; Niu et al., 2018) and in *Xenopus laevis* oocytes (Wu et al., 2018). We used the voltage-clamp fluorometry (VCF) technique (Mannuzzu et al., 1996; Gandhi and Olcese, 2008) to resolve the depolarization-induced structural changes of the four $Ca_v1.1$ VSDs in a cellular environment. We found that each VSD of human $Ca_v1.1$ channels exhibits distinct biophysical properties. VSD-I time-dependent properties were strikingly similar to ionic current activation kinetics, while VSDs II–IV displayed faster activation, compatible with SR Ca^{2+} -release kinetics, suggesting that VSD-I plays a major role in pore opening. The relevance of VSD-I to $Ca_v1.1$ activation was reinforced using a naturally occurring, charge-neutralizing mutation in VSD-I (R174W; Eltit et al., 2012), which ablates $Ca_v1.1$ current at physiological membrane potentials by stabilizing VSD-I resting state. Using a structurally relevant allosteric model of Ca_v activation, which accounted for both time- and voltage-dependent properties of $Ca_v1.1$, we quantified the energetic interactions of each VSD with pore opening. Overall, this study revealed a new mechanism for voltage sensing among the voltage-gated superfamily of ion channels, whereby the open state of the human $Ca_v1.1$ channel is mainly stabilized by one voltage sensor, leaving the other three VSDs available for other voltage-dependent tasks, such as RYR1 activation.

Materials and methods

Ca^{2+} release measurement

Enzymatically dissociated flexor digitorum brevis fibers from mice were loaded with the dye OGB-5N (250 μ M) and voltage-clamped using the two-electrode voltage-clamp technique. The intracellular solution was (in mM) 75 aspartate, 5 ATP- Na_2 , 5 phospho-creatine di-Tris, 5 reduced glutathione, 5 $MgCl_2$, 30 EGTA, 15 $Ca(OH)_2$, 20 3-(N-morpholino)propanesulfonic acid, and 4 MOPS, pH 7.4 with KOH. The extracellular solution was (in mM) 150 TEA-Cl, 10 CsCl, 2 $CaCl_2$, 1 $MgCl_2$, and 10 MOPS, pH 7.4. Fluorescence was filtered at 2 kHz.

Xenopus oocytes isolation

A *Xenopus* frog is anesthetized by immersion in water containing 0.17% tricaine for ~ 30 min. The anesthetized frog is euthanized by central nervous system pithing and laid supine on ice. Ovarian lobes are taken out and placed in sterile OR-2 solution (in mM: 82.5 NaCl, 2.5 KCl, 1 $MgCl_2$, and 5 HEPES, pH 7). After shredding the ovarian lobes, ~ 5 ml shredded ovaries are incubated with 20 ml of fresh collagenase type-I solution (207 U/ml dissolved in OR-2) in a 50-ml centrifuge tube. The tube is secured horizontally to an orbital shaker and shaken vigorously for 10–20 min to enzymatically and mechanically defolliculate oocytes. After rinsing five or six times with OR-2 to remove the collagenase, oocytes are incubated with a 1:4 SOS:OR-2 solution to gradually increase Ca^{2+} and osmolarity (SOS in mM: 100 NaCl, 2 KCl, 1.8 $CaCl_2$, 1 $MgCl_2$, and 5 HEPES, pH 7, with 100 U/ml penicillin, 100 μ g/ml streptomycin, and 50 μ g/ml gentamicin). After removing damaged and undeveloped oocytes, mature cells are incubated at 18°C for 2 h. Oocytes are then incubated with a 1:2 SOS:OR-2 solution for 30 min and finally transferred in pure SOS solution for use.

Molecular biology

The human α_{1S} subunits (GenBank accession no. BC133671) of skeletal $Ca_v1.1$ channels, with a Cys substituted at the extracellular flank of the S4 helix of each VSD (L159C, M519C, V893C, or

S1231C for VSDs I–IV, respectively; Fig. S1 B), was coexpressed with mouse Stac3 (UniProt accession no. Q8BZ71) and rabbit β_{1a} (UniProt accession no. P19517) in *Xenopus* oocytes. Single-point mutations were generated using the QuikChange Site-Directed Mutagenesis Kit (Agilent Technologies) and confirmed by sequencing. The coding RNA of the different subunits was transcribed in vitro (AmpliCap-Max T7 High Yield Message Maker Kit; CellScript) and injected into stage VI *Xenopus* oocytes (50 nl at 0.1–0.5 $\mu\text{g}/\mu\text{l}$) using a Drummond nano-injector.

VCF

4–5 d after injection, oocytes were incubated with thiol-reactive fluorophores sensitive to environmental changes (10 μM tetramethylrhodamine-6-maleimide [TMRM-6'] for VSD-I or 20 μM MTS-5(6)-carboxytetramethylrhodamine [MTS-TAMRA] for VSDs II, III, or IV) in a depolarizing solution (in mM: 120 K-methanesulfonate [MES], 2 Ba(MES)₂, and 10 HEPES, pH 7.0) for 5–20 min on ice. Subsequently, oocytes were voltage-clamped using the cut-open oocyte technique implemented for epifluorescence measurements (Stefani and Bezanilla, 1998; Pantazis and Olcese, 2013). Fluorescence changes and ionic currents were acquired simultaneously from the same membrane area (Gandhi and Olcese, 2008). The extracellular solution for ionic current recordings was (in mM) 2 Ba(MES)₂, 120 NaMES, and 10 HEPES, pH 7.0. To isolate gating currents, the extracellular solution was supplemented with (in mM) 0.5 CdCl₂, 0.1 LaCl₃, and 0.1 ouabain to block Ca_v1.1 ionic currents and the Na⁺/K⁺ pump, respectively. Intracellular solution contained (in mM) 120 K-glutamate and 10 HEPES, pH 7.0. Pipette solution was (in mM) 2,700 Na-MES, 10 NaCl, and 10 Na-HEPES, pH 7.0. Prior to experiments, oocytes were injected with 100 nl of 80 mM BAPTA•4K, pH 7.0, to prevent activation of endogenous Ca²⁺- and Ba²⁺-dependent Cl⁻ channels (Barish, 1983). Holding potential was –90 mV. Ionic current and fluorescence were filtered at 1/5 of the sampling frequency (typically 1–5 kHz).

Data analysis

The voltage dependence of ionic conductance ($G(V)$, estimated from the peaks of the tail currents), gating charge ($Q(V)$), and fluorescence changes ($F(V)$) was characterized by fitting the data points to one Boltzmann function as $F(V) = \{ [f_{\max} - f_{\min}] / [1 + \exp(z \cdot (V_m - V_{\text{half}})(F/RT))] \} + f_{\min}$, where f_{\max} and f_{\min} are the maximum and minimum values of the function, respectively; z is the effective valence; V_{half} is the half-activation potential; V_m is the membrane potential; T the absolute temperature; and F and R are the Faraday and Gas constants, respectively. For $G(V)$ datasets, f_{\min} was 0. $F(V)$ curves were calculated at steady-state (200-ms pulses; Fig. 3 C). The $F(V)$ curves used to compute their weighed sum were constructed from the fluorescence recording at 10 ms, which is the time of gating current integration used to construct $Q(V)$ curves (Fig. 4 C and Fig. S1 D). Ionic current and fluorescence kinetics were fit to one or two exponential function(s). Fittings were performed by least squares using Microsoft Excel. Data are presented as mean \pm SEM.

Allosteric model of Ca_v activation and statistical analysis

Ca_v1.1 kinetics and steady-state data were described by an allosteric model of five particles: four nonidentical voltage sensors

(with voltage-dependent equilibria $J_{L...J_4}$), coupled to a central pore that was allowed to be intrinsically voltage-dependent (equilibrium L ; Fig. 6), as previously described (Pantazis et al., 2014; Savalli et al., 2016). VSDs and the pore interact with each other via coupling energies ($W_{L...W_4}$).

The equilibrium constant of each VSD is described by

$$J_i = \exp \left[\frac{q_i e}{kT} (V - V_i) \right],$$

where q_i corresponds to the effective valance, V_i to the voltage at which $J_i = 1$, T the absolute temperature, k the Boltzmann constant, and e the charge of an electron. Similarly, the intrinsic equilibrium constant of the pore is described by

$$L = \exp \left[\frac{q_L e}{kT} (V - V_L) \right].$$

The partition function approach was used (Sigg, 2013) to extract the steady-state voltage dependence of each particle. The partition function governing channel gating is given by $Z = Z_c + LZ_o$, where

$$Z_c = (1 + J_1)(1 + J_2)(1 + J_3)(1 + J_4)$$

corresponds to the contracted partition function for the 16 closed states, while

$$Z_o = (1 + J_1 D_1)(1 + J_2 D_2)(1 + J_3 D_3)(1 + J_4 D_4)$$

corresponds to the contracted partition function for the 16 open states. $D_1...D_4$ are related to interaction energies W_i through $D_i = \exp(-W_i/kT)$.

The equilibrium curves for the five gating particles are derived from the partition function through the relations $\langle k \rangle = \partial \ln Z / \partial \ln K$, which were used to simulate the experimental conductance ($G(V)$) and fluorescence ($F(V)$) curves. For kinetic modeling, the forward (α) and backward (β) rate constants for each transition between state n and any accessible state m are expressed as

$$\alpha_{n,m} = \nu_i (Z_n Z_m)^{x_i}$$

and

$$\beta_{n,m} = \nu_i (Z_n Z_m)^{1-x_i},$$

where i refers to the transitioning particle connecting states n and m , and Z_n and Z_m are the configuration-specific contributions to the overall partition function Z . The transition barrier between states n, m is defined by a frequency factor ν_i and a fractional position x_i . Time evolution of all states is solved by integrating $S(t) = S(0) \cdot \exp(Qt)$. Q is the standard rate matrix (Colquhoun and Hawkes, 1981). The initial conditions $S(0)$ for the holding potential were obtained from $S(t \rightarrow \infty)$. The time dependence of a quantity of interest A (ionic current or fluorescence) was obtained from

$$\langle A(t) \rangle = N \sum_n a_n S_n(t),$$

where a_n is the value of the desired quantity of state n . To find the set of parameters (θ) that best reproduced all the experimental data simultaneously, we sampled the parameters space

by the Markov chain Monte Carlo method using the Metropolis-Hasting algorithm as previously (Savalli et al., 2016). Briefly, posterior probabilities distributions of θ were built selecting the one that satisfies

$$\alpha = \min\left(1, \exp\left[\frac{\text{err}(\theta_{i-1}) - \text{err}(\theta_i)}{T}\right]\right)$$

as in Li (2012). The error function on trial i ($\text{err}(\theta_i)$) was as follows:

$$\text{err}(\theta_i) = \sum a_j [\exp_j - \text{sim}_j(\theta_i)]^2.$$

Experiment type (exp_j) refers to $G(V)$ for $j = 1$, $F(V)$ of VSD I-IV for $j = 2..5$, $\text{Im}(t)$ for $j = 6$, $F(V, t)$ of VSD I-IV for $j = 7..10$, and the corresponding calculated function sim_j generated by the model with parameters θ_i of i^{th} trial in the Markov Chain. The set θ_i is included in the chain with probability α , as described in Li (2012).

Online supplemental material

Fig. S1 shows topology of $\text{Ca}_v1.1$ channels, S4 segments sequence alignment, and voltage dependence of $\text{Ca}_v1.1$ channel opening for WT and Cys mutants. Fig. S2 shows that the VSD-I time course of activation follows ionic current kinetics. Fig. S3 shows that the R174W mutation disfavors $\text{Ca}_v1.1$ channel activation. Fig. S4 shows optically tracked voltage-dependent rearrangements of the individual VSD in human $\text{Ca}_v1.1$ R174W mutant. Fig. S5 shows the model prediction of each VSD contribution to pore opening. Table S1 shows fitting parameters and confidence intervals (CIs) for the allosteric model predictions. The parameters that have changed in the presence of the R174W mutation are in bold.

Results

Depolarization-driven structural rearrangements of each VSD in the human $\text{Ca}_v1.1$ channel exhibit distinct time- and voltage-dependent properties

To understand how $\text{Ca}_v1.1$ voltage-sensing machinery can control both the $\text{Ca}_v1.1$ pore itself and the RYR1-induced Ca^{2+} release, we optically tracked the structural rearrangements of each of the four VSDs of this Ca_v channel (Fig. 2 A), using the VCF technique, a hybrid electrophysiological-optical approach (see VCF; Mannuzzu et al., 1996; Gandhi and Olcese, 2008; Pantazis and Olcese, 2013). We engineered each VSD of the human pore-forming α_{1S} subunit for site-directed fluorescent labeling by substituting amino acids at strategic positions in the extracellular end of the S4 helix with a cysteine suitable for labeling with thiol-reactive fluorophores (Fig. S1 B; see Molecular biology for Cys positions). Among the four helices forming each VSD, S4 segments carry a signature motif of positively charged residues able to sense changes of membrane potential and rearrange in response to this electrical stimulus (Catterall, 2010; Wu et al., 2016). The Cys constructs chosen for this study did not perturb channel function: the voltage dependence of channel activation ($G(V)$) and of $Q(V)$ of Cys mutant channels appeared identical to that of WT channels (Fig. S1, C and D; Table 1; and Table 2).

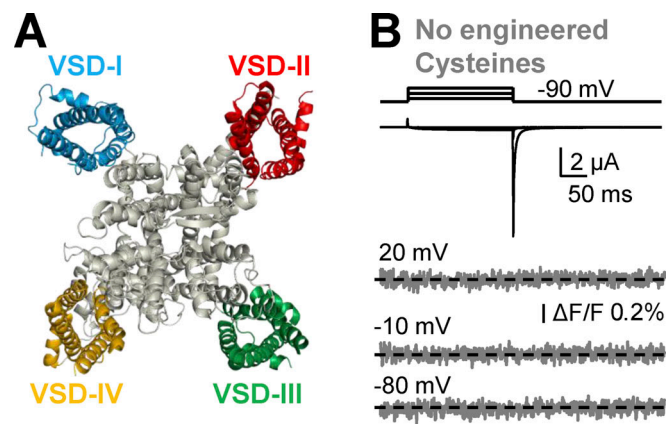


Figure 2. **WT $\text{Ca}_v1.1$ does not elicit voltage-dependent fluorescence change when labeled with a thiol-reactive fluorophore.** (A) Top view of a cryo-EM structure of the pore-forming α_{1S} subunit of $\text{Ca}_v1.1$ channels (Protein Data Bank accession no. 5GJV; Wu et al., 2016), illustrating four VSDs that surround and control the central pore. (B) Simultaneously recorded Ba^{2+} currents (black) and fluorescence signals (gray traces) at the indicated membrane potentials from human $\text{Ca}_v1.1$ channels ($\alpha_{1S}+\beta_{1a}+\text{Stac3}$) without an engineered Cys, expressed in *Xenopus* oocytes and labeled with thiol-reactive fluorophores, are shown.

We expressed human $\text{Ca}_v1.1$ channels in *Xenopus* oocytes (Wu et al., 2018). Oocytes were voltage-clamped using the cut-open oocyte Vaseline gap technique (Stefani and Bezanilla, 1998; Pantazis and Olcese, 2013): we simultaneously recorded membrane current and fluorescence emission from channels labeled with thiol-reactive fluorophores, used as optical reporters of VSD structural rearrangements. Voltage-dependent fluorescence signals were not detected in $\text{Ca}_v1.1$ WT channels (no engineered cysteines but 13 endogenous extracellular cysteines are present; Fig. 2 B). Also, fluorescent labeling of endogenous cysteines had no effect on the voltage dependence of channel activation (Fig. S1 C). Notably, when engineered Cys were fluorescently labeled one at the time, we resolved distinct voltage-dependent conformational changes of each $\text{Ca}_v1.1$ voltage sensor (Fig. 3 A). Fluorescence signals from VSD-I and VSD-III decreased upon depolarization, implying that fluorophores conjugated to these VSDs experienced a more quenching environment in their active state, while fluorophores conjugated to VSD-II and VSD-IV were brighter during depolarization. Overall, these results support the premise that fluorescence changes from channels with introduced Cys report VSD-specific structural rearrangements.

Each voltage sensor exhibited distinct kinetic properties that could be well-described by the sum of two exponential functions: VSD-I time-dependent properties were overall similar to ionic current activation kinetics, while VSDs II-IV displayed a faster activation component, compatible with SR Ca^{2+} release kinetics (Fig. 3 B and Fig. S2). Nevertheless, all VSDs exhibited a slow kinetic component of $\tau \approx 100$ ms (Fig. S2 A), which is prevalent in VSD-I and less represented in VSD-II, VSD-III, and VSD-IV (Fig. S2 B). Thus, using VCF, we demonstrated the existence of fast- and slow-activating $\text{Ca}_v1.1$ VSDs by directly measuring their activation kinetics, a result that confirms the predictions of Feldmeyer et al. (1990) based on ionic current

Table 1. Fitting parameters for the Boltzmann functions fitting the voltage dependence of Ca_v1.1 activation data (curves in Fig. S1 C and Fig. 5 A)

	Parameter	Mean ± SEM
G(V) WT no fluorophore	z (e^0)	2.0 ± 0.04 ($n = 7$)
	V_{half} (mV)	31 ± 1.1
G(V) WT with TAMRA	z (e^0)	2.0 ± 0.02 ($n = 3$)
	V_{half} (mV)	30 ± 1.3
G(V) L159C (VSD-I) with TMRM	z (e^0)	1.9 ± 0.02 ($n = 6$)
	V_{half} (mV)	29 ± 1.1
G(V) M519C (VSD-II) with TAMRA	z (e^0)	2.0 ± 0.05 ($n = 7$)
	V_{half} (mV)	28 ± 0.6
G(V) V893C (VSD-III) with TAMRA	z (e^0)	2.1 ± 0.07 ($n = 5$)
	V_{half} (mV)	31 ± 1.9
G(V) S1231C (VSD-IV) with TAMRA	z (e^0)	1.8 ± 0.03 ($n = 6$)
	V_{half} (mV)	32 ± 1.1
G(V) R174W no fluorophore	z (e^0)	1.8 ± 0.06 ($n = 3$)
	V_{half} (mV)	64 ± 0.6

recordings and those of the Flucher laboratory (Fernández-Quintero et al., 2021) based on molecular dynamics simulations, which estimated slow and fast activation kinetics for VSD-I and VSD-IV, respectively.

The voltage dependence of activation for each Ca_v1.1 VSD (from experiments as in Fig. 3 A) was inferred by plotting the change in fluorescence intensity (ΔF) at 200 ms against the corresponding membrane potentials ((F(V) curve, Fig. 3 C): each VSD of human Ca_v1.1 channels exhibited distinct voltage-dependent activation curves, all preceding the G(V) curve (voltage dependence of channel opening) on the voltage axis (Fig. 4): VSD-I was the most sensitive to changes in membrane potential (effective valence $z = 3.1 \pm 0.05 e^0$, $n = 6$), while VSD-IV was the least ($z = 0.68 \pm 0.01 e^0$, $n = 6$). Moreover, the half-activation potential (V_{half}) of the four F(V) curves spanned a range of ~40 mV along the membrane potential axis: VSD-I was the most depolarized ($V_{\text{half}} = 4.2 \pm 0.8$ mV, $n = 6$), followed by VSD-II, -III, and -IV (Fig. 3 C and Table 3).

These results reveal the striking functional diversity of the four VSDs in human Ca_v1.1 channels in terms of time and voltage dependence, possibly underlying distinct physiological roles.

Charge movement and fluorescence signals arise from the same conformational changes

Before VCF was developed, gating current recordings represented the gold standard measurement to extrapolate information about the properties of voltage sensors (Bezannilla and Stefani, 1998). However, gating currents are ensemble composite signals generated by the movement of the four charged voltage sensors, and thus the computed voltage dependence of the charge movement (Q(V) curve) blends together information from all four heterologous VSDs. The Q(V) curve of human Ca_v1.1 channels falls within the voltage range of the four F(V) curves describing the voltage dependence of each distinct VSD

Table 2. Fitting parameters for the Boltzmann functions fitting the voltage dependence of Ca_v1.1 gating charge data (curves in Fig. S1 D)

	Parameter	Mean ± SEM
Q(V) WT	z (e^0)	1.1 ± 0.03 ($n = 5$)
	V_{half} (mV)	-1.4 ± 0.9
Q(V) L159C (VSD-I)	z (e^0)	1.1 ± 0.03 ($n = 3$)
	V_{half} (mV)	-1.3 ± 1.5
Q(V) M519C (VSD-II)	z (e^0)	1.1 ± 0.03 ($n = 3$)
	V_{half} (mV)	-3.5 ± 0.8
Q(V) V893C (VSD-III)	z (e^0)	1.0 ± 0.01 ($n = 4$)
	V_{half} (mV)	-1.1 ± 1.2
Q(V) S1231C (VSD-IV)	z (e^0)	1.1 ± 0.03 ($n = 4$)
	V_{half} (mV)	-1.4 ± 1.4

(Fig. 4). As charge movement (Q(V)) and fluorescence signals (F(V)s) are expected to arise from the same voltage-dependent conformational rearrangements, a reasonable prediction is that the sum of four F(V) curves weighed by their respective effective valence (z) would approximate the Q(V) curve. For this purpose, the four F(V) curves were constructed from the amplitude of fluorescence signals after 10-ms depolarizations, which is the time of gating current integration to construct Q(V) curves. The result of this operation is reported in Fig. 4 C, which shows that Q(V) and F(V) weighed sum have practically identical voltage dependence: in other words, VCF allowed decomposition of the Q(V) curve into its four components, providing previously unattainable information.

A naturally occurring, charge-neutralizing mutation (R174W) impairs VSD-I activation and voltage-dependent channel opening

The relevance of VSD-I to Ca_v1.1 activation, highlighted by the compatible kinetics (Fig. 3 B and Fig. S2), was confirmed by introducing a naturally occurring mutation that neutralizes the innermost charge of VSD-I S4 helix (R174W) and that has been linked to a skeletal muscle disorder called malignant hyperthermia (MH; Eltit et al., 2012; Bannister and Beam, 2013b). We expressed either WT or mutant Ca_v1.1 channels in *Xenopus* oocytes and measured ionic currents (Fig. S3). The activation voltage dependence of R174W channels shifted to more depolarized membrane potentials by ~35 mV as compared with WT channels, impairing Ca²⁺ influx at physiological membrane potentials (Fig. 5 A). To gain a mechanistic understanding of how R174W impairs Ca_v1.1 pore activation, we optically tracked the movement of VSD-I using the VCF technique (Fig. S4 A). We found that the MH-linked mutation caused a ~30 mV rightward-shift of VSD-I voltage-dependent activation and reduced the sensitivity to changes in membrane potentials (effective charge, z ; Fig. 5 B and Table 3). These results demonstrate that R174 is indeed a voltage-sensing charge and further support the role of VSD-I as the main driver of pore opening.

Moreover, we found that the voltage- and time-dependent properties of VSDs II, III, and IV were not affected by the

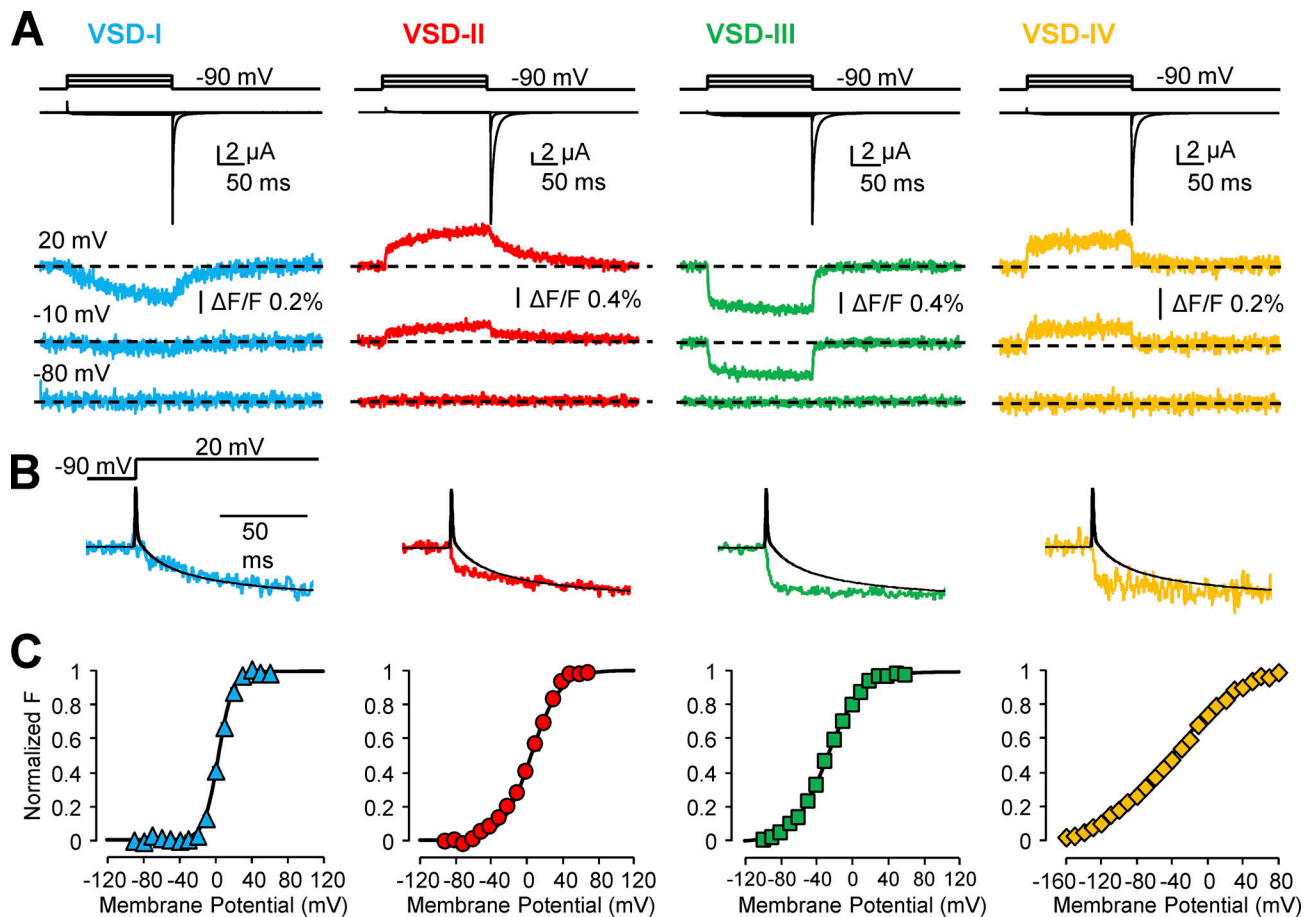


Figure 3. Depolarization-driven structural rearrangements of each VSD in the human $Ca_v1.1$ channel exhibit distinct time- and voltage-dependent properties. (A) Simultaneously recorded Ba^{2+} currents (black) and fluorescence signals (colored traces) reporting local protein structural changes at the indicated membrane potentials from human $Ca_v1.1$ channels ($\alpha_{1S}+\beta_{1a}+Stac3$) expressed in *Xenopus* oocytes and labeled with thiol-reactive fluorophores are shown. Fluorophore conjugated at the extracellular flank of S4 helices of each VSD reported time- and voltage-dependent structural rearrangements upon depolarization. (B) Ionic current (black) elicited by 20 mV depolarization is shown superimposed to the fluorescence traces from each VSD (holding potential was -90 mV). Note that only VSD-I fluorescence signal exhibited kinetics compatible with pore opening (see also Fig. S2). (C) Mean voltage dependence of VSD activation constructed at 200 ms from experiments as in A. Lines represent fits to single Boltzmann distributions (SEM bars are within the symbols, when not visible; $n = 5-7$). Note that each VSD exhibited distinct voltage-dependent properties. Table 3 reports fitting parameters of Boltzmann functions describing these $F(V)$ curves.

R174W mutation (Fig. 5 B and Table 3), ruling out the possibility of significant cooperativity among voltage sensors.

VSD-I contributes the most energy to stabilizing WT $Ca_v1.1$ open states

To quantify the energetic contribution of the individual $Ca_v1.1$ VSDs to channel opening, we used a structurally relevant, allosteric model of Ca_v activation, previously developed for $Ca_v1.2$ channels (Pantazis et al., 2014; Savalli et al., 2016).

This model accounts for both time- and voltage-dependent properties of Ca_v channels and comprises five two-state gating particles, resulting in $2^5 = 32$ possible states (16 closed states and 16 open states): a pore, which can exist either in the open or closed state, and four voltage sensors, each transitioning between resting and active states (Fig. 6; Pantazis et al., 2014; Savalli et al., 2016). The voltage-dependent equilibrium of each particle was characterized by V_i , the voltage at which they are equally distributed among the two states, and q_i , the apparent

number of elementary charges displaced during activation (see Allosteric model of $Ca_v...$ for further details). This allosteric model has no a priori assumptions, i.e., the channel can potentially open from any of the 16 closed states. The activation of each VSD contributes some energy (W_i) to the stabilization of the open state of the pore. We performed a global simultaneous fit of ionic currents and fluorescence changes (which report the movements of each VSD) at four different membrane potentials together with their corresponding steady-state curves $G(V)$ and $F(V)$ s (voltage dependence of activation of the pore and VSDs, respectively) for WT and R174W channels. As shown in Fig. 7, we found a parameter set that faithfully reproduced the experimental data obtained with WT as well as R174W $Ca_v1.1$ channels simultaneously; only parameters pertaining to VSD-I were allowed to differ between WT and mutant channels (Table S1). This solution was found by Markov chain Monte Carlo sampling with $5 \cdot 10^6$ samples in three replicas that also tested for uniqueness and provided CIs for all parameters (Fig. 7 and Table S1).

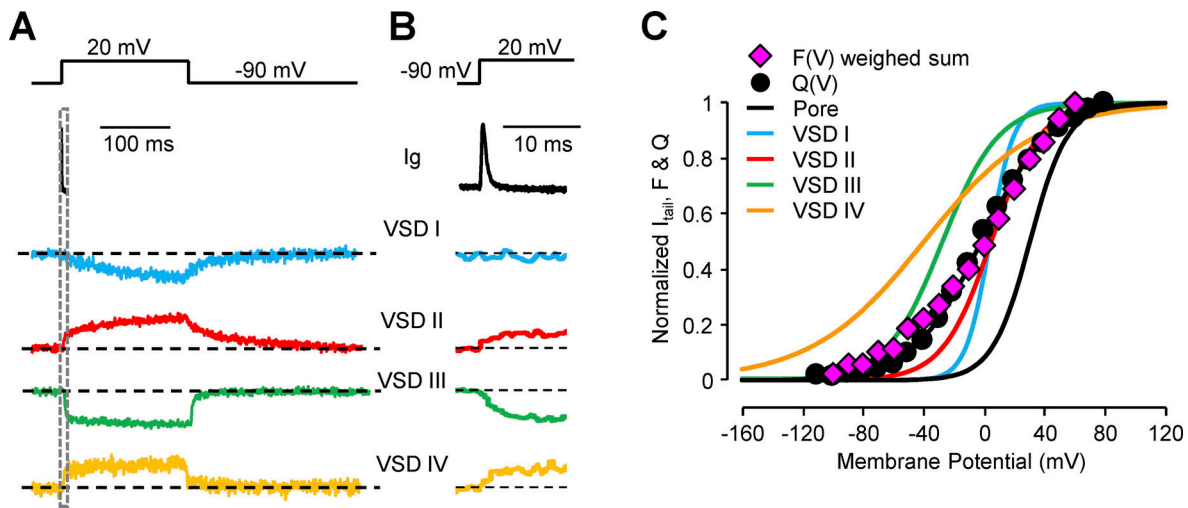


Figure 4. Charge movement and fluorescence signals arise from the same conformational changes. (A and B) Gating current and fluorescence recordings are shown in the same time scale (enlarged view in B). Note that VSD-I barely activates during the time course of gating current measurements (10 ms). **(C)** Mean voltage dependence of charge movement (Q(V)), channel activation (G(V)), and individual VSD activations (F(V)) are shown. For clarity, only Boltzmann distributions describing G(V) and F(V) datasets are plotted (data points were already presented in Fig. S1 C and Fig. 3 C, respectively). The sum of F(V) curves weighed by their respective valence (pink diamonds) resembles the voltage dependence of the mean Q(V) curve (black circles; SEM bars are within the symbols, when not visible, $n = 5$).

This analysis revealed that VSD-I contributes the most energy to stabilizing the open state in WT channels ($-99 < W_{1WT} < -71$ meV; 95% CI; Table S1). The other three VSDs were predicted to have a smaller or negligible contribution ($W_i > -21$ meV), as illustrated in Fig. S5, which compares the impact of each VSD on the facilitation of voltage dependence of activation (i.e., leftward shift of G(V) curve with respect to the intrinsic voltage dependence of the pore). These plots show that the largest contribution is conferred by VSD-I (Fig. S5 A), with a smaller role of VSD-IV (Fig. S5 D) and negligible influence of VSD-II and VSD-III (Fig. S5, B and C).

Sampling the parameters space by Markov chain Monte Carlo as in Savalli et al. (2016) yields the probabilities distributions for the parameters describing the data according to the allosteric model. These distributions, depicted as violin plots in Fig. 8, indicate that the likelihood that VSD-II, VSD-III, or VSD-IV contribute to pore opening >1 kT (i.e., $W_i < -25$ meV) is <0.00075 , <0.03 , and <0.15 , respectively.

Table 3. Fitting parameters for the Boltzmann functions fitting the voltage dependence of each VSD structural changes (curves in Figs. 3 and 5)

	Parameter	WT (mean ± SEM)	R174W (mean ± SEM)
F(V) L159C (VSD-I)	z (e^0)	3.1 ± 0.05 ($n = 6$)	1.8 ± 0.06 ($n = 5$)
	V_{half} (mV)	4.2 ± 0.8	35 ± 1.1
F(V) M519C (VSD-II)	z (e^0)	1.6 ± 0.06 ($n = 7$)	1.3 ± 0.08 ($n = 4$)
	V_{half} (mV)	4.6 ± 1.1	4.2 ± 1.9
F(V) V893C (VSD-III)	z (e^0)	1.4 ± 0.03 ($n = 5$)	1.5 ± 0.1 ($n = 4$)
	V_{half} (mV)	-27 ± 1.1	-28 ± 0.7
F(V) S1231C (VSD-IV)	z (e^0)	0.7 ± 0.01 ($n = 6$)	0.6 ± 0.02 ($n = 3$)
	V_{half} (mV)	-38 ± 1.3	-36 ± 1.5

Analyzing VCF data with an allosteric model for Ca_v activation, we also found that a single charge-neutralizing mutation in VSD-I not only made this sensor reluctant to activate but also drastically decreased the energetic coupling between VSD-I and the pore ($-42 < W_{1R174W} < -10$ meV; 95% CI; Table S1). In other words, in R174W channels, when VSD-I activates, its contribution to the stabilization of the open configuration of the channel is weaker, resulting in reduced Ca^{2+} influx at physiological membrane potentials. Also, the valence (q_1) of the perturbed VSD-I was reduced by $\sim 60\%$, consistent with the neutralization of a relevant gating charge. The fitting parameter set and relative CIs are presented in Table S1.

The allosteric model developed here predicts that the pore has an intrinsic voltage dependence of $\sim 1.7 e^0$ ($1.6 < q_L < 1.8 e^0$; 95% CI). A salient feature of allosteric interactions is that channel opening will still occur when all the sensors are at the resting state. However, if the pore domain conformational changes during channel gating are intrinsically voltage-dependent, a continuous increase in the channel P_{open} should be observed after all voltage sensors are maximally active. This behavior can be visualized by plotting the G(V) as a Hill plot adapted for voltage-dependent equilibrium $\ln[G(V)/(1 - G(V))]$ (Sigg, 2013). With such transformation, a two-state system yields a straight line with a slope corresponding to the effective valence and intercept ($G(V) = 0.5$) at $V_{1/2}$. The Hill-transformed G(V) for both WT and R174W channels became asymptotic for positive membrane potentials with a slope representing the effective valence of the intrinsic voltage dependence of the pore (i.e., without the contribution of the VSDs; Sigg, 2013). Note that the model approximates the data well, yielding the intrinsic effective valence of the pore ($q_L = 1.7 e^0$). The allosteric model also predicted that R174W mutation is associated with a reduction of VSD-pore coupling energy of 59 meV ($\Delta\Delta G = \sum W_{WT} - \sum W_{R174W}$) (Fig. 9).

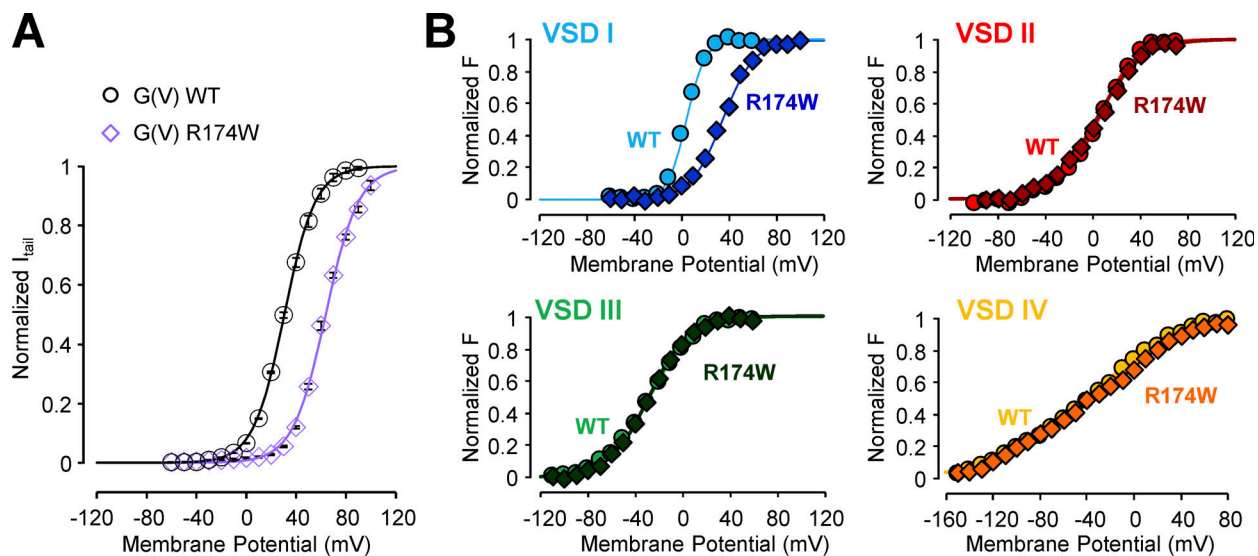


Figure 5. A naturally occurring, charge-neutralizing mutation (R174W) impairs VSD-I activation and voltage-dependent channel opening, leaving VSDs II, III, and IV unaffected. (A) Voltage dependence of pore opening, as measured by normalized Ba^{2+} current tails for WT or R174W channels. Lines are fits to single Boltzmann distributions. Note that the R174W mutation caused a rightward-shift of the current voltage dependence $G(V)$. (B) Mean voltage dependence of VSD activation constructed from experiments as in Fig. S4. Lines are fits to single Boltzmann distributions. Note that the R174W mutation impaired VSD-I activation, as revealed by a more depolarized voltage dependence, leaving VSDs II, III, and IV unaffected. Tables 1 and 3 report fitting parameters of Boltzmann functions describing $G(V)$ and $F(V)$ curves for R174W $Ca_v1.1$ channels, respectively.

In summary, the 32-state allosteric model of Ca_v gating lends further support to a predominant role of VSD-I in $Ca_v1.1$ activation and assigned a smaller contribution of VSD-IV. Based on this analysis, VSD-II and VSD-III would not contribute to channel opening. We speculate that VSD-II and VSD-III remain available for other voltage-dependent channel functions, such as RYR1 activation and, consequently, SR Ca^{2+} release, since EC

coupling remains functional in patients carrying a R174W missense mutation of $Ca_v1.1$ (Eltit et al., 2012).

Discussion

Using VCF and computational modeling, we have dissected the operation of the voltage-sensing apparatus of the human skeletal muscle $Ca_v1.1$ channel, revealing the functional properties of each of its four voltage sensors. The experimental results expose a striking heterogeneity in their voltage- and time-dependent properties and shed light on the apparent paradox whereby an extremely slowly activating channel controls a very fast process, SR Ca^{2+} release, that takes place during 2–5 ms of the skeletal muscle action potential. We found that VSD-I plays a major role in $Ca_v1.1$ channel activation, based on several pieces of evidence: (1) VSD-I time-dependent properties are compatible with ionic current activation kinetics (Fig. 3 B and Fig. S2); (2) the neutralization of the innermost charge of VSD-I (R174W) impairs the activation of this voltage sensor, in turn compromising voltage-dependent $Ca_v1.1$ pore opening at physiological membrane potentials (Fig. 5); and (3) a statistical mechanical model relevant to Ca_v molecular architecture predicts that the open state of the human $Ca_v1.1$ pore is mostly stabilized by VSD-I activation ($W_1 = -81$ meV or ~ 3 kT) with a minimal contribution of the other VSDs ($W_{2-4} > -25$ meV or < 1 kT; Fig. 7 and Table S1). Other mutations of voltage-sensing charges in VSD-I also affect ionic current voltage dependence (García et al., 1997; El Ghaleb et al., 2019), in agreement with a role of VSD-I in channel opening. On the other hand, VSD-II, -III, and -IV display activation components ~ 20 -fold faster than VSD-I (Fig. 3 B and Fig. S2), a feature that qualifies them as kinetically compatible candidates for a role as voltage sensor(s) of SR Ca^{2+} release. Since a large body of

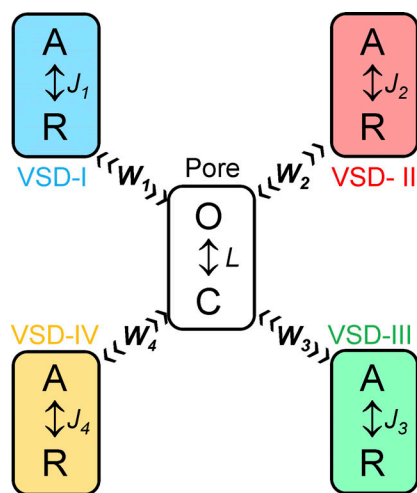


Figure 6. Scheme of a structurally relevant, allosteric model of Ca_v activation, accounting for both time- and voltage-dependent properties of VSD activation and pore opening. See Pantazis et al. (2014), Savalli et al. (2016), and Allosteric model of Ca_v ... Briefly, each VSD and the pore (equilibrium constant J and L) are modeled as two-state particles, undergoing resting (R)–active (A), or closed (C)–open (O), voltage-dependent transitions, respectively. VSD activation allosterically stabilizes the pore open state by coupling energy W .

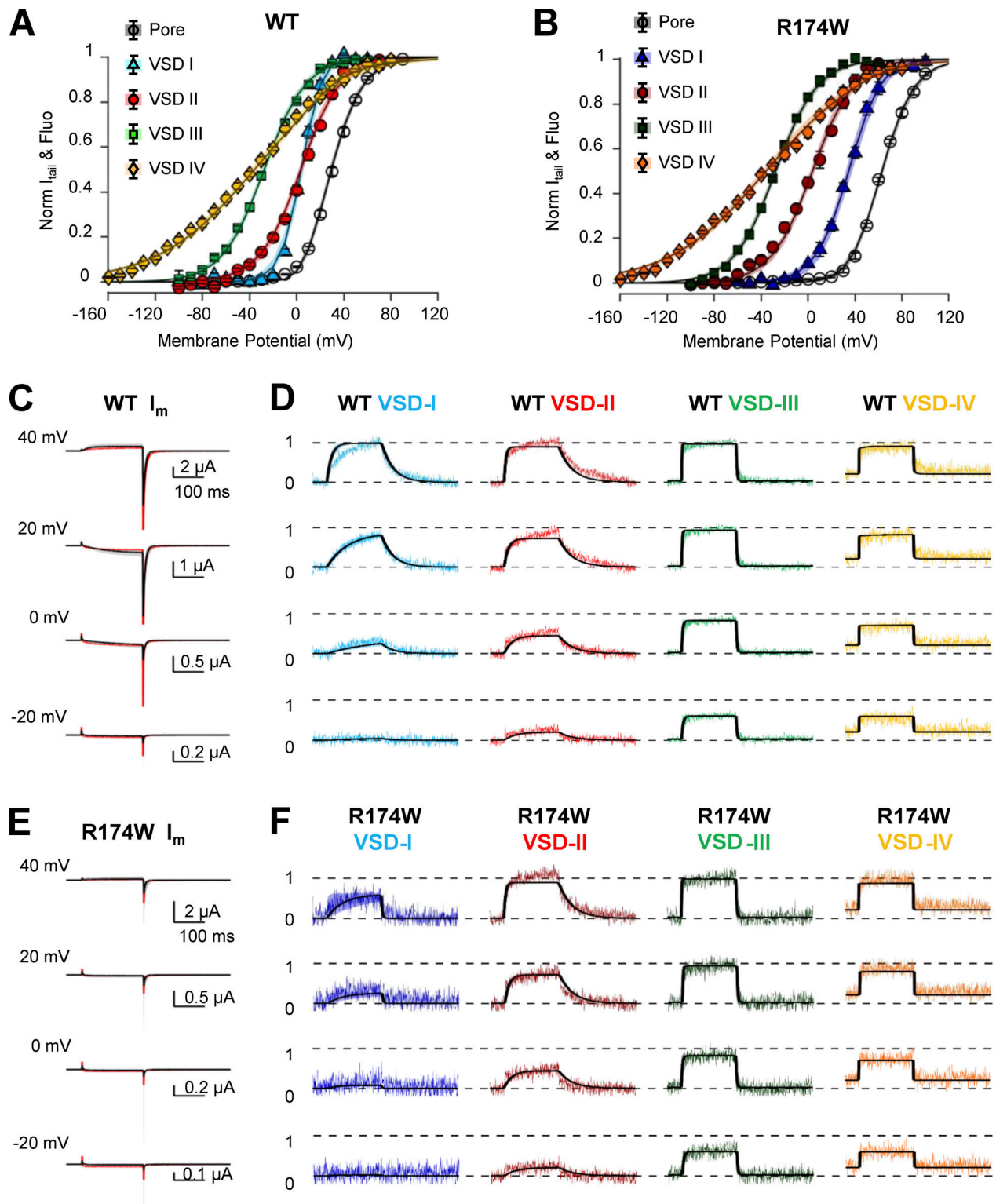


Figure 7. **VSD-I is the main contributor to $Ca_v1.1$ pore opening.** A Ca_v allosteric model (scheme in Fig. 6) was used to simultaneously fit steady-state and kinetics data in both WT and R174W channels. An error function was minimized using a Markov chain Monte Carlo sampling as in Savalli et al. (2016). Only parameters characterizing VSD-I activity could vary independently for WT and R174W channels. **(A and B)** Experimental G(V) and F(V) data points are shown superimposed to the model predictions (black lines) for WT (A) and R174W (B) channels. **(C–F)** Ionic currents (C and E) and fluorescence traces (D and F) from each VSD (normalized to the steady-state probability of activation) in both WT (C and D) and R174W (E and F) channels are shown superimposed with model predictions (black lines, best solutions out of $1.5 \cdot 10^6$ trials from three replicas). Shaded areas depict all solutions within the 95% CI. Solution uniqueness and CIs are described in Fig. 8 and Table S1.

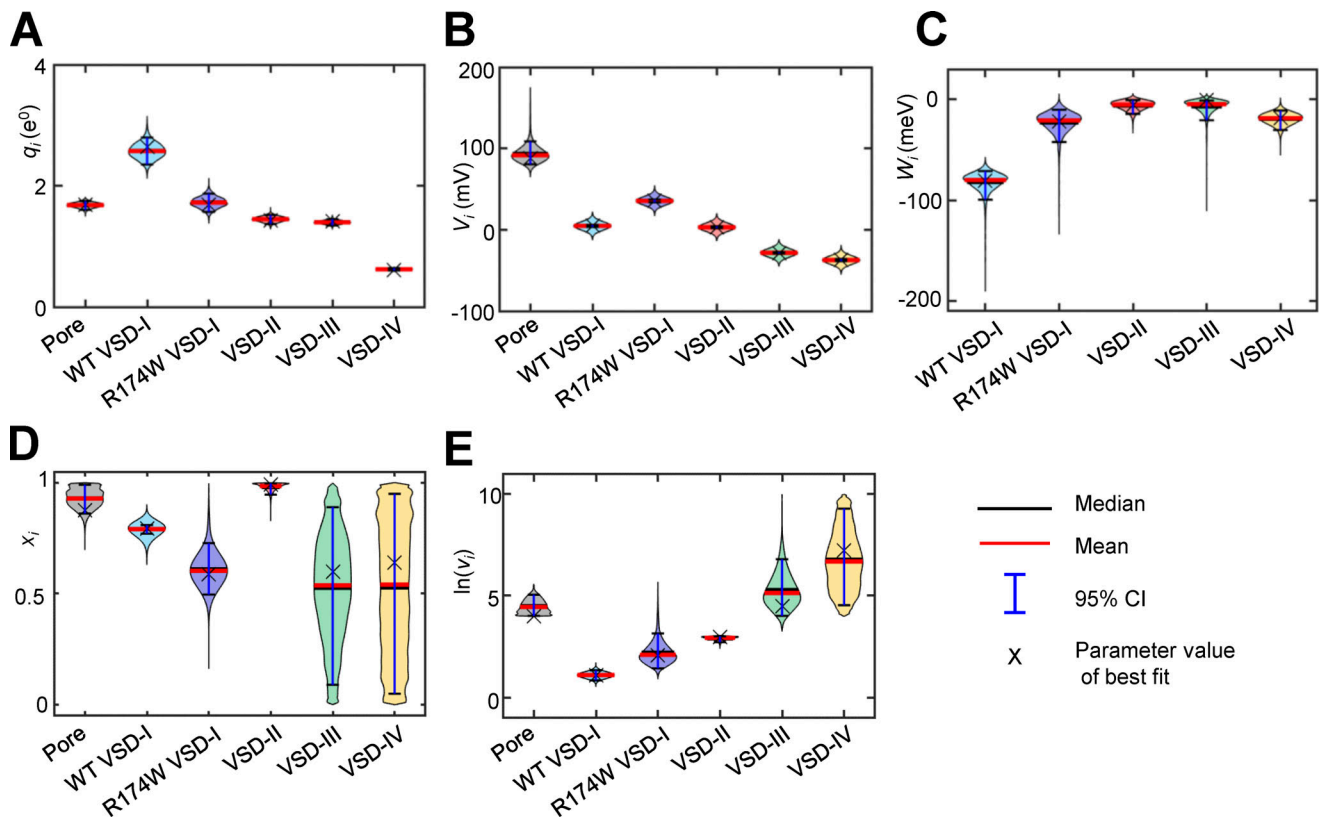


Figure 8. **Violin plots describing the estimated probability distributions of parameters.** (A–E) q_i (A), V_i (B), W_i (C), x_i (D), and $\ln(v_i)$ (E). The best fit solution (X) exhibits the smallest error out of $1.5 \cdot 10^6$ samples distributed in three replicas and corresponds to the model predictions presented in Fig. 7 (black lines). The mean and median of each parameter are shown as red and black horizontal lines, respectively. The vertical blue line indicates the 95% CI for each parameter. The shaded areas depict the posterior probability density function for each parameter obtained by the Markov chain Monte Carlo sampling smoothed by a kernel density estimator (Hoffmann, 2021). The computational model yielded a highly constrained set of parameters describing simultaneously datasets from both WT and R174W mutants (Table S1). Note that, since VSD-III and VSD-IV activation kinetics are extremely fast, the actual relative position in the electric field of the transitions energy barrier (x_3 and x_4) has little influence on the goodness of fit, as illustrated by the vertical spreading of these parameter distributions (D).

evidence implicates the intracellular II–III loop for a major role in transducing depolarization sensed by Ca_v1.1 to RYR1 opening (Bannister and Beam, 2013a), we speculate that either VSD-II or VSD-III (or both) represent the voltage sensor(s) of skeletal EC coupling (Fig. 10).

Ca_v1.1 channels exhibit a unique mechanism for voltage-dependent channel opening, among the super family of voltage-gated ion channels

The present study suggests that Ca_v1.1 complexes operate mainly upon activation of a single voltage sensor (VSD-I), a feature which has not been observed in any other voltage-gated ion channel (Smith-Maxwell et al., 1998; Chanda and Bezanilla, 2002; Pantazis et al., 2014). Indeed, K_v channels typically require activation of all four VSDs to favor pore opening (Smith-Maxwell et al., 1998), while Na_v channels require the activation of three VSDs (specifically, VSDs I, II, and III; Chanda and Bezanilla, 2002; Goldschen-Ohm et al., 2013). In addition, we recently discovered that pore opening in Ca_v1.2 channels is mainly driven by two voltage sensors (VSDs II and III; Pantazis et al., 2014; Savalli et al., 2016).

Previous studies in rabbit embryonic and adult Ca_v1.1 variants suggested that VSD-IV controls voltage sensitivity of pore

opening (Tuluc et al., 2016). However, in the human adult Ca_v1.1 channel used in our study, the computational analysis with a Ca_v allosteric model predicts a small energetic contribution of VSD-IV activation to the stabilization of the pore open state (Table S1). The difference with previous studies regarding the role of VSD-IV may arise from the different Ca_v1.1 isoform (human in this study versus rabbit in Tuluc et al. [2016]) or from the different cellular environment (*Xenopus* oocytes in this study versus mouse dysgenic myotubes in Tuluc et al. [2016]). It is also possible that the deletion of 19 amino acids in VSD-IV of embryonic channels increases the energetic contribution of this sensor to channel activation.

Different L-type Ca²⁺ channels engage different VSDs to open their pores

In skeletal Ca_v1.1 channels composed of α_{1S}/β_{1a} , the mid-point of VSDs activation spans a range of ~ 40 mV (Table 3), while in Ca_v1.2 channels (α_{1C}/β_3), the extent is larger (~ 80 mV; Savalli et al., 2016), implying a more loose coupling between voltage sensors and pore in the latter case. Indeed, the overall energetic coupling ($\sum W$) between VSDs and pore quantified by an allosteric model of Ca_v channel activation supports this view: in

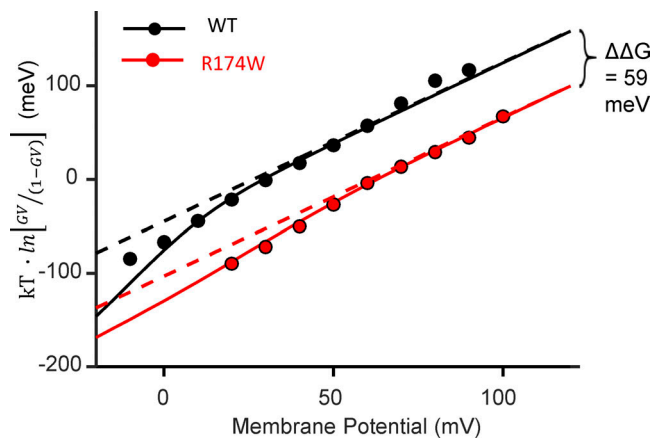


Figure 9. **Hill plot of $\text{Ca}_v1.1$ WT and R174W channels activity highlights the intrinsic voltage dependence of the pore.** The filled circles represent the Hill-transformed experimental $G(V)$ data points for WT and R174W channels. Continuous lines are the Hill-transformed $G(V)$ curves predicted by the allosteric model. Dashed lines correspond to straight lines with slope of $1.7 e / kT$ obtained as described in the text. Note that the two channels exhibit a difference in the overall pore-VSD coupling energy ($\Delta\Delta G$) of 59 meV (as estimated from ΣW_i for the WT and R174W obtained from the model best fit).

skeletal channels, ΣW is ~ 100 meV (Table S1), while in $\text{Ca}_v1.2$ channels, ΣW corresponds to a smaller value (~ 40 meV; Savalli et al., 2016). Thus, the mechanism of voltage-dependent pore opening in L-type Ca_v channels appears to be isoform-specific

and does not conform to a single conserved mechanism, despite $\sim 90\%$ sequence homology in the transmembrane segments and practically identical S4 helices. Conceivably, the difference in extracellular and intracellular linkers mediates the large functional difference of $\text{Ca}_v1.1$ and $\text{Ca}_v1.2$ channels, resulting in very different physiological functions. Indeed, previous studies in Ca_v channels (Nakai et al., 1994; Tuluc et al., 2016; Liu et al., 2017) and other voltage-gated ion channels (Priest et al., 2013) demonstrate the importance of the S3-S4 linker sequence and length in defining the biophysical properties of channel activation.

Conclusions and perspectives

We have pioneered VCF in human $\text{Ca}_v1.1$ complexes and resolved unique time- and voltage-dependent properties of its four VSDs. We explained how $\text{Ca}_v1.1$ channels solve the task of controlling both the fast (1–3 ms) SR Ca^{2+} release via RYR1 activation and the slow (40–60 ms) opening of its own pore, by assigning each function to distinct VSDs. VSD-I qualifies as the main contributor of $\text{Ca}_v1.1$ activation, a new solution for voltage-dependent channel activation, while VSD-II and -III exhibit biophysical properties compatible with the timing of SR Ca^{2+} release, likely representing the voltage sensor(s) of skeletal EC-coupling mechanism. More studies are certainly needed to reveal the precise role of $\text{Ca}_v1.1$ VSDs in RYR1 gating and EC coupling. However, the experimental strategy developed here sets a framework to mechanistically address clinically relevant questions on the functional consequences of disease-causing mutations in $\text{Ca}_v1.1$ voltage dependence (e.g., hypokalemic

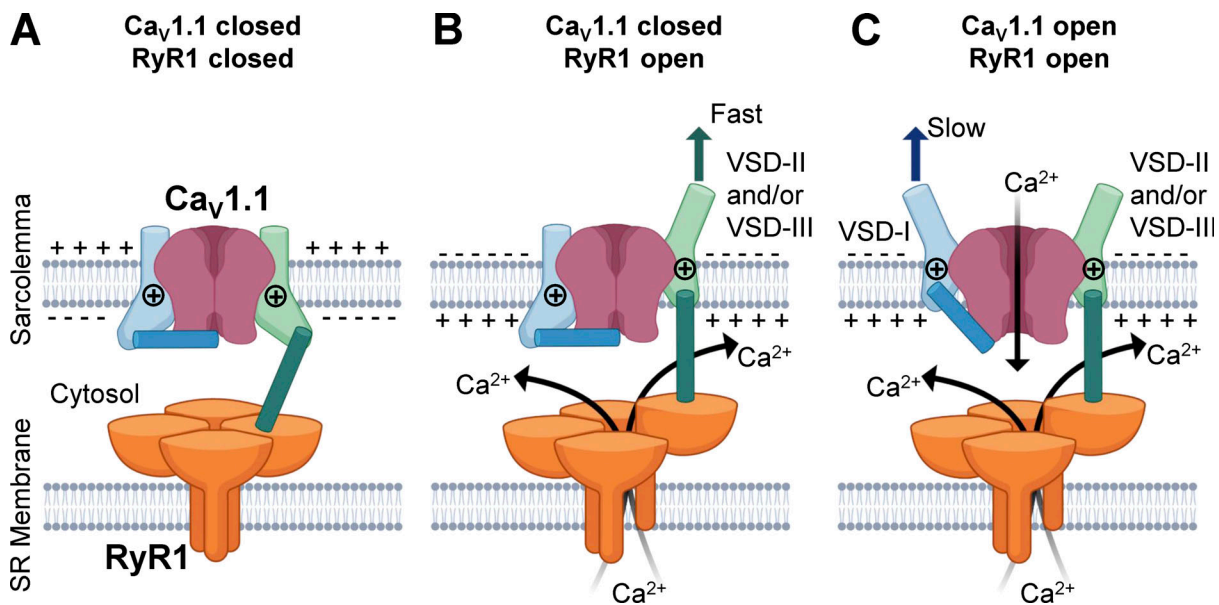


Figure 10. **The role of $\text{Ca}_v1.1$ VSDs: fast and slow VSDs control RYR1 and $\text{Ca}_v1.1$ activation, respectively.** (A) Scheme depicting the main players in the skeletal muscle EC coupling process: RYR1 (orange) is unable to sense depolarizations of the sarcolemma because of its localization in the intracellular SR. RYR1 is in physical contact (directly or via auxiliary proteins) with $\text{Ca}_v1.1$ channel (red), which is inserted in the sarcolemma and confers voltage dependence to RYR1. At rest, both channels are closed, and the skeletal muscle is relaxed. (B and C) Upon depolarization, the VSDs of $\text{Ca}_v1.1$ channels (blue and green) rearrange. VSD-II and VSD-III kinetics are compatible with the SR Ca^{2+} -release time course; thus, we propose that their movement mechanically and rapidly propagates to RYR1 (B), allowing for SR Ca^{2+} -release: VSD-II and/or VSD-III constitute the voltage sensor(s) of skeletal muscle contraction. On the other hand, VSD-I (blue) activates with slower kinetics compatible with $\text{Ca}_v1.1$ opening. Indeed, combining fluorometry, mutagenesis, and mathematical modeling, we demonstrated that VSD-I contributes the most energy to $\text{Ca}_v1.1$ activation (C). While each homotetrameric RYR1 interacts with four $\text{Ca}_v1.1$ channels, for clarity, the cartoon only depicts one $\text{Ca}_v1.1$ interacting with one monomer of RYR1. This scheme was created with <http://www.BioRender.com>.

periodic paralysis and MH-associated mutations; [Flucher, 2020](#)). The approach developed in this work can also advance our knowledge on the fundamental mechanisms underlying $\text{Ca}_v1.1$ modulation by auxiliary subunits or alternative splicing, benefiting from the new level of information attainable by simultaneously acquiring structural data from functional channel proteins operating in a membrane environment.

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Supplemental material

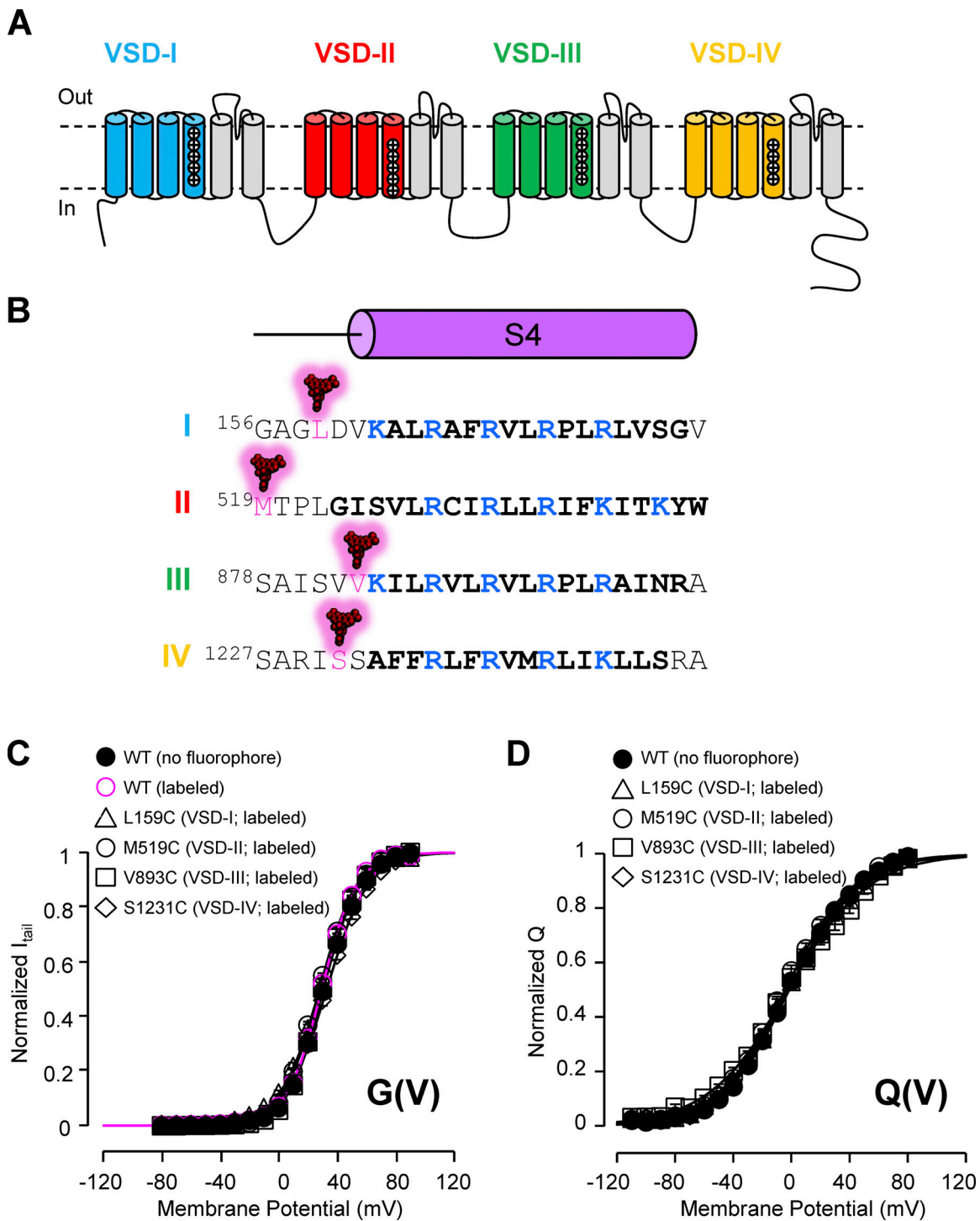


Figure S1. **Topology of $Ca_v1.1$ channels, S4 segments sequence alignment, and voltage dependence of $Ca_v1.1$ channel opening for WT and Cys mutants.** (A) The topology of the pore-forming α_{1S} subunit of skeletal $Ca_v1.1$ channels is shown: four concatenated homologous but nonidentical repeats (I–IV) form the α_{1S} subunit. Each repeat includes six transmembrane segments (S1–S6): S1–S4 make the VSD (colored cylinders), while S5 and S6 contribute to one quarter of the pore (gray cylinders). (B) A sequence alignment of the four S4 segments is based on the most recent structure of $Ca_v1.1$ channels (bold font corresponds to residues included in S4 helices; Protein Data Bank accession no. 6JP5; Zhao et al., 2019). Part of S3 and S4 loops are also reported to illustrate the location of the amino acids substituted into cysteines for fluorophore conjugation (pink, with a rhodamine molecule above them). Putative voltage-sensing, charged amino acids are in blue. (C) Mean voltage dependence of channel opening ($G(V)$) for WT and Cys mutants is shown ($n = 3–7$). $G(V)$ s for WT channels have been measured from oocytes with (pink circle) or without (black circles) fluorophore labeling. $G(V)$ s from Cys mutants are all from fluorophore-labeled channels. Note that fluorophore conjugation to the 13 endogenous extracellular cysteines (WT channels) did not modify channel activation. (D) Mean voltage dependence of gating charge ($Q(V)$) for WT and Cys mutants was calculated by integrating 10-ms gating current recordings. Lines in C and D are fits to single Boltzmann distributions (fitting parameters are reported in Tables 1 and 2, respectively). Note that Cys substitutions in the four VSDs did not perturb $Ca_v1.1$ voltage dependence of $G(V)$ and $Q(V)$.

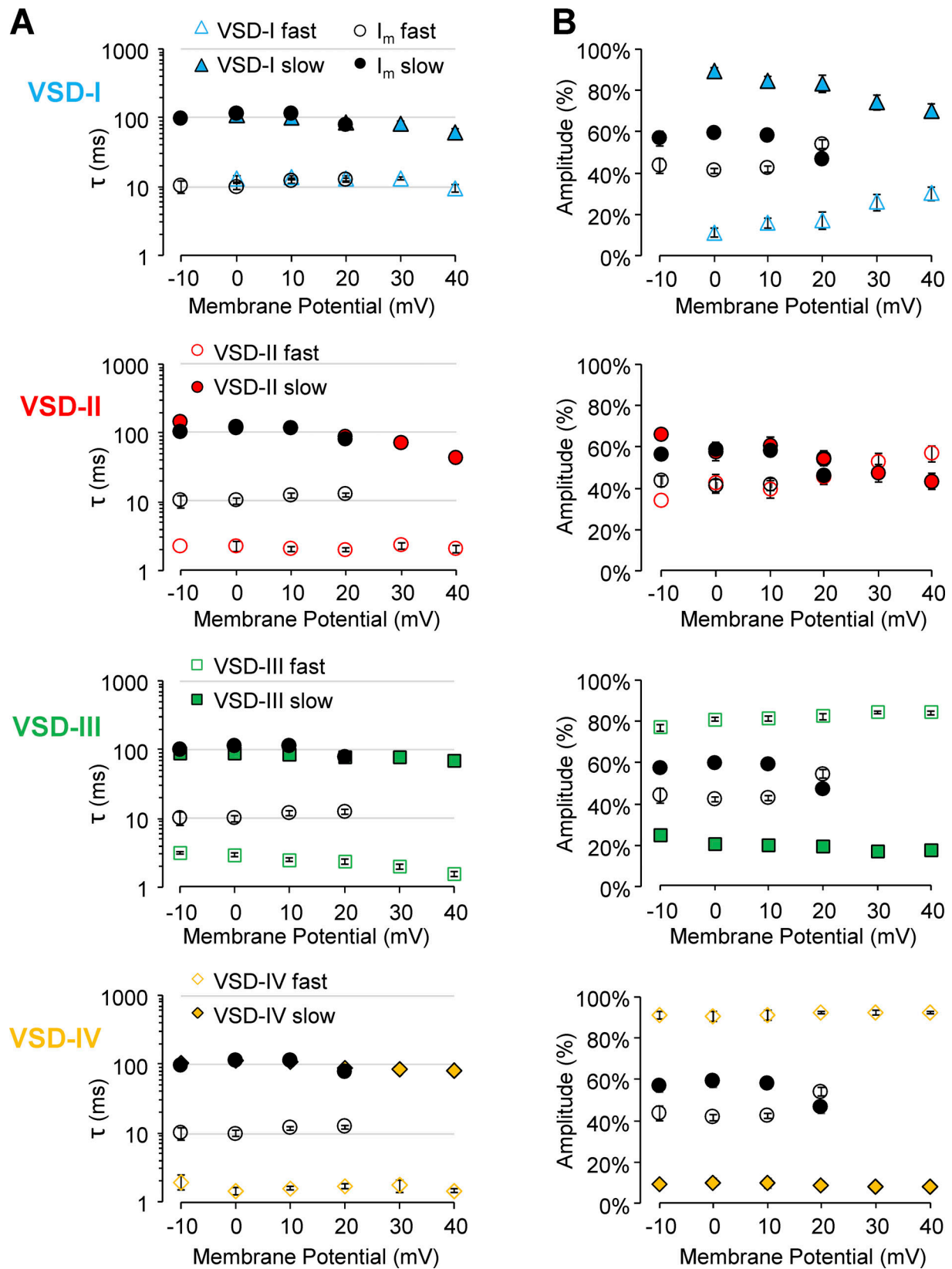


Figure S2. **VSD-I time course of activation follows ionic current kinetics.** (A and B) The activation kinetics of ionic current (black symbols) and of each VSD (colored symbols) were well described by the sum of two exponential functions (τ_{fast} , empty symbols; τ_{slow} , filled symbols). In the plots, fast and slow time constants (A) and their relative amplitudes (B) are compared for each individual VSD with those of the ionic current. Note that all domains share with the pore a kinetic component with $\tau_{slow} \sim 100$ ms. However, only VSD-I exhibits a fast component compatible with that of the ionic current; the other VSDs display a τ_{fast} approximately fivefold faster, likely more suitable for RYR1 activation.

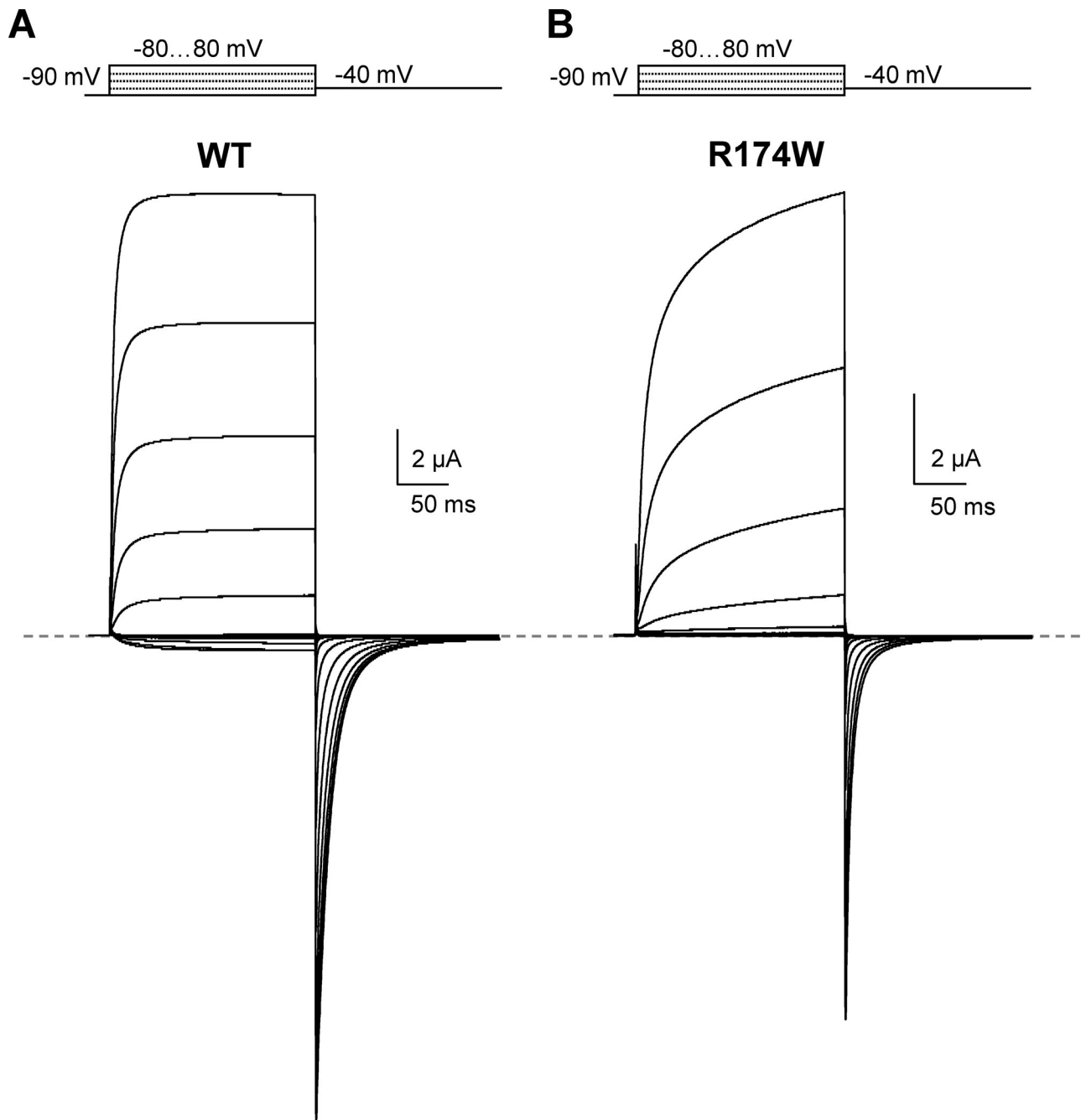


Figure S3. **The R174W mutation disfavors $\text{Ca}_v1.1$ channel activation.** (A and B) Ba^{2+} currents from *Xenopus* oocytes expressing human $\text{Ca}_v1.1$ WT (A) or R174W (B) channels are shown. Holding potential was -90 mV . Membrane potential steps are 10 mV apart.

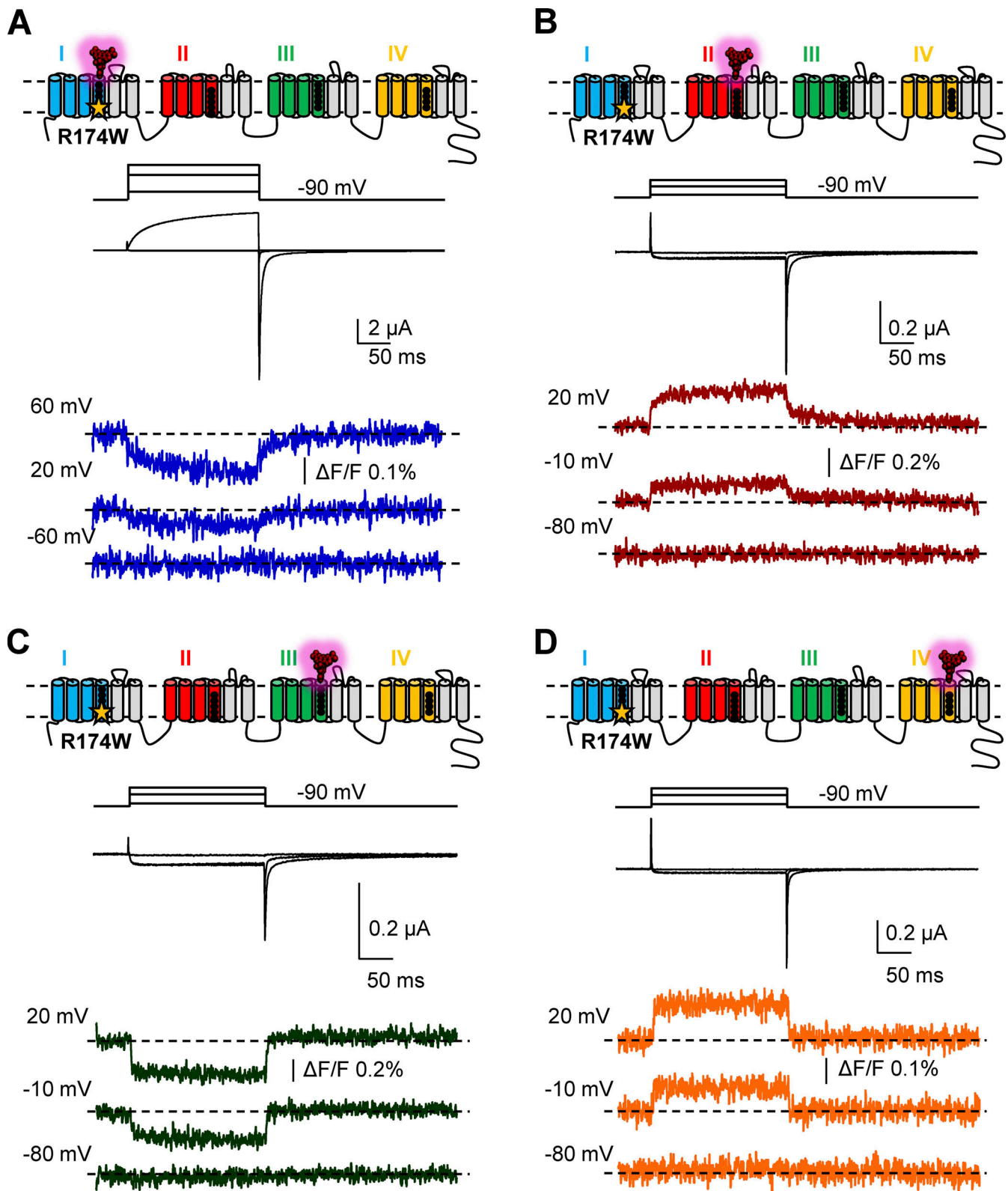


Figure S4. **Optically tracked voltage-dependent rearrangements of the individual VSD in human $Ca_v1.1$ R174W mutant.** (A–D) Simultaneously recorded Ba^{2+} currents (black) and fluorescence signals reporting local protein structural changes (colored traces) from human R174W $Ca_v1.1$ channels ($\alpha_{1S}+\beta_{1a}+Stac3$) expressed in *Xenopus* oocytes are shown. The topology above the recorded traces highlights the position of the R174W mutation (innermost gating charge of S4 in VSD-I; yellow star) and the location of the conjugated thiol-reactive fluorophore (pink rhodamine molecule). Note that, for VSD-I (A), larger depolarizations are needed to achieve voltage sensor activation as compared with WT VSD-I (Fig. S4 A versus Fig. 3 A, blue traces), since the neutralization of one of its gating charges (R174W) impaired its voltage-dependent activation (Fig. 5 B). Note that the current scale in A is 10-fold bigger than in B, C, and D.

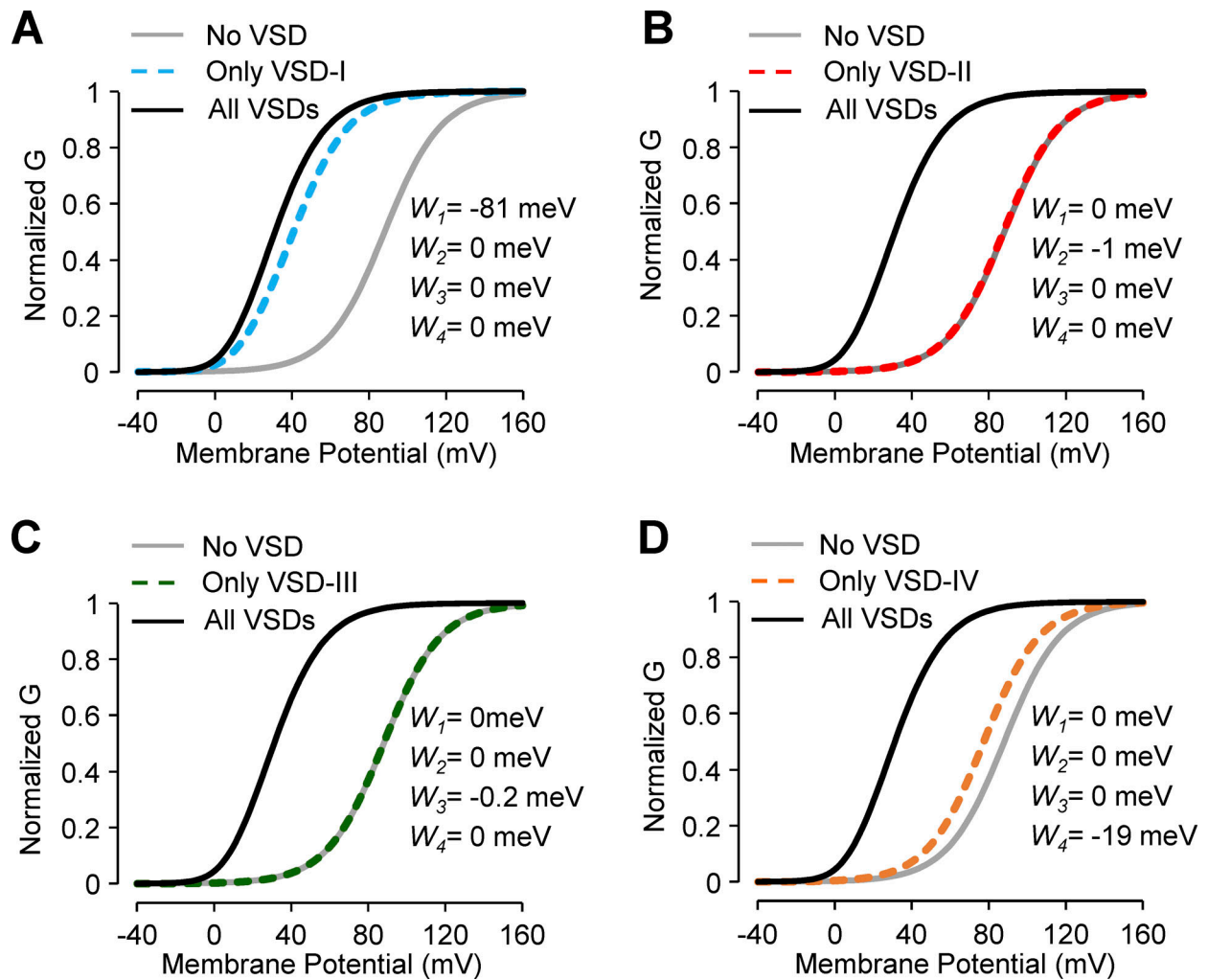


Figure S5. **Model prediction of each VSD contribution to pore opening.** The intrinsic voltage dependence of the pore is extremely rightward-shifted (no VSDs coupled; gray curves). The activation of each voltage sensor provides an energetic contribution to the stabilization of the open state of the channel, resulting in an overall facilitation of channel opening (leftward shift of the $G(V)$; dotted colored lines). Please note that VSD-I activation caused the largest leftward shift of the $G(V)$ (A; blue dotted line), with a smaller contribution of VSD-IV (D; orange dotted line) and negligible roles of VSD-II (B) and VSD-III (C).

Table S1 is provided online as a separate file. Table S1 shows fitting parameters and CIs for the allosteric model predictions.